Deep Information Theoretic Registration

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Considering a pair of intensity values a,b of a pair of images, as random variables A and B. It is possible to estimate marginal p_A, p_B and joint distributions $p_{A,B}$ by normalization of the marginal and joint histograms h(a,b) of the images:

$$\tilde{p}_{A}(a) = \sum_{b} \tilde{p}_{A,B}(a,b), \tilde{p}_{B}(b) = \sum_{a} \tilde{p}_{A,B}(a,b)$$
 (5)

with

$$\tilde{p}_{A,B}(a,b) = h(a,b) \cdot \left\{ \sum_{c,d} p_{A,B}(c,d) \right\}^{-1}$$



Figure 2. MRI image, and joint histograms before and after registration.

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Motivation

- 1. Mutual information (MI) and its variants have resulted in notable successes
- 2. Despite their strength, MI and its variants do not perform well for intermodality image registration where, e.g., one modality has "tissue contrast" while the other has "boundary contrast" (e.g., CT to ultrasound registration).

$$\hat{\beta} = \underset{\beta}{\operatorname{argmax}} \ln p(U, V; \beta, \hat{\theta}) = \underset{\beta}{\operatorname{argmax}} \sum_{i} \ln p(u_i, v_i; \beta, \hat{\theta}) .$$

Pipeline

1. The network has a 5-layer architecture consisting of strided 3D convolutions of size 3 ×3 ×3 and ReLU activation functions followed by an average pooling layer and a sigmoid.

1. Out put of the network

$$p(z=1|u,v;\theta) \doteq \sigma(f(u,v,\theta))$$
,

3. Cross entropy loss: maximum likelihood

$$\hat{\theta} = \underset{\theta}{\operatorname{argmax}} \sum_{i} \ln p(z_i | u_i, v_i; \theta) .$$

4. Construct a joint distribution on registered patches that is based on the classifier. From Bayes' rule, and noting that zi does not depend on the parameters

$$p(u_i, v_i|z_i; \theta)p(z_i) = p(z_i|u_i, v_i; \theta)p(u_i, v_i; \theta).$$

5. Taking logs and subtracting over the two cases on the value of zi

$$p(u_i, v_i|z_i; \theta)p(z_i) = p(z_i|u_i, v_i; \theta)p(u_i, v_i; \theta).$$

$$\ln p(u_i, v_i | z_i = 1; \theta) = \\ \ln p(u_i, v_i | z_i = 0; \theta) + \ln \left(\frac{p(z_i = 1 | u_i, v_i; \theta)}{p(z_i = 0 | u_i, v_i; \theta)} \right) - \ln \left(\frac{p(z_i = 1)}{p(z_i = 0)} \right) .$$

6. Sigmoid function is a logistic function, so we apply a logit transformation

$$\begin{cases} \ln p(u_i, v_i | z_i = 1; \theta) = \\ \ln p(u_i, v_i | z_i = 0; \theta) + \ln \left(\frac{p(z_i = 1 | u_i, v_i; \theta)}{p(z_i = 0 | u_i, v_i; \theta)} \right) - \ln \left(\frac{p(z_i = 1)}{p(z_i = 0)} \right) \\ p(z = 1 | u, v; \theta) \doteq \sigma(f(u, v, \theta)) \end{cases},$$

$$\ln p(u_i, v_i | z_i = 1; \theta) = \ln(p(u_i, v_i | z_i = 0; \theta)) + f(u_i, v_i; \theta) + C.$$

For the purpose of ML registration, we construct the joint distribution on patches conditioned on a transformation with parameters β as follows:

$$\begin{cases} p(u_i, v_i; \beta, \hat{\theta}) \propto p(u_i, {}^{\beta}v_i | z_i = 1; \hat{\theta}) . \\ \ln p(u_i, v_i | z_i = 1; \theta) = \ln(p(u_i, v_i | z_i = 0; \theta)) + f(u_i, v_i; \theta) + C . \end{cases}$$

$$\ln p(u_i, v_i; \beta, \hat{\theta}) = \ln p(u_i^{\beta} v_i | z_i = 0) + f(u_i, {}^{\beta} v_i) + C.$$

For the purpose of ML registration, we construct the joint distribution on patches conditioned on a transformation with parameters β as follows:

$$\ln p(u_i, v_i; \beta, \hat{\theta}) = \ln p(u_i^{\beta} v_i | z_i = 0) + f(u_i, {}^{\beta} v_i) + C.$$

$$\hat{\beta} = \underset{\beta}{\operatorname{argmax}} \sum_{i} \ln p(u_i, v_i; \beta, \hat{\theta}) \approx \underset{\beta}{\operatorname{argmax}} \sum_{i} f(u_i, {}^{\beta}v_i, \hat{\theta}) \ .$$

Iterative Maximum Likelihood

$$\hat{\beta}^{n+1} = \underset{\beta}{\operatorname{argmax}} \sum_{i} \ln p(u_i, v_i; \beta, \theta^n) \approx \underset{\beta}{\operatorname{argmax}} \sum_{i} f(u_i, {}^{\beta}v_i, \hat{\theta^n})$$

$$\hat{\theta}^{n+1} = \underset{\theta}{\operatorname{argmax}} \sum_{i} \ln p(u_i, v_i, \hat{\beta}^n, \theta) \approx \underset{\theta}{\operatorname{argmax}} \sum_{i} \ln p(z_i | u_i, \hat{\beta}^n v_i; \theta) .$$

Experiments

- 1. IXI Brain Development Dataset [17] which contains aligned T1-T2 image pairs from healthy subjects.
- 2. In the experiments, use 60 subjects for training and another 60 subjects for validation.
- 3. All images are resampled to $1 \times 1 \times 1$ mm, and their intensity is normalized between the range of [0, 1]
- 4. 3D patches, ui, vi, of size $17 \times 17 \times 17$ with labels zi = 1 or 0
- 5. Learning rate of 5×10–5, batch size of 256 and L2-regularization (weight decay) of 0.005

Data Augmentation

1. Dithering: randomly (normal distribution) moving images for mm

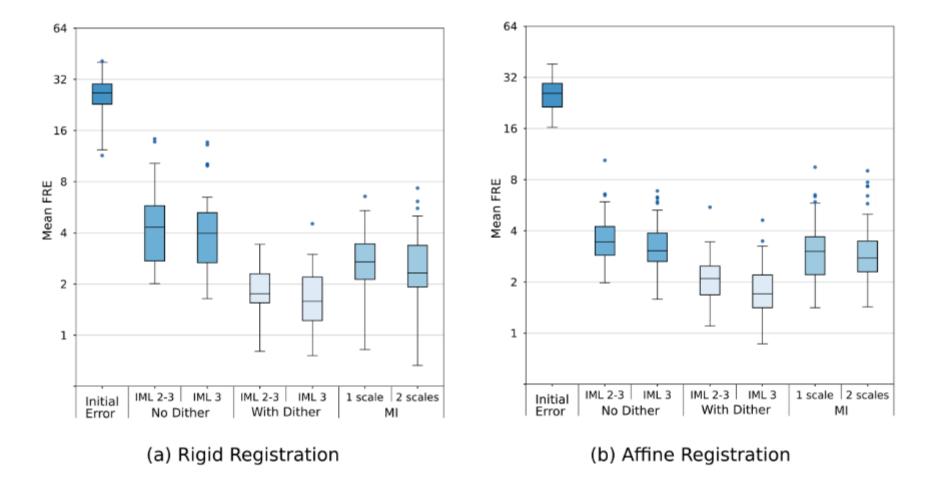


Fig. 1. Box plots of mean FRE for rigid (a) and affine (b) registration between T1 and T2 images.

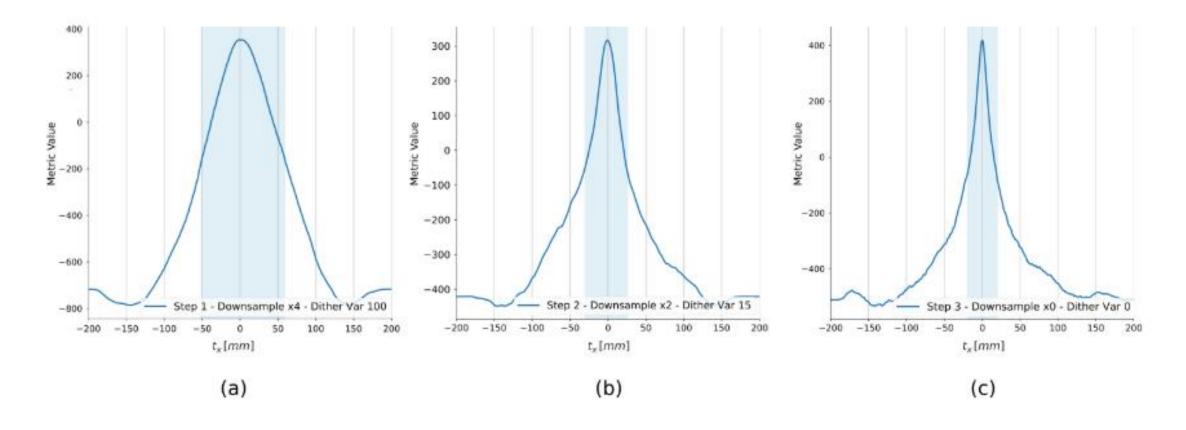


Fig. 2. Response functions for each iteration of IML for rigid registration plotted as a function of translation for a pair of registered fixed and moving images. Shading illustrates full-width half max.

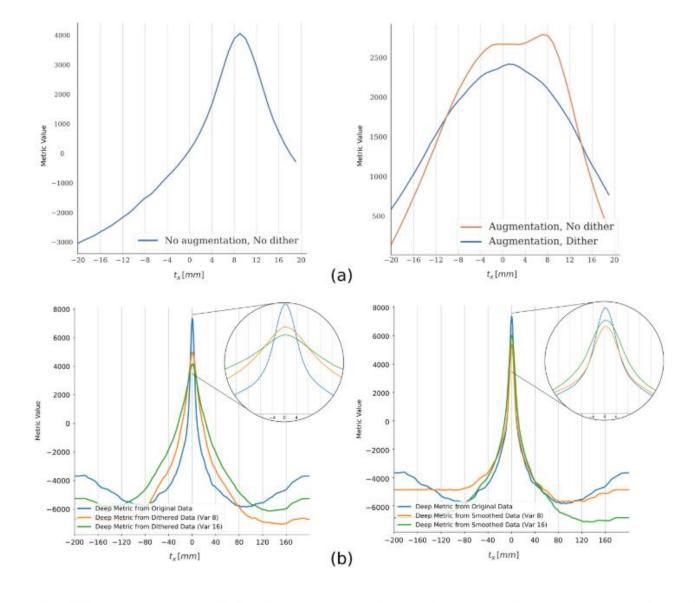


Fig. 3. (a) Characteristics of the deep metric learned from different training data. (b) Impact of dithering (left) and smoothing (right) on the deep metric response function.

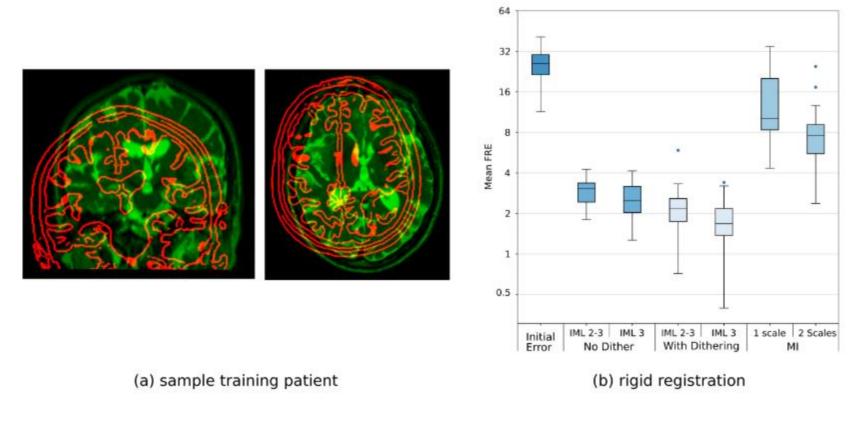


Fig. 4. (a) An example case from the edge-to-image registration experiment (b) mean FRE achieved by different methods.

Conclusions

- 1) An information theoretical (IT) foundation for iterated maximum likelihood (IML) registration with deep image metrics, DITR.
- 2) Focused on the analysis of registration objective functions rather than transformation modeling and optimization methods