An Automatic Framework for the Graph-based Representation of Coronary Arteries

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Introduction

We present an automatic framework for the segmentation and graph-based representation of coronary arteries in X-ray angiograms.

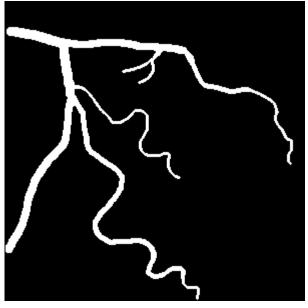
The first stage of vessel segmentation is carried out by using Gaussian matched filters trained by the Univariate Marginal Distribution Algorithm. In the second step, the line simplification algorithm of Ramer-Douglas-Peucker is used to represent the coronary artery skeleton as a graph, where the nodes are the dominant pixels for shape preservation.

Introduction

- In clinical practice, the coronary angiography represents current gold standard for detecting and monitoring vessel abnormalities.
- Disadvantages with X-ray angiograms: nonuniform illumination and low contrast between vessel-like structures and background.
- In literature, these two drawbacks have been addressed in two different steps; enhancement and binary classification.



Input image



Segmented image

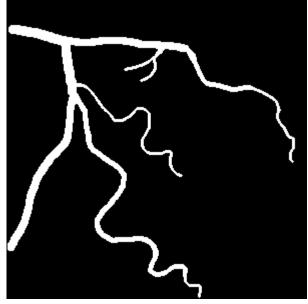
Introduction

The second main problem focuses on simplify the vessel-like structures.

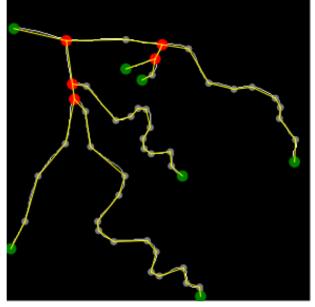
- Try to reduce the number of points, needed to resume the arterial information.
- Main purposes:
 - Compressing data,
 - Reconstruction of structures,
 - 3D image registration / rendering,
 - Simulate motion and blood flow on arteries,
 - Reduce complexity.
- Suitable for computer-aided diagnosis.



Input image



Segmented image



Simplified structure

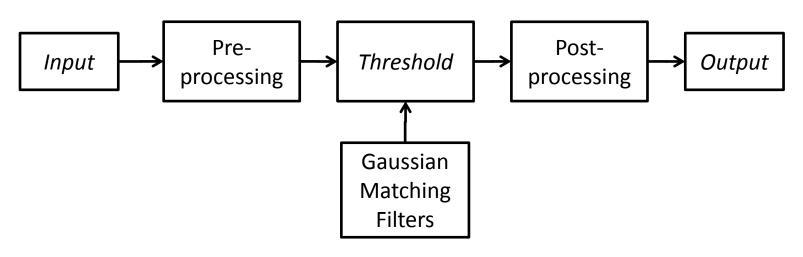
In the enhancement step, different techniques have been proposed:

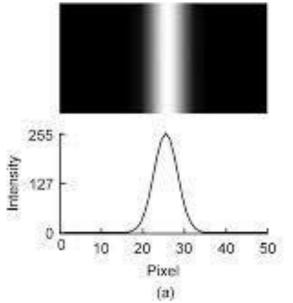
- mathematical morphology, Gaussian filters,
- linear operators, and so on ...

The Gaussian matched filters (GMF) were originally proposed by Chaudhuri et al. [1].

The GMF method represents an spatial template image strategy.

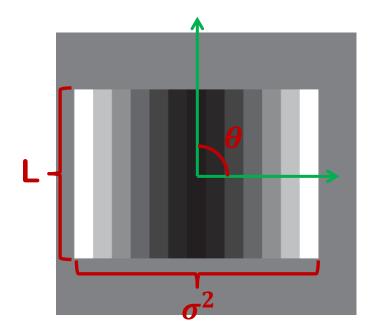
The Idea: the shape of the blood vessels can be approximated by a Gaussian profile at different orientations!





$$G(x,y) = -\exp\left(\frac{x^2 + y^2}{2\sigma^2}\right), |y| \le \frac{L}{2}$$

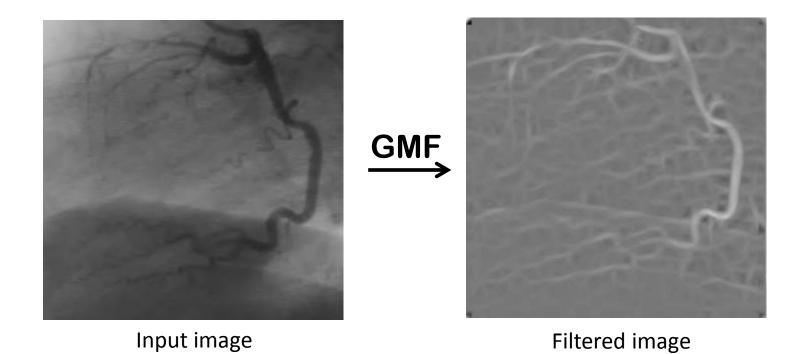
Gaussian template



Parameters:

- Length (L)
- Width of vessel (σ^2)
- Orientation (angle θ) usually one set the number of oriented filters k at orientations

$$\theta = \frac{\pi j}{k}$$
, $j = 1, 2, ..., k$

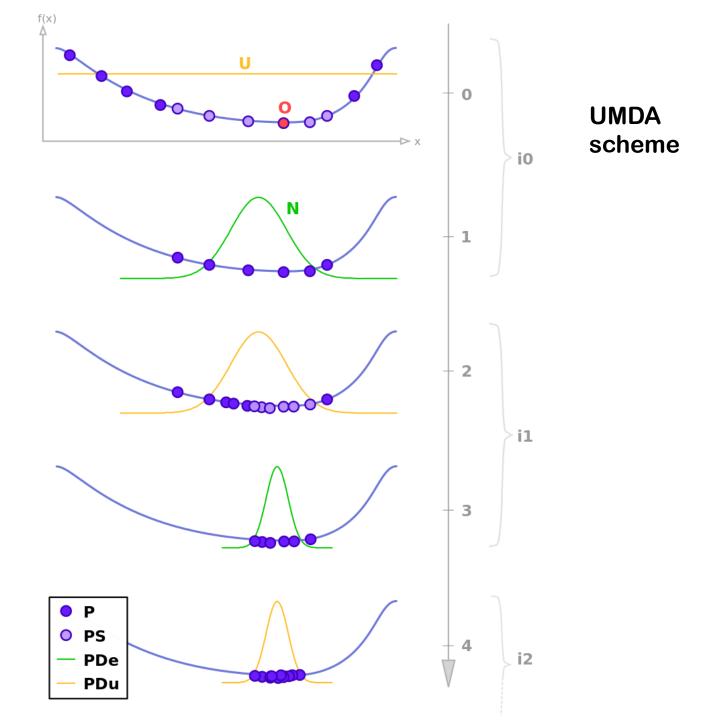


Many researchers have suggested strategies, applications or empirically values for the GMF parameters, in order to improve its performance in vessel detection.

- Kang et al. [2], [3] proposes new values for σ^2 , while reducing the number k.
- Chanwimaluang et al. [4] used the original method in retinal registration.
- Cinsdikici and Aydin [5] proposed a new number of oriented filters k for retinal vessel segmentation.
- Al-Rawi et al. [6], [7] proposed a new search space and optimization strategies to find the optimal set of parameters.

Cruz et al. [8], [9] proposed the use of population-based methods (evolutive heuristics) for the parameter optimization in a new search space focused on coronary arteries.

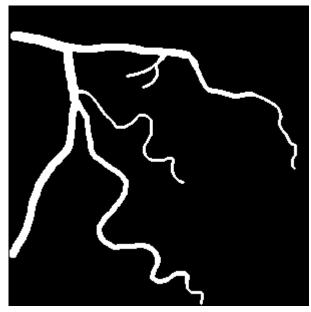
This strategy has been adopted in the present work. As optimization strategy we use Univariate Marginal Distribution Algorithm (UMDA) [10], since it works suitable for linear problems [11], [12], [13].



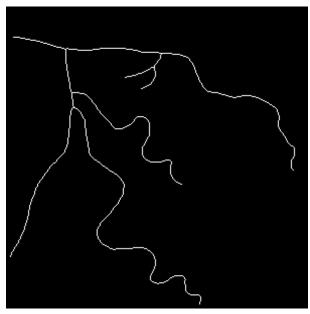
Simplification method

Graph-based representation

Second stage: Graph-based representation of the segmented coronary artery tree. In this step, the Ramer-Douglas-Peucker method (RDP) is used to reduce the number of pixels of the blood vessel skeleton.



Segmented image



Skeletonization

Graph-based representation

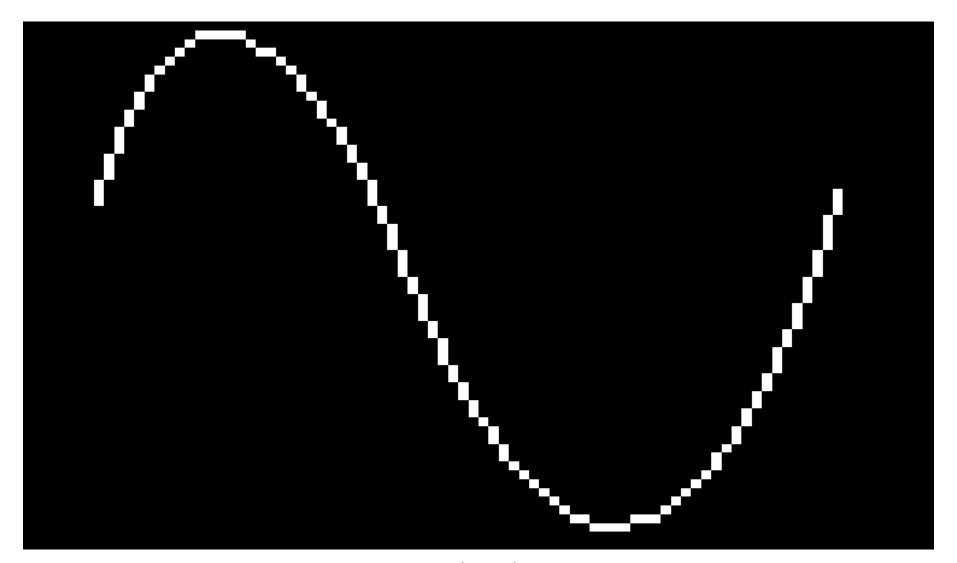
RDP algorithm reduces the number of existent points in a line, based on divide and conquer approach [$O(n \log n)$ average, $O(n^2)$ worst].

It is widely used in applications such as:

- traffic signs detection,
- compressing GPS trajectory data,
- reconstruction of building ground plans,
- robotics

<u>Idea</u>: reduce the complexity of lines which expressed trajectories or vectors.

Ramer-Douglas-Peucker



RDP iterations

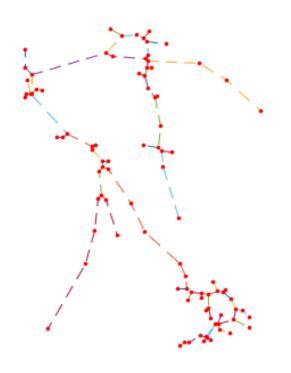
Graph-based representation

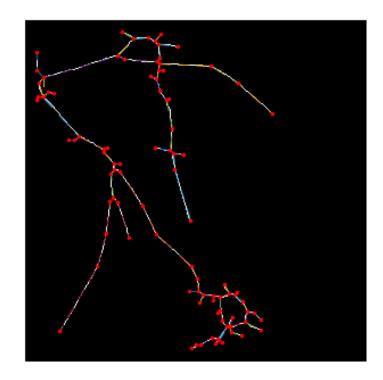
Several approaches to construct the graph:

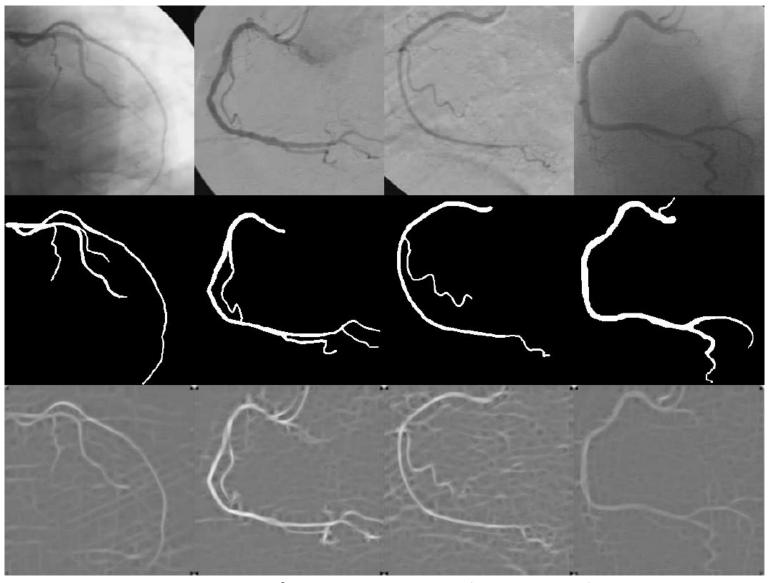
- Detect branch points
- Then:
 - PFS or BFS over the associated graph, by using simplified skeleton as base, or
 - Split connected components (after remove branch points) and construct incidence relations.

Graph-based representation

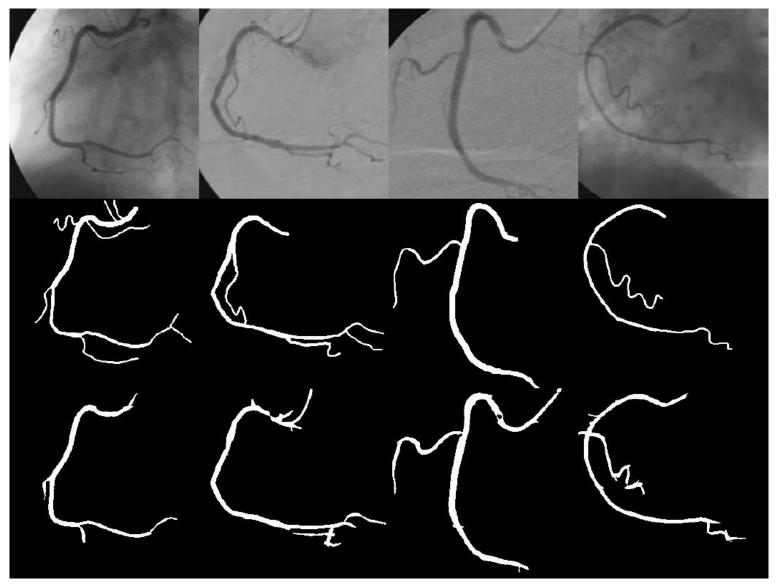
RDP algorithm depends on an ε parameter.



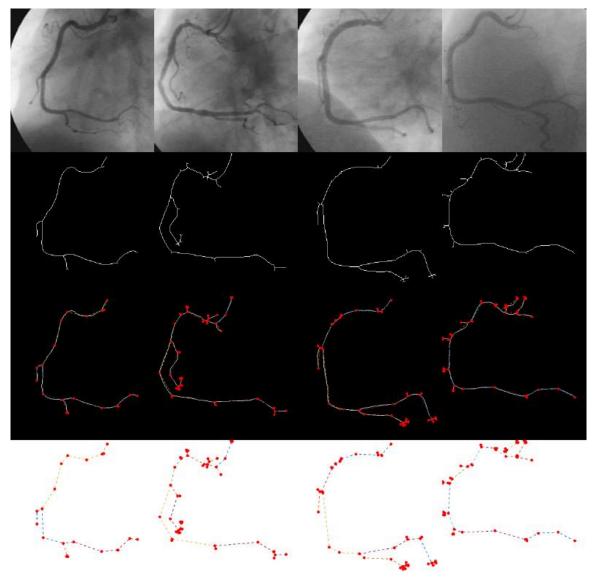




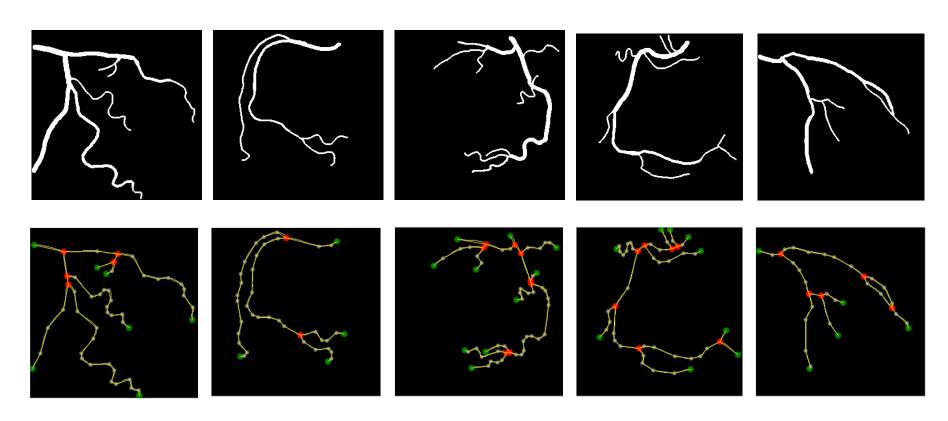
Gaussian response from images using the proposed strategy.



Automatic blood vessel segmentation of angiograms using the proposed method.



Graph-based approach of angiograms using the proposed framework.



Graph-based approach of angiograms using the proposed framework.

TABLE I
PERFORMANCE ANALYSIS BETWEEN DIFFERENT GMF-BASED
TECHNIQUES AND THE PROPOSED METHOD.

Method	A_z value
Proposed method	0.9135
Chaudhuri et al.	0.8954
Kang et al.	0.8723

Metric used: ROC curve.

All methods were tested over a 30 coronary angiogram image database, (300x300 pixels).

In the binary classification step, to classify the Gaussian response, five thresholding methods of the state-of-the-art have been selected:

- Methods based on entropy measure [15,16],
- Mean value [17],
- Histogram concavity [18],
- Inter-class variance [19] were tested.

Metric used: accuracy.

TABLE II
PERFORMANCE ANALYSIS OF DIFFERENT THRESHOLDING METHODS
USING THE GAUSSIAN RESPONSE IMAGE ON THE TEST SET.

Method	Accuracy
Otsu [19]	0.9215
Pal and Pal [16]	0.9202
Ridler and Calvard [17]	0.9185
Rosenfeld and De la Torre [18]	0.9102
Kapur et al. [15]	0.8941

The simplification step is assessed in terms of the data compression ratio (CR) as follows:

$$CR = 1 - \frac{compressed\ data}{uncompressed\ data}$$

Where

- compressed data is the number of nodes obtained from the parametric line simplification method
- and uncompressed data represents the number of pixels of the automatic segmented coronary artery skeleton.

TABLE III
PERFORMANCE ANALYSIS FOR DIFFERENT VALUES OF THE RDP METHOD USING THE SEGMENTED ANGIOGRAMS.

Epsilon value	CR	time (in seconds)
$\epsilon = 5$	0.9370	0.0069
$\epsilon = 4$	95.7328	0.0245
$\epsilon = 3$	95.1763	0.0300
$\epsilon = 2$	94.0631	0.0316
$\epsilon = 1$	91.2801	0.0247

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