

# Bayesian Dictionary Learning for EEG Source Identification

Trine Nyholm Kragh & Laura Nyrup Mogensen  
Mathematical Engineering, MATTEK

Master's Thesis







**Mathematical Engineering**  
Aalborg University  
<http://www.aau.dk>

# **AALBORG UNIVERSITY**

## STUDENT REPORT

**Title:**

Bayesian Dictionary Learning for EEG  
Source Identification

**Abstract:**

Here is the abstract
----------------------

**Theme:**

**Project Period:**

Fall Semester 2019

**Project Group:**

Mattek9

**Participant(s):**

Trine Nyholm Kragh  
Laura Nyrup Mogensen

**Supervisor(s):**

Jan Østergaard

**Copies:** 1

**Page Numbers:** 13

**Date of Completion:**

September 18, 2019

*The content of this report is freely available, but publication (with reference) may only be pursued due to agreement with the author.*





**AALBORG UNIVERSITET**  
STUDENTERRAPPORT

**Matematik-Teknologi**  
Aalborg Universitet  
<http://www.aau.dk>

**Titel:**

Bayesian Bibliotek Læring for EEG Kilde  
Identifikation

**Abstract:**

Her er resuméet
-----------------

**Tema:**

**Projektperiode:**

Efterårssemestret 2019

**Projektgruppe:**

Mattek9

**Deltager(e):**

Trine Nyholm Kragh  
Laura Nyrup Mogensen

**Vejleder(e):**

Jan Østergaard

**Oplagstal: 1**

**Sidetæl: 13**

**Afleveringsdato:**

18. september 2019

*Rapportens indhold er frit tilgængeligt, men offentliggørelse (med kildeangivelse) må kun ske efter aftale med forfatterne.*



# Preface

Here is the preface. You should put your signatures at the end of the preface.

Aalborg University, September 18, 2019

---

Trine Nyholm Kragh  
<trijen15@student.aau.dk>

---

Laura Nyrup Mogensen  
<lmogen15@student.aau.dk>





# Danish Summary

Dansk resume ?



# Contents

<b>Preface</b>	<b>vii</b>
<b>Danish Summary</b>	<b>ix</b>
<b>Introduction</b>	<b>3</b>
<b>1 Problem Analysis</b>	<b>5</b>
1.1 Motivation . . . . .	5
1.2 Related Work and Our Contribution . . . . .	6
<b>2 Sparse Signal Recovery</b>	<b>7</b>
2.1 Compressive Sensing . . . . .	7
2.2 ICA . . . . .	9
2.3 Cov-DL . . . . .	9
2.4 MSB . . . . .	9
<b>Bibliography</b>	<b>11</b>
<b>A Appendix A</b>	<b>13</b>



# Introduction

Introduktion til hele projektet, skal kunne læses som en appetitvækker til resten af rapporten, det vi skriver her skal så uddybes senere. Brug dog stadigvæk kilder.

- kort intro a EEG og den brede anvendelse, anvendelse indenfor høreapparat.
- intro af model, problem med overbestemt system
- Seneste forslag til at løse dette
- vi vil efterviser dette og udvide til realtime tracking
- opbygningen af rapporten



# Chapter 1

## Problem Analysis

This chapter examines existing literature concerning source localisation from EEG measurements. At first a motivation for the problem is given, considering especially the application within the hearing aid industry. Further, the state of the art methods are presented follow by a description of the desired contribution.

### 1.1 Motivation

(Hvad er EEG)

EEG recordings or measurements are used within medicine as an imaging technique measuring electric signals on the scalp, caused by brain activity.

The brain consist of a enormous amounts of cells, called neurons. These neurons are mutually connected in neural nets and when a neuron is activated, for instance by some physical stimuli, local current flows are produced[2]. As such the neurons are somehow communicating(?).

The EEG measurements are provided by a varies number of metal electrodes referred to as sensors, places on the head surface reading the electrical signals which are masively amplified and displayed on the computer as a sum of sinusoidal waves relative to time. It takes a large amount of active neurons to generate an electrical activity that is recordable on the scalp as the current then have to penetrate the skull, skin and several other layers.

From this it is clear that the measurements from a single sensor do not correspond to the activity of a single neuron in the brain, but rather a collection of many activities. Here the same neuron activities can be measured by two or more sensors. Furthermore, interfering signals can occur resulting from physical movement of e.g. eyes and jawbone[2].

The waves resulting from EEG have been classified into four groups...use photo from EEG signal processing p. 12

(Hvad bruges det til)

(Hvad er problemet, localisation)

(Anvendelse i praksis)

evt. lave subsections her..

## **1.2 Related Work and Our Contribution**



## Chapter 2

# Sparse Signal Recovery

Through this chapter an introduction to the concept compressive sensing is described with associated theory which later on will be used in the development of the algorithm with used methods known from compressive sensing to estimate the mixing matrix  $A$  and the sparse source matrix  $X$ .

### 2.1 Compressive Sensing

Compressive sensing is the theory of efficient recover/reconstruct a signal from minimal measurements. This recovery is often described as a linear model/system

$$\mathbf{y} = \mathbf{A}\mathbf{x},$$

which consist of observed data  $\mathbf{y} \in \mathbb{R}^M$ , a matrix  $\mathbf{A} \in \mathbb{R}^{M \times N}$  which models the linear measurements and signal  $\mathbf{x} \in \mathbb{R}^N$ . In compressive sensing terminology,  $\mathbf{y}$  is the signal of interest that is wish recovered from minimal measurements meaning that the signal  $\mathbf{x}$  must be sparse.

A signal is said to be  $k$ -sparse if the signal has at most  $k$  non-zeros coefficient

$$\|\mathbf{x}\|_0 = \text{card}(\text{supp}(\mathbf{x})) \leq k,$$

where the  $\ell_0$ -norm is used. The function  $\text{card}$  is the cardinality of the support of  $\mathbf{x}$ . The support of  $\mathbf{x}$  is giving as

$$\text{supp}(\mathbf{x}) = \{j \in [N] : x_j \neq 0\},$$

where  $[N]$  a set [1, p. 41]. The set of all  $k$ -sparse signals is denoted as

$$\Sigma_k = \{\mathbf{x} : \|\mathbf{x}\|_0 \leq k\}.$$

It is of interest to recover the signal  $\mathbf{y}$  when  $M \ll N$  and  $k < M$  [3, p. 8]. This lead to that the matrix  $\mathbf{A}$  becomes rank-deficient and therefore have a non-empty

null-space [3, p. ix].

The linear model and finding the sparse signal  $\mathbf{x}$  can be written as an optimisation problem

$$\min_{\mathbf{z}} \|\mathbf{z}\|_0 \quad \text{s.t.} \quad \mathbf{y} = \mathbf{Az},$$

where  $\mathbf{z}$  is all possible candidates to an  $k$ -sparse signal  $\mathbf{x}$ .

Unfortunately, this optimisation problem is non-convex because of  $\ell_0$ -norm and is therefore difficult to solve – it is a NP-hard problem. Instead by replacing the  $\ell_0$ -norm with its convex approximation, the  $\ell_1$ -norm, the optimisation problem become computational feasible [3, p. 27]

$$\min_{\mathbf{z}} \|\mathbf{z}\|_1 \quad \text{s.t.} \quad \mathbf{y} = \mathbf{Az}, \quad (2.1)$$

and instead we find the best  $k$ -term approximation of the signal  $\mathbf{x}$ .

### 2.1.1 Conditions on the Mixing Matrix

To ensure an exact or an approximate reconstruction of the sparse signal  $\mathbf{x}$  some conditions associated on the matrix  $\mathbf{A}$  must be satisfied.

#### Null Space Conditions

The null space property (NSP) is some necessary and sufficient condition for exact recovery. The null space of the matrix  $A$  is defined as

$$\mathcal{N}(A) = \{z : Az = 0\}.$$

#### Restricted Isometry Conditions

NSP do not take account for noise and we must therefore look at some stronger conditions which incorporate noise, the following restricted isometry property (RIP)

##### Definition 2.1 (Restricted Isometry Property)

A matrix  $A$  satisfies the RIP of order  $k$  if there exists a  $\delta_k \in (0, 1)$  such that

$$(1 - \delta_k) \|x\|_2^2 \leq \|Ax\|_2^2 \leq (1 + \delta_k) \|x\|_2^2,$$

holds for all  $x \in \Sigma_k$

If a matrix  $A$  satisfy RIP then it will also satisfy the NSP as RIP is strictly stronger than NSP.

**Theorem 2.1.1**

If  $A$  satisfies the RIP of order  $2k$  with the constant  $\delta_{2k} < \sqrt{2} - 1$ . Then

$$C = \frac{2}{1 - (1 + \sqrt{2})\delta_{2k}}$$

**Coherence**

The NSP provide a unique solution to the optimisation problem, (2.1), but is unfortunately complicated to investigate. Instead an alternative measure used for sparsity is presented.

Coherence is a measure of quality and determine if the matrix  $A$  is a good choice for the optimisation problem (2.1). A small coherence describe the performance of a recovery algorithm as good with that choice of  $\mathbf{A}$ .

**Definition 2.2 (Coherence)**

Coherence of the matrix  $A \in \mathbb{R}^{M \times N}$ , denoted as  $\mu(A)$ , with columns  $\mathbf{a}_1, \dots, \mathbf{a}_N$  for all  $i \in [N]$  is given as

$$\mu(A) = \max_{1 \leq i < j \leq n} \frac{|\langle a_i, a_j \rangle|}{\|a_i\|_2 \|a_j\|_2}.$$

**2.2 ICA****2.3 Cov-DL****2.4 MSB**



# Bibliography

- [1] Simon Foucart, Hoyer Rauhut. *A Mathematical Introduction to Compressive Sensing*. Springer Science+Business Media New York, 2013.
- [2] Teplan, M. “Fundamentals of EEG”. In: *Measurement science review* 2 (2002).
- [3] Yonina C. Eldar, Gitta Kutyniok. *Compressed Sensing: Theory and Application*. Cambridge University Presse, New York, 2012.



Appendix A

Appendix A