# Manual
# Computation Anatomy Toolbox - CAT12

## *Quick start guide*

**VBM data**
- Segment data using defaults (for longitudinal data use longitudinal pipeline)

- Check data quality using sample homogeneity for VBM data

- Smooth data (suggested starting value 8mm)

- Estimate total intracranial volume (TIV) in order to correct for different head size and volume

- Build 2nd-level model: Use "Full factorial" for cross-sectional data and "Flexible factorial" for longitudinal data and use TIV as covariate and select threshold masking with an absolute value of 0.1.

- Estimate model

- Optionally transform and threshold SPM-maps to (log-scaled) p-maps or correlation maps

- Optionally overlay selected slices

**Additional surface data**
- Segment data and additionally select "Surface and thickness estimation" in "Writing options"

- Optionally extract additional surface parameters (e.g. suclus depth, gyrification index, cortical complexity)

- Resample and smooth surface data (suggested starting value 15mm)

- Check data quality using sample homogeneity for surface data

- Build 2nd-level model: Use "Full factorial" for cross-sectional data and "Flexible factorial" for longitudinal data

- Estimate surface model

## *Introduction and Overview*

This manual is intended to help any user to perform a computational anatomy analysis using the CAT12 Toolbox. Although it will mainly focus on voxel-based morphometry (VBM) other variants of computational analysis such as deformation-based morphometry (DBM), surface-based morphometry (SBM), and region of interest (ROI) morphometric analysis will be also introduced and can be applied with a few changes.

Basically the manual may be divided into four main sections:

- Naturally, a quick guide of how to *get started* is given at the beginning. This section provides information how to *download and install* the software and *start* the Toolbox. Furthermore, a short *overview* on the steps of a VBM analysis is given.

- A *detailed description of a basic VBM analysis* is subsequently given, which will guide the user step by step through the whole process – from preprocessing to the selection of contrasts. This description should provide all necessary information to analyze most studies successfully.

- There are a few *special cases* of VBM analyses, for which the basic analysis workflow has to be adapted. These cases are *longitudinal studies* and studies in *children or special patient populations*. Relevant changes to a basic VBM analysis are described here and a description of how to apply these changes is provided. Importantly, only the changes are described – steps like for example quality control or smoothing are the same as in the basic analysis and not described a second time.

- The manual closes with *information on native, normalized and modulated volumes*, which determines how the results may be interpreted. Furthermore an overview of the naming conventions used as well as technical information is given.

## *Getting Started*

### DOWNLOAD AND INSTALLATION

• The CAT12 Toolbox runs within SPM12. That is, SPM12 needs to be installed and added to your Matlab search path before the CAT12 Toolbox can be installed (see http://www.fil.ion.ucl.ac.uk/spm/ and http://en.wikibooks.org/wiki/SPM).

• Download (http://dbm.neuro.uni-jena.de/cat12/) and unzip the CAT12 Toolbox. You will get a folder named "cat12", which contains various matlab files and compiled scripts. Copy the folder "cat12" into the SPM12 "toolbox" folder.

### STARTING THE TOOLBOX

• Start Matlab

• Start SPM12 (i.e., type "spm fmri")

• Select "cat12" from the SPM menu (see Figure 1). You will find the drop-down menu between the "Display" and the "Help" button (you can also call the Toolbox directly by typing "cat12" on the Matlab command line). This will open the CAT12 Toolbox as additional window (Fig. 2).
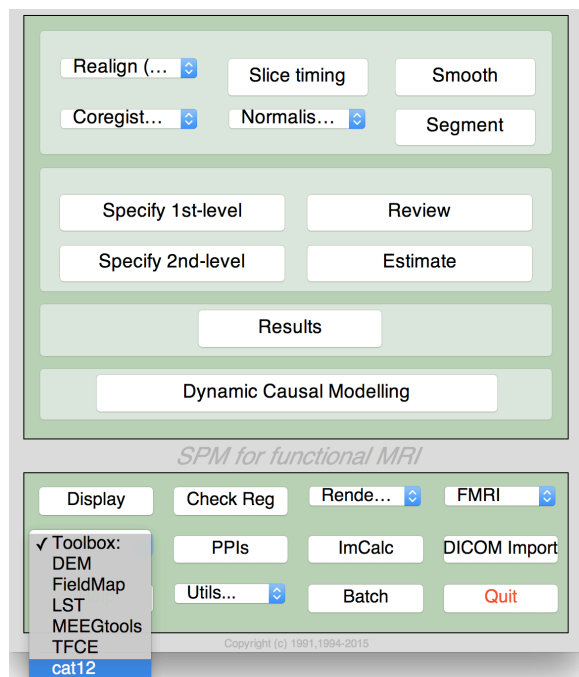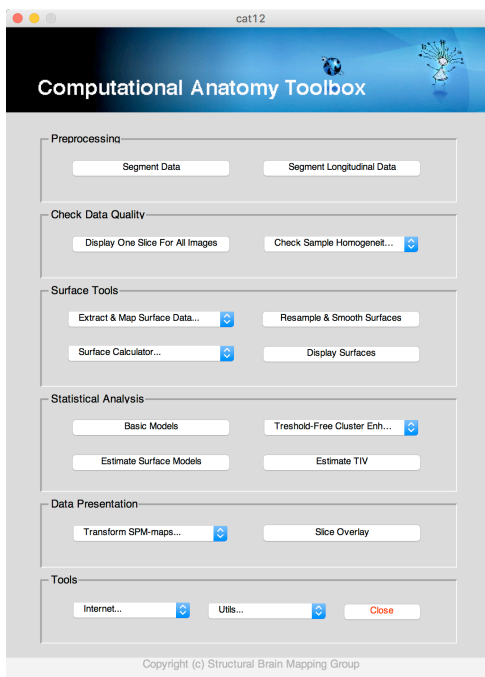


**Figure 1**: SPM menu



**Figure 2**: CAT12 Window

**BASIC VBM ANALYSIS (OVERVIEW)**
The CAT12 Toolbox comes with different modules, which may be used for an analysis. Usually, a VBM analysis comprises the following steps

**(a) Preprocessing:**

1. T1 images are **normalized** to a template space and **segmented** into gray matter (GM), white matter (WM) and cerebrospinal fluid (CSF). The preprocessing parameters can be adjusted via the module "Segment Data".

2. After the preprocessing is finished, a **quality check** is highly recommended. This can be achieved via the modules "Display one slice for all images" and "Check sample homogeneity ". Both options are located in the CAT12 window under "Check Data Quality".

3. Before entering the GM images into a statistical model, image data need to be **smoothed**. Of note, this step is not implemented into the CAT12 Toolbox but achieved via the standard SPM module "Smooth".

**(b) Statistical analysis:**

4. The smoothed GM images are entered into a statistical analysis. This requires building a statistical model (e.g., T-Tests, ANOVAs, multiple regressions). This is done by the standard SPM modules "Specify 2nd Level" or "Basic Models" in the CAT12 window covering the same function.

5. The statistical model is estimated. This is done by the standard SPM module "Estimate".

6. After estimating the statistical model, contrasts will be defined to get the results of the analysis. This is done by the standard SPM module "Results".

**The sequence of "preprocessing → quality check → smoothing → statistical analysis" remains the same for every VBM analysis, even when different steps are adapted (see "special cases").**

***A few words about the Batch Editor…***

– As soon as you select a module from the CAT12 Toolbox menu, a new window (the Batch Editor) will open. The Batch Editor is the environment where you will set up your analysis (see **Figure 3**). For example, an "<-X" indicates where you need to select files (e.g., your image files, the template, etc.). Other parameters have either default settings (which can be modified) or require input (e.g., choosing between different options, providing text or numeric values, etc.).

– Once all missing parameters are set, a green arrow will appear on the top of the window (the current snapshots in **Figure 3** show the arrow still in gray). Click this arrow to run the module or select "File → Run Batch". It is very useful to save the settings before you run the batch (click on the disk symbol or select "File → Save Batch").

– Of note, you can always find helpful information and parameter-specific explanations at the bottom of the Batch Editor window.[1]

– All settings can be saved either as .mat file or as .m script file and reloaded for later use. The .m script file has the advantage to be editable with a text editor.
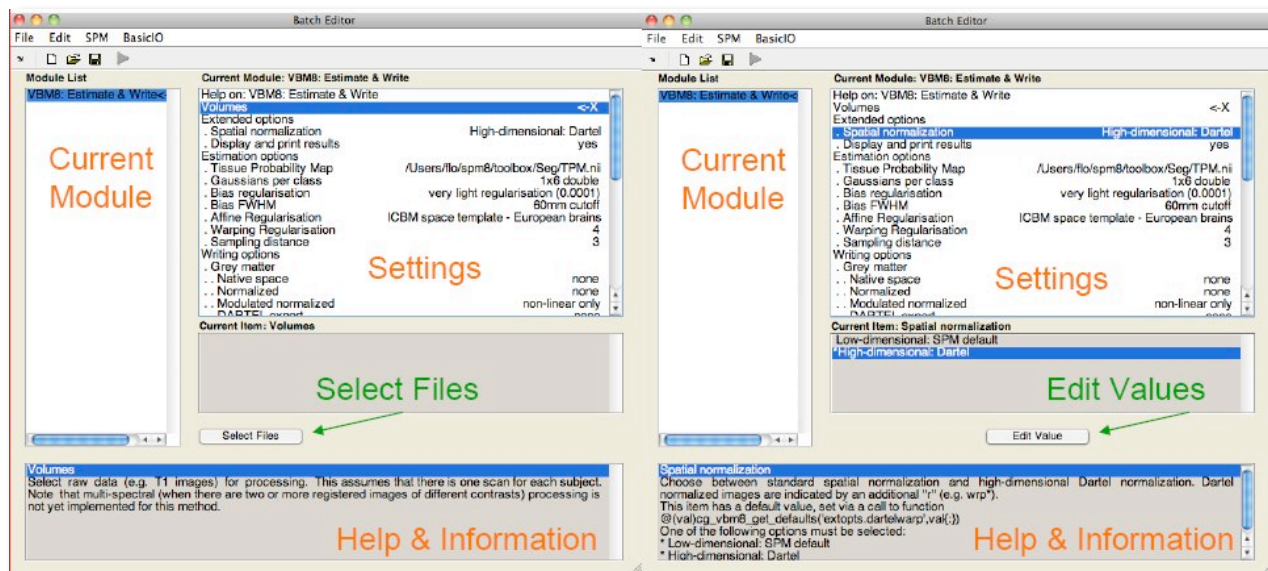


**Figure 3:** The Batch Editor is the environment where the analysis is set up. *Left*: For all settings marked with "<-X", files have to be selected ("Select Files"). *Right*: Parameters can be edited and adapted ("Edit Value").

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[1] Additional CAT12-related information can be found by selecting "VBM Website" in the CAT12 window (Tools → Internet → VBM Website"). This will open a website. Here, look for "VBM subpages" on the right.

# *Basic VBM analysis (detailed description)*

<span style="color:red">Text in preparation…
Set origin…</span>

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**SECOND MODULE: DISPLAY ONE SLICE FOR ALL IMAGES**

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CAT12 → Check data quality → Display one slice for all images

Parameters:

- o  Sample data <-X → Select Files → *[select the new files]* → Done

    - Select the newly written data [e.g. the "wm*" files, which are the normalized bias corrected volumes]. This tool will display one horizontal slice for each subject, thus giving a good overview if the segmentation and normalization procedures yielded reasonable results. For example, if the native volume had artifacts or if the native volumes had a wrong orientation, the results may look odd. Solutions: Use "Check Reg" from the SPM main menu to make sure that the native images have the same orientation like the MNI Template ("SPM → templates → T1"). Adjust if necessary using "Display" from the SPM main menu.

- o  Proportional scaling →*[use defaults or modify]*
    - Check "yes", if you display T1 volumes.
- o  Spatial orientation
- o  Show slice in mm → [use defaults or modify]

    - This module displays horizontal slices. This default setting provides a good overview.

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**THIRD MODULE: CHECK SAMPLE HOMOGENEITY**

---

CAT12 → Check data quality → Check sample homogeneity → VBM data

Parameters:

- o  Data → New: Sample data <-X → Select Files → *[select gray matter volumes]* → Done
    - Select the newly written data [e.g. the "mwp1*" files, which are the modulated (m) normalized (w) GM segments (p1)]. This tool visualizes the correlation between the volumes using a boxplot and correlation matrices. Thus, it will help identifying outliers. Any outlier should be carefully inspected for artifacts or pre-processing

errors using "Check Reg" from the SPM main menu. If you specify different samples the mean correlation is displayed in separate plots for each sample.

- ○ Load quality measures → New: XML files → *[optionally select xml-files with quality measures]*
  - Optionally select the xml-files that are saved for each data set. These files contain useful information about some estimated quality measures that can be also used for checking sample homogeneity. Please note, that the order of the xml-files must be the same as the other data files.
- ○ Separation in mm → *[use defaults or modify]*
  - To speed up calculations you can define that correlation is estimated only every x voxel. Smaller values give slightly more accurate correlation, but will be much slower.
- ○ Nuisance → *[enter nuisance variables if applicable]*
  - For each nuisance variable which you want to remove from the data prior to calculating the correlation, select "New: Nuisance" and enter a vector with the respective variable for each subject (e.g. age in years). All variables have to be entered in the same order as the respective volumes. You can also type "spm_load" to upload a *txt file with the covariates in the same order as the volumes. A potential nuisance parameter can be TIV if you check segmented data with the default modulation.

A window with a correlation matrix will open, which depict the correlation between the volumes. The correlation matrix shows the correlation between all volumes. High correlation values mean that your data are more similar to each other. If you click in the correlation matrix the corresponding data pairs will be displayed at the right bottom corner and allow a more careful inspection. The slider below the image changes the displayed slice. The popup menus at the right top corner provide more options. Here you can select other measures that are displayed in the boxplot (e.g. mean squared error or optionally quality measures if loaded), can change the order of the correlation matrix (by filename or mean correlation). Finally, the worst data can be shown in the SPM graphics window to check the data more carefully.

The boxplot in the SPM graphics window averages all correlation values for each subject and shows the homogeneity of your sample. A small overall correlation in the boxplot not always means that this volume is an outlier or contains an artifact. If there are no artifacts in the image and if the image quality is reasonable you don't have to exclude this volume from the sample. This tool is intended to utilitize the process of quality checking and there is no clear criteria defined to exclude a volume only based on the overall correlation value. However, volumes with a noticeable lower overall correlation (e.g. below two standard deviations) are indicated and should be checked more carefully.

**FOURTH MODULE: SMOOTH**

SPM menu → Smooth

> Parameters:
>
> > o Images to Smooth <-X → Select Files → *[select grey matter volumes]* → Done
> > > - Select the newly written data [e.g. the "m0wrp1" files, which are the normalized (wr) grey matter segments (p1) modulated for the non-linear components (m0)].
> >
> > o FWHM → *[use defaults or modify]*
> > > - 8-12mm kernels are widely used for VBM. To use this setting select "edit value" and type "8 8 8" (or "12 12 12", respectively) for a kernel with 8mm (with 12mm) FWHM.
> >
> > o Data Type → *[use defaults or modify]*
> >
> > o Filename Prefix → *[use defaults or modify]*

**FIFTH MODULE: ESTIMATE TOTAL INTRACRANIAL VOLUME (TIV)**

CAT12 → Statistical Analysis → Estimate TIV

> Parameters:
>
> > o XML files <-X → Select Files → *[select xml-files]* → Done
> > > - Select the xml-files in the report-folder [e.g. the "cat_*.xml"].
> >
> > o Save values → *TIV only*
> > > - This option will save the TIV values for each data set in the same order as the selected xml-files. Optionally you can also save the global values for each tissue class, which might be interesting for further analysis, but is not recommended if you are interested in only using TIV as covariate.
> >
> > o Output file → *[use defaults or modify]*

**Please note that TIV is strongly recommended to use as covariate for all VBM analysis in order to correct for different brain sizes. For deformation- or surface-based data it is not necessary.**

## *Building the statistical model*

Although there are many potential designs offered in the 2nd-level analysis I recommend to use the "Full factorial" design because it covers most statistical designs. For cross-sectional VBM data you have usually 1..n samples and optionally covariates and nuisance parameters:

| Number of factor levels | Number of covariates | Statistical Model |
|---|---|---|
| 1 | 0 | one-sample t-test |
| 1 | 1 | single regression |
| 1 | >1 | multiple regression |
| 2 | 0 | two-sample t-test |
| >2 | 0 | Anova |
| >1 | >0 | Ancova (for nuisance parameters) or Interaction (for covariates) |

**TWO-SAMPLE T-TEST**

CAT12 → Statistical Analysis → Basic Models

Parameters:

- o Directory <-X → Select Files → *[select the working directory for your analysis]* → Done
- o Design → "Two-sample t-test"
  - ▪ Group 1 scans → *Select Files → [select the smoothed grey matter volumes for group 1; following this script these will be the "sm0wp1" files]* → Done
  - ▪ Group 2 scans → *Select Files → [select the smoothed grey matter volumes for group 2]* → Done
  - ▪ Independence → Yes
  - ▪ Variance → Equal or Unequal
  - ▪ Grand mean scaling → No
  - ▪ ANCOVA → No
- o **Covariates**[*]
- o Masking
  - ▪ Threshold Masking → Absolute → *[specify value (e.g., "0.1")]*
  - ▪ Implicit Mask → Yes
  - ▪ Explicit Mask → <None>
- o Global Calculation → Omit

[*]You could specify one or many covariates (i.e., partial out the variance of specific factors when looking at group differences).
It is strongly recommended to always use total intracranial volume (TIV) as covariate if you use modulated data in VBM in order to correct for different brain sizes.
- • Covariates → New Covariate
- • Vector <-X → enter the values of the covariates (e.g., TIV and optionally age in years) in the same order as the respective file names or type "spm_load" to upload a *.txt file with the covariates in the same order as the volumes
- • Name <-X → Specify Text (e.g., "age")
- • Interactions → None
- • Centering → No centering

- o Global Normalization
  - ▪ Overall grand mean scaling → No
- o Normalization → None

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## USING THE FULL FACTORIAL MODEL (FOR A 2X2 ANOVA)

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CAT12 → Statistical Analysis → Basic Models

Parameters:

- o Directory <-X → Select Files → *[select the working directory for your analysis]* → Done
- o Design → "Full Factorial"
  - ▪ Factors → *"New: Factor; New: Factor"*
    Factor
    - • Name → *[specify text (e.g., "sex")]*
    - • Levels → 2
    - • Independence → Yes
    - • Variance → Equal or Unequal
    - • Grand mean scaling → No
    - • ANCOVA → No
    Factor
    - • Name → *[specify text (e.g., "handedness")]*
    - • Levels → 2
    - • Independence → Yes
    - • Variance → Equal or Unequal
    - • Grand mean scaling → No
    - • ANCOVA → No
  - ▪ Specify Cells → *"New: Cell; New: Cell; New: Cell; New: Cell"*
    Cell
    - • Levels → *[specify text (e.g., "1 1")]*
    - • Scans → *[select files (e.g., the smoothed GM volumes of the left-handed males)]*
    Cell
    - • Levels → *[specify text (e.g., "1 2")]*
    - • Scans → *[select files (e.g., the smoothed GM volumes of the right-handed males)]*
    Cell
    - • Levels → *[specify text (e.g., "2 1")]*
    - • Scans → *[select files (e.g., the smoothed GM volumes of the left-handed females)]*
    Cell

- Levels → *[specify text (e.g., "2 2")]*
- Scans → *[select files e.g., the smoothed GM volumes of the right-handed females)]*

- o Covariates*

- o Masking
    - Threshold Masking → Absolute → *[specify value (e.g., "0.1")]*
    - Implicit Mask → Yes
    - Explicit Mask → <None>

- o Global Calculation → Omit

- o Global Normalization
    - Overall grand mean scaling → No

- o Normalization → None

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## MULTIPLE REGRESSION (CORRELATION)

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CAT12 → Statistical Analysis → Basic Models

Parameters:

- o Directory <-X → Select Files → *[select the directory for your analysis]* → Done

- o Design → "Multiple Regression"
    - Scans → [select files (e.g., the smoothed GM volumes of all subjects)] → Done
    - Covariates → "New: Covariate"

      Covariate
      - Vector → *[enter the values in the same order as the respective file names of the smoothed GM images]*
      - Name → [specify test (e.g, "*age*")]
      - Centering → No centering
      - Intercept → Include Intercept
- o Covariates*
- o Masking
    - Threshold Masking → Absolute → *[specify value (e.g., "0.1")]*
    - Implicit Mask → Yes
    - Explicit Mask → <None>

- o Global Calculation → Omit

- o Global Normalization
    - Overall grand mean scaling → No

- o Normalization → None

**USING THE FULL FACTORIAL MODEL (FOR AN INTERACTION)**

CAT12 → Statistical Analysis → Basic Models

Parameters:

- o Directory <-X → Select Files → *[select the working directory for your analysis]* → Done
- o Design → "Full Factorial"
    - ▪ Factors → *"New: Factor"*
      Factor
        - • Name → *[specify text (e.g., "sex")]*
        - • Levels → 2
        - • Independence → Yes
        - • Variance → Equal or Unequal
        - • Grand mean scaling → No
        - • ANCOVA → No
    - ▪ Specify Cells → *"New: Cell; New: Cell"*
      Cell
        - • Levels → *[specify text (e.g., "1")]*
        - • Scans → *[select files (e.g., the smoothed GM volumes of the males)]*
      Cell
        - • Levels → *[specify text (e.g., "2")]*
        - • Scans → *[select files (e.g., the smoothed GM volumes of the females)]*
- o Covariates → "New: Covariate"
    - ▪ Covariate
        - • Vector → *[enter the values in the same order as the respective file names of the smoothed GM images]*
        - • Name → [specify test (e.g, "*age*")]
        - • Interactions → With Factor 1
        - • Centering → No centering
- o Masking
    - ▪ Threshold Masking → Absolute → *[specify value (e.g., "0.1")]*
    - ▪ Implicit Mask → Yes
    - ▪ Explicit Mask → <None>
- o Global Calculation → Omit
- o Global Normalization
    - ▪ Overall grand mean scaling → No
- o Normalization → None

**ESTIMATING THE STATISTICAL MODEL**

SPM menu → Estimate

    Parameters:

        o  Select SPM.mat <-X → Select Files → *[select the SPM.mat which you just built]* → Done

        o  Method → "Classical"

**DEFINING CONTRASTS**

SPM menu → Results → *[select the SPM.mat file]* → Done *(this opens the Contrast Manager)* → Define new contrast *(i.e., choose "t-contrast" or "F-contrast"; type the contrast name and specify the contrast by typing the respective numbers, as shown below):*

**T-contrasts:**

    a.  Simple group difference

       ⇒ Use SPM.mat from model **"2 sample T-test"**

| | |
|---|---|
| •   For Group A > Group B: | specify *"1 -1"* |
| •   For Group A < Group B: | specify *"-1 1"* |

    b.  2x2 ANOVA

       ⇒ Use SPM.mat from model "**2x2 ANOVA**"

| | |
|---|---|
| •   For left-handed males > right-handed males: | specify *"1 -1 0 0"* |
| •   For left-handed females > right-handed females: | specify *"0 0 1 -1"* |
| •   For left-handed males > left-handed females: | specify *"1 0 -1 0"* |
| •   For right-handed males > right-handed females: | specify *"0 1 0 -1"* |

<div align="center">etc.</div>

| | |
|---|---|
| •   For males > females: | specify *"1 1 -1 -1"* |
| •   For left-handers > right-handers: | specify *"1 -1 1 -1"* |

    c.  Multiple Regression (Correlation)

       ⇒ Use SPM.mat from model "**CORRELATION**"

| | |
|---|---|
| •   For positive correlation: | specify *"1"* |
| •   For negative correlation: | specify *"-1"* |

*In case that the first column in the design matrix is a constant (sample effect) you have to prepend a "0" to all contrasts (e.g. "0 1").*

d.  Interaction

⇒ Use SPM.mat from model "**INTERACTION**"
- For regression slope Group A > Group B:  specify *"0 0 1 -1"*
- For regression slope Group A < Group B:  specify *"0 0 -1 1"*

→ Done

**F-contrasts:**

If you would like to use the old SPM2 F-contrast "Effects of interest" the respective contrast vector is:

*eye(n)-1/n*

where *n* is the number of columns of interest. This F-contrast is often helpful for plotting parameter estimates of effects of interest.

**<u>Getting Results:</u>**
SPM menu → Results → *[select a contrast from Contrast Manager]* → Done
- Mask with other contrasts → No
- Title for comparison: *[use the pre-defined name from the Contrast Manager or change it]*
- P value adjustment to:
  - None (uncorrected for multiple comparisons), set threshold to 0.001
  - FDR (false discovery rate), set threshold to 0.05, etc.
  - FWE (family-wise error), set threshold to 0.05, etc.
- Extent threshold: [either use "none" or specify the number of voxels[2])

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[2] In order to *empirically* determine the extent threshold (rather than saying 100 voxels or 500 voxels, which is completely arbritrary), simply run this first without specifying an extent threshold. This will give you an output (i.e., the standard SPM glass brain with significant effects). When you click "Table" (SPM main menu) you will get a table with all relevant values (MNI coordinates, p-values, cluster size etc). Below the table you will find additional information, such as "Expected Number of Voxels per Cluster". Remember this number (this is your empirically determined extent threshold). Re-run SPM → Results etc. and specify this number when asked for the "Extent Threshold". There is also a hidden option in "CAT12 → Data presentation → Threshold and transform spmT-maps" to define the extent threshold in terms of a p-value or to use the "Expected Number of Voxels per Cluster".

## *Special Cases*

### *CAT12 for longitudinal data*

**BACKGROUND**

The majority of VBM studies are based on cross-sectional data, where one image is acquired for each subject. However, in order to track e.g. learning effects over time longitudinal designs are necessary, where additional time-points are acquired for each subject. The analysis of these longitudinal data requires a customized processing, that considers the characteristics of intra-subject analysis. While for cross-sectional data images can be processed independently for each subject longitudinal data has to be registered to the baseline image (or mean image) for each subject. Furthermore, spatial normalization is estimated for the baseline image only and applied to all images (Figure 4). Additional attention is then needed for the setup of the statistical model. The following section will therefore describe data preprocessing and model setup for longitudinal data.

Text and figure in preparation

*Fig 4.: Flow diagram for processing longitudinal data with CAT12. This figure demonstrates the steps for processing longitudinal data. After an initial realignment, the mean of the realigned images is calculated (mean) and used as reference image in a subsequent realignment. The realigned images ($ri_x$) are then corrected for signal inhomogeneities with regard to the reference mean image. Spatial normalization parameters are estimated in the next step using the segmentations of the mean image. These normalization parameters are applied to the segmentations of the bias-corrected images ($p1mri_x$). The resulting normalized segmentations ($wp1mri_x$) are finally again realigned.*

## Preprocessing of longitudinal data - overview

The CAT12 Toolbox supplies a batch for longitudinal study design. Here, for each subject the respective images need to be selected. Intra-subject realignment, bias correction, segmentation, and normalization are calculated automatically. Preprocessed images are written as wp1mr* and wp2mr* for grey and white matter respectively. To define the segmentation and normalization parameters, the defaults in cat_defaults.m are used.

**CHANGE SETTINGS FOR PREPROCESSING**

Change your working directory to "/toolbox/CAT12" in your SPM directory:
→ select "Utilities → cd" in the SPM menu and change to the respective folder.
Then type "open cg_CAT12_defaults.m" in your matlab command window. The file will open in the editor. If you are unsure how to change the values, open the module "Segment Data" in the batch editor for reference.

The most interesting parameters to change here may be:

- The Tissue Probability Maps:
    Line 16 → replace "{fullfile(spm('dir'),'toolbox','Seg','TPM.nii')}" with the path to your maps.

It is always a great idea to memorize or record the changes and change all values back to default after the Analysis.

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**PREPROCESSING OF LONGITUDINAL DATA**

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CAT12 → Segment longitudinal data

    Parameters:

-   ○  Data <-X → New: Subject →Subject →Longitudinal data for one subject →Select Files → *[select raw data]* → Done
    - Select all volumes for each subject. As the Toolbox does not support multispectral data yet (i.e., different imaging methods for the same brain, such as T1-, T2-, diffusion-weighted or CT images), it is recommended to choose a T1-weighted image.
    - Select "New: Subject" to add data for a new subject
      The data for each subject should be listed as one "subject" in the Batch Editor, i.e. there are as many subjects listed as included in the analysis.
- → For all other options you can follow the instructions for preprocessing of cross-sectional data as described before. Please note that not all writing options are available for longitudinal data.

For the naming conventions of all written files see "Naming convention of output files". The final GM segments are mwp1r*, the final WM segments are named mwp2r* if you have selected to option to modulate the data. Without modulation the leading "m" is omitted.

## Statistical analysis of longitudinal data - overview

The main interest in longitudinal studies is the common change of tissue volume over time in a group of subjects or the difference in these changes between two or more groups. The setup of the statistical model needed to assess these questions will be described on two examples. First, the case of only one group of 4 subjects with 2 time points each (e.g. normal aging) is presented. Subsequently, the case of two groups of subjects with 4 time points per subject will be described. These examples should cover most analyses – the number of time points / groups just have to be adapted. In contrast to the analysis of cross-sectional data as described before we have to use the flexible factorial model that considers that the time points for each subject are dependent data.

**STATISTICAL ANALYSIS OF LONGITUDINAL DATA IN ONE GROUP**

CAT12 → Statistical Analysis → Basic Models

Parameters:

- o Directory <-X → Select Files → *[select the working directory for your analysis]* → Done

- o Design → "Flexible Factorial"
  - ▪ Factors → *"New: Factor; New: Factor"*
    Factor
    - • Name → *[specify text (e.g., "subject")*]*
    - • Independence → Yes
    - • Variance → Equal or Unequal
    - • Grand mean scaling → No
    - • ANCOVA → No
    
    Factor
    - • Name → *[specify text (e.g., "time")]*
    - • Independence → No
    - • Variance → Equal or Unequal
    - • Grand mean scaling → No
    - • ANCOVA → No

    > *SPM is internally handling some keyword factors such as "subject" or "repl". If you use "subject" as keyword for the first factor the conditions can be easier defined by only labeling the time points as input (see below).

  - ▪ Specify Subjects or all Scans & Factors → *"Subjects"* → *"New: Subject; New: Subject; New: Subject; New: Subject;"*
    Subject
    - • Scans → *[select files (the smoothed GM volumes of the first Subject)]*
    - • Conditions → "1 2" *[for two time points]*
    
    Subject
    - - Scans → *[select files (the smoothed GM volumes of the second Subject)]*
    - - Conditions → "1 2" *[for two time points]*
    
    Subject
    - • Scans → *[select files (the smoothed GM volumes of the third Subject)]*
    - • Conditions → "1 2" *[for two time points]*
    
    Subject
    - - Scans → *[select files (the smoothed GM volumes of the fourth Subject)]*
    - - Conditions → "1 2" *[for two time points]*

  - ▪ Main effects & Interaction → *"New: Main effect"*
    Main effect
    - • Factor number → 2
    
    Main effect
    - • Factor number → 1

- o Covariates (see "basic VBM analysis (detailed description)")

- o Masking

- ▪ Threshold Masking → Absolute → *[specify value (e.g., "0.1")]*
- ▪ Implicit Mask → Yes
- ▪ Explicit Mask → <None>
- ○ Global Calculation → Omit
- ○ Global Normalization
  - ▪ Overall grand mean scaling → No
- ○ Normalization → None

---

**STATISTICAL ANALYSIS OF LONGITUDINAL DATA IN TWO GROUPS**

---

CAT12 → Statistical Analysis → Basic Models

Parameters:

- ○ Directory <-X → Select Files → *[select the working directory for your analysis]* → Done
- ○ Design → "Flexible Factorial"
  - ▪ Factors → *"New: Factor; New: Factor; New: Factor"*
    Factor
    - • Name → *[specify text (e.g., "subject")*<sup>*</sup>*]*
    - • Independence → Yes
    - • Variance → Equal
    - • Grand mean scaling → No
    - • ANCOVA → No

    Factor
    - • Name → *[specify text (e.g., "group")]*
    - • Independence → Yes
    - • Variance → Unequal
    - • Grand mean scaling → No
    - • ANCOVA → No

    Factor
    - • Name → *[specify text (e.g., "time")]*
    - • Independence → No
    - • Variance → Equal
    - • Grand mean scaling → No
    - • ANCOVA → No
  - ▪ Specify Subjects or all Scans & Factors → *"Subjects"* → *"New: Subject; New: Subject; New: Subject; New: Subject;"*
    Subject
    - • Scans → *[select files (the smoothed GM volumes of the 1st Subject of first group)]*

> [*]SPM is internally handling some keyword factors such as "subject" or "repl". If you use "subject" as keyword for the first factor the conditions can be easier defined by only labeling the time points as input (see below).

- Conditions → " [1 1 1 1; 1 2 3 4]' " *[first group with four time points]*
  <span style="color:red">*Do not forget the additional single quote! Otherwise you have to define the conditions as " [1 1; 1 2; 1 3; 1 4] "*</span>

Subject
- Scans → *[select files (the smoothed GM volumes of the 2nd Subject of first group)]*
- Conditions → " [1 1 1 1; 1 2 3 4]' " *[first group with four time points]*

Subject
- Scans → *[select files (the smoothed GM volumes of the 3rd Subject of first group)]*
- Conditions → " [1 1 1 1; 1 2 3 4]' " *[first group with four time points]*

Subject
- Scans → *[select files (the smoothed GM volumes of the 4th Subject of second group)]*
- Conditions → " [2 2 2 2; 1 2 3 4]' " *[second group with four time points]*

Subject
- Scans → *[select files (the smoothed GM volumes of the 1st Subject of second group)]*
- Conditions → " [2 2 2 2; 1 2 3 4]' " *[second group with four time points]*

Subject
- Scans → *[select files (the smoothed GM volumes of the 2nd Subject of second group)]*
- Conditions → " [2 2 2 2; 1 2 3 4]' " *[second group with four time points]*

Subject
- Scans → *[select files (the smoothed GM volumes of the 3rd Subject of second group)]*
- Conditions → " [2 2 2 2; 1 2 3 4]' " *[second group with four time points]*

Subject
- Scans → *[select files (the smoothed GM volumes of the 4th Subject of second group)]*
- Conditions → " [2 2 2 2; 1 2 3 4]' " *[second group with four time points]*

- Main effects & Interaction → *"New: Interaction; New: Main effect"*
  Interaction
  - Factor numbers → 2 3 *[Interaction between group and time]*
  Main effect
  - Factor number → 1

o Covariates (see "basic VBM analysis (detailed description)")

o Masking
  - Threshold Masking → Absolute → *[specify value (e.g., "0.1")]*
  - Implicit Mask → Yes
  - Explicit Mask → <None>

o Global Calculation → Omit

o Global Normalization

- - Overall grand mean scaling → No
  - Normalization → None

## *Altered Workflows for VBM-analyses*

### Background

For most analyses the VBM Toolbox will supply all tools needed. That is, as the new segmentation algorithm is not dependent on Tissue Probability Maps (TPMs) anymore and as predefined DARTEL-templates for healthy adults exist, most questions can be assessed using the toolbox settings. However, for some special cases such as analyses in children or special patient populations, the toolbox settings might not be optimal. For these cases the CAT12 Toolbox provides an integration into the SPM12 environment that can be used to optimize the preprocessing. In the following, we will present strategies how to deal with these special cases.

### Standard VBM preprocessing: Input, Output and where to modify

The first module of the CAT12 Toolbox ("Segment Data") processes all preprocessing steps except for the smoothing. Basically, it takes structural volumes and TPMs as input. It will then segment the data, apply a registration to MNI Space (either rigid or affine) and subsequently a non-linear deformation. The non-linear deformation parameters can be calculated via the low dimensional SPM default approach or the high dimensional DARTEL algorithm and the predefined templates. Figure 5 depicts this preprocessing workflow and highlights possibilities where to modify.

*Fig. 5: Flow-chart of the preprocessing steps within the module "Estimate and Write". Marked in red are those steps, where the preprocessing can be customized. Per default, the built-in DARTEL normalization works with the CAT12 DARTEL templates of 550 healthy adult control subjects. Affine registered tissue segments can be used to create customized DARTEL-templates, which can then be used to replace the default DARTEL template.*

## *Adapting the workflows*

### Customized tissue probability maps - overview

For data on children it will be a good idea to create customized TPMs, which reflect age and gender of the population. The TOM8 Toolbox (available via: https://irc.cchmc.org/software/tom.php) provides the means to customize these TPMs. To learn more about the TOM toolbox, see also http://dbm.neuro.uni-jena.de/software/tom/.

---

### CUSTOMIZED TISSUE PROBABILITY MAPS

---

*About the TOM8 Toolbox:*

> → *select Module "create new template"*
>
>> → *select "TOM.mat" (you will have to download this file together with the toolbox)*
>>
>> → *write priors/template as single file*
>>
>> → *for all others use default settings or modify. For "Age" either a vector or a mean age (when using the average approach) must be specified.*

*Implementation into CAT12:*

CAT12 → Segment Data

> Parameters:
>
>> o Options for initial SPM12 affine registration
>>
>>> ▪ Tissue Probability Map (→ Select your customized TPMs here)

### Customized DARTEL-template - overview

For all cases that include at least 50-100 subjects a customized DARTEL template can be created. That is, grey matter and white matter tissue segments of all subjects are used to create a mean template of the study sample. As the CAT12 toolbox writes all files needed to create these templates ("DARTEL export"), this requires only two additional steps. In order to use these newly created DARTEL-Templates with the CAT12 Toolbox, an affine registration of the DARTEL export should be used. From these affine registered segments customized DARTEL templates can then be created and used with the CAT12 module "Segment Data".

**CUSTOMIZED DARTEL-TEMPLATE**

---

Several steps are needed to create normalized tissue segments with customized DARTEL Templates. These steps can be batched using dependencies in the Batch Editor. The last step can be rerun using the customized templates, if additional output files are needed. In the first step the T1 images are segmented, and the tissue segments normalized to the Tissue Probability Maps using an affine transformation. Start with selecting the module "Segment Data".

CAT12 → Segment Data

    Parameters:

    → for all options except "writing options" use settings like for a "standard" VBM analysis.

        o   Writing Options

- "Grey Matter"→ "Modulated normalized" → "No"
- "Grey Matter"→ "DARTEL export" → "affine"
- "White Matter"→ "Modulated normalized" → "No"
- "White Matter"→ "DARTEL export" → "affine"

These settings will produce the volumes "rp1*-affine.nii" and "rp2*-affine.nii", which are the grey (rp1) and white (rp2) matter segments after affine registration. The following modules can be chosen directly in the batch editor (SPM → Tools → DARTEL Tools → Run DARTEL (create Templates), and SPM → Tools → CAT12 → CAT12: Segment Data). It makes sense to add and specify these modules together with the "Segment Data" module within the Batch Editor and to set dependencies.

SPM → Tools → Dartel Tools → Run DARTEL (create Templates)

    Parameters:

        Images → *select two times* "new: Images"

- Images: → select the "rp1*-affine.nii" files or create a dependency.
- Images: → select the "rp2*-affine.nii" files or create a dependency.

    → all other options: *use defaults or modify*

SPM → Tools → Dartel Tools → Normalise to MNI space

    Parameters:

        Dartel Template → select the final created template with the ending "_6".

        o   Select according to → "Many Subjects"

- Flow fields: → select the "u_*.nii" files or create a dependency.
  - Images: → New: Images → *select the* "rp1*-affine.nii" *files or create a dependency.*

- Images: → New: Images → *select the "rp2\*-affine.nii" files or create a dependency.*
  - ○ Preserve: → "Preserve Amount"
  - ○ Gaussian FWHM: → use defaults or modify

→ all other options: *use defaults or modify*

The thus created customized DARTEL Templates are now used in the CAT12 Toolbox after an additional registration to MNI (ICBM) space:

SPM → Tools → Dartel Tools → Run DARTEL (Population to ICBM Registration)

    Parameters:

    Dartel Template → select the final created template with the ending "\_6".

SPM → Util → Deformations

    Parameters:

    Composition → "New: Deformation Field"

- Deformation Field: → *select the* "y\_\*2mni.nii" *file from step above.*
  - ○ Output → "New: Pushforward"
    - Apply to → select all "Template" files with the ending "\_0" to "\_6".
    - Output destination → Output directory → *select directory for saving files.*
    - Field of View → Image Defined → *select final* "Template" *file with the ending* "\_6".
    - Preserve → Preserve Concentrations (no "modulation").

CAT12 → Segment Data

    Parameters:

- ○ Volumes <-X → Select the original T1 images like in the first module "Segment Data".
- ○ Extended Options for CAT12 segmentation → "Spatial normalization Template" → *Select normalized DARTEL Template "*wTemplate\*\_1.nii*"*
  - For all other options use the same settings as in the first module, or modify.
- ○ Writing Options → *select the output files just like in any standard VBM analysis:*

***How to proceed:***

All steps described above are just an adaption of the CAT12 Toolbox module "Segment Data". A subsequent smoothing is not necessary before statistics if you have used the option "Normalise to MNI space" with a defined Gaussian FWHM. As always it is a good idea to save the applied modules and to perform quality control. Here, the modules "Display one slice for all images" and "Check sample homogeneity" from the CAT12 Toolbox will be helpful.

# Other variants of computational morphometry

## Deformation-based morphometry (DBM)

**Background**

DBM is based on the application of non-linear registration procedures to spatially normalise one brain to another one. The simplest case of spatial normalisation is to correct the orientation and size of the brains. In addition to these global changes, a non-linear normalisation is necessary to minimise the remaining regional differences by means of local deformations. If this local adaptation is possible, the deformations now reveal information about the type and localization of the structural differences between the brains and can undergo subsequent analysis.

Differences between both images are minimized and are now coded in the deformations. Finally, a map of local volume changes can be quantified by a mathematical property of these deformations – the Jacobian determinant. This parameter is well known from continuum mechanics and is usually used for the analysis of volume changes in flowing liquids or gases. The Jacobian determinant allows a direct estimation of the percentage change in volume in each voxel and can be statistically analyzed (Gaser et al. 2001). This approach is also known as tensor-based morphometry because the Jacobian determinant represents such a tensor.

A deformation-based analysis can be carried out not only on the local changes in volume but also on the entire information of the deformations, which also includes the direction and strength of the local deformations (Gaser et al. 1999). Since each voxel contains three-dimensional information, a multivariate statistical test is necessary for analysis. A multivariate general linear model or Hotelling's T2 test is commonly used for this type of analysis (Gaser et al. 1999; Thompson et al. 1997).

**Additional Steps in CAT12**

CAT12 → Segment Data

       Parameters:

           o  Writing options → Jacobian determinant → *Normalized* → Yes

              -  In order to save the estimated volume changes change the writing option for the normalized Jacobian determinant to "yes".

**Changes in statistical analysis**

Follow the steps for the statistical analysis as described for VBM, select the smoothed Jacobian determinants (e.g. sxj_*.nii ) and change the following parameters:

CAT12 → Statistical Analysis → Basic Models

       Parameters:

           o  Covariates: **Don't use TIV as covariate**

           o  Masking

                ▪  Threshold Masking → **None**

                ▪  Implicit Mask → Yes

                ▪  Explicit Mask → **../spm12/tpm/mask_ICV.nii**

### Surface-based morphometry (SBM)

**Background**

Surface-based morphometry has several advantages over using volumetric data alone. For instance, brain surface meshes have been shown to increase the accuracy of brain registration compared with Talairach registration (Desai et al. 2005). Brain surface meshes also permit new forms of analyses, such as gyrification indices that measure surface complexity in 3D (Yotter et al. 2011b) or cortical thickness. Furthermore, inflation or spherical mapping of the cortical surface mesh raises the buried sulci to the surface so that mapped functional activity in these regions can be easily visualized.

*Local adaptive segmentation*

Gray matter regions with high iron concentration, like the motor cortex and the occipital regions, often have increased intensities that lead to misclassications. In addition to our adaptive MAP approach for partial volume segmentation we use an approach that allows adaptation of local intensity changes in order to deal with varying tissue contrast (Dahnke et al. 2012a).

*Cortical thickness and central surface estimation*

We use a fully automated method that allows for measurement of cortical thickness and reconstructions of the central surface in one step. It uses a tissue segmentation to estimate the white matter (WM) distance, then projects the local maxima (which is equal to the cortical thickness) to other gray matter voxels by using a neighbor relationship described by the WM distance. This projection-based thickness allows the handling of partial volume information, sulcal blurring, and sulcal asymmetries without explicit sulcus reconstruction (Dahnke et al. 2012b).

*Topological correction*

In order to repair topological defects we use a novel method that relies on spherical harmonics (Yotter et al. 2011a). First, the original MRI intensity values are used as a basis to select either a ''fill'' or ''cut'' operation for each topological defect. We modify the spherical map of the uncorrected brain surface mesh, such that certain triangles are favored while searching for the bounding triangle during reparameterization. Then, a low-pass filtered alternative reconstruction based on spherical harmonics is patched into the reconstructed surface in areas that previously contained defects.

*Spherical mapping*

A spherical map of a cortical surface is usually necessary to reparameterize the surface mesh into a common coordinate system to allow intersubject analysis. We use a fast algorithm to reduce area distortion resulting in an improved reparameterization of the cortical surface mesh (Yotter et al. 2011c).

*Spherical registration*

We have adapted the volume-based diffeomorphic Dartel algorithm to the surface (Ashburner, 2007) to work with spherical maps (Yotter et al. 2011d). We apply a multi-grid approach that uses reparameterized values of sulcal depth and shape index defined on the sphere to estimate a flow field that allows deforming a spherical grid.

**Additional Steps in CAT12**

CAT12 → Segment Data

Parameters:

- Writing options → Surface and thickness estimation → Yes

   Use projection-based thickness to estimate cortical thickness and to create the central cortical surface for the left and right hemisphere.

CAT12 → Surface Tools → Resample & Smooth Surfaces

Parameters:

- Surface Data <-X → Select the surface data (e.g. [lr]h.thickness.*)

- Smoothing Filter Size in FWHM *[use defaults or modify]*
   - 12-18mm kernels are widely used for SBM and I recommend to start with a value of 15mm.
- Split job into separate processes

   - In order to use multi-threading the CAT12 segmentation job with multiple subjects can be split into separate processes that run in the background. If you don not want to run processes in the background then set this value to 0.
   - Keep in mind that each process needs about 1.5..2GB of RAM, which should be considered to choose the right number of processes.
   - Please further note that no additional modules in the batch can be run except CAT12 segmentation. Any dependencies will be broken for subsequent modules.

**Extract optional surface parameters**

You can also extract additional surface parameters that have to be resampled and smoothed with the before mentioned tool.

CAT12 → Surface Tools → Extract & Map Surface Data → Extract Additional Surface Parameters

Parameters:

- Central Surfaces <-X → Select the central surface data (e.g. [lr]h.central.*)

- Gyrification index
   - Extract gyrification index (GI) based on absolute mean curvature. The method is described in Luders et al. NeuroImage, 29: 1224-1230, 2006.
- Cortical complexity (fractal dimension)
   - Extract Cortical complexity (fractal dimension) which is described in Yotter et al. Neuroimage, 56(3): 961-973, 2011.
   - Warning: Estimation of cortical complexity is very slow!
- Sulcus depth

- Extract sqrt-transformed sulcus depth based on the euclidean distance between the central surface and its convex hull.
- Transformation with sqrt-function is used to render the data more normally distributed.

**Changes in statistical analysis**

Follow the steps for the statistical analysis as described for VBM and change the following parameters:

CAT12 → Statistical Analysis → Basic Models

Parameters:

o Covariates: **Don't use TIV as covariate**

o Masking
  ▪ Threshold Masking → **None**
  ▪ Implicit Mask → Yes
  ▪ Explicit Mask → <none>

Do not use the "Estimate" function in the SPM window, but rather use the respective function in CAT12. This allows to overlay your results automatically onto the Freesurfer average surface:

CAT12 → Statistical Analysis → Estimate Surface Models

## *Region of interest (ROI) analysis*

Text in preparation…

## *Additional information on native, normalized and modulated volumes*

When preprocessing the images (see "First Module: Segment Data", on pages 5-6), the decision about the normalization parameters will determine the interpretation of the analysis outcomes. Please note that some of the output options are only available in the expert mode.

"**Native space**" produces tissue class images in spatial correspondence to the original data. Although this could be useful for estimating global tissue volumes (e.g., GM+WM+CSF=TIV) it is not suitable to conduct VBM analyses due to the missing voxel-wise correspondence across brains). Of note, if one is interested in these global tissue volumes in native space ("raw values"), it won't be necessary to actually output the tissue class images in native space. The "Segment Data"-function automatically generates an xml file for each subject (cat_*.xml), which contains the raw values for GM, WM, and CSF. The subject-specific values can be combined (i.e., integrated into a single text file) by using the function: CAT12 → Statistical Analysis → Estimate TIV.

"**Normalized**" produces tissue class images in spatial correspondence to the template. This is useful for VBM analyses (e.g., "concentration" of gray matter; Good et al. 2001; Neuroimage).

"**Modulated normalized**" produces tissue class images in alignment with the template, but multiplies ("modulates") the voxel values by the Jacobian determinant (i.e., linear and non-linear components) derived from the spatial normalization. This is useful for VBM analyses and allows comparing the *absolute amount of tissue* (e.g., "volume" of gray matter; Good et al. 2001; Neuroimage). Please note that by using this type of modulation you have to use TIV as covariate in order to correct for different brain sizes.

If you use the expert mode you can optionally choose to modulate your data for non-linear terms only. This produces tissue class images in alignment with the template, but multiplies the voxel values by the non-linear components only. This is useful for VBM analyses and allows comparing the *absolute amount of tissue corrected for individual brain sizes*. Of note, this option is similar to using "Affine+non-linear" (see above) in combination with "global normalization" (when later building the statistical model using the traditional PET designs). That is, when building the statistics, one would specify "Global normalization" → "Overall grand mean scaling – No" → "Normalization – Proportional". Although this type of modulation was used in previous VBM versions as default it is not recommended anymore because the use of the standard modulation in combination with TIV as covariate gives more reliable results (Malone et al. 2015; Neuroimage).

For further explanation see also:
http://www.neuro.uni-jena.de/vbm/segmentation/modulation

## *Naming convention of output files*

Please note that the resulting files of CAT12 are organized in separate subfolders (e.g. mri, report, surf, label). If you don't want to use subfolders you can change the option "cat12.extopts.subfolders" in cat_default.m to "0".

**Images (saved in subfolder "mri")**

| | | |
|---|---|---|
| Segmented Images: | #p[0123]* | [m[0]w]p[0123]*[_affine].nii |
| Bias, noise and intensity corrected T1 image: #m* | | [w]m*.nii |

| | |
|---|---|
| * | filename |
| # | image space prefix |

**Image space prefix:**

| | |
|---|---|
| m | modulated |
| m0 | modulated non-linear only (expert mode only) |
| w | warped (spatially normalized using DARTEL) |

**Image space extension:**

| | |
|---|---|
| _affine | affine registered only |

**Image data prefix:**

| | |
|---|---|
| p | partial volume (PV) segmentation |
| 0 | PV label |
| 1 | GM |
| 2 | WM |
| 3 | CSF |

**Surfaces in native space (saved in subfolder "surf")**

SURF.TYPE.*.gii

| | |
|---|---|
| SURF | left, right hemisphere [ lh \| rh ] |
| TYPE | surface data file [ central \| sphere \| thickness \| gyrification \| ... ] |
| | central - coordinates and faces of the central surface |
| | sphere - coordinates and faces of the spherical projection of the central surface |
| | sphere.reg - coordinates and faces of the sphere after spherical registration |
| | thickness - thickness values of the surface |

sqrtsulc - sqrt-transformed values of sulcul depth based on the euclidian distance between the central surface and its convex hull

gyrification - gyrification values based on absolute mean curvature

fractaldimension - fractal dimension values (cortical complexity)

**Surfaces in (normalized) template space (after resampling and smoothing; saved in subfolder "surf")**

FWHM.SURF.TYPE.resampled.*.gii

FWHM      filtersize in FWHM after smoothing

SURF      left, right hemisphere [ lh | rh ]

TYPE      surface data file [ thickness | gyrification | fractaldimension | ... ]

thickness - thickness values of the surface

sqrtsulc - sqrt-transformed values of sulcul depth based on the euclidian distance between the central surface and its convex hull

gyrification - gyrification values based on absolute mean curvature

fractaldimension - fractal dimension values (cortical complexity)

**Images and surface of longitudinal data**

After processing longitudinal data the filenames additionally contain an "r" between the original filename and the other prefixes to indicate the additional registration step. Please also note that only the bias, noise and intensity corrected average image of all time points for each subject is saved.

**Reports (saved in subfolder "report")**

Global morphometric and image quality measures are stored in the *cat_*.xml* file. This file also contains other useful information about software versions and the used options for preprocessing the data. You can use the cat_io_xml function to read data from xml-files. Furthermore, a report for each data set is saved as pdf-file *catreport_*.pdf*.

**Regions of interest (ROI) data (saved in subfolder "label")**

ROI data is optionally saved as csv-file *catROI_[ATLASNAME]_*.csv*.

## *Technical information*

This toolbox is an extension of the segmentation in SPM12, but uses a completely different segmentation approach.[3]

*AMAP Segmentation*

The segmentation approach is based on an Adaptive Maximum A Posterior (AMAP) technique without the need for a priori information about tissue probabilities. That is, the Tissue Probability Maps (TPM) are not used constantly in the sense of the classical Unified Segmentation approach (Ashburner et. al. 2005), but only for spatial normalization and the initial skull-stripping. The following AMAP estimation is adaptive in the sense that local variations of the parameters (i.e., means and variance) are modeled as slowly varying spatial functions (Rajapakse et al. 1997). This not only accounts for intensity inhomogeneities but also for other local variations of intensity.

*Mixed Model*

Additionally, the segmentation approach uses a Partial Volume Estimation (PVE) with a simplified mixed model of at most two tissue types (Tohka et al. 2004). We start with an initial segmentation into three pure classes: gray matter (GM), white matter (WM), and cerebrospinal fluid (CSF) based on the above described AMAP estimation. The initial segmentation is followed by a PVE of two additional mixed classes: GM-WM and GM-CSF. This results in an estimation of the amount (or fraction) of each pure tissue type present in every voxel (as single voxels - given by their size - probably contain more than one tissue type) and thus provides a more accurate segmentation.

*Noise Filter*

Furthermore, we apply three denoising methods. The first method is an block-wise adaptive Non-Local Means (SANLM) denoising filter (Manjón et al. 2010). After global intensity correction a 2nd SANLM filter or optionally a block-wise optimized non-local means (ORNLM) denoising filter is applied (Coupe et al. 2008). These filters remove noise while preserving edges and are implemented as preprocessing step. The third method is a classical Markov Random Field (MRF) approach, which incorporates spatial prior information of adjacent voxels into the segmentation estimation (Rajapakse et al. 1997) and is part of the AMAP segmentation. The strength of the filters are automatically obtained by estimating the remaining noise in the image.

*Dartel Normalisation*

Another important extension to the SPM12 segmentation is the integration of the Dartel normalisation (Ashburner 2007) into the toolbox by an already existing Dartel template in MNI space. This template was derived from 555 healthy control subjects of the IXI-database (http://www.brain-development.org) and is provided in MNI space[4] for six different iteration steps of Dartel

---

[3] The classic SPM12 segmentation is still used in addition, but only to initially remove non-brain tissue from the image and to get a starting estimate for the segmentation.

[4] Thus, no additional MNI normalization is necessary.

normalisation. Thus, for the majority of studies the creation of sample-specific Dartel templates is not necessary anymore[5].

*Local Adaptive Segmentation (LAS)*
Beside WM-inhomogeneities, also the GM intensity can vary for different regions like the motor cortex, the basal ganglia, or the occipital lobe. Although, these changes have an anatomical background (e.g. iron content, myelenization), they depend on the MR-protocol and often lead to GM-underestimations for higher intensities and CSF-overestimations for lower intensities. Therefore, a local intensity transformation of all tissue classes is used to reduce this effects in the m*-image before the final AMAP segmentation. The strength of the changes is controlled by the LASstr parameter, with 0 for no LAS, small values (0.01-0.5) for small adaptations, 0.5 for average adaptation (default), and higher values (0.5-1) for strong adaptations.

*Skull-Stripping*
CAT12 contains a revised graph-cut based skull-stripping with a arbitrary strength, with 0 for a more liberal and wider brain masks and 1 for a more aggressive skull-stripping. The default is 0.5 and was successfully tested on a variety of different images.
The strength parameter affects multiple internal parameters:
- Intensity thresholds to deal with blood-vessels and meninges
- Distance and growing parameters for the graph-cut/region-growing
- Closing parameters that fill the sulci
- Smoothing parameters that allow sharper or wider results

If your segmentations still contain skull and other non-brain tissue (e.g. dura) you can try to increase the strength. If parts of the brain are missing in the segmentations the strength can be decreased.

*Cleanup*
CAT12 includes a new cleanup routine that uses morphological, distance and smoothing operations to remove reminding meninges from the final segmentation. The strength of the cleanup is controlled by the cleanupstr parameter, with 0 for no cleanup, low values

*Interpolation*
CAT12 uses an internal interpolation in order to allow more relaible results also for low resolution images. Although an interpolation cannot add further details to the images, some of the used functions benefit from the higher number of voxels and the common striped artefacts in modulated images are strongly diminished.

---

[5] For studies investigating data of children I still recommend creating a customized Dartel template. Of note, for this option a representative sample with a sufficient number of subjects is required (n>50-100). Alternatively, if a sufficient sample size cannot be achieved, the low-dimensional SPM12 normalization approach combined with customized Tissue Probability Maps (e.g. from the TOM8 toolbox) can be selected.

# References

Good, C.D. et al. (2001): A voxel-based morphometric study of ageing in 465 normal adult human brains. *Neuroimage*. **14(1 Pt 1)**:21-36.

Rajapakse, J.C. et al. (1997): Statistical Approach to Segmentation of Single-Channel Cerebral MR Images. *IEEE Trans. Med. Imag*. **16(2):**176-186.

Tohka, J. et al. (2004): Fast and robust parameter estimation for statistical partial volume models in brain MRI. *Neuroimage* **23(1):**84-97.

Ashburner, J. (2007): A fast diffeomorphic image registration algorithm. *Neuroimage* **38(1):**95-113.

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