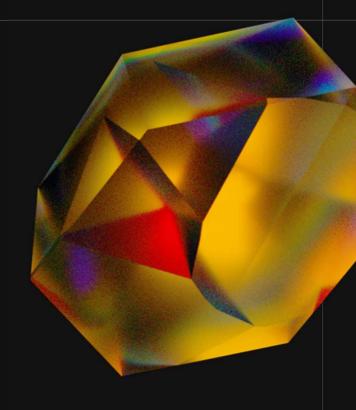
# Closed-loop optimization of hydrogel formulations using dynamic light scattering



**Acceleration Consortium Team:** 

Owen Melville, Ilya Yakavets, Yimu Zhao, Nipun Gupta, Jeff Watchorn



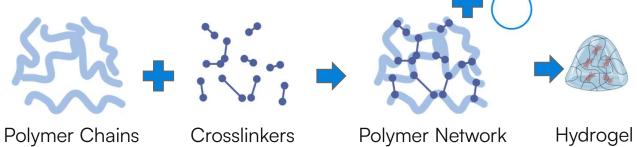


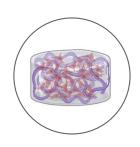


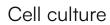


# **Hydrogels are Awesome!**











3D Printing



Drug Delivery

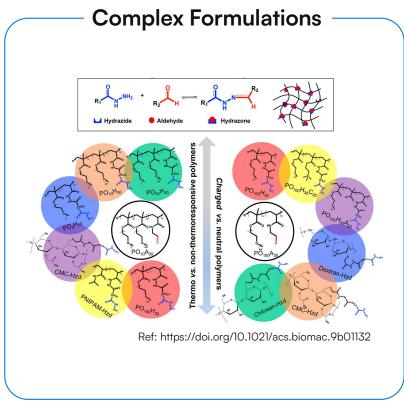




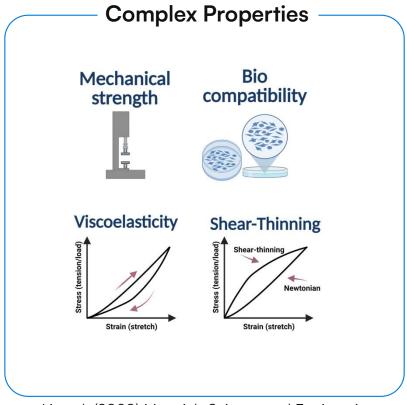




# **Hydrogels are Complicated!**



Xu et al. (2020). Biomacromolecules



Li et al. (2020) Materials Science and Engineering











# **Measuring Hydrogel Properties**

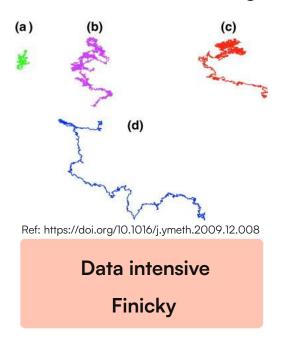
# Rheology



Slow

Difficult to Automate

## **Video Particle Tracking**



Mao et al. (2022). Front. Bioeng. Biotechnol.

# **Dynamic Light Scattering**



Well plate compatible

Fast measurements

Krajina et al. (2017). ACS Central Science





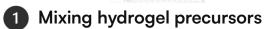






# A Hydrogel Self-Driving Lab!







2 Crosslinking





3 Dynamic Light Scattering characterization



#### Inputs:

- 1. Precursor descriptors (substance)
- 2. Precursor concentrations (discrete)







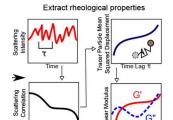
- 2. Gelation time
- 3. Viscosity
- 4. Viscoelasticity (G' and G")

#### **BO** Features:

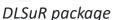
- Precursor representation (mixture constraints)
- > Sequence optimization















BayBE package

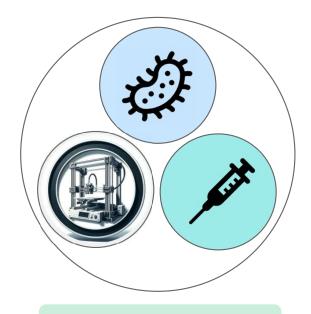








# The Future Needs Hydrogels!



Cell culture

3D Printing

Drug Delivery



Faster Data

Reliable Data

Self-Driving Labs



Healthy People

Happy Robots

Healthy Planet

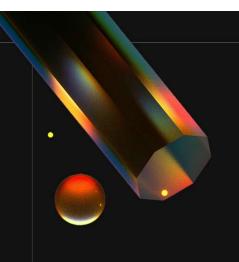


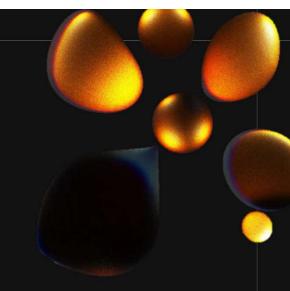














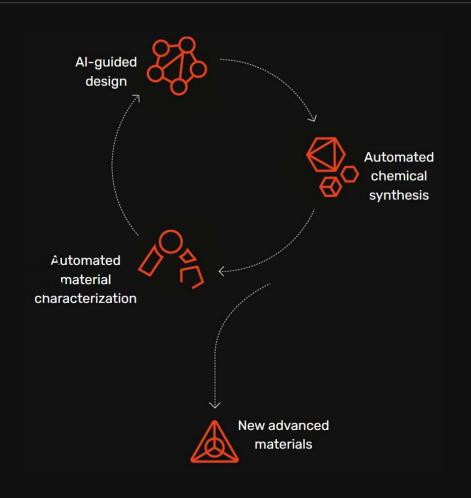








# SELF-DRIVING LABS ACCELERATING MATERIALS DISCOVERY



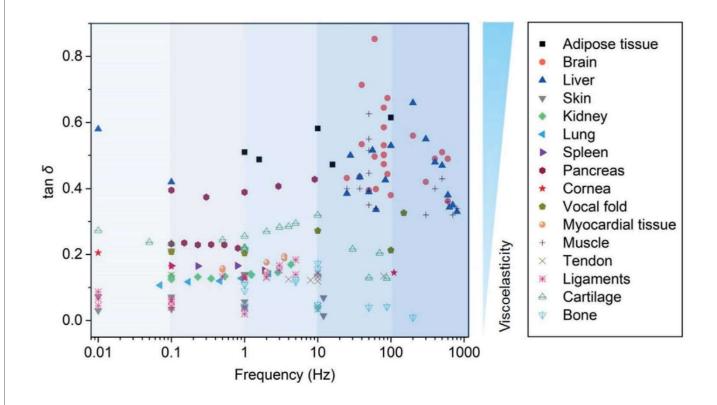








# Various biological tissues show frequency-dependent viscoelastic features











#### Theory (Cai et al, 2021)

Incident light is scattered by embedded probe particles in a sample volume, and the scattering intensity is measured over time to derive the intensity autocorrelation function  $g_2(\tau) = \langle I(t)I(t+\tau)\rangle\langle I(t)\rangle^{-2}$ , where  $\tau$  is the lag time between two time points and  $\langle I(t)\rangle^{-2}$  is the normalization factor. This autocorrelation function relates to the mean-squared displacement  $\Delta r^2$  ( $\tau$ ) of the probe particles through the intermediate scattering function

$$g_1(\tau) = \exp\left(\frac{-q^2 \Delta r^2(\tau)}{6}\right),\tag{1}$$

where the scattering vector  $q = 4\pi n \sin(\theta/2)/\lambda$ . The intermediate scattering function  $g_1(\tau)$  for ergodic systems is derived from

$$g_2(\tau) = 1 + (g_0 - 1) |g_1(\tau)|^2,$$
 (2)

where  $g_0 = g_2(0)$ . From the mean-squared displacement, we then obtain the frequency-dependent complex modulus using the generalized Stokes-Einstein equation<sup>21,22</sup>

$$G^*(\omega) = \frac{k_B T}{\pi a(i\omega) \mathcal{F}_u \{\langle \Delta r^2(t) \rangle\}}$$
(3)

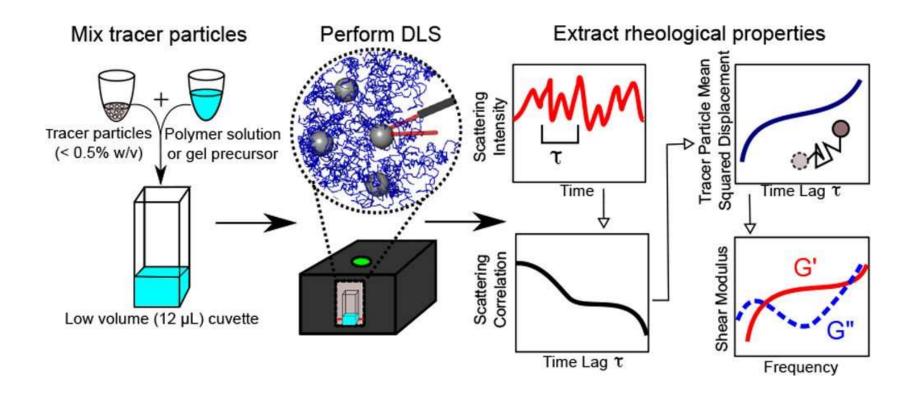
where  $k_BT$  denotes the thermal energy, a is the particle radius, and  $\mathcal{F}_u\{\langle \Delta r^2(r) \rangle\}$  is the unilateral Fourier transform of the mean-squared displacement. This relation is extended from the purely viscous regime to continuum viscoelastic fluids and connects macroscopic stress relaxations to microscopic stress relaxations.<sup>23,35</sup> Besides the complex modulus, another interesting and valuable interpretation of the mean-squared displacement is the creep compliance, which directly relates to the mean-squared displacement.<sup>36</sup> It should be noted that Equation 3 assumes that there is negligible impact from inertia of the probe, which is very sensitive to probe size and material properties of both the probe and the fluid. For a particle in a fluid, the timescale at which inertial effects are non-negligible can be estimated using the ratio of  $m/\zeta = 2\rho_p a^2/9 \eta_s$ , where m is the mass of the particle,  $\zeta$  is the drag coefficient,  $\rho_p$  is the density of the particle, a is the radius of the particle, and a is the viscosity of the fluid.<sup>37</sup> Particle sizes used in DLS $\mu$ R are on the order of 1  $\mu$ m, which requires a timescale of a 6 × 10<sup>-8</sup> s for the inertia to dampen out in a material with a viscosity of 10<sup>-3</sup> Pa·s. Thus, for the frequency range probed by DLS $\mu$ R (up to 10<sup>6</sup> Hz), inertial effects can be neglected.<sup>22</sup>











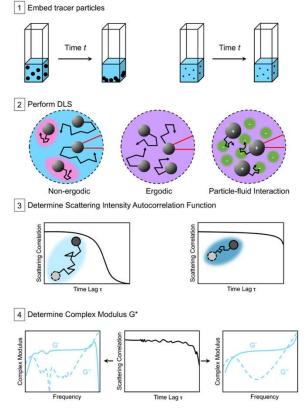


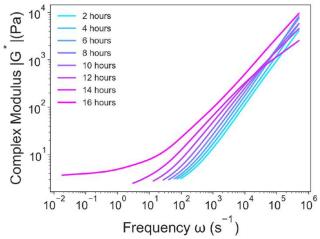




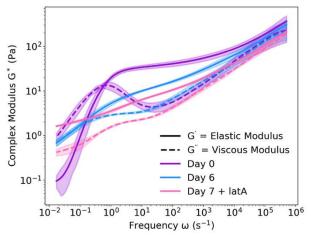


## DLSµ R Workflow Scenarios Summary. (Cai et al, 2021)





Gelation Process of a Covalently Crosslinked PEGbased Gel.



Multi-day Rheology of a Living Composite of Human Breast Cancer Cells Encapsulated in Collagen I.

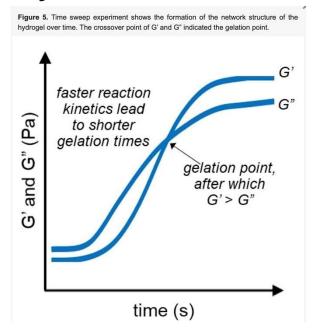


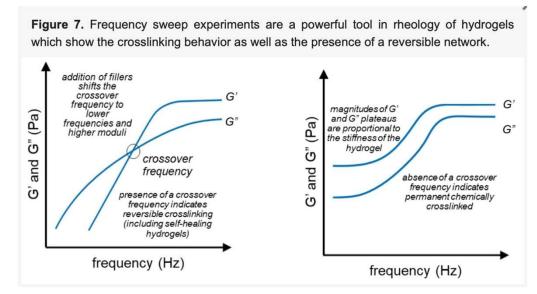






# Relationship between Structure and Rheology of Hydrogels for Various Applications Stojkov et al, 2021





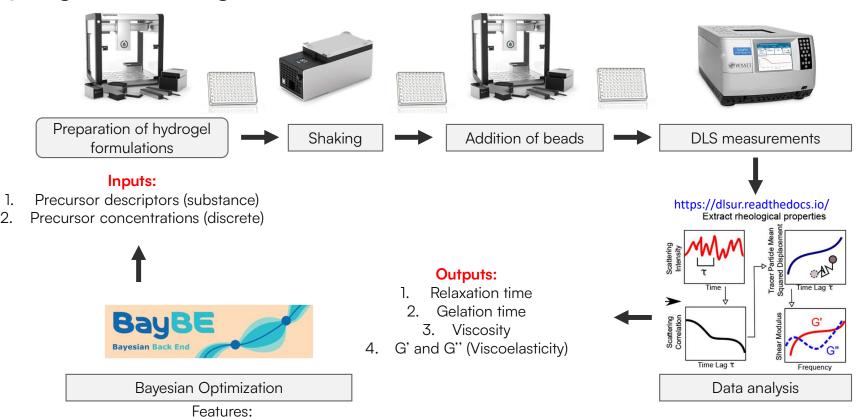








# A Hydrogel Self-Driving Lab!







Precursor representation (mixture constraints)
- Sequence optimization





