

# MS\_DS-19 - Introduction to Deep Learning for Image Analysis and Computer Vision with Examples in Medical Applications



## Lecture 4 – Medical Imaging & Imaging IT

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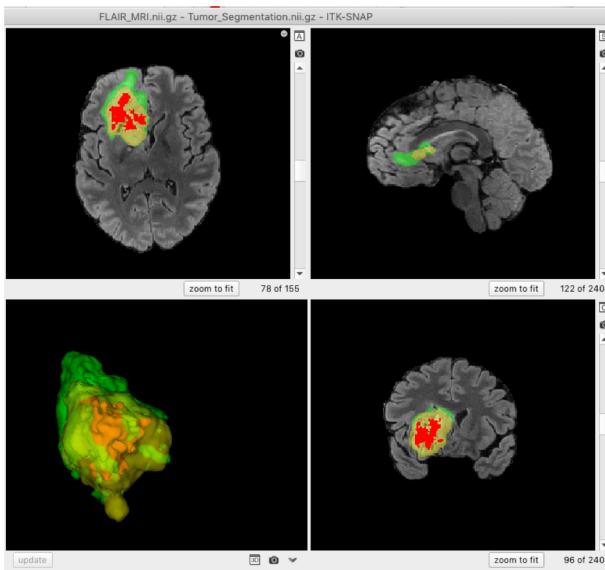
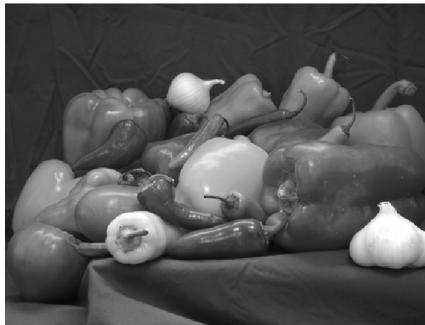
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# Recap last lecture

- Image Enhancement
- Filtering and Kernels
- Edge Detectors / Differential Operators
- Morphological Operators
- Segmentation



$$\begin{array}{c} \begin{array}{|c|c|} \hline 1 & 0 \\ \hline 0 & -1 \\ \hline \end{array} \quad \begin{array}{|c|c|} \hline 0 & 1 \\ \hline -1 & 0 \\ \hline \end{array} \end{array} \quad \begin{matrix} \Delta_x & & \Delta_y \end{matrix}$$

Roberts Cross

$$\begin{array}{c} \begin{array}{|c|c|c|} \hline 1 & 1 & 1 \\ \hline 0 & 0 & 0 \\ \hline -1 & -1 & -1 \\ \hline \end{array} \quad \begin{array}{|c|c|c|} \hline 1 & 0 & -1 \\ \hline 1 & 0 & -1 \\ \hline 1 & 0 & -1 \\ \hline \end{array} \end{array} \quad \begin{matrix} \Delta_x & & \Delta_y \end{matrix}$$

Prewitt

$$\begin{array}{c} \begin{array}{|c|c|c|} \hline 1 & 2 & 1 \\ \hline 0 & 0 & 0 \\ \hline -1 & -2 & -1 \\ \hline \end{array} \quad \begin{array}{|c|c|c|} \hline 1 & 0 & -1 \\ \hline 2 & 0 & -2 \\ \hline 1 & 0 & -1 \\ \hline \end{array} \end{array} \quad \begin{matrix} \Delta_x & & \Delta_y \end{matrix}$$

Sobel

+	+	+
+	⊕	+
+	+	+

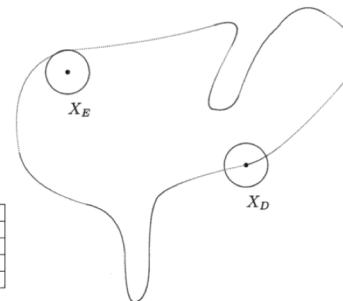
Elementraute

++	++	++
++	⊕	++
++	++	++

Rechteck-1

+	⊕	+
+	+	+
+	+	+

Rechteck-2



# Imaging IT

# Imaging IT - Typical General Purpose Raster Image Formats

- BMP
- JPEG
- TIFF
- PNG
- GIF
- ...

Made for 2D imaging data, max. bit depth and options for metadata varying by the format

# Imaging IT - Typical General Purpose Raster Image Formats

## *Typical* images properties

- BMP: 8 bit RGB ( $3 \times 8 = 24$  bit per pixel) *uncompressed*
- JPEG: 8 bit RGB ( $3 \times 8 = 24$  bit per pixel, with **lossy compression**)
- TIFF: 8 bit or 16 bit (!) RGB ( $3 \times 8$  or  $3 \times 16 = 48$  bit per pixel), *lossless* compression possible, meta data in header possible, multiple image versions per file possible
- PNG: often 8 bit RGBA , *lossless* compressed,  $4 \times 8 = 32$  bit per pixel
- GIF: 256 colors using 8 bit colormap (8 bit per pixel + colormap in header)

Some formats allow the use with other bit depths, for example BMP also possible as 1 bit black and white or adding alpha channel

# Imaging IT - Typical General Purpose Raster Image Formats

## **General Purpose Raster Image Formats are not well suited for medical imaging**

- Limited range (for example 8 bit as uint8 i.e. 0..255
  - For example problems to encode a CT using Hounsfield units ranging from -1024 to 3072?
- Made for 2D data
  - Medical often 3D or even higher dimensional!
- No encoding of geometry
  - E.g. patient position in scanner; coordinate system of the image;
  - What is the “size” of a voxel in mm?
  - How do deal with anisotropic voxels eg 0.5mmx0x5mmx2mm?
- Encoding of metadata (patient name, sex, ...) difficult

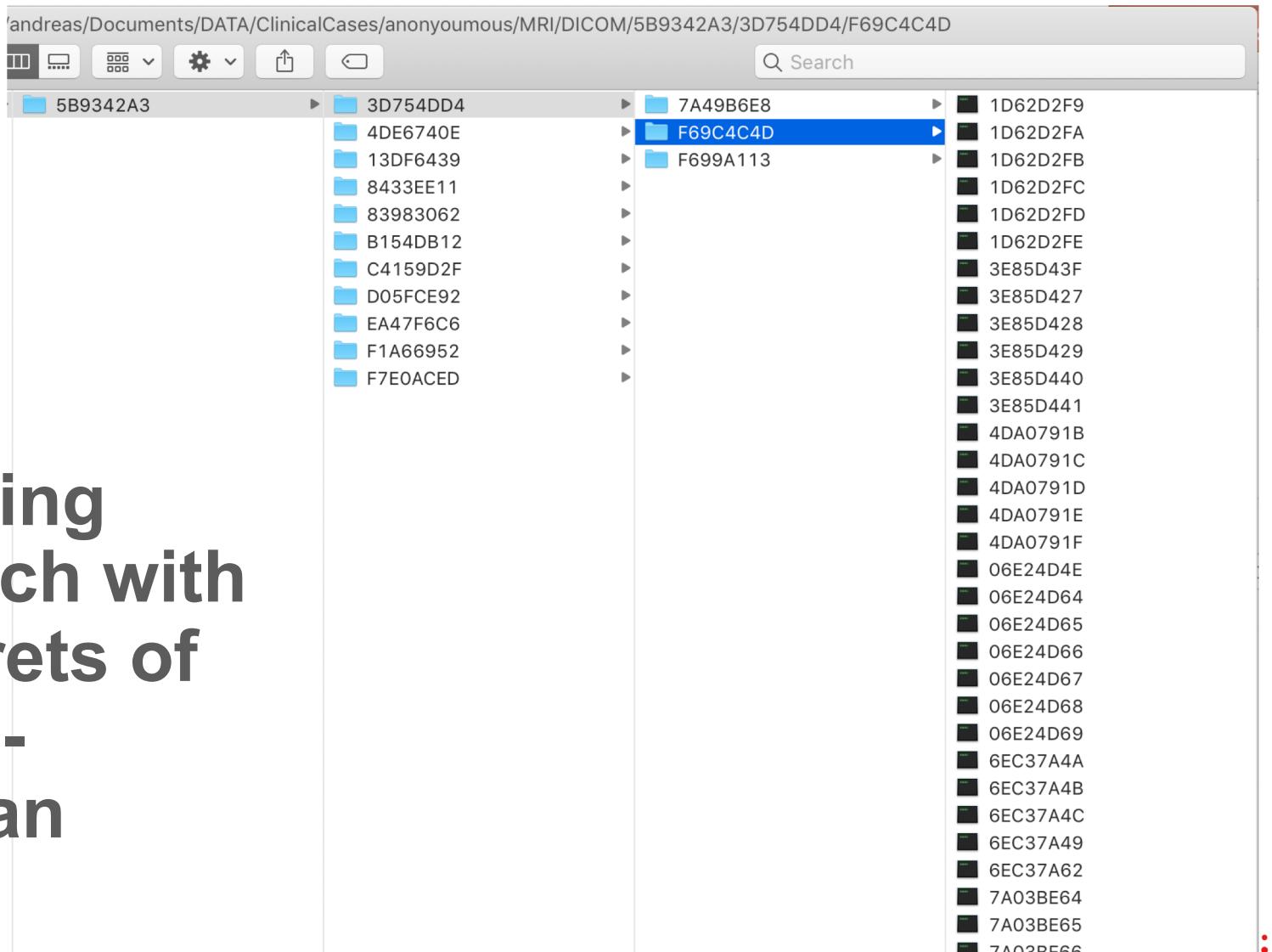
# Imaging IT – Special Formats for Medicine

## In **Clinical application: DICOM (.dcm)**

- **Extremely flexible format!**
- “Everybody” can define own “tags” and add specific metainformation to the -> enables product innovations! (e.g. a new scanner type that can encode things not known at the time the DICOM standard was defined)
- 3D imaging normally stored as “series” of 2D images, joined via header information (SeriesID tag)
- **Extremely annoying format for research with potentially hundreds of files for one high-resolution 3D scan**

# Imaging IT – Special Formats for Medicine

- **DICOM**  
**Extremely annoying  
format for research with  
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# Imaging IT – Special Formats for Medicine

## In *Research* : NiFTI (.nii / .nii.gz)

- “One file per scan”
- Able to store *high dimensional data* (3D, 4D, ...) in **one** file
  - More data processing (array) thinking
- Stores up to two transformation matrices in the header to encode image geometry (“Voxel2World”)
  - An Affine Matrix (homogenous coordinates)
  - A unit quaternion representation
- Does not store metadata – ensures a lot of data protection by design (can’t accidentally forget to remove the patient name)

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# Imaging IT – Special Formats for Medicine

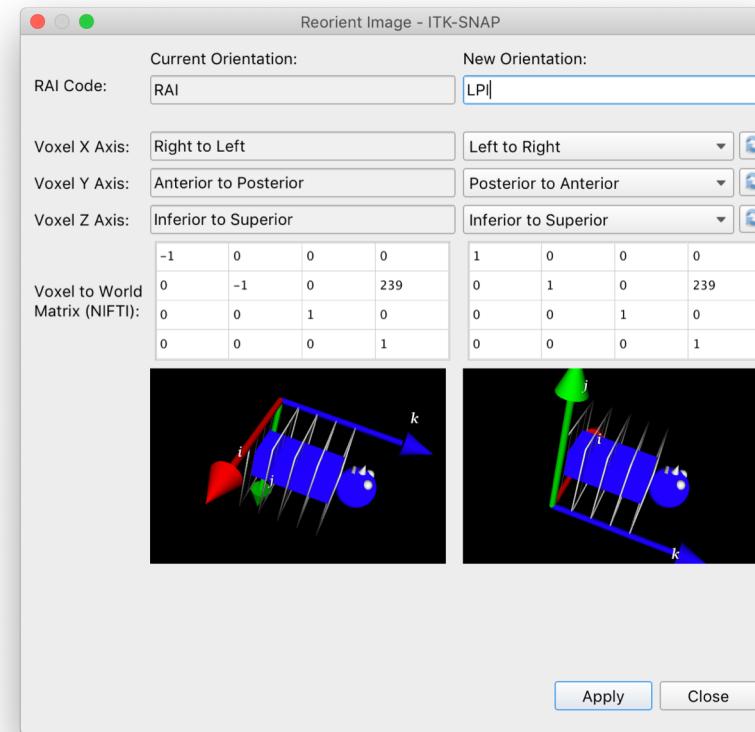
## In Research: NiFTI (.nii / .nii.gz)

```
/*
 * NiFTI-2 usage          /* NiFTI-1 usage      /* offset */
 ****
 int sizeof_hdr;           /*!< MUST be 540          /* int sizeof_hdr; (348) /* 0 */
 char magic[8];            /*!< MUST be valid signature. /* char magic[4]; /* 4 */
 int16_t datatype;         /*!< Defines data type! /* short datatype; /* 12 */
 int16_t bitpix;           /*!< Number bits/voxel. /* short bitpix; /* 14 */
 int64_t dim[8];           /*!< Data array dimensions. /* short dim[8]; /* 16 */
 double intent_p1;         /*!< 1st intent parameter. /* float intent_p1; /* 80 */
 double intent_p2;         /*!< 2nd intent parameter. /* float intent_p2; /* 88 */
 double intent_p3;         /*!< 3rd intent parameter. /* float intent_p3; /* 96 */
 double pixdim[8];          /*!< Grid spacings. /* float pixdim[8]; /* 104 */
 int64_t vox_offset;        /*!< Offset into .nii file /* float vox_offset; /* 168 */
 double scl_slope;          /*!< Data scaling: slope. /* float scl_slope; /* 176 */
 double scl_inter;          /*!< Data scaling: offset. /* float scl_inter; /* 184 */
 double cal_max;            /*!< Max display intensity /* float cal_max; /* 192 */
 double cal_min;            /*!< Min display intensity /* float cal_min; /* 200 */
 double slice_duration;    /*!< Time for 1 slice. /* float slice_duration; /* 208 */
 double toffset;             /*!< Time axis shift. /* float toffset; /* 216 */
 int64_t slice_start;       /*!< First slice index. /* short slice_start; /* 224 */
 int64_t slice_end;          /*!< Last slice index. /* short slice_end; /* 232 */
 char descrip[80];          /*!< any text you like. /* char descrip[80]; /* 240 */
 char aux_file[24];         /*!< auxiliary filename. /* char aux_file[24]; /* 320 */
 int qform_code;            /*!< NiFTI_XFORM_* code. /* short qform_code; /* 344 */
 int sform_code;            /*!< NiFTI_XFORM_* code. /* short sform_code; /* 348 */
 double quatern_b;          /*!< Quaternion b param. /* float quatern_b; /* 352 */
 double quatern_c;          /*!< Quaternion c param. /* float quatern_c; /* 360 */
 double quatern_d;          /*!< Quaternion d param. /* float quatern_d; /* 368 */
 double qoffset_x;           /*!< Quaternion x shift. /* float qoffset_x; /* 376 */
 double qoffset_y;           /*!< Quaternion y shift. /* float qoffset_y; /* 384 */
 double qoffset_z;           /*!< Quaternion z shift. /* float qoffset_z; /* 392 */
 double srow_x[4];           /*!< 1st row affine transform. /* float srow_x[4]; /* 400 */
 double srow_y[4];           /*!< 2nd row affine transform. /* float srow_y[4]; /* 432 */
 double srow_z[4];           /*!< 3rd row affine transform. /* float srow_z[4]; /* 464 */
 int slice_code;             /*!< Slice timing order. /* char slice_code; /* 496 */
 int xyz_units;              /*!< Units of pixdim[1..4] /* char xyz_units; /* 500 */
 int intent_code;            /*!< NiFTI_INTENT_* code. /* short intent_code; /* 504 */
 char intent_name[16];        /*!< 'name' or meaning of data. /* char intent_name[16]; /* 508 */
 char dim_info;              /*!< MRI slice ordering. /* char dim_info; /* 524 */
 char unused_str[15];        /*!< unused, filled with \0 */ /* 525 */
}
**** 540 bytes total ****
typedef struct nifti_2_header nifti_2_header;
```

# Imaging IT – Image Orientation

There are **24 different** ways to order the image information in a 3D image.

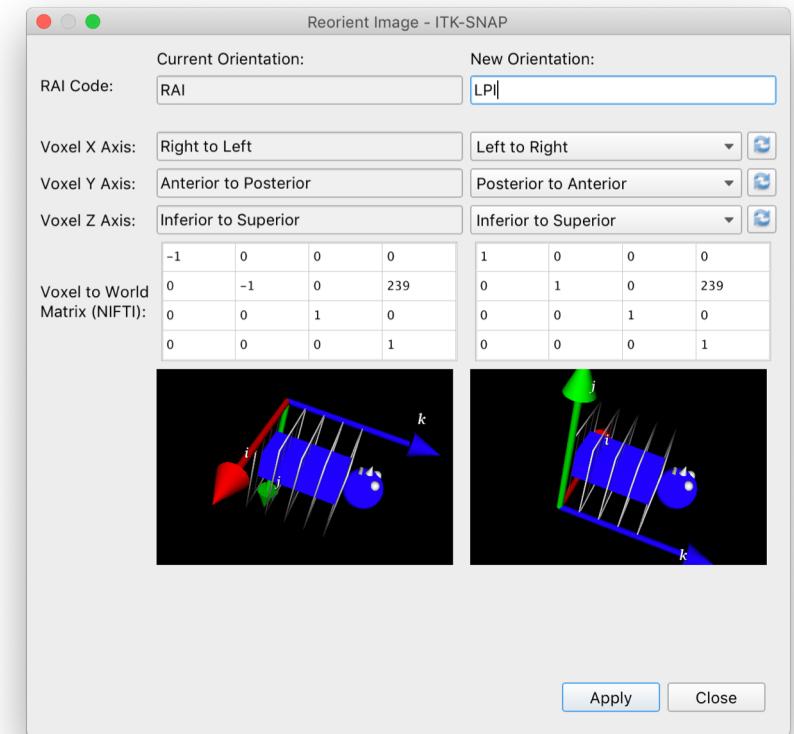
- Unfortunately most of them have been used somewhere ;-)
- Often encoded using three letter code over the sets {R,L}, {I,S}, {A,P}



# Imaging IT – Image Orientation

Most common:

- LPI, RAS and RAI
- Still not well defined as some people refer to “LPI” as
  - From L -> R, from P->A, from I -> S
  - but others as
    - From R ->L, from A->P, from S -> I
- We will use a - to indicate the first form and + to indicate the second, i.e. LPI-.



# Imaging IT – Image Orientation

## Woxel2World Matrix

- Many libraries to load nifti data *apply* the voxel2world matrix stored in the nifty header *at loading time* to get a well defined image in mm scale.
- Ideally you then always get a defined orientation in your software, regardless how the data was stored in the file, often *LPI*-
- Unfortunately the matrix might be wrong 😊
- Orientation mishaps might **not** be easily noticed. Why?

