

Bayesian Dictionary Learning for EEG Source Identification

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Here is the abstract

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Rapportens indhold er frit tilgængeligt, men offentliggørelse (med kildeangivelse) må kun ske efter aftale med forfatterne.

Preface

Here is the preface. You should put your signatures at the end of the preface.

Aalborg University, December 10, 2019

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Danish Summary

Dansk resume ?

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Introduction

Introduktion til hele projektet, skal kunne læses som en appetitvækker til resten af rapporten, det vi skriver her skal så uddybes senere. Brug dog stadigvæk kilder.

- kort intro a EEG og den brede anvendelse, anvendelse indenfor høreapparat.
- intro af model, problem med overbestemt system
- Seneste forslag til at løse dette
- vi vil efterviser dette og udvide til realtime tracking
- opbygningen af rapporten

Chapter 1

Motivation

This chapter examines existing literature concerning source localization from EEG measurements. At first a motivation for the source localization problem is given, considering the application within the hearing aid industry. Further, the state of the art methods are presented followed by a description of the contribution proposed in this thesis.

Localization or recovering?

1.1 EEG Measurements

Electroencephalography (EEG) is a technique used within the medical field. It is an imaging technique measuring electric signals on the scalp, caused by brain activity. The human brain consist of an enormous amounts of cells, called neurons. These neurons are mutually connected in neural nets and when a neuron is activated, for instance by a physical stimuli, local current flows are produced [21]. This is what makes a kind of neural interaction across different parts of the brain.

(?)

EEG measurements are provided by a varies number of metal electrodes, referred to as sensors, carefully placed on a human scalp. Each sensor read the present electrical signals, which are then displayed on a computer, as a sum of sinusoidal waves relative to time.

It takes a large amount of active neurons to generate an electrical signal that is recordable on the scalp as the current have to penetrate the skull, skin and several other thin layers. Hence it is clear that the EEG measurements from a single sensor do not correspond to the activity of a single specific neuron in the brain, but rather a collection of many activities within the range of the one sensor. Nor is the range of a single sensor separated from the other sensors thus the same activity can easily be measured by two or more sensors. Furthermore, interfering signals can occur in the measurments resulting from physical movement of e.g. eyes and jawbone [21]. Lastly, the transmission of the electric field through the biological tissue to the sensor

has an unknown mixing effect on the signal, this process is called volume conduction [18, p. 68] [19].

This clarifies the mixture of electrical signals with noise that form the EEG measurements. The concept is sought illustrated on figure 1.1.

It will be clear later that it is of highly interest to separate and localize the sources of the neural activities measured on the scalp. Note that a source do not correspond to a single neuron but is typically a collection of synchronized/phase locked active neurons which are generating a constructive interference resulting in a measurable signal on the scalp.

The waves resulting from EEG measurements have been classified into four groups according to the dominant frequency. The delta wave (0.5 – 4 Hz) is observed from infants and sleeping adults, the theta wave (4 – 8 Hz) is observed from children and sleeping adults, the alpha wave (8 – 13 Hz) is the most extensively studied brain rhythm, which is induced by an adult laying down with closed eyes. Lastly, the beta wave (13 – 30 Hz) is considered the normal brain rhythm for adults, associated with active thinking, active attention or solving concrete problems [18, p. 11]. An example of EEG measurements within the four categories is illustrated by figure 1.2.

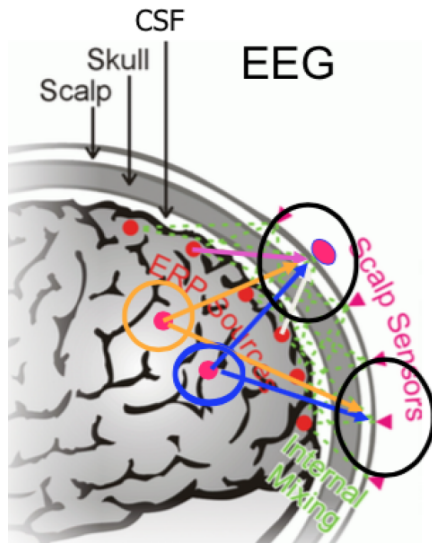


Figure 1.1: Illustration of volume conduction, source: [5](we will make our own figure here instead)

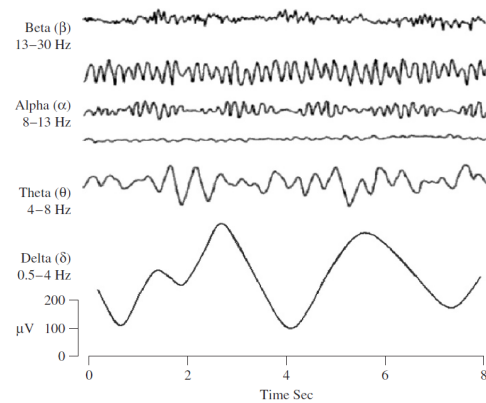


Figure 1.2: Example of time dependent EEG measurements within the four defined categories, source: [18]

EEG is widely used within the medical field, especially research of the cognitive processes in the brain. Diagnosis and management of neurological disorders such as epilepsy is one example.

EEG capitalize on the procedure being non-invasive and fast. Neural activity can be measured within fractions of a second after a stimuli has been provided [21, p. 3]. When a person is exposed to a certain stimuli, e.g. visual or audible, the measured activity is said to result from evoked potential.

Over the past two decades, especially functional integration has become an area of interest [11]. Within neurobiology functional integration refers to the study of the correlation among activities in different regions of the brain. In other words, how do different part of the brain work together to process information and conduct a response [12]. For this purpose separation and localization of the single sources which contribute to the EEG measurement is of interest. An article from 2016 point out the importance of performing analysis regarding functional integration at source level rather than at EEG level. It is argued through experiments that analysis at EEG level do not allow interpretations about the interaction between sources [19].

The hearing aid industry is one example where this research is highly prioritized. At Eriksholm research center which is a part of the hearing aid manufacture Oticon cognitive hearing science is a research area within fast development [20]. One main purpose of Eriksholm is to make it possible for a hearing aid to identify the attended sound source and hereby exclude noise from elsewhere [2] [6]. This is where EEG and occasionally so called in-ear EEG is interesting, especially in conjunction with the technology of beamforming, which allows for receiving only signals from a specific direction. It is essentially the well known but unsolved cocktail problem which is sought improved by use of EEG. However, the focus of this research do consider the correlation between EEG measurements and the sound source rather than localization of the activated source from the EEG [2]. Hence a source localization approach could potentially be of interest regarding hearing aids in order to improve the results. (Furthermore, a real-time application to provide feedback from EEG measurements would be essential.).

?

1.1.1 Modelling

Considering the issue of localizing activated sources from EEG measurements, a known option is to model the observed data by the following linear system

$$\mathbf{Y} = \mathbf{A}\mathbf{X},$$

where $\mathbf{Y} \in \mathbb{R}^{M \times N_d}$ is the EEG measurements from M sensors at N_d data points, $\mathbf{A} \in \mathbb{R}^{M \times N}$ is an unknown mixing matrix and $\mathbf{X} \in \mathbb{R}^{N \times N_d}$ is the actual activation of sources within the brain. The i -th column of \mathbf{A} represent the relative projection weights from the i -th source to every sensor [5]. This is in general referred to as a multiple measurement vector model. The aim in this case is to identify both \mathbf{A} and \mathbf{X} given the measurements \mathbf{Y} . For this specific set up the model is referred to as the EEG inverse problem.

Tjek lige denne sætning

To solve the EEG inverse problem the concept of compressive sensing makes a solid foundation including sparse signal recovery and dictionary learning. Independent Component Analysis (ICA) is a common applied method to solve the inverse problem [15], [14], here statistical independence between source activity is assumed. Application of ICA have shown great results regarding source separation of high-density EEG. Furthermore, an enhanced signal-to-noise ratio of the unmixed independent source time series processes allow essential study of the behaviour and relationships between multiple EEG source processes [8].

However a significant flaw to this method is that the EEG measurements are only separated into a number of sources that are equal or less than the number of sensors [3].

This means that the EEG inverse problem can not be over-complete. That is an assumption which undermines the reliability and usability of ICA, as the number of simultaneous active sources easily exceed the number of sensors [5]. This is especially a drawback when low-density EEG are considered, that is EEG equipment with less than 32 sensors. Improved capabilities of low-density EEG devices are desirable due to its relative low cost, mobility and ease to use.

This makes a foundation to look at the existing work considering the over-complete inverse EEG problem.

1.2 Related Work and Our Contribution

As mentioned above ICA has been a solid method for source localization in the case where a separation into a number of sources equal to the number of sensors was adequate. To overcome this issue an extension of ICA was suggested, referred to as the ICA mixture model [3]. Instead of identifying one mixing matrix $\mathbf{A} \in \mathbb{R}^{M \times N}$ this approach learns N_{model} different mixing matrices $\mathbf{A}_i \in \mathbb{R}^{M \times M}$. The method was further adapted into the Adaptive Mixture ICA (AMICA) which showed successful results regarding identification of more sources than available sensors [17]. However an assumption of no more than M simultaneously active sources has to be made which is still an essential limitation, especially when considering low-density EEG. Other types of over-complete ICA algorithms have been proposed to overcome the problem of learning over-complete systems. One is the Restricted ICA (RICA), an efficient method used for unsupervised learning in neural networks [22]. Here the hard orthonormal constraint in ICA is replaced with a soft reconstruction cost.

In 2015 O. Balkan et. al., [3], suggested a new approach also targeting the identification of more sources than sensors regarding EEG. The suggested method, referred to as Cov-DL, is a covariance based dictionary learning algorithm. The point is to transfer the forward problem into the covariance domain, which has higher dimen-

(er det correct i forhold til teorien om ICA?)

(number of sources? or datapoints)

(?)

sionality than the original EEG sensor domain. This can be done when assuming the scalp mixing is linear and using the assumed natural non-correlation of sources within a certain time-window. The Cov-DL algorithm stands out from the other straight forward dictionary learning methods as it does not relay on the sparsity of active sources, this is an essential advantage when low-density EEG is considered. Cov-DL was tested on found to outperform both AMICA and RICA [3], thus it is considered the state of the art within the area of source identification.

It is essential to note that the Cov-DL algorithm do only learn the mixing matrix \mathbf{A} , the projection of sources to the scalp sensors, and not the explicit source activity time series \mathbf{X} .

For this purpose a multiple measurement sparse bayesian learning (M-SBL) algorithm was proposed in [4] also by O. Balkan et. al., also targeting the case of more active sources than sensors [4]. Here the mixing matrix which is known should fulfil the exact support recovery conditions. Though, the method was proven to outperform the recently used algorithm M-CoSaMP even when the defined recovery conditions was not fulfilled.

Find ud af hvad forkortelsen står for

The two state of the art methods for source identification makes the foundation of this thesis. This thesis propose an algorithm with the purpose of solving the EEG inverse problem using the presented methods on EEG measurement. To extent the existing results the algorithm is expanded into a real-time application, in order to provide feedback based on the source activity.

The intention of the feedback is to adjust the direction of the beam within the hearing aid depending on the source activity. For this, the application is tested within a simulation environment where the receiving direction of the test person can be adjusted in real-time. The quality of the final results is measured by the capability of improving the listener experience and the time used to proved useful feedback.

As such our contribution (*hopefully*) consists of tests of existing methods on new real-time measurement and furthermore include a feedback to control the microphone beam on a hearing aid.

note: Evt. kunne vi lave en figur der lidt ala mindmap sætte et system overblik op og så highlighte de "bokse" vi vælger at arbejde med.

Chapter 2

Problem Statement

From the motivation and related work described in chapter 1 it is stated that EEG measurement of the brain activity has great potential to contribute within the hearing aid industry, regarding the development of hearing aids with improved performance in situations as the cocktail party problem. By solving the over-complete EEG inverse problem, in order to localize the sources of the brain activity, the results could be used to guide and adapt the hearing aids performance such as move the microphone beam in the direction of interest. This lead to the following problem statement.

How can sources of activation within the brain be localized from the EEG inverse problem, in the over-complete case of less sensors than sources and how can such algorithm be extended to a real-time application providing feedback to improve the intentional listening experience?

From the problem statement some clarifying sub-questions have been made.

- How can the over-complete EEG inverse problem be solved by use of compressive sensing included domain transformation?
- How can Cov-DL be used to estimate the mixing matrix \mathbf{A} from the over-complete EEG inverse problem?
- How can M-SBL be used to estimate the source matrix \mathbf{X} from the over-complete EEG inverse problem?
- How can an application be formed to constitute this source identification process operating in real-time?
- How can the feedback of the system be used to control the microphone beam of a simulated hearing aid. Especially how to analyse the feedback versus the listening experience in order to improve this.

Chapter 3

Sparse Signal Recovery

This chapter gives an introduction to the sparse signal recovery. Associated theory regarding compressive sensing is described along the common solution approaches and their limitations.

3.1 Linear Algebra

Some measurement vector \mathbf{y} can be described as a linear combinations of a coefficient matrix \mathbf{A} and some vector \mathbf{x} such that

$$\mathbf{y} = \mathbf{A}\mathbf{x}, \quad (3.1)$$

where $\mathbf{y} \in \mathbb{R}^M$ is the observed measurement vector consisting of M measurements, $\mathbf{x} \in \mathbb{R}^N$ is an unknown vector of N elements, and $\mathbf{A} \in \mathbb{R}^{M \times N}$ is a coefficient matrix which models the linear measurement process column-wise. The linear model makes a system of linear equations with M equations and N unknowns.

In the case of \mathbf{A} being a square matrix, $M = N$, a solution can be found to the linear model if \mathbf{A} has full rank – \mathbf{A} consist of linearly independent columns or rows. A linear systems with $M = N$ is called determined, $M > N$ over-determined and $M < N$ under-determined. When full rank do not occur the matrix is then called rank-deficient.

By inverting \mathbf{A} from (3.1) the unknown vector \mathbf{x} can be achieved. Square matrix is invertible if and only if it has full rank or its determinant $\det(\mathbf{A}) \neq 0$. For rectangular matrices, $M > N$ and $M < N$, left-sided and right-sided inverse exists.

For an determined system there will exist a unique solution. For an over-determined system there do not exist a solution and for under-determined systems there exist infinitely many solutions [7, p. ix].

As described in chapter 1 the linear model of interest consist of M sensors which makes the observed measurements \mathbf{y} and N sources which makes the unknown vector \mathbf{x} . Here it is of interest to find a solution to the case where the system consist of more sources than sensors – hence a solution has to be found within the infinitely solution set.

3.2 Compressive Sensing

Compressive sensing is the theory of efficient recovery or reconstruction of a signal from a minimal number of observed measurements. It is build upon empirical observations assuring that many signals can be approximated by remarkably sparser signals. Assume linear acquisition of the original measurements, then the relation between the measurements and the signal to be recovered can be described by the linear model (3.1) [10].

In compressive sensing terminology, $\mathbf{x} \in \mathbb{R}^N$ is the signal of interest which is sought recovered from the measurements $\mathbf{y} \in \mathbb{R}^M$ by solving the linear system (3.1). The coefficient matrix \mathbf{A} is in the context of compressive sensing referred to as the mixing matrix or the dictionary matrix.

In the typical compressive sensing case the system is under-determined, $M < N$, and there exist infinitely many solutions, provided that a solution exist.

However, by enforcing certain sparsity constraints it is possible to recover the wanted signal, hence the term sparse signal recovery [10].

3.2.1 Sparseness

A signal is said to be k -sparse if the signal has at most k non-zero coefficients. For the purpose of counting the non-zero entries of a vector representing a signal the ℓ_0 -norm is defined

$$\|\mathbf{x}\|_0 := \text{card}(\text{supp}(\mathbf{x})).$$

The function $\text{card}(\cdot)$ gives the cardinality of the input and the support vector of \mathbf{x} is given as

$$\text{supp}(\mathbf{x}) = \{j \in [N] : x_j \neq 0\},$$

where $[N]$ is a set of integers $\{1, 2, \dots, N\}$ [10, p. 41]. The set of all k -sparse signals is denoted as

$$\Omega_k = \{\mathbf{x} : \|\mathbf{x}\|_0 \leq k\}.$$

3.2.2 Optimisation Problem

To find a solution to the linear model (3.1) assuming the solution is k -sparse, it can be view as an optimisation problem. An optimisation problem is defined as

$$\min f_0(\mathbf{x}) \quad \text{subject to} \quad f_i(\mathbf{x}) \leq b_i, \quad i = 1, 2, \dots, n,$$

where $f_0 : \mathbb{R}^N \mapsto \mathbb{R}$ is an objective function and $f_i : \mathbb{R}^N \mapsto \mathbb{R}$ are the constraint functions.

To find the k -sparse solution the optimisation problem can be written as

$$\mathbf{x}^* = \arg \min_{\mathbf{x} \in \Omega_k} \|\mathbf{x}\|_0 \quad \text{subject to} \quad \mathbf{y} = \mathbf{A}\mathbf{x},$$

The objective function is given by an ℓ_0 norm with the constraint function being the linear model (3.1). Unfortunately, this optimisation problem is non-convex due to the definition of ℓ_0 -norm and is therefore difficult to solve – it is a NP-hard problem. Instead, by replacing the ℓ_0 -norm with the ℓ_1 -norm, the optimisation problem can be approximated and hence become computational feasible [7, p. 27]

$$\mathbf{x}^* = \arg \min_{\mathbf{x} \in \Omega_k} \|\mathbf{x}\|_1 \quad \text{subject to} \quad \mathbf{y} = \mathbf{A}\mathbf{x}. \quad (3.2)$$

3.2: skal vi indføre z som en approximation til x. og så et nyt omega eller? eller kan vi beholde x

With this optimisation problem we find the best k -sparse solution \mathbf{x}^* . This method is referred to as Basis Pursuit.

The following theorem justifies that the ℓ_1 optimisation problem finds a sparse solution [10, p. 62-63].

Theorem 3.2.1

A mixing matrix $\mathbf{A} \in \mathbb{R}^{M \times N}$ is defined with columns $\mathbf{A} = [\mathbf{a}_1, \dots, \mathbf{a}_N]$. By assuming uniqueness of a solution \mathbf{x}^* to

$$\min_{\mathbf{x} \in \mathbb{R}^N} \|\mathbf{x}\|_1 \quad \text{subject to} \quad \mathbf{A}\mathbf{x} = \mathbf{y},$$

the system $\{\mathbf{a}_j, j \in \text{supp}(\mathbf{x}^*)\}$ is linearly independent, and in particular

$$\|\mathbf{x}^*\|_0 = \text{card}(\text{supp}(\mathbf{x}^*)) \leq M.$$

To prove this theorem one need to realise that the set $\{\mathbf{a}_j, j \in S\} \leq M$, with $S = \text{supp}(\mathbf{x}^*)$, can not have more than M linearly independence columns. So when $M \ll N$ a sparse signal is automatically achieved.

Proof

For the case of contradiction, assume that the set $\{\mathbf{a}_j, j \in S\}$ is linearly dependent. Thus there exists a non-zero vector $\mathbf{v} \in \mathbb{R}^N$ supported on S such that $\mathbf{A}\mathbf{v} = \mathbf{0}$. Then, for any $t \neq 0$,

$$\|\mathbf{x}^*\|_1 < \|\mathbf{x}^* + t\mathbf{v}\|_1 = \sum_{j \in S} |x_j^* + tv_j| = \sum_{j \in S} \text{sgn}(x_j^* + tv_j)(x_j^* + tv_j).$$

If $|t|$ is small enough, namely, $|t| < \min_{j \in S} \frac{|x_j^*|}{\|\mathbf{v}\|_\infty}$, then

$$\text{sgn}(x_j^* + tv_j) = \text{sgn}(x_j^*), \quad \forall j \in S.$$

It then follows that

$$\|\mathbf{x}^*\|_1 < \sum_{j \in S} \text{sgn}(x_j^*)(x_j^* + tv_j) = \sum_{j \in S} \text{sgn}(x_j^*)x_j^* + t \sum_{j \in S} \text{sgn}(x_j^*)v_j = \|\mathbf{x}^*\|_1 + t \sum_{j \in S} \text{sgn}(x_j^*)v_j.$$

This is a contradiction, because one can always choose a small $t \neq 0$ such that

$$t \sum_{j \in S} \text{sgn}(x_j^*)v_j \leq 0,$$

and therefore the set $\{\mathbf{a}_j, j \in S\}$ must be linearly independent. ■

The Basis Pursuit makes the foundation of several algorithms solving alternative versions of (3.2) where noise is incorporated. An alternative solution method includes greedy algorithms such as the Orthogonal Matching Pursuit(OMP) [10, P. 65]. At each iteration of the OMP algorithm an index set S is updated by adding the index corresponding to the column in \mathbf{A} that best describes the residual, hence greedy. That is the part of \mathbf{y} that is not yet explained by $\mathbf{A}\mathbf{x}$ is included. Then \mathbf{x} is updated as the vector, supported by S , which minimize the residual, that is also the orthogonal projection of \mathbf{y} onto the span $\{\mathbf{a}_j \mid j \in S\}$. The algorithm for OMP can be seen in 1 where \mathbf{A}^* be the adjoint of a matrix \mathbf{A} .

Algorithm 1 Orthogonal Matching Pursuit (OMP)

```

1:  $k = 0$ 
2: Initialize  $S_{(0)} = \emptyset$ 
3: Initialize  $\mathbf{x}_{(0)} = \mathbf{0}$ 
4: procedure OMP( $\mathbf{A}, \mathbf{y}$ )
5:   while stopping criteria not meet do
6:      $k = k + 1$ 
7:      $j_{(k)} = \arg \max_{j \in [N]} \{ |(\mathbf{A}^*(\mathbf{y} - \mathbf{A}\mathbf{x}_{(k-1)}))_j| \}$ 
8:      $S_{(k)} = S_{(k-1)} \cup \{j_{(k)}\}$ 
9:      $\mathbf{x}_{(k)} = \arg \min_{\mathbf{z} \in \mathbb{C}^N} \{ \|\mathbf{y} - \mathbf{A}\mathbf{z}\|_2 \mid \text{supp}(\mathbf{z}) \subset S_{(k)} \}$ 
10:   end while
11:    $\mathbf{x}^* = \mathbf{x}_{(k)}$ 
12: end procedure

```

3.2.3 Conditions on the Mixing Matrix

In section 3.2.2 the mixing matrix \mathbf{A} was assumed known, in order to solve the optimisation problem (3.2). However, in practise it is only the measurement vector \mathbf{y} which is known. In this case the mixing matrix \mathbf{A} is considered a estimate of the true mixing matrix. In general compressive sensing terminology \mathbf{A} is also referred to as a dictionary matrix.

To ensure exact or approximately reconstruction of the sparse signal \mathbf{x} , the mixing matrix must be constructed with certain conditions in mind.

Null Space Condition

The the null space property is a necessary and sufficient condition to \mathbf{A} for exact reconstruction of every sparse signal \mathbf{x} that solves the optimisation problem (3.2)[10, p. 77]. The null space of the matrix \mathbf{A} is defined as

$$\mathcal{N}(\mathbf{A}) = \{\mathbf{z} : \mathbf{A}\mathbf{z} = \mathbf{0}\}.$$

The null space property is defined as

Definition 3.1 (Null Space Property)

A matrix $\mathbf{A} \in \mathbb{R}^{M \times N}$ is said to satisfy the null space property relative to a set $S \subset [N]$ if

$$\|\mathbf{v}_S\|_1 < \|\mathbf{v}_{\bar{S}}\|_1 \quad \text{for all } \mathbf{v} \in \text{null}(\mathbf{A} \setminus \{\mathbf{0}\}), \quad (3.3)$$

where the vector \mathbf{v}_S is the restriction of \mathbf{v} to the indices in S , and \bar{S} is the set $[N] \setminus S$.

Theorem 3.2.2

Given a matrix $\mathbf{A} \in \mathbb{R}^{M \times N}$, every vector $\mathbf{x} \in \mathbb{R}^N$ with $\text{supp}(\mathbf{x}) \subset S$ is the unique solution of (3.2) with $\mathbf{y} = \mathbf{A}\mathbf{x}$ if and only if \mathbf{A} satisfies the null space property relative to S .

Proof

\Rightarrow :

Let $S \subseteq [N]$ be a fixed index set. Assume that any vector $\mathbf{x} \in \mathbb{R}^N$ with support $\text{supp}(\mathbf{x}) \subset S$ is the unique minimizer of $\|\mathbf{z}\|_1$ with respect to $\mathbf{A}\mathbf{z} = \mathbf{A}\mathbf{x}$. Thus, for any vector $\mathbf{v} \in \text{null}(\mathbf{A}) \setminus \{\mathbf{0}\}$, the vector \mathbf{v}_S is the unique minimizer of $\|\mathbf{z}\|_1$ with respect to $\mathbf{A}\mathbf{z} = \mathbf{A}\mathbf{v}_S$. But

$$\mathbf{0} = \mathbf{A}(\mathbf{v}_S + \mathbf{v}_{\bar{S}}) \implies \mathbf{A}\mathbf{v}_S = \mathbf{A}(-\mathbf{v}_{\bar{S}}), \quad \text{with } -\mathbf{v}_{\bar{S}} \neq \mathbf{v}_S,$$

or else $\mathbf{v} = \mathbf{0}$. It is concluded that $\|\mathbf{v}_S\|_1 < \|\mathbf{v}_{\bar{S}}\|_1$. This establishes the null space property relative to S .

\Leftarrow :

Conversely, assume that the null space property relative to S holds. Given an index set $S \subseteq [N]$ with null space property and a vector $\mathbf{x} \in \mathbb{R}^N$ with $\text{supp}(\mathbf{x}) \subset S$. Furthermore, given a vector $\mathbf{z} \in \mathbb{R}^N$ where $\mathbf{z} \neq \mathbf{x}$, such that $\mathbf{A}\mathbf{z} = \mathbf{A}\mathbf{x}$. Consider then a vector \mathbf{v} given by $\mathbf{v} := \mathbf{x} - \mathbf{z} \in \text{null}(\mathbf{A}) \setminus \{\mathbf{0}\}$. From the null space property, the following is obtained:

$$\begin{aligned} \|\mathbf{x}\|_1 &\leq \|\mathbf{x} - \mathbf{z}_S\|_1 = \|\mathbf{v}_S\|_1 + \|\mathbf{z}_S\|_1 \\ &< \|\mathbf{v}_{\bar{S}}\|_1 + \|\mathbf{z}_S\|_1 \\ &= \|\mathbf{v}\|_1 + \|\mathbf{z}_S\|_1 = \|\mathbf{z}\|_1. \end{aligned}$$

This establishes the required sparseness of $\|\mathbf{x}\|_1$. ■

Unfortunately, this is a condition which is hard to check in practice.

Coherence

The null space property provide a unique solution to the optimisation problem (3.2), but it is unfortunately complicated to investigate. Instead an alternative measure is presented.

Coherence is a measure of quality, it determines whether a matrix \mathbf{A} is a good choice for the optimisation problem (3.2). A small coherence describes the performance of a recovery algorithm as good with that choice of \mathbf{A} .

Definition 3.2 (Coherence)

Coherence of the matrix $\mathbf{A} \in \mathbb{R}^{M \times N}$, denoted as $\mu(\mathbf{A})$, with columns $\mathbf{a}_1, \dots, \mathbf{a}_N$ for all $i \in [N]$ is given as

$$\mu(\mathbf{A}) = \max_{1 \leq i < j \leq n} \frac{|\langle \mathbf{a}_i, \mathbf{a}_j \rangle|}{\|\mathbf{a}_i\|_2 \|\mathbf{a}_j\|_2}.$$

Restricted Isometry Condition

Restricted isometry condition is a stronger condition concerning the orthogonality of the matrix \mathbf{A} .

Definition 3.3 (Restricted Isometry Property (RIP))

A matrix \mathbf{A} satisfies the RIP of order k if there exists a $\delta_k \in (0, 1)$ such that

$$(1 - \delta_k) \|\mathbf{x}\|_2^2 \leq \|\mathbf{Ax}\|_2^2 \leq (1 + \delta_k) \|\mathbf{x}\|_2^2,$$

Theorem 3.2.3

Suppose that the $2s$ -th restricted isometry constant of the matrix $\mathbf{A} \in \mathbb{R}^{M \times N}$ satisfies

$$\delta_{2s} < \frac{1}{3}.$$

Then every s -sparse vector $\mathbf{x}^* \in \mathbb{R}^N$ is the unique solution of

$$\min_{\mathbf{z} \in \mathbb{R}^N} \|\mathbf{z}\|_1 \quad \text{subject to} \quad \mathbf{Az} = \mathbf{Ax}.$$

Proof

To proof the theorem one only need to show the null space condition:

$$\|\mathbf{v}\|_1 < \frac{1}{2} \|\mathbf{v}\|_1, \quad \forall \mathbf{v} \in \ker(\mathbf{A}) \setminus \{\mathbf{0}\}, \quad S \subseteq [N], \quad \text{card}(S) \leq s.$$

Cf. Cauchy-Schwarz or $\|\mathbf{v}_S\|_1 \leq \|\mathbf{v}_S\|_2 \sqrt{s}$, one only need to show

$$\begin{aligned} \|\mathbf{v}_S\|_2 &\leq \frac{\rho}{2\sqrt{s}} \|\mathbf{v}\|_1 \\ \rho &= \frac{2\delta_{2s}}{1 - \delta_{2s}} < 1, \end{aligned}$$

whenever $\delta_{2s} < 1/3$. Given $\mathbf{v} \in \ker(\mathbf{A}) \setminus \{\mathbf{0}\}$, it is enough to consider an index set $S = S_0$ of s largest absolute entries of the vector \mathbf{v} . The complement $\overline{S_0}$ of S_0 in $[N]$ is partition as $S_0 = S_1 \cup S_2 \cup \dots$, where

$$\begin{aligned} S_1 &: \text{index set of } s \text{ largest absolute entries of } \mathbf{v} \text{ in } \overline{S_0}, \\ S_2 &: \text{index set of } s \text{ largest absolute entries of } \mathbf{v} \text{ in } \overline{S_0 \cup S_1}. \end{aligned}$$

With $\mathbf{v} \in \ker(\mathbf{A})$:

$$\mathbf{A}(\mathbf{v}_{S_0}) = \mathbf{A}(-\mathbf{v}_{S_1} - \mathbf{v}_{S_2} - \dots),$$

so that

$$\begin{aligned} \|\mathbf{v}_{S_0}\|_2^2 &\leq \frac{1}{1 - \delta_{2s}} \|\mathbf{A}(\mathbf{v}_{S_0})\|_2^2 = \frac{1}{1 - \delta_{2s}} \langle \mathbf{A}(\mathbf{v}_{S_0}), \mathbf{A}(-\mathbf{v}_{S_1}) + \mathbf{A}(-\mathbf{v}_{S_2}) + \dots \rangle \\ &= \frac{1}{1 - \delta_{2s}} \sum_{k \geq 1} \langle \mathbf{A}(\mathbf{v}_{S_0}), \mathbf{A}(-\mathbf{v}_{S_k}) \rangle. \end{aligned} \tag{3.4}$$

According to Proposition 6.3 [10, p. 135], one also have

$$\langle \mathbf{A}(\mathbf{v}_{S_0}), \mathbf{A}(-\mathbf{v}_{S_k}) \rangle \leq \delta_{2s} \|\mathbf{v}_{S_0}\|_2 \|\mathbf{v}_{S_k}\|_2. \quad (3.5)$$

Substituting (3.5) into (3.4) and dividing by $\|\mathbf{v}_{S_0}\|_2 > 0$ ■

3.2.4 Multiple Measurement Vector Model

The linear model (3.1) is also referred to as a single measurement vector (SMV) model. In order to adapt the model (3.1) to a practical use the model is expanded to include multiple measurement vectors and take noise into account.

A multiple measurement vector (MMV) model consist of the observed measurement matrix $\mathbf{Y} \in \mathbb{R}^{M \times L}$, the source matrix $\mathbf{X} \in \mathbb{R}^{N \times L}$, the dictionary matrix $\mathbf{A} \in \mathbb{R}^{M \times N}$ and the noise vector $\mathbf{E} \in \mathbb{R}^{M \times L}$:

$$\mathbf{Y} = \mathbf{A}\mathbf{X} + \mathbf{E}. \quad (3.6)$$

L denote the number of observed measurement vectors each consisting of M measurements, that is L samples is given. For $L = 1$ the linear model will just be the SMV model (3.1).

The matrix \mathbf{X} consist of $\{\mathbf{x}_i\}_{i=1}^L$ k -sparse vectors which has been stacked column-wise such that \mathbf{X} consist of at most k non-zero rows. As for the SMV model (3.1) the MMV model (3.6) is under-determined with $M \ll N$ and $k < M$ [7, p. 42].

The support of \mathbf{X} denote the index set of non-zero rows of \mathbf{X} and \mathbf{X} is said to be row-sparse. As the columns in \mathbf{X} are k -sparse and as mention before \mathbf{X} has at most k non-zero rows, the non-zero values occur in common location for all columns. By using this joint information it is possible to recover \mathbf{X} from fewer measurements. By using the rank of \mathbf{X} , which give us information of the amount of linearly independent rows or columns, and the spark of \mathbf{A} which is the minimum set of linearly dependent columns, it is possible to set some conditions on the system to ensure recovery.

When $|\text{supp}(\mathbf{X})| = k$ then $\text{rank}(\mathbf{X}) \leq k$. If $\text{rank}(\mathbf{X}) = 1$ then are the k -sparse vectors $\{\mathbf{x}_i\}_{i=1}^L$ multiples of each other and the joint information can not be taken advantage of. But for large rank it is possible to exploit the diversity of the columns in \mathbf{X} . This can be defined as a sufficient and necessary condition of the MMV model (3.6). MMV system $\mathbf{Y} = \mathbf{A}\mathbf{X}$ must have

$$|\text{supp}(\mathbf{X})| < \frac{\text{Spark}(\mathbf{A}) - 1 + \text{rank}(\mathbf{X})}{2}$$

such that \mathbf{X} can uniquely be determined.

This result says that a row-sparse matrix \mathbf{X} with large rank can be recovered from fewer measurement [7, p. 43].

Skal "fewer" udspecificeres yderligere?

3.3 Dictionary learning

As clarified in section 3.2.3 the estimation of dictionary matrix \mathbf{A} is essential to achieve the best recovery of the sparse signal \mathbf{x} from the measurements \mathbf{y} . Pre-constructed dictionaries do exist which in many cases results in simple and fast algorithms for reconstruction of \mathbf{x} [9]. Pre-constructed dictionaries are typically fitted to a specific kind of data, for instance the discrete Fourier transform or the discrete wavelet transform are used especially for sparse representation of images[9]. Hence the results of using such dictionaries depend on how well they fit the data of interest, which is creating a certain limitation. An alternative is to consider an adaptive dictionary based on a set of training data that resembles the data of interest. For this purpose learning methods are considered to empirically construct a fixed dictionary which can take part in the application. Different dictionary learning algorithms exist, one is the K-SVD which is to be elaborated in this section. The K-SVD algorithm was presented in 2006 by Elad et al. and found to outperform pre-constructed dictionaries when computational cost is of secondary interest[1].

Consider now $\mathbf{Y} = [\mathbf{y}_1, \dots, \mathbf{y}_L]$, $\mathbf{y}_i \in \mathbb{R}^M$ as a training database, created by $\mathbf{y}_i = \mathbf{A}\mathbf{x}_i$ for which we want to learn the best suitable dictionary \mathbf{A} and sparse representation $\mathbf{X} = [\mathbf{x}_1, \dots, \mathbf{x}_L]$, $\mathbf{x}_i \in \mathbb{R}^N$. For a known sparsity constraint k this can be defined by an optimisation problem similar to the general compressive sensing problem of multiple measurements [9]

$$\min_{\mathbf{A}, \mathbf{X}} \sum_{i=1}^L \|\mathbf{y}_i - \mathbf{A}\mathbf{x}_i\|_2^2 \quad \text{st. } \|\mathbf{x}_i\|_0 \leq k, \quad 1 \leq i \leq L. \quad (3.7)$$

The learning consist of jointly solving the optimization problem on \mathbf{X} and \mathbf{A} . The uniqueness of \mathbf{A} depends on the recovery sparsity condition. As clarified earlier recovery is only possible if $k < M$ [5]. Furthermore, consider \mathbf{A}_0 such that every training signal can be represented by $k_0 < \text{spark}(\mathbf{A}_0)/2$ columns of \mathbf{A}_0 , then \mathbf{A}_0 is a unique dictionary, up to scaling and permutation of columns[9]. Again the ℓ_0 -norm lead to an NP-hard problem an heuristic methods are need.

fungerer disse to uniqueness parameter sammen?

3.3.1 K-SVD

The dictionary learning algorithm K-SVD provide an update rule which is applied to each column of $\mathbf{A}_0 = [\mathbf{a}_0, \dots, \mathbf{a}_N]$. Updating first \mathbf{a}_i and then the corresponding coefficients in \mathbf{X} which it is multiplied with, that is the i^{th} row in \mathbf{X} denoted by \mathbf{x}_i^T . Let \mathbf{a}_{i_0} be the column to be updated and let the remaining columns be fixed. By rewriting the objective function in (3.7) using matrix notation it is possible to isolate

the contribution from \mathbf{a}_{i_0} .

$$\begin{aligned}\|\mathbf{Y} - \mathbf{A}\mathbf{X}\|_F^2 &= \left\| \mathbf{Y} - \sum_{i=1}^M \mathbf{a}_i \mathbf{x}_i^T \right\|_F^2 \\ &= \left\| \left(\mathbf{Y} - \sum_{i \neq i_0}^M \mathbf{a}_i \mathbf{x}_i^T \right) - \mathbf{a}_{i_0} \mathbf{x}_{i_0}^T \right\|_F^2,\end{aligned}\quad (3.8)$$

where F is the Frobenius norm that works on matrices

$$\|\mathbf{A}\|_F = \sqrt{\sum_{i=1}^M \sum_{j=1}^N |a_{i,j}|^2}.$$

In (3.8) the term in the parenthesis makes the an error matrix \mathbf{E}_{i_0} without the contribution from i_0 , hence minimising (3.8) with respect to \mathbf{a}_{i_0} and $\mathbf{x}_{i_0}^T$ leads to the optimal contribution from i_0 (can I say it this way..?).

$$\min_{\mathbf{a}_{i_0}, \mathbf{x}_{i_0}^T} \left\| \mathbf{E}_{i_0} - \mathbf{a}_{i_0} \mathbf{x}_{i_0}^T \right\|_F^2 \quad (3.9)$$

The optimal solution to (3.9) is known to be the rank-1 approximation of \mathbf{E}_{i_0} . This comes from the Eckart–Young–Mirsky theorem[?] saying that a partial single value decomposition(SVD) makes the best low-rank approximation of a matrix such as \mathbf{E}_{i_0} .

That is specifically that for $\mathbf{E}_{i_0} = \mathbf{U}\mathbf{\Sigma}\mathbf{V}^T \in \mathbb{R}^{M \times N}$, $M \leq N$ with

$$\mathbf{U} = [\mathbf{u}_1, \dots, \mathbf{u}_M] \in \mathbb{R}^{M \times M}, \quad \mathbf{\Sigma} = \text{diag}[\sigma_1, \dots, \sigma_m] \in \mathbb{R}^{M \times N}, \quad \mathbf{V} = [\mathbf{v}_1, \dots, \mathbf{v}_N] \in \mathbb{R}^{N \times N}$$

where \mathbf{U} and \mathbf{V} are unitary matrices, i.e. $\mathbf{U}^T \mathbf{U} = \mathbf{U} \mathbf{U}^T = \mathbf{I}$, and σ_j is the non-negative singular values of \mathbf{E}_{i_0} such that $\sigma_1 \geq \sigma_2 \geq \dots \geq 0$. The best k -rank approximation to \mathbf{E}_{i_0} , with $k < \text{rank}(\mathbf{E}_{i_0})$ is then given by [Wiki..]

$$\mathbf{E}_{i_0}^{(k)} = \sum_{j=1}^k \sigma_j \mathbf{u}_j \mathbf{v}_j^T.$$

Since the outer product always have rank-1 letting $\mathbf{a}_{i_0} = \mathbf{u}_1$ and $\mathbf{x}_{i_0}^T = \sigma_1 \mathbf{v}_1^T$ solves the optimisation problem (3.9). However in order to preserve the sparsity in \mathbf{X} while optimising, only the non-zero entries in $\mathbf{x}_{i_0}^T$ are allowed to vary. For this purpose only a subset of columns in \mathbf{E}_{i_0} is considered, those which correspond to the non-zero entries of $\mathbf{x}_{i_0}^T$. A matrix \mathbf{P}_{i_0} is defined such that $\mathbf{x}_{i_0}^{T(R)} = \mathbf{x}_{i_0}^T \mathbf{P}_{i_0}$ is restricted to contain only the M_{j_0} non-zero entries of $\mathbf{x}_{i_0}^T$. By applying SVD to the sub-matrix $\mathbf{E}_{i_0} \mathbf{P}_{i_0}$ and updating \mathbf{a}_{i_0} and $\mathbf{x}_{i_0}^{T(R)}$ the rank-1 approximation is found and the original representation vector is updated as $\mathbf{x}_{i_0}^T = \mathbf{x}_{i_0}^{T(R)} \mathbf{P}_{i_0}^T$.

The main steps of K-SVD is described in algorithm 2.

Algorithm 2 K-SVD

```

1:  $k = 0$ 
2: Initialize random  $\mathbf{A}_{(0)}$ 
3: Initialize  $\mathbf{X}_{(0)} = \mathbf{0}$ 
4:
5: procedure K-SVD( $\mathbf{A}_{(0)}$ )
6:   normilize columns of  $\mathbf{A}_{(0)}$ 
7:   while  $error \geq limit$  do
8:      $j = j + 1$ 
9:     for  $j \leftarrow 1, 2, \dots, L$  do  $\triangleright$  updating each col. in  $\mathbf{X}_{(k)}$ 
10:       $\hat{\mathbf{x}}_j = \min_{\mathbf{x}} \|\mathbf{y}_j - \mathbf{A}_{(k-1)}\mathbf{x}_j\| \quad s.t. \quad \|\mathbf{x}_j\| \leq k_0$ 
11:    end for
12:     $\mathbf{X}_{(k)} = \{\hat{\mathbf{x}}_j\}_{j=1}^L$ 
13:    for  $i_0 \leftarrow 1, 2, \dots, N$  do
14:       $\Omega_{i_0} = \{j | 1 \leq j \leq L, \mathbf{X}_{(k)}[i_0, j] \neq 0\}$ 
15:      From  $\Omega_{i_0}$  define  $\mathbf{P}_{i_0}$ 
16:       $\mathbf{E}_{i_0} = \mathbf{Y} - \sum_{i \neq i_0}^M \mathbf{a}_i \mathbf{x}_i^T$ 
17:       $\mathbf{E}_{i_0}^R = \mathbf{E}_{i_0} \mathbf{P}_{i_0}$ 
18:       $\mathbf{E}_{i_0}^R = \mathbf{U} \mathbf{\Sigma} \mathbf{V}^T$   $\triangleright$  perform SVD
19:       $\mathbf{a}_{i_0} \leftarrow \mathbf{u}_1$   $\triangleright$  update the  $i_0$  col. in  $\mathbf{A}_{(k)}$ 
20:       $(\mathbf{x}_{i_0}^T)^R \leftarrow \sigma_1 \mathbf{v}_1$ 
21:       $\mathbf{x}_{i_0}^T \leftarrow (\mathbf{x}_{i_0}^T)^R \mathbf{P}_{i_0}^T$   $\triangleright$  update the  $i_0$  row in  $\mathbf{X}_{(k)}$ 
22:    end for
23:     $error = \|\mathbf{Y} - \mathbf{A}_{(k)} \mathbf{X}_{(k)}\|_F^2$ 
24:  end while
25: end procedure

```

The dictionary learning algorithm K-SVD is a generalisation of the well known K-means clustering also referred to as vector quantization. In K-means clustering a set of K vectors is learned referred to as mean vectors, each signal sample is then represented by its nearest mean vector. That corresponds to the case with sparsity constrict $k = 1$ and the representation reduced to a binary scalar $x = 1, 0$. Further instead of computing the mean of K sub-sets the K-SVD algorithm computes the SVD factorisation of the K different sub-matrices that correspond to the K columns of \mathbf{A} .

3.4 Independent Component Analysis

Independent component analysis (ICA) is a method that applies to the general problem of decomposition of a measurement vector into a source vector and a mixing matrix. The intention of ICA is to separate a multivariate signal into statistical independent and non-Gaussian signals and furthermore identify the mixing matrix \mathbf{A} , given only the observed measurements \mathbf{Y} . A well known application example of source separation is the cocktail party problem, where it is sought to listen to one specific person speaking in a room full of people having interfering conversations. Let $\mathbf{y} \in \mathbb{R}^M$ be a single measurement from M microphones containing a linear mixture of all the speak signal that are present in the room. When additional noise is not considered the problem can be described as the familiar linear model,

$$\mathbf{y} = \mathbf{A}\mathbf{x} \quad (3.10)$$

where $\mathbf{x} \in \mathbb{R}^N$ contain the N underlying speak signals and \mathbf{A} is a mixing matrix where the coefficients depends (more or less?) on the distance from the source to the microphone. As such each y_i is a weighted sum of all the present sources of speak.

By ICA both the mixing matrix \mathbf{A} and the sources signals \mathbf{x} are sought estimated from the observed measurements \mathbf{y} . The main attribute of ICA is the assumption that the sources in \mathbf{x} are statistical independent and non-Gaussian distributed, hence the name independent components.

By independence, one means that changes in one source signal do not affect the other source signals. Theoretically that is the joint probability density function (pdf) of \mathbf{x} can be factorised into the product of the marginal pdfs of the components x_i

$$p(x_1, x_2, \dots, x_n) = p_1(x_1)p_2(x_2)\cdots p_n(x_n),$$

The possibility of separating a signal into independent and non-Gaussian components originates from the central limit theorem[13, p. 34]. The theorem state that the distribution any linear mixture of two or more independent random variables tents toward a Gaussian distribution, under certain conditions. Thus, when a non-Gaussian distribution of the independent components is achieved through optimization it must be the original sources.

3.4.1 Assumptions and Preprocessing

For simplicity assume \mathbf{A} is square i.e. $M = N$ and invertible. As such when \mathbf{A} has been estimated the inverse is computed the components can simply be estimated as $\mathbf{x} = \mathbf{A}^{-1}\mathbf{y}$ [13, p. 152-153].

As both \mathbf{A} and \mathbf{x} are unknown the variances of the independent components can not be determined. However it is reasonable to assume that \mathbf{x} has unit variance, as \mathbf{A}

when we assume independence it is enough to solve system, why?

herover er ukommenteret et afsnit jeg ikke forstår

will adapt to this restriction. Any scalar multiplier within a source can be cancelled out by dividing the corresponding column in \mathbf{A} with the same scalar [13, p. 154].

For further simplification it is assumed without loss of generality that $\mathbb{E}[\mathbf{y}] = 0$ and $\mathbb{E}[\mathbf{x}] = 0$ [13, p. 154]. In case this assumption is not true, the measurements can be centred by subtracting the mean as preprocessing before doing ICA.

A preprocessing step central to ICA is to whiten the measurements \mathbf{y} . By the whitening process any correlation in the measurements are removed and unit variance is ensured. This ensures that the independent components \mathbf{x} are uncorrelated and have unit variance (true?). Furthermore, this reduces the complexity of ICA and therefore simplifies the recovering process.

Whitening is a linear transformation of the observed data. That is multiplying the measurement vector \mathbf{y} with a whitening matrix \mathbf{V} ,

$$\mathbf{y}_{white} = \mathbf{V}\mathbf{y}$$

to obtain a new measurement vector \mathbf{y}_{white} that is white. To obtain a whitening matrix the eigenvalue decomposition (EVD) of the covariance matrix can be used,

$$\mathbb{E}[\mathbf{y}\mathbf{y}^T] = \mathbf{E}\mathbf{D}\mathbf{E}^T$$

here \mathbf{D} is a diagonal matrix of eigenvalues and \mathbf{E} is the associated eigenvectors. From \mathbf{E} and \mathbf{D} a whitening matrix is constructed [13, p.159].

$$\mathbf{V} = \mathbf{E}\mathbf{D}^{-1/2}\mathbf{E}^T.$$

Where $\mathbf{D}^{-1/2} = \text{diag}d_1^{-1/2}, \dots, d_n^{-1/2}$ is a componentwise operation.

By multiplying the measurement vector \mathbf{y} with a whitening matrix \mathbf{V} the data becomes white

$$\mathbf{y}_{white} = \mathbf{V}\mathbf{y} = \mathbf{V}\mathbf{A}\mathbf{x} = \mathbf{A}_{white}\mathbf{x}$$

Furthermore the mixing matrix \mathbf{A}_{white} becomes orthogonal

$$\mathbb{E}[\mathbf{y}_{white}\mathbf{y}_{white}^T] = \mathbf{A}_{white}\mathbb{E}[\mathbf{x}\mathbf{x}^T]\mathbf{A}_{white}^T = \mathbf{A}_{white}\mathbf{A}_{white}^T = \mathbf{I}.$$

Consequently ICA can restrict its search for the mixing matrix to the orthogonal matrix space – That is instead of estimating n^2 parameters ICA now only has to estimate an orthogonal matrix which has $n(n-1)/2$ parameters/degrees of freedom [13, p. 159].

whitening is a linear change of coordinates of the mixed data http://arnauddeleorme.com/ica_for_dummies/ "By rotating the axis and minimizing Gaussianity of the projection in the first scatter plot, ICA is able to recover the original sources which are statistically independent"

se udkommentering herunder?

3.4.2 Recovery of the Independent Components

Now the ICA model is established, the next step is the estimation of the mixing coefficients a_{ij} and independent components x_i . The simple and intuitive method

is to take advantage of the assumption of non-Gaussian independent components. Consider again the ICA model of a single measurement vector $\mathbf{y} = \mathbf{A}\mathbf{x}$ where the independent components can be estimated by the inverted model $\mathbf{x} = \mathbf{A}^{-1}\mathbf{y}$. Let $\mathbf{A}^{-1} = \mathbf{B}$, now a single independent component can be seen as the linear combination

$$x_j = \mathbf{b}_j^T \mathbf{y} = \sum_i b_{ji} y_i \quad (3.11)$$

where \mathbf{b}_j^T is the j^{th} row of \mathbf{B} . The issue is now to determine \mathbf{b}_j such that it equals the j^{th} row from the inverse \mathbf{A} . As \mathbf{A} is unknown it is not possible to determine \mathbf{b}_j exactly, but an estimate can be found to make a good approximation. Rewriting (3.11)

$$x_j = \mathbf{b}_j^T \mathbf{y} = \mathbf{b}_j^T \mathbf{A}\mathbf{x} = \mathbf{q}^T \mathbf{x} = \sum_{i=1} q_i x_i$$

it is seen how x_j is a linear combination of all \mathbf{x}_i , thus the equality only holds true when \mathbf{q} consist of only one non-zero element that equals 1. Due to the central limit theorem the distribution of $\mathbf{q}^T \mathbf{x}$ most non-Gaussian when it equals one of the independent components which was assumed non-Gaussian. Then, since $\mathbf{q}^T \mathbf{x} = \mathbf{b}_j^T \mathbf{y}$, it is possible to vary the coefficients in \mathbf{b} and look at the distribution of $\mathbf{b}_j^T \mathbf{y}$. Finding the vector \mathbf{b} that maximize the non-Gaussianity would then corresponds to $\mathbf{q} = \mathbf{A}^T \mathbf{b}$ having only a single non-zero element. Thus maximizing the non-Gaussianity of $\mathbf{b}_j^T \mathbf{y}$ results in one of the independent components [13, p. 166].

Considering the n -dimensional space of vectors \mathbf{b} there exist $2n$ local maxima, corresponding to x_i and $-x_i$ for all n independent components [13, p. 166].

3.4.3 Kurtosis

To maximize the non-gaussianity a measure for gaussianity is needed. Kurtosis is a quantitative measure used for nongaussianity of random variables. Kurtosis of a random variable y is the fourth-order cumulant denoted by $\text{kurt}(y)$. For y with zero mean and unit variance kurtosis reduces to

$$\text{kurt}(y) = \mathbb{E}[y^4] - 3.$$

It is seen that the kurtosis is a normalized version of the fourth-order moment defined as $\mathbb{E}[y^4]$. For a Gaussian random variable the fourth-order moment equals $3(\mathbb{E}[y^2])^2$ hence the corresponding kurtosis will be zero [13, p. 171]. Consequently the kurtosis of non-Gaussian random variables will almost always be different from zero.

The kurtosis is a common measure for non-Gaussianity due to its simplicity both theoretical and computational. The kurtosis can be estimated computationally by the forth-order moment of sample data when the variance is constant. Furthermore,

uddyb? og tilføj kilde til kurtosis

for two independent random variables x_1, x_2 the following linear properties applies to the kurtosis of the sum

$$\text{kurt}(x_1 + x_2) = \text{kurt}(x_1) + \text{kurt}(x_2) \quad \text{and} \quad \text{kurt}(\alpha x_1) = \alpha^4 \text{kurt}(x_1)$$

However, one complication concerning kurtosis as a measure is that kurtosis is sensitive to outliers [13, p. 182].

Consider again the vector $\mathbf{q} = \mathbf{A}^T \mathbf{b}$ such that $\mathbf{b}_j^T \mathbf{y} = \sum_{i=1} q_i x_i$. By the additive property of kurtosis

$$\text{kurt}(\mathbf{b}_j^T \mathbf{y}) = \sum_{i=1} q_i^4 \text{kurt}(x_i).$$

Then the assumption of the independent components having unit variance results in $\mathbb{E}[x_j] = \sum_{i=1} q_i^2 = 1$. That is geometrically that \mathbf{q} is constraint to the unit sphere, $\|\mathbf{q}\|^2 = 1$. By this the optimisation problem of maximising the kurtosis of $\mathbf{b}_j^T \mathbf{y}$ is similar to maximizing $|\text{kurt}(x_j)| = |\sum_{i=1} q_i^4 \text{kurt}(x_i)|$ on the unit sphere.

hvordan kommer dette frem?

Due to the described preprocessing \mathbf{b} is assumed to be white and it can be shown that $\|\mathbf{q}\| = \|\mathbf{b}_j\|$ [13, p. 174]. This show that constraining $\|\mathbf{q}\|$ to one is similar to constraining $\|\mathbf{b}_j\|$ to one.

3.4.4 The Gradient Algorithm with Kurtosis

In practise, to recover the mixing matrix \mathbf{A} by maximizing the kurtosis of $\mathbf{b}_j^T \mathbf{y}$, gradient optimisation methods are used.

The general idea behind a gradient algorithm is to determine the direction for which $\text{kurt}(\mathbf{b}_j^T \mathbf{y})$ is growing the most, based on the gradient.

The gradient of $|\text{kurt}(\mathbf{b}_j^T \mathbf{y})|$ is computed as

$$\frac{\partial |\text{kurt}(\mathbf{b}_j^T \mathbf{y})|}{\partial \mathbf{b}_j} = 4 \text{sign}(\text{kurt}(\mathbf{b}_j^T \mathbf{y})) (\mathbb{E}[\mathbf{y}(\mathbf{b}_j^T \mathbf{y})^3] - 3\mathbf{y} \mathbb{E}[(\mathbf{b}_j^T \mathbf{y})^2]) \quad (3.12)$$

As $\mathbb{E}[(\mathbf{b}_j^T \mathbf{y})^2] = \|\mathbf{y}\|^2$ for whitened data the corresponding term does only affect the norm of \mathbf{b}_j within the gradient algorithm. Thus, as it is only the direction that is of interest, this term can be omitted. Because the optimisation is restricted to the unit sphere a projection of \mathbf{b}_j onto the unit sphere must be performed in every step of the gradient method. This is done by dividing \mathbf{b}_j by its norm. This gives update step

$$\begin{aligned} \Delta \mathbf{b}_j &\propto \text{sign}(\text{kurt}(\mathbf{b}_j^T \mathbf{y})) \mathbb{E}[\mathbf{y}(\mathbf{b}_j^T \mathbf{y})^3] \\ \mathbf{b}_j &\leftarrow \mathbf{b}_j / \|\mathbf{b}_j\| \end{aligned}$$

The expectation operator can be omitted in order to achieve an adaptive version of the algorithm, now using every measurement \mathbf{y} . However, the expectation operator from the definition of kurtosis can not be omitted and must therefore be estimated. This can be done by a time-average estimate, denoted as γ and serving as the learning rate of the gradient method.

$$\Delta\gamma \propto ((\mathbf{b}_j^T \mathbf{y})^4 - 3) - \gamma$$

3.4.5 Basic ICA algorithm

Algorithm 3 combined the above theory, to give an overview of the ICA procedure. Estimating the mixing matrix and the corresponding independent components, from the given measurements.

Algorithm 3 Basis ICA

```

1: procedure PRE-PROCESSING( $\mathbf{y}$ )
2:   Center measurements  $\mathbf{y} \leftarrow \mathbf{y} - \bar{\mathbf{y}}$ 
3:   Whitening  $\mathbf{y} \leftarrow \mathbf{y}_{white}$ 
4: end procedure
5:
6: procedure ICA( $\mathbf{y}$ )
7:    $k = 0$ 
8:   Initialise random vector  $\mathbf{b}_{j(k)}$  ▷ unit norm
9:   Initialise random value  $\gamma_{(k)}$ 
10:  for  $j \leftarrow 1, 2, \dots, N$  do
11:    while convergence critia not meet do
12:       $k = k + 1$ 
13:       $\mathbf{b}_{j(k)} \leftarrow \text{sign} \gamma_{(k-1)} \mathbf{y} (\mathbf{b}_{j(k-1)}^T \mathbf{y})^3$ 
14:       $\mathbf{b}_{j(k)} \leftarrow \mathbf{b}_{j(k)} / \|\mathbf{b}_{j(k)}\|$ 
15:       $\gamma_{(k)} \leftarrow ((\mathbf{b}_{j(k)}^T \mathbf{y})^4 - 3) - \gamma_{(k-1)}$ 
16:    end while
17:     $x_j = \mathbf{b}_{j(k)}^T \mathbf{y}$ 
18:  end for
19: end procedure

```

3.4.6 ICA for sparse signal recovery

ICA is widely used within sparse signal recovery. When ICA is applied to a measurement vector $\mathbf{y} \in \mathbb{R}^M$ it is possible to separate the mixed signal into M or less independent components. However, by assuming that the independent components makes a k -sparse signal it is possible to apply ICA within sparse signal recovery of cases where $M < N$ and $k \leq M$.

To apply ICA to such case the independent components are obtained by the pseudo-inverse solution

$$\hat{\mathbf{x}} = \mathbf{A}_S^\dagger \mathbf{y}$$

where \mathbf{A}_S is derived from the dictionary matrix \mathbf{A} by containing only the columns associated with the non-zero entries of \mathbf{x} , specified by the support set S .

henvis til appendix

3.5 Limitations of compressive sensing

Through this chapter the concept of sparse signal recovery have been explained. It is seen that to recover the a sparse signal from the

The essential limitation of signal recovery from an under-determined system is that $k \leq M$ is necessary in order to uniquely recover the k -sparse signal $\mathbf{X} \in \mathbb{R}^N$ from the measurements $\mathbf{Y} \in \mathbb{R}^M$. That is the number of measurements must be greater than the number of active sources within the signal to be recovered. Similarly it is not possible to recover the true dictionary \mathbf{A} by dictionary learning methods if $k > M$. Because in that case any random dictionary of full rank can be used to create \mathbf{y} from $\geq M$ basis vectors[5, p. 30].

When considering source recovery from EEG measurements, described in section 1.1, it is not reasonable to assume that $k < M$ especially not in the case of low density EEG measurements. This motives the next two chapters where the possibility of sources recovery for $k > M$ is explored. The methods, proposed recently by O. Balkan, are taking advantage of the covariance domain and..

skal dette argumenteres yderligere, som værende uafhængig af motivations kapitlet?

Chapter 4

Covariance-Domain Dictionary Learning

The section is inspired by chapter 3 in [5] and the article [3]. INTRO..

4.1 Introduction

Covariance-domain dictionary learning (Cov-DL) is an algorithm proposed by O. Balkan [3], claiming to successfully identify more active sources k than available measurements M from the multiple measurement vector model

$$\mathbf{Y} = \mathbf{A}\mathbf{X} + \mathbf{E}.$$

where $\mathbf{Y} \in \mathbb{R}^{M \times L}$ is the observed measurement matrix, $\mathbf{X} \in \mathbb{R}^{N \times L}$ the the source matrix and $\mathbf{E} \in \mathbb{R}^{M \times L}$ is the additional noise matrix .

Let f be the sample frequency of the observed data \mathbf{Y} and let s denoted a segment index. As such the observed data can be divided into segments $\mathbf{Y}_s \in \mathbb{R}^{M \times t_s f}$, possibly overlapping, where t_s is the length of the segments in seconds. For each segment the linear model still holds and is rewritten into

$$\mathbf{Y}_s = \mathbf{A}\mathbf{X}_s + \mathbf{E}_s, \quad \forall s.$$

Cov-DL takes advantage of the covariance domain where the dimensionality is increased allowing for an enlarged number of sources to be active while the dictionary remains recoverable. An important aspect of this method is the prior assumption that the sources within one segment are uncorrelated, that is the rows of \mathbf{X}_s being mutually uncorrelated. From the assumption of uncorrelated sources it can be assumed that the sample covariance of \mathbf{X}_s becomes nearly diagonal. This is of importance when the system is transformed to the covariance domain.

f er samples pr sek., L er antal sampels i alt, L_s er antal samples pr segment og t_s er længen pr segment i sekunder

The Cov-DL do only recover the mixing matrix \mathbf{A} given the measurements \mathbf{Y} . Given \mathbf{A} the source matrix \mathbf{X} is to be recovered by use of the Multiple Sparse Bayesian Learning algorithm, this is described in section 5

4.2 Covariances domain representation

Consider the covariance of a vector \mathbf{x}_i

$$\mathbf{\Sigma} = \mathbb{E}[(\mathbf{x}_i - \mathbb{E}[\mathbf{x}_i])(\mathbf{x}_i - \mathbb{E}[\mathbf{x}_i])^T].$$

Assume that all samples has zero mean and the same distribution within one segment. The observed measurements $\mathbf{Y}_s \in \mathbb{R}^{M \times L}$ can be described in the covariance domain by the sample covariance $\hat{\mathbf{\Sigma}}$ which is defined as the covariance among the M measurements across the L_s samples. That is a $M \times M$ matrix $\mathbf{\Sigma}_{\mathbf{Y}_s} = [\sigma_{jk}]$ with entries

$$\sigma_{jk} = \frac{1}{L} \sum_{i=1}^L y_{ji} y_{ki}^T.$$

Using matrix notation the sample covariance of \mathbf{Y}_s can be written as

$$\hat{\mathbf{\Sigma}}_{\mathbf{Y}_s} = \frac{1}{L} \mathbf{Y}_s \mathbf{Y}_s^T.$$

Similar the source matrix \mathbf{X}_s can be described in the covariance domain by the sample covariance matrix

$$\hat{\mathbf{\Sigma}}_{\mathbf{X}_s} = \frac{1}{L} \mathbf{X}_s \mathbf{X}_s^T = \mathbf{\Lambda}_s + \boldsymbol{\varepsilon}$$

From the assumption of uncorrelated sources within \mathbf{X}_s the sample covariance matrix is expected to be nearly diagonal, thus it can be written as $\mathbf{\Lambda}_s + \boldsymbol{\varepsilon}$ where $\mathbf{\Lambda}_s$ is a diagonal matrix consisting of the diagonal entries of $\hat{\mathbf{\Sigma}}_{\mathbf{X}_s}$ and $\boldsymbol{\varepsilon}$ is the estimation error[3].

Each segment is then modelled in the covariance domain as

$$\begin{aligned} \hat{\mathbf{\Sigma}}_{\mathbf{Y}_s} &= \frac{1}{L_s} \mathbf{Y}_s \mathbf{Y}_s^T = \frac{1}{L_s} (\mathbf{A} \mathbf{X}_s + \mathbf{E}_s) (\mathbf{A} \mathbf{X}_s + \mathbf{E}_s)^T \\ \mathbf{Y}_s \mathbf{Y}_s^T &= (\mathbf{A} \mathbf{X}_s) (\mathbf{A} \mathbf{X}_s)^T + \mathbf{E}_s \mathbf{E}_s^T + \mathbf{E}_s (\mathbf{A} \mathbf{X}_s)^T + \mathbf{A} \mathbf{X}_s \mathbf{E}_s^T \\ &= \mathbf{A} \mathbf{X}_s \mathbf{X}_s^T \mathbf{A}^T + \mathbf{E}_s \mathbf{E}_s^T + \mathbf{E}_s \mathbf{X}_s^T \mathbf{A}^T + \mathbf{A} \mathbf{X}_s \mathbf{E}_s^T \\ &= \mathbf{A} (\mathbf{\Lambda}_s + \boldsymbol{\varepsilon}) \mathbf{A}^T + \mathbf{E}_s \mathbf{E}_s^T + \mathbf{E}_s \mathbf{X}_s^T \mathbf{A}^T + \mathbf{A} \mathbf{X}_s \mathbf{E}_s^T \\ &= \mathbf{A} \mathbf{\Lambda}_s \mathbf{A}^T + \mathbf{A} \boldsymbol{\varepsilon} \mathbf{A}^T + \mathbf{E}_s \mathbf{E}_s^T + \mathbf{E}_s \mathbf{X}_s^T \mathbf{A}^T + \mathbf{A} \mathbf{X}_s \mathbf{E}_s^T \end{aligned} \quad (4.1)$$

$$= \mathbf{A} \mathbf{\Lambda}_s \mathbf{A}^T + \tilde{\mathbf{E}} \quad (4.2)$$

$$(4.3)$$

igere argumenta-
tievendig her?

From (4.1) to (4.2) all terms where noise is included are defined as a united noise term $\tilde{\mathbf{E}}$. By vector notation (4.2) is rewritten and then vectorised. Because the covariance matrix $\hat{\Sigma}_{\mathbf{Y}_s}$ is symmetric it is sufficient to vectorize only the lower triangular parts, including the diagonal. For this the function $\text{vec}(\cdot)$ is defined to map a symmetric $M \times M$ matrix into a vector of size $\frac{M(M+1)}{2}$ making a row-wise vectorization of its upper triangular part. Furthermore, let $\text{vec}^{-1}(\cdot)$ be the inverse function for de-vectorisation. This results in the following model

$$\begin{aligned}
 \Sigma_{\mathbf{Y}_s} &= \sum_{i=1}^N \Lambda_{s_{ii}} \mathbf{a}_i \mathbf{a}_i^T + \tilde{\mathbf{E}} \\
 \text{vec}(\Sigma_{\mathbf{Y}_s}) &= \sum_{i=1}^N \Lambda_{s_{ii}} \text{vec}(\mathbf{a}_i \mathbf{a}_i^T) + \text{vec}(\tilde{\mathbf{E}}) \\
 &= \sum_{i=1}^N \mathbf{d}_i \Lambda_{s_{ii}} + \text{vec}(\tilde{\mathbf{E}}) \\
 &= \mathbf{D} \boldsymbol{\delta}_s + \text{vec}(\tilde{\mathbf{E}}), \quad \forall s.
 \end{aligned} \tag{4.4}$$

Here $\boldsymbol{\delta}_s \in \mathbb{R}^N$ contains the diagonal entries of the source sample-covariance matrix Λ_s and the matrix $\mathbf{D} \in \mathbb{R}^{M(M+1)/2 \times N}$ consists of the columns $\mathbf{d}_i = \text{vec}(\mathbf{a}_i \mathbf{a}_i^T)$. Note that \mathbf{D} and $\boldsymbol{\delta}_s$ are unknown while $\text{vec}(\Sigma_{\mathbf{Y}_s})$ is known from the observed data. By this transformation to the covariance domain one segment is now represented as the single measurement model with $M(M+1)/2$ "measurements". It has been shown that this model allow for identification of $k \leq M(M+1)/2$ active sources [16], which is a much weaker sparsity constraint than the original sparsity constraint $k \leq M$. The purpose of the Cov-DL algorithm is to leverage this model to find the dictionary \mathbf{A} from \mathbf{D} and then still allow for $k \leq M(M+1)/2$ active sources to be identified. That is the number of active sources are allowed to exceed the number of observations as intended.

4.3 Determination of the Dictionary

The goal is now to learn first \mathbf{D} and then the associated mixing matrix \mathbf{A} . Two methods are considered relying on the relation of M and N .

Cov-DL1 – under-determined \mathbf{D}

In the case of $N > \frac{M(M+1)}{2}$ \mathbf{D} becomes under-determined. This is similar to the original system being under-determined when $N > M$. Thus, it is again possible to solve the under-determined system if certain sparsity is withhold. Namely $\boldsymbol{\delta}_s$ being $\frac{M(M+1)}{2}$ -sparse. Assuming the sufficient sparsity on $\boldsymbol{\delta}_s$ is withhold it is possible to learn the dictionary matrix of the covariance domain \mathbf{D} by traditional dictionary learning methods applied to the observations represented in the covariance domain

$\text{vec}(\mathbf{\Sigma}_{\mathbf{Y}_s})$ for all s . For this K-SVD algorithm, described in section 3.3 is used. Note here that the number of samples that are used to learn the dictionary is remarkable reduces as one segment effectively corresponds to one sample in the covariance domain.

When \mathbf{D} is learned it is possible to find the original mixing matrix \mathbf{A} that generated \mathbf{D} through the relation $\mathbf{d}_i = \text{vec}(\mathbf{a}_i \mathbf{a}_i^T)$. Here each column is found by the optimisation problem

$$\min_{\mathbf{a}_i} \|\text{vec}^{-1}(\mathbf{d}_i) - \mathbf{a}_i \mathbf{a}_i^T\|_2^2,$$

for which the global minimizer is $\mathbf{a}_i^* = \sqrt{\lambda_i} \mathbf{b}_i$. Here λ_i is the largest eigenvalue of $\text{vec}^{-1}(\mathbf{d}_i)$,

$$\text{vec}^{-1}(\mathbf{d}_i) = \begin{bmatrix} d_{11} & d_{12} & \cdots & d_{1N} \\ d_{21} & d_{22} & \cdots & d_{2N} \\ \vdots & \vdots & \ddots & \vdots \\ d_{N1} & d_{N2} & \cdots & d_{NN} \end{bmatrix}, \quad i \in [N]$$

and \mathbf{b}_i is the corresponding eigenvector.

Cov-DL2 – undercomplete \mathbf{D}

In the case of $N < \frac{M(M+1)}{2}$ an over-determined system is achieved and it is not possible to find \mathbf{D} by dictionary learning methods.

By assuming that $\frac{M(M+1)}{2}$ will be close to N , because $N > M$ is given, then the measurements in the covariance domain $\text{vec}(\mathbf{\Sigma}_{\mathbf{Y}_s})$ will live on or near a subspace of dimension N . This subspace is spanned by the columns of \mathbf{D} , and is denoted as (\mathbf{D}) . To learn $\mathcal{R}(\mathbf{D})$ without having to impose any sparsity constraint on δ_s it is possible to use Principal Component Analysis (PCA). By use of PCA a set of basis vectors \mathbf{U} is achieved such that $\mathcal{R}(\mathbf{U}) = \mathcal{R}(\mathbf{D})$. This however do not imply that $\mathbf{D} = \mathbf{U}$.

In the case of two sets of basis vectors span the same space, namely $\mathcal{R}(\mathbf{U}) = \mathcal{R}(\mathbf{D})$, the projection operator of the given subset must be unique. Which is true if and only if $\mathbf{D}(\mathbf{D}^T \mathbf{D})^{-1} \mathbf{D}^T = \mathbf{U}(\mathbf{U}^T \mathbf{U})^{-1} \mathbf{U}^T$. Remember from the above derivation the condition that $\mathbf{d}_i = \text{vec}(\mathbf{a}_i \mathbf{a}_i^T)$. From this it is possible to obtain \mathbf{A} through the optimisation problem

$$\begin{aligned} \min_{\mathbf{a}_i} \|\mathbf{D}(\mathbf{D}^T \mathbf{D})^{-1} \mathbf{D}^T - \mathbf{U}(\mathbf{U}^T \mathbf{U})^{-1} \mathbf{U}^T\|_F^2 \\ \text{s.t. } \mathbf{d}_i = \text{vec}(\mathbf{a}_i \mathbf{a}_i^T) \end{aligned}$$

where \mathbf{U} is learned by use of PCA performed on $\text{vec}(\mathbf{\Sigma}_{\mathbf{Y}_s})$.

To solve this optimization problem the gradient of the cost function is computed with respect to \mathbf{A} by use of the chain rule

...

then the cost function is minimized by use of quasi-Newton optimization methods

redegørelse for resultatet her skal laves

how else can they live on the same space??

evt. teoretisk beskrivelse af PCA i appendix?

kilde foruden phd p. 51?

4.3.1 Pseudo Code of the Cov-DL Algorithm

Algorithm 4 Cov-DL

```

1: procedure COV-DL( $\mathbf{Y}_s$ )
2:   for  $s \leftarrow 1, \dots, n\_seg$  do
3:     compute sample covariance matrix  $\widehat{\Sigma}_{\mathbf{Y}_s}$ 
4:      $\mathbf{y}_{cov_s} = \text{vec}(\widehat{\Sigma}_{\mathbf{Y}_s})$ 
5:   end for
6:    $\mathbf{Y}_{cov} = \{\mathbf{y}_{cov_s}\}_{s=1}^{n\_seg}$ 
7:   if  $N > \frac{M(M+1)}{2}$  then
8:     procedure K-SVD( $\mathbf{Y}_{cov}$ )
9:       returns  $\mathbf{D} \in \mathbb{R}^{M(M+1)/2 \times N}$ 
10:    end procedure
11:    for  $i \leftarrow 1, \dots, N$  do
12:       $\mathbf{T} = \text{vec}^{-1}(d_i)$ 
13:       $\lambda_i \leftarrow \max\{\text{eigenvalue}(\mathbf{T})\}$ 
14:       $\mathbf{b}_i \leftarrow \text{eigenvector}(\lambda_i)$ 
15:       $\mathbf{a}_i \leftarrow \sqrt{\lambda_i} \mathbf{b}_i$ 
16:    end for
17:     $\mathbf{A} = \{\mathbf{a}_i\}_{i=1}^N$ 
18:  end if
19:  if  $N < \frac{M(M+1)}{2}$  then
20:    ...
21:  end if
22: end procedure

```

4.3.2 Remarks to be considered and investigated in the code

- the number of samples for dictionary learning is reduced remarkably when Cov-DL is used, this is mentioned above. increasing overlap will improved this.
- the effect of the length of segments L_s . it will effect the diagonality of $cov(X)$
- the values of the individual sources must not be constant over time, that is the power of the sourced, it will not be at problem for EEG data.
- for Cov-DL2 the solution tends to be unique when $M < N < M(M+1)/2$, that is the found cost function may have a local minima. for this it is recommended to use several random initial point.

Chapter 5

Multiple Sparse Bayesian Learning

INTRODUCTION!!!!

For the multiple measurement vector model (MMV)

$$\mathbf{Y} = \mathbf{A}\mathbf{X} + \mathbf{E},$$

the unknown matrices $\mathbf{A} \in \mathbb{R}^{M \times N}$ and $\mathbf{X} \in \mathbb{R}^{N \times L}$ are wished recovered from the known measurement matrix $\mathbf{Y} \in \mathbb{R}^{M \times L}$ with $M < N$. In chapter 4 the mixing matrix \mathbf{A} was found. In this chapter, a method to recover the source matrix \mathbf{X} is sought. A way to do this is to find the support set S of the non-zeros rows k (the active sources) of \mathbf{X} which corresponds to localisation of the active and non-active sources. The chapter is inspired by [23] and the articles [25], [4].

5.1 Maximum a Posterior Estimation

A possible solution to recover \mathbf{X} with the knowledge of \mathbf{A} and \mathbf{Y} is by finding its estimate, e.g. from the maximum a posterior (MAP) with a prior which induce the wanted sparsity of \mathbf{X} . By maximising the likelihood $p(\mathbf{Y}|\mathbf{X})$ a solution for an estimate of \mathbf{X} is achieved when more sources than sensors are presented in the MMV model. But it is not always the case where \mathbf{X} has a smaller dimensionality than \mathbf{Y} because of the wanted sparsity of \mathbf{X} leading to a matrix of greater dimensionality because of the added zeros. Hence the estimation becomes complicate as the MMV model becomes under-determined – an infinitely number of solutions with equal likelihoods.

As the optimisation problem of the MMV model is NP-hard another estimation method must be used.

when? er det et krav.
måske vi skal præcisere
at vi ønsker et estimat
for $k > m$

indsæt her hvad tanken
bag Bayesian egentlig er

Bayesian probability ... With this Bayesian framework the source matrix \mathbf{X} seen as a variable can be drawn from some distribution $p(\mathbf{X})$ such that the infinitely solution space is narrowed.

E.g. \mathbf{X} could be drawn from a Gaussian prior with zero-mean and covariance $\sigma_X^2 \mathbf{I}$ where the additional noise \mathbf{E} is independently Gaussian with covariance $\sigma_E^2 \mathbf{I}$. The MAP estimator could then be rewritten to

$$\hat{\mathbf{X}} = \arg \max_{\mathbf{X}} p(\mathbf{Y}|\mathbf{X})p(\mathbf{X}) = \mathbf{A}^T (\lambda \mathbf{I} + \mathbf{A}\mathbf{A}^T)^{-1} \mathbf{Y},$$

with $\lambda = \sigma_E^2 / \sigma_X^2$. With this distribution the estimate of the source matrix $\hat{\mathbf{X}}$ would have a large number of small non-zero coefficients.

By applying an exponential function $\exp(-(\cdot))$ transformation onto our optimisation problem a Gaussian likelihood function $p(\mathbf{Y}|\mathbf{X})$ with a λ -dependent variance is achieved:

$$p(\mathbf{Y}|\mathbf{X}) \propto \exp\left(-\frac{1}{\gamma} \|\mathbf{Y} - \mathbf{A}\mathbf{X}\|_2^2\right),$$

with a prior distribution $p(\mathbf{X}) \propto \exp(-\|\mathbf{X}\|_0)$ [23, p. 137]. The MAP estimation problem is then rewritten to

$$\begin{aligned} \hat{\mathbf{X}} &= \arg \max_{\mathbf{X}} p(\mathbf{Y}|\mathbf{X})p(\mathbf{X}) \\ &= \arg \max_{\mathbf{X}} \frac{p(\mathbf{Y}|\mathbf{X})p(\mathbf{X})}{p(\mathbf{Y})} \quad (\text{Bayes Formular}) \\ &= \arg \max_{\mathbf{X}} p(\mathbf{X}|\mathbf{Y}). \end{aligned}$$

5.2 Empirical Bayesian Estimation

From earlier MAP estimation approaches some problems occurs when using a fixed and algorithm-dependent prior as the posterior is not sparse enough if a prior is not as sparse leading to a non-recovery . In other cases the prior can become to sparse and then lead to a combinatorial problem when looking for the global optima.

By using automatic relevance determination (ARD) the problem of using sparse prior can be overcome. ARD is a method where a prior is introduced to determine the relevance of a parameter. The rest will become zero. This can also be view as a regularisation of the solution space which has been narrowed because of the prior and only consist of the relevance information [24].

An empirical prior can be used with ARD as the empirical prior is flexible and dependent on the unknown hyperparameter γ and therefore more data-dependent – the prior can be controlled to induce sparsity.

Let $p(\mathbf{Y}|\mathbf{X})$ be a Gaussian prior with a known noise variance σ^2 . Then for each columns in \mathbf{Y} and \mathbf{X} the likelihood is written as

$$\begin{aligned} p(\mathbf{y}_{\cdot j}|\mathbf{x}_{\cdot j}) &= \mathcal{N}(\mathbf{A}\mathbf{x}_{\cdot j}, \sigma^2\mathbf{I}) \\ &= (2\pi\sigma^2)^{-N/2} \exp\left(-\frac{1}{2\sigma^2}\|\mathbf{y}_{\cdot j} - \mathbf{A}\mathbf{x}_{\cdot j}\|_2^2\right). \end{aligned}$$

With the used of ARD the i -th row of the sources matrix \mathbf{X} , $\mathbf{x}_{i\cdot}$, is assigned an L -dimensional independent Gaussian prior with zero mean and a variance controlled by γ_i which is unknown:

$$p(\mathbf{x}_{i\cdot}; \gamma_i) = \mathcal{N}(0, \gamma_i\mathbf{I}).$$

By combing the row priors

$$p(\mathbf{X}; \gamma) = \prod_{j=1}^L p(\mathbf{x}_{\cdot j}; \gamma_j),$$

a full prior of \mathbf{X} is achieved with the hyperparameter vector $\gamma = [\gamma_1, \dots, \gamma_M]^T$. By combining the full prior and the likelihood $p(\mathbf{y}_{\cdot j}|\mathbf{x}_{\cdot j})$ the posterior of the j -th column of the source matrix \mathbf{X} is defined as

$$p(\mathbf{x}_{\cdot j}|\mathbf{y}_{\cdot j}; \gamma) = \frac{p(\mathbf{x}_{\cdot j}, \mathbf{y}_{\cdot j}; \gamma)}{\int p(\mathbf{x}_{\cdot j}, \mathbf{y}_{\cdot j}; \gamma) d\mathbf{x}_{\cdot j}} = \mathcal{N}(\boldsymbol{\mu}_{\cdot j}, \boldsymbol{\Sigma}),$$

with the mean and covariance given as

$$\boldsymbol{\Sigma} = \text{Cov}(\mathbf{x}_{\cdot j}|\mathbf{y}_{\cdot j}; \gamma) = \boldsymbol{\Gamma} - \boldsymbol{\Gamma}\mathbf{A}^T (\sigma^2\mathbf{I} + \mathbf{A}\boldsymbol{\Gamma}\mathbf{A}^T)^{-1} \mathbf{A}\boldsymbol{\Gamma}, \quad \forall j = 1, \dots, L \quad (5.1)$$

$$\mathcal{M} = [\boldsymbol{\mu}_{\cdot 1}, \dots, \boldsymbol{\mu}_{\cdot L}] = \mathbb{E}[\mathbf{X}|\mathbf{Y}; \gamma] = \boldsymbol{\Gamma}\mathbf{A}^T (\sigma^2\mathbf{I} + \mathbf{A}\boldsymbol{\Gamma}\mathbf{A}^T)^{-1} \mathbf{Y}, \quad (5.2)$$

where $\boldsymbol{\Gamma} = \text{diag}(\gamma)$. The posterior mean is the point estimate for \mathbf{X} without involving the support set S .

The row sparsity is achieved whenever $\gamma_i = 0$ leading to that the posterior must have the following probability

$$P(\mathbf{x}_{i\cdot} = \mathbf{0}|\mathbf{Y}; \gamma_i = 0) = 1,$$

which ensure that the posterior mean \mathcal{M} of the i -th row, $\boldsymbol{\mu}_{i\cdot}$, will be zero. Instead of estimating our source matrix \mathbf{X} we instead estimate the hyperparameter γ_i .

Each of the hyperparameters γ_i correspond to different hypothesis for the prior distribution of the underlying generation of \mathbf{Y} . Therefore the determining of γ_i must be seen as a model selection in which we can use the empirical Bayesian strategy. This evolve the task of treating the unknown source matrix \mathbf{X} as nuisance parameters and integrating them out.

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- de brugte dette ord i
phden

By integrating the unknown sources \mathbf{X} the marginal likelihood of the observed mixed data \mathbf{Y} , $p(\mathbf{Y}; \gamma)$ is achieved [23, p. 146]. By applying the $-2\log(\cdot)$ transformation the marginal likelihood function is transformed to the cost function

$$\begin{aligned}\mathcal{L}(\gamma) &= -2\log(p(\mathbf{Y}; \gamma)) = -2\log\left(\int p(\mathbf{Y}|\mathbf{X})p(\mathbf{X}; \gamma) d\mathbf{X}\right) \\ &= \log(|\sigma^2\mathbf{I} + \mathbf{A}\Gamma\mathbf{A}^T|) + \frac{1}{L} \sum_{j=1}^L \mathbf{y}_{\cdot j}^T (\sigma^2\mathbf{I} + \mathbf{A}\Gamma\mathbf{A}^T)^{-1} \mathbf{y}_{\cdot j}\end{aligned}$$

To minimise the marginal likelihood $\mathcal{L}(\gamma)$ with respect to γ the evidence maximisation (EM) algorithm can be used. The E-step of the EM algorithm is to compute the posterior moments as mention in (5.1) while the M-step is a update rule of γ_i :

$$\gamma_i^{(k+1)} = \frac{1}{L} \|\boldsymbol{\mu}_{i\cdot}\|_2^2 + \Sigma_{ii}, \quad \forall i = 1, \dots, M.$$

The M-step is very slow on large data. Instead one could use a fixed point update to fasten the convergence on large data. The fixed point updating step is achieved by taking the derivative of the marginal likelihood $\mathcal{L}(\gamma)$ with respect to γ and equating it with zero. This lead to the updating equation which can replace the one from M-step in the EM-algorithm:

$$\gamma_i^{(k+1)} = \frac{\frac{1}{L} \|\boldsymbol{\mu}_{i\cdot}\|_2^2}{1 - \gamma_i^{-1(k)} \Sigma_{ii}}, \quad \forall i = 1, \dots, M.$$

After convergence the support set S is extracted from the solution of $\hat{\gamma}$

$$S = \{i, \hat{\gamma}_i \neq 0\},$$

which give the non-zero indexes of the final posterior mean \mathcal{M}^* . The estimate for \mathbf{X} is constructed which used of the non-zero indices of \mathcal{M}^* :

$$\hat{\mathbf{X}}^* = \begin{cases} \mathbf{x}_{i\cdot} = \boldsymbol{\mu}_i^*, & i \in S \\ \mathbf{x}_{i\cdot} = \mathbf{0}, & i \notin S \end{cases}$$

Algorithm 5 M-SBL

1. Given \mathbf{Y} and a dictionary matrix \mathbf{A} .
 2. Initialise $\boldsymbol{\gamma}$, e.g $\boldsymbol{\gamma} = \mathbf{1}$.
 3. Compute the posterior moments $\boldsymbol{\Sigma}$ and \mathcal{M} .
 4. Update $\boldsymbol{\gamma}$ using EM or fixed-point.
 5. Repeat step 3 and 4 until convergence to a fixed point $\boldsymbol{\gamma}^*$.
 6. Update the posterior moments $\boldsymbol{\Sigma}^*$ and \mathcal{M}^* with $\boldsymbol{\gamma}^*$.
 7. Extract support set S
 8. Set source matrix estimate $\hat{\mathbf{X}}^* = \mathcal{M}_S^*$
-

Notes:

- Bayesian replace the troublesome prior with a distribution that, while still encouraging sparsity, is somehow more computationally convenient. Bayesian approaches to the sparse approximation problem that follow this route have typically been divided into two categories: (i) maximum a posteriori (MAP) estimation using a fixed, computationally tractable family of priors and, (ii) empirical Bayesian approaches that employ a flexible, parameterized prior that is ‘learned’ from the data

Bibliography

- [1] Aharon, M., Elad, M., and Bruckstein, A. “K-SVD: An Algorithm for Designing Overcomplete Dictionaries for Sparse Representation”. In: *IEEE Transactions on signal processing* Vol. 54, No. 11 (2006).
- [2] Alickovic, Emina et al. “A Tutorial on Auditory Attention Identification Methods”. In: *Front. Neurosci* 13:153 (2019).
- [3] Balkan, Ozgur, Kreutz-Delgado, Kenneth, and Makeig, Scott. “Covariance-Domain Dictionary Learning for Overcomplete EEG Source Identification”. In: *ArXiv* (2015).
- [4] Balkan, Ozgur, Kreutz-Delgado, Kenneth, and Makeig, Scott. “Localization of More Sources Than Sensors via Jointly-Sparse Bayesian Learning”. In: *IEEE Signal Processing Letters* (2014).
- [5] Balkan, Ozgur Yigit. “Support Recovery and Dictionary Learning for Uncorrelated EEG Sources”. Master thesis. University of California, San Diego, 2015.
- [6] Bech Christensen, Christian et al. “Toward EEG-Assisted Hearing Aids: Objective Threshold Estimation Based on Ear-EEG in Subjects With Sensorineural Hearing Loss”. In: *Trends Hear, SAGE* 22 (2018).
- [7] C. Eldar, Yonina and Kutyniok, Gitta. *Compressed Sensing: Theory and Application*. Cambridge University Presse, New York, 2012.
- [8] Delorme, Arnaud et al. “Blind separation of auditory event-related brain responses into independent components”. In: *PLoS ONE* 7(2) (2012).
- [9] Elad, M. *Sparse and Redundant Representations*. Springer, 2010.
- [10] Foucart, Simon and Rauhut, Hoyer. *A Mathematical Introduction to Compressive Sensing*. Springer Science+Business Media New York, 2013.
- [11] Friston, Karl J. “Functional and Effective Connectivity: A Review”. In: *BRAIN CONNECTIVITY* 1 (2011).
- [12] Friston, Karl J. “Functional integration and inference in the brain”. In: *Progress in Neurobiology* 590 1-31 (2002).

- [13] Hyvarinen, A., Karhunen, J., and Oja, E. *Independent Component Analysis*. Ed. by Haykin, Simon. John Wiley and Sons, Inc., 2001.
- [14] Makeig, Scott et al. "Blind separation of auditory event-related brain responses into independent components". In: *Proc. Natl. Acad. Sci. USA* 94 (1997).
- [15] Makeig, Scott et al. "Independent Component Analysis of Electroencephalographic Data". In: *Advances in neural information processing systems* 8 (1996).
- [16] Pal, Piya and Vaidyanathan, P. P. "Pushing the Limits of Sparse Support Recovery Using Correlation Information". In: *IEEE TRANSACTIONS ON SIGNAL PROCESSING* VOL. 63, NO. 3, Feb. (2015).
- [17] Palmer, J. A. et al. "Newton Method for the ICA Mixture Model". In: *ICASSP 2008* (2008).
- [18] Sanei, Saeid and Chambers, J.A. *EEG Signal Processing*. John Wiley and sons, Ltd, 2007.
- [19] Steen, Frederik Van de et al. "Critical Comments on EEG Sensor Space Dynamical Connectivity Analysis". In: *Brain Topography* 32 p. 643-654 (2019).
- [20] *Studies within Steering of hearing devices using EEG and Ear-EEG*. <https://www.eriksholm.com/research/cognitive-hearing-science/eeg-steering>. Accessed: 2019-10-03.
- [21] Teplan, M. "Fundamentals of EEG". In: *Measurement science review* 2 (2002).
- [22] V. Le, Quoc et al. "ICA with Reconstruction Cost for Efficient Overcomplete Feature Learning". In: *NIPS'11 International Conference on Neural Information Processing Systems P. 1017-1025* (2011).
- [23] Wipf, D. P. "Bayesian Methods for Finding Sparse Representations". PhD thesis. UNIVERSITY OF CALIFORNIA, SAN DIEGO, 2006.
- [24] Wipf, D. P. and Nagarajan, S. S. "A New View of Automatic Relevance Determination". In: *Advances in Neural Information Processing Systems 20, MIT Press* (2008).
- [25] Wipf, D. P. and Rao, B. D. "An Empirical Bayesian Strategy for Solving the Simultaneous Sparse Approximation Problem". In: *IEEE TRANSACTIONS ON SIGNAL PROCESSING* Vol. 55.No. 7 (2007).

Appendix A

Extended ICA Algorithms

This appendix provide an extension to the basic algorithm for ICA regarding the measure of non-Gaussianity and the computation method. This extended algorithm is referred to as fast ICA and is more commonly used for source separation. This is the algorithm used to apply ICA on EEG measurements for comparison within the thesis.

A.1 Fixed-Point Algorithm - FastICA

An advantage of gradient algorithms is the possibility of fast adoption in non-stationary environments due the use of all input, \mathbf{y} , at once. A disadvantage of the gradient algorithm is the resulting slow convergence, depending on the choice of γ for which a bad choice in practise can disable convergence. A fixed-point iteration algorithm to maximise the non-Gaussianity is an alternative that could be used.

Consider the gradient step derived in section 3.4.4. In the fixed point iteration the sequence of γ is omitted and replaced by a constant. This builds upon the fact that for a stable point of the gradient algorithm the gradient must point in the direction of \mathbf{b}_j , hence be equal to \mathbf{b}_j . In this case adding the gradient to \mathbf{b}_j does not change the direction and convergence is achieved.

Letting the gradient given in (3.12) be equal to \mathbf{w} and considering the same simplifications again suggests the new update step as [13, p. 179]

$$\mathbf{b}_j \leftarrow \mathbb{E}[\mathbf{y}(\mathbf{b}_j^T \mathbf{y})^3] - 3\mathbf{b}_j.$$

After the fixed point iteration \mathbf{b}_j is again divided by its norm to withhold the constraint $\|\mathbf{b}_j\| = 1$. Instead of γ the fixed-point algorithm compute \mathbf{b}_j directly from previous \mathbf{b}_j .

The fixed-point algorithm is referred to as FastICA. The algorithm has shown to converge fast and reliably, then the current and previous \mathbf{w} laid in the same direction [13, p. 179].

wiki: The fixed point is stable if the absolute value of the derivative of \mathbf{w} at the point is strictly less than 1?

A.1.1 Negentropy

An alternative measure of non-Gaussianity is the negentropy, which is based on the differential entropy. The differential entropy H of a random vector \mathbf{y} with density $p_y(\boldsymbol{\eta})$ is defined as

$$H(\mathbf{y}) = - \int p_y(\boldsymbol{\eta}) \log(p_y(\boldsymbol{\eta})) d\boldsymbol{\eta}.$$

The entropy describes the information that a random variable gives. The more unpredictable and unstructured a random variable is higher is the entropy, e.g. Gaussian random variables have a high entropy, in fact the highest entropy among the random variables of the same variance [13, p. 182].

Negentropy is a normalised version of the differential entropy such that the measure of non-Gaussianity is zero when the random variable is Gaussian and non-negative otherwise. The negentropy J of a random vector \mathbf{y} is defined as

$$J(\mathbf{y}) = H(\mathbf{y}_{\text{gaus}}) - H(\mathbf{y}),$$

with \mathbf{y}_{gaus} being a Gaussian random variable of the same covariance and correlation as \mathbf{y} [13, p. 182].

As the kurtosis is sensitive for outliers the negentropy is instead difficult to compute computationally as the negentropy require a estimate of the pdf. As such an approximation of the negentropy is needed.

To approximate the negentropy it is common to use the higher order cumulants including the kurtosis. The following approximation is stated without further elaboration, the derivation can be found in [13, p. 182].

A.1.2 Fixed-Point Algorithm with Negentropy

Maximization of negentropy by use of the fixed-point algorithm is now presented, for derivation of the fixed point iteration see [13, p. 188]. Algorithm 6 show Fast ICA using negentropy, this is the algorithm which is implemented for comparison with the source separation methods which are tested in this thesis.

Algorithm 6 Fast ICA – with negentropy

```

1: procedure PRE-PROCESSING( $\mathbf{y}$ )
2:   Center measurements  $\mathbf{y} \leftarrow \mathbf{y} - \bar{\mathbf{y}}$ 
3:   Whitening  $\mathbf{y} \leftarrow \mathbf{y}_{white}$ 
4: end procedure
5:
6: procedure FASTICA( $\mathbf{y}$ )
7:    $k = 0$ 
8:   Initialise random vector  $\mathbf{b}_{j(k)}$   $\triangleright$  unit norm
9:   for  $j \leftarrow 1, 2, \dots, N$  do
10:    while convergence critia not meet do
11:       $k = k + 1$ 
12:       $\mathbf{b}_{j(k)} \leftarrow \mathbb{E}[\mathbf{y}(\mathbf{b}_j^T \mathbf{y})] - \mathbb{E}[g'(\mathbf{b}_j^T \mathbf{y})]\mathbf{b}_j$   $\triangleright g$  defined in [13, p. 190]
13:       $\mathbf{b}_{j(k)} \leftarrow \mathbf{b}_j / \|\mathbf{b}_j\|$ 
14:    end while
15:     $x_j = \mathbf{b}_j^T \mathbf{y}$ 
16:  end for
17: end procedure

```

Appendix B

Cases

B.1 Toy Test Example, M-SDL

General Setup

Consider the linear multiple measurement vector model

$$\mathbf{Y} = \mathbf{A}\mathbf{X},$$

with $\mathbf{Y} \in \mathbb{R}^{m \times L}$ being a known measurement matrix, $\mathbf{A} \in \mathbb{R}^{m \times n}$ a known mixing matrix and $\mathbf{X} \in \mathbb{R}^{n \times L}$ being the source matrix we wish to recover in this case.

For this toy example consider a signal \mathbf{X} that is constructed as a merge of k independent signals. As such one column of \mathbf{X} is one sample containing k active signals(sources) and $n-k$ zero entries.

A random mixing matrix \mathbf{A} is generated as a random Normal distributed hence it has normalised columns:

```
A = np.random.randn(m, n)
```

The measurements \mathbf{Y} is generated as the product of \mathbf{A} and \mathbf{X} :

```
Y = np.dot(A, X)
```

The error between all the elements of the true \mathbf{X} and the recovered $\hat{\mathbf{X}}$ by using the mean square error (MSE):

$$\text{MSE} = \frac{1}{L} \sum_{i=1}^L (\mathbf{X} - \hat{\mathbf{X}}_i)^2$$

Consider now \mathbf{Y} and \mathbf{A} known then by use of the M-SDL algorithm \mathbf{X} is sought recovered as $\hat{\mathbf{X}}$. The true \mathbf{X} is then to be used for comparison.

Case 1 - $k > m$

The following variables are used:

- $m = 3$ (number of sensors)
- $n = 8$ (number of sources)
- $L = 100$ (number of samples)
- No segmentations – $\mathbf{Y} = \mathbf{A}\mathbf{X}$
- Iterations = 1000
- $k = 4$ is active sources (row-wise)

Results

The MSE of case 1 was found to be 0.141 when rounded to the nearest three decimal. For visual comparison each active source are plotted against the reconstructed source in figure ??.

Comparison of each active source in \mathbf{X} and corresponding reconstruction

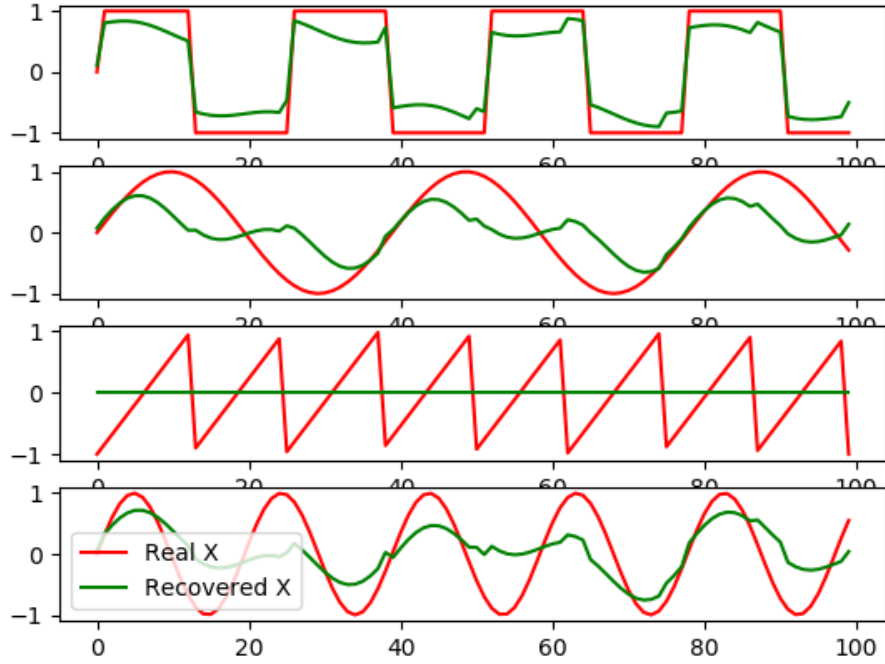


Figure B.1: Comparison of each source for $k = 4$

It is seen that one source was reconstructed as zero, that is the source was not reconstructed in the right location but in another. figure B.2 show the comparison for

one random chosen sample(row of \mathbf{X}),

For the next visualisation we look at the first 4 sources of \mathbf{X} and $\hat{\mathbf{X}}$ to see how well the estimation is.

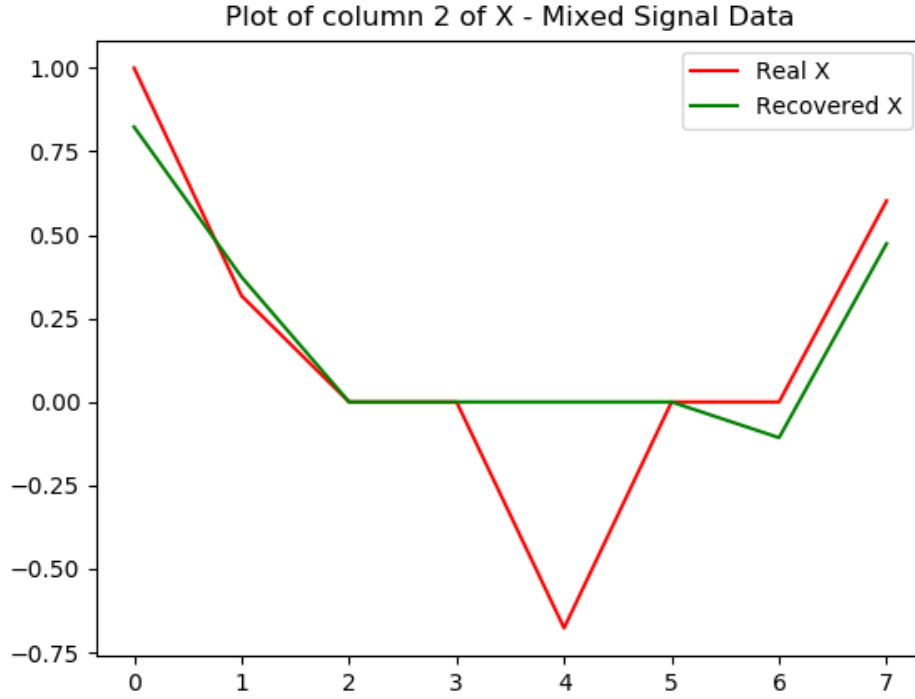


Figure B.2: comparison of a single sample

Case 2 - $k < m$

The following variables are used:

- $m = 6$ (number of sensors)
- $n = 8$ (number of sources)
- $L = 100$ (number of samples)
- No segmentations – $\mathbf{Y} = \mathbf{A}\mathbf{X}$
- Iterations = 1000
- $k = 4$ is active sources (row-wise)

Results

The MSE of case 1 was found to be 0.010 when rounded to the nearest three decimal. For visual comparison each active source are plotted against the reconstructed source in figure ??.

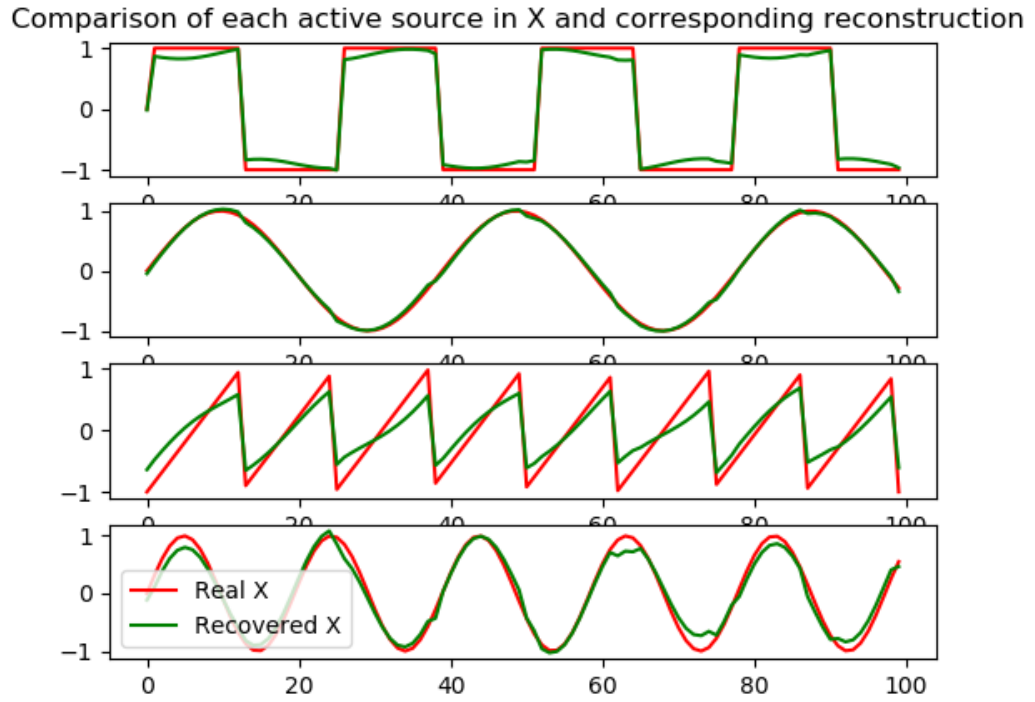


Figure B.3: Comparison of each source for $k = 4$

Figure B.4 show the comparison for one random chosen sample(row of \mathbf{X}),

For the next visualisation we look at the first 4 sources of \mathbf{X} and $\hat{\mathbf{X}}$ to see how well the estimation is.

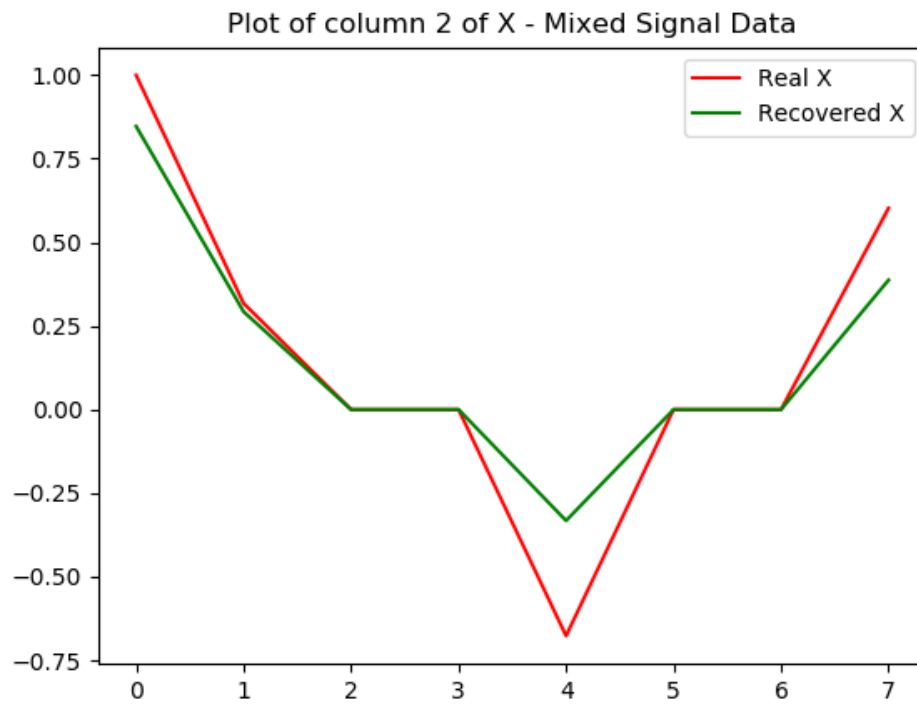


Figure B.4: comparison of a single sample

B.2 Rossler data test, M-SDL

General Setup