



UNIVERSITÀ
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CiMeC
Center for Mind/Brain Sciences

Brain Structural MRI Introduction

Louvain-la-Neuve - Neuroimaging Workshop 2019

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Concept map for lectures

Lecture 1

NMR Signal origin

- Powerful magnet
- Radio frequency
- Magnetic field gradients

MR Image & Contrast

- Spatial encoding
- Magnetic gradients
- Pulse sequences

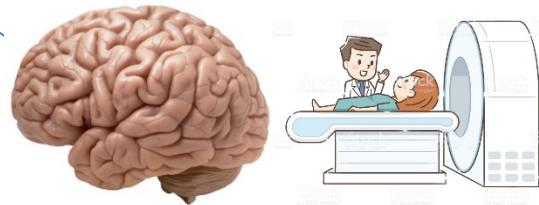
MR Safety

- Powerful magnet
- Radio frequency
- Magnetic field gradients

Lecture 2

Structural MRI

- Contrast, important parameters
- Sequences & artifacts
- Analyses & applications



Lecture 3

Diffusion MRI

- Contrast, important parameters
- Sequences & artifacts
- Analyses & applications

Lecture 4

Functional MRI

- Contrast, important parameters
- Sequences & artifacts
- Pre-processing

Lecture 2 outline

Brain structure MRI

- 
- o What is a structural MRI?
 - o What is image contrast?
 - o How can image contrast be manipulated?
 - o What image analyses are common from brain structural MRI?
 - o What are some structural MRI applications?
 - o What are some structural MRI challenges?

Structural versus Functional MRI

- **Structural MRI:**
 - Contrast sensitive to macro- or micro-structural anatomy in space
 - Examples
 - Gray matter, white matter, cerebral spinal fluid (CSF)
 - Iron content
 - Myelin content
 - Fat tissue
 - Etc.
- **Functional MRI:**
 - Contrast sensitive to blood oxygenation, or perfusion or metabolism in time
 - Examples
 - Hemodynamic changes in time (during task or rest)
 - Blood perfusion changes
 - Blood volume changes
 - Concentration of metabolite changes
 - Etc.

The key thing is contrast. What is it?

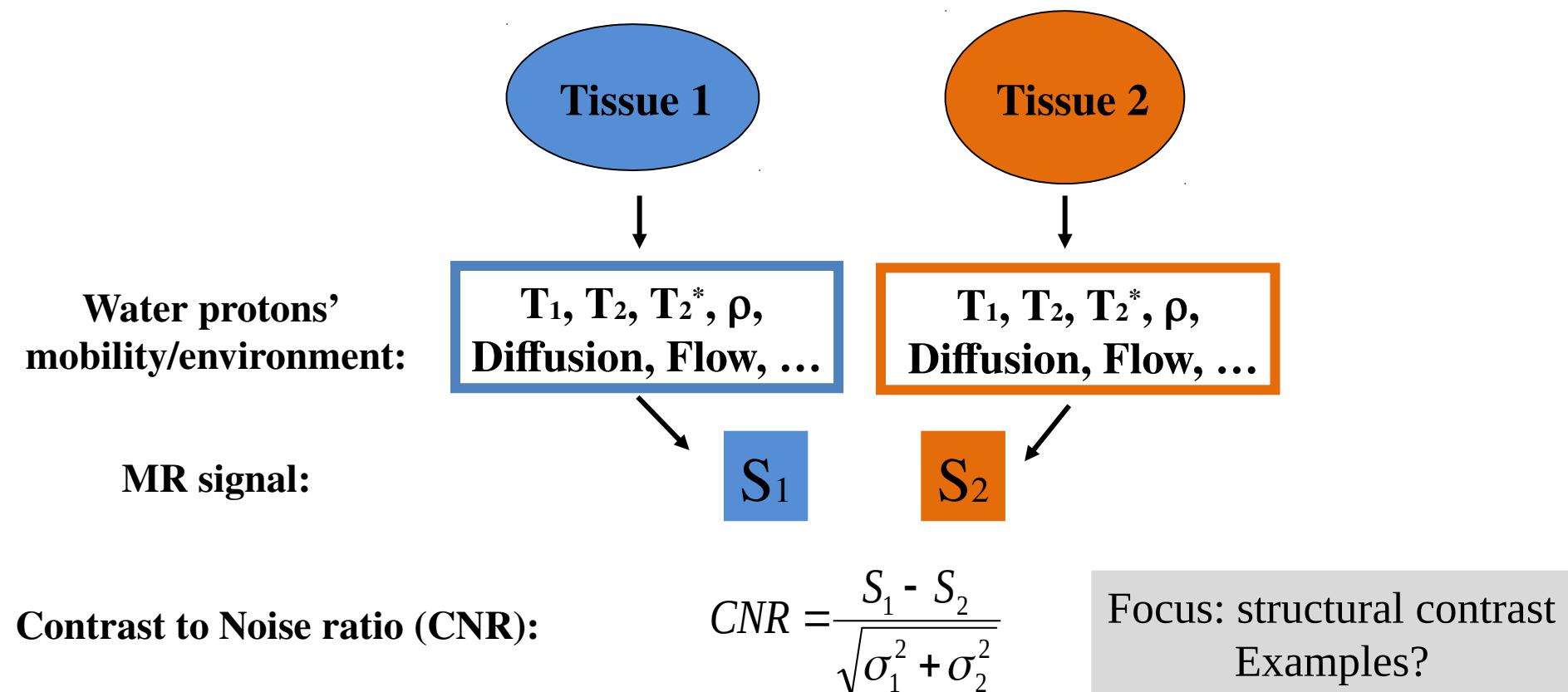
Lecture 2 outline

Brain structure MRI

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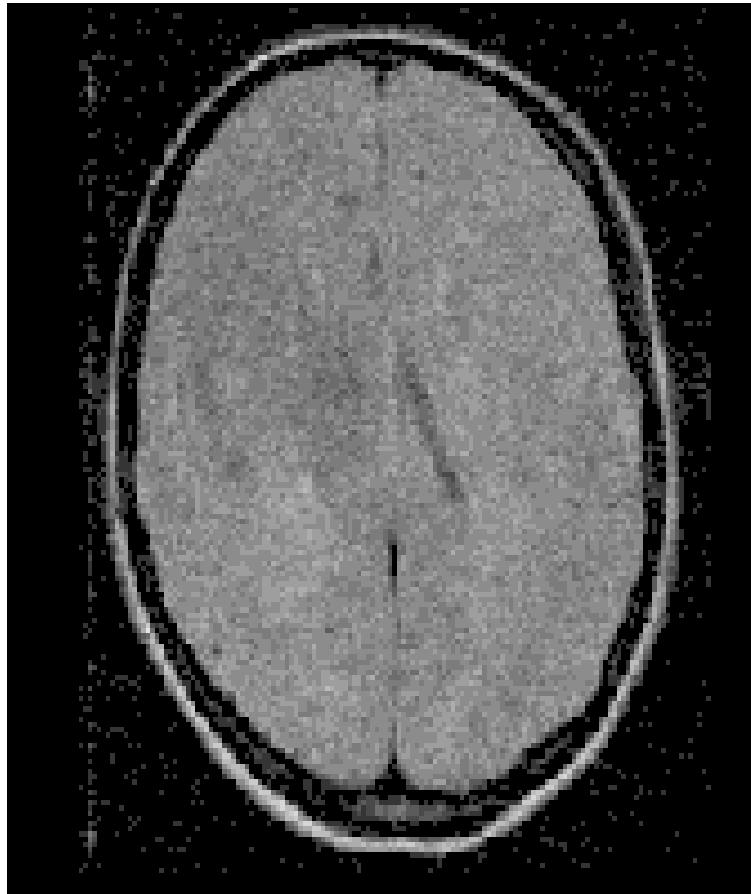
Image contrast definition

- **Structural contrast:** difference in MR signals between different tissues
- **Goal:** maximize the contrast of interest (USEFUL IMAGES!)

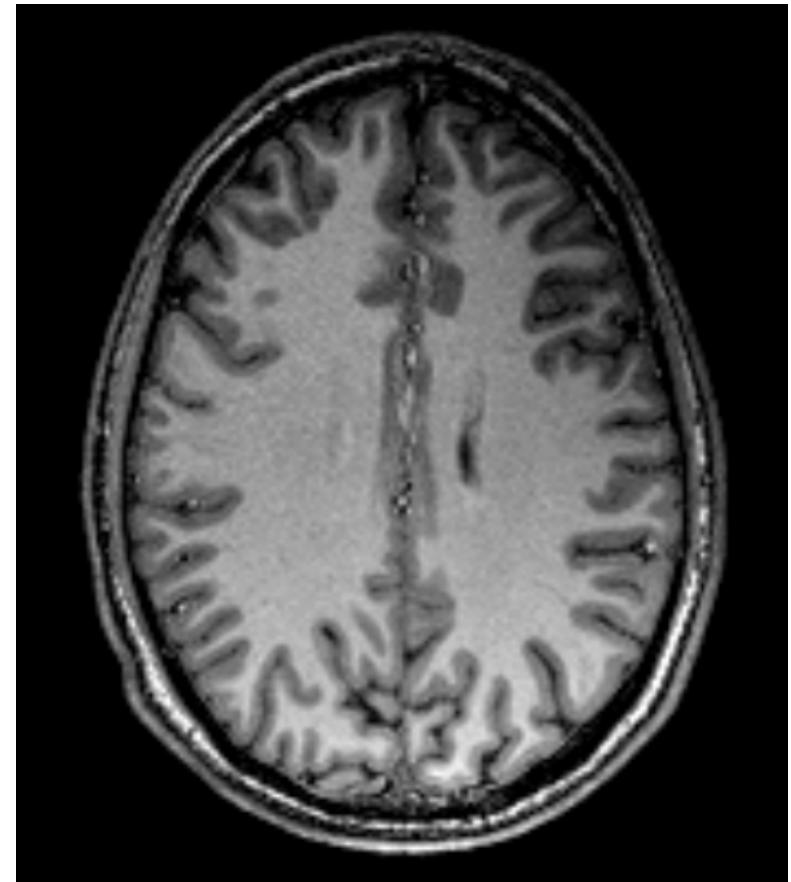


Structural image example

Poor gray/white matter contrast



Good gray/white matter contrast
(T1 contrast)



MRI contrast: what can be manipulated?

Tissue Properties: fixed

Tissue	T_1^+ (ms)	T_2 (ms)	ρ^*
Fat	260	84	0.90
White Matter	780	90	0.72
Gray Matter	920	100	0.84
CSF	3000	300	1.00

T_1 values for $B_0 = 1.5T$

ρ^* : % H_2O relative to CSF

Experimental Variables

- Magnetic field
- Pulse sequence
- Pulse sequence parameters
 - Repetition time: TR
 - Echo time: TE
 - Inversion time: TI
 - RF flip angle: α
- Contrast agent

What's the effect of these variables?

Contrast weight on the MRI signal

- **General MRI pulse sequence:** combination of contrasts

Signal Intensity:

$$S(x,y) = k \times \rho \times T_1 \times T_2 \times \dots$$

- **Contrast Weighting:** maximize one term, minimize the others

Example: T_1 -weighting

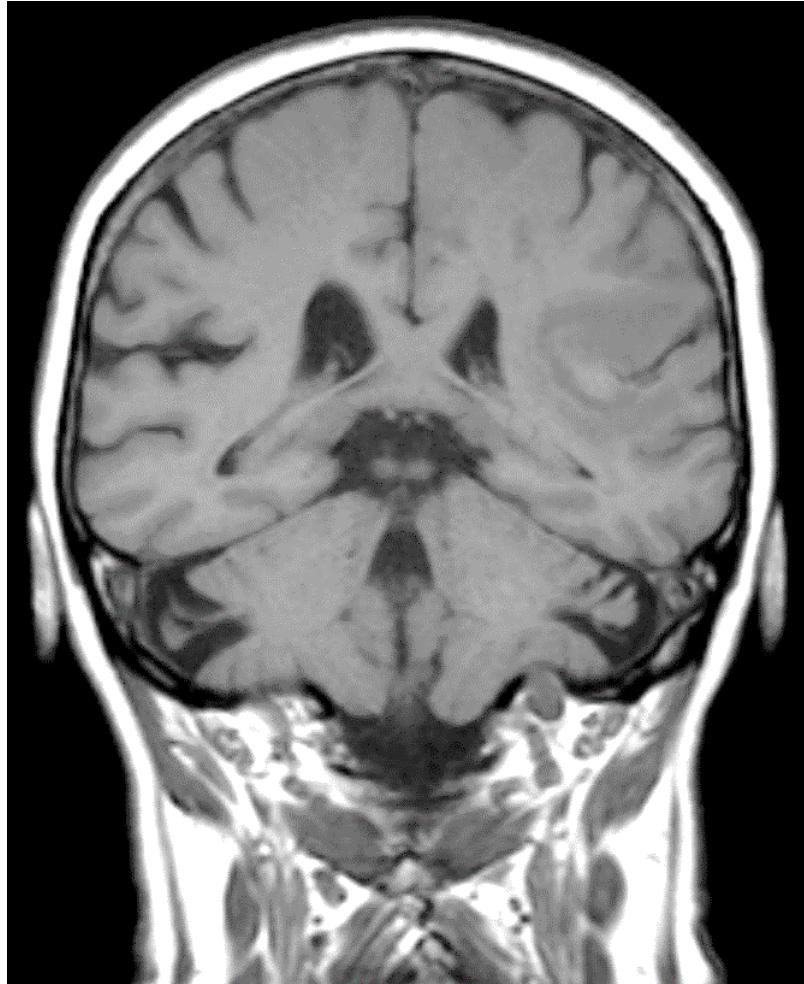
$$S(x,y) = k \times \rho \times T_1 \times T_2 \times \dots$$

by choosing adequate sequence & sequence parameters

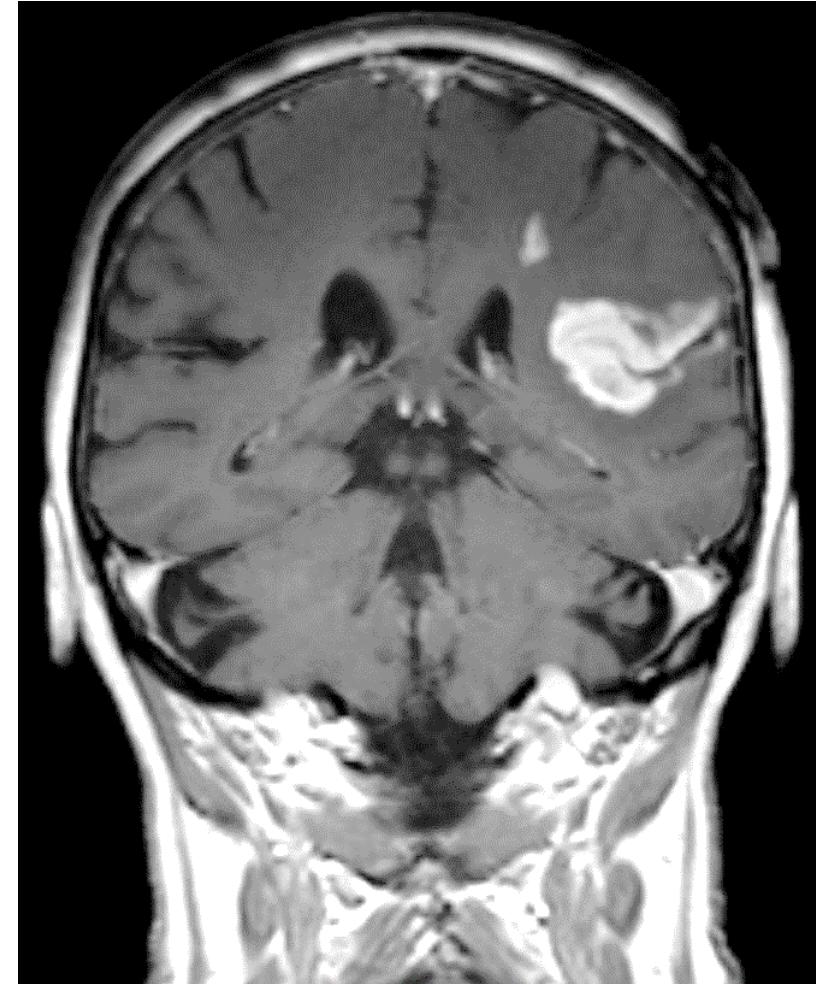
Examples?

Using image contrast agents in clinics

Without contrast agent



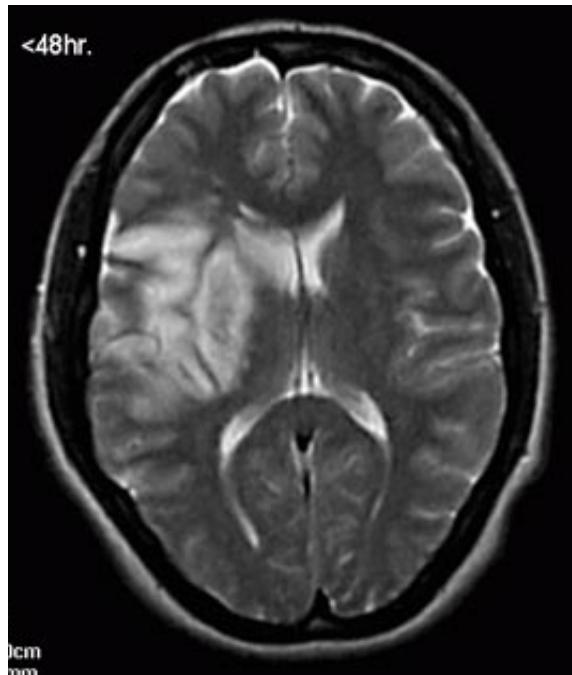
With contrast agent



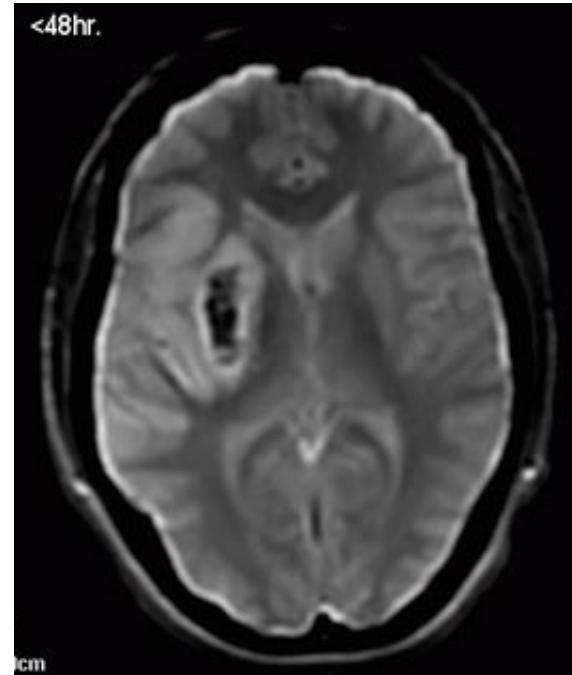
Defect of the blood-brain barrier after stroke
shown in MRI T1-weighted images.

Multiple contrasts are used for diagnosis

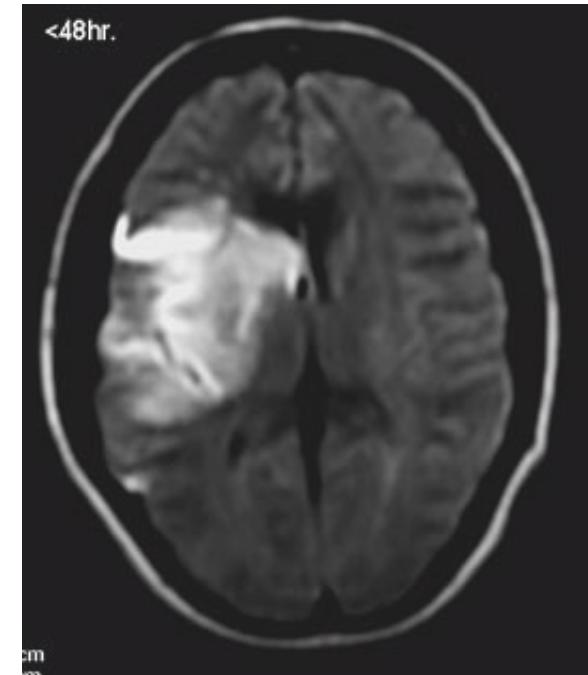
< 48 hours postictal acute infarct in right hemisphere



T₂-weighted



T₂*-weighted
(presence of blood)

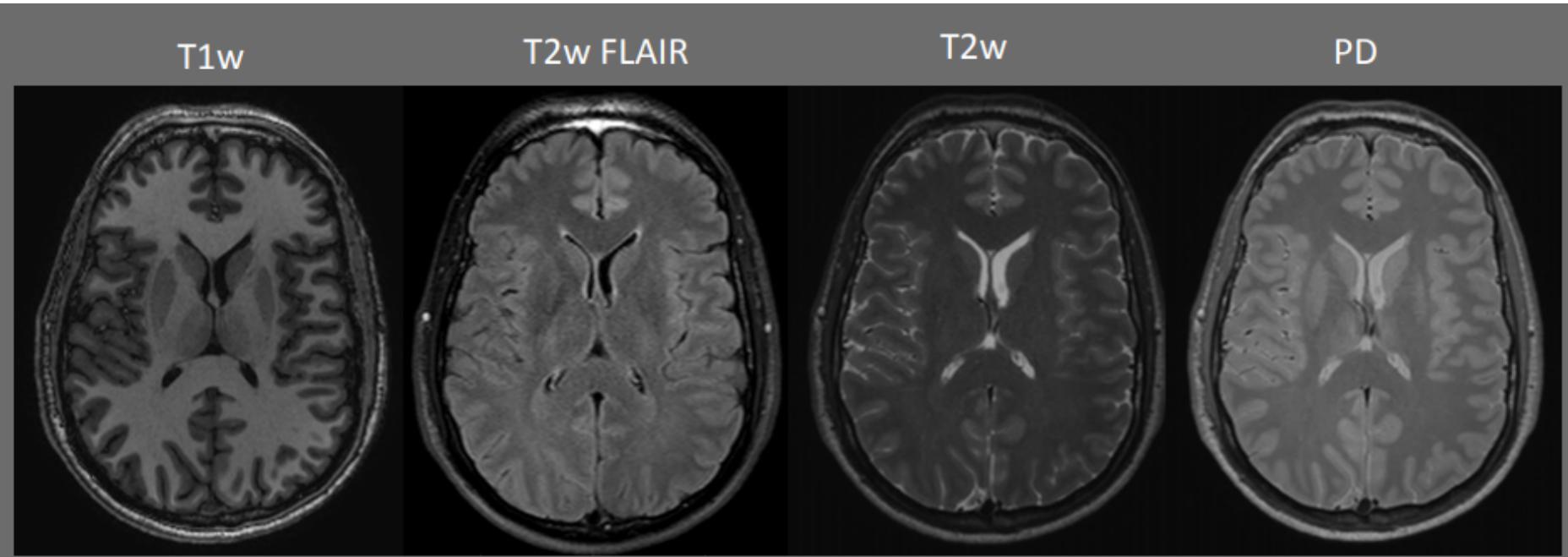


Diffusion-weighted
(full infarct extent)

Images from Toshiba Image gallery

Multiple contrasts in healthy tissue

Research with healthy volunteers: endogenous natural tissue contrast



http://www.mc.vanderbilt.edu/documents/fMRI/files/2013_Phys352A_StructuralMRI.pdf

T1w: T1-weighted MRI

T2w: T2-weighted MRI

T2w FLAIR: T2-weighted Fluid Attenuation Inversion Recovery

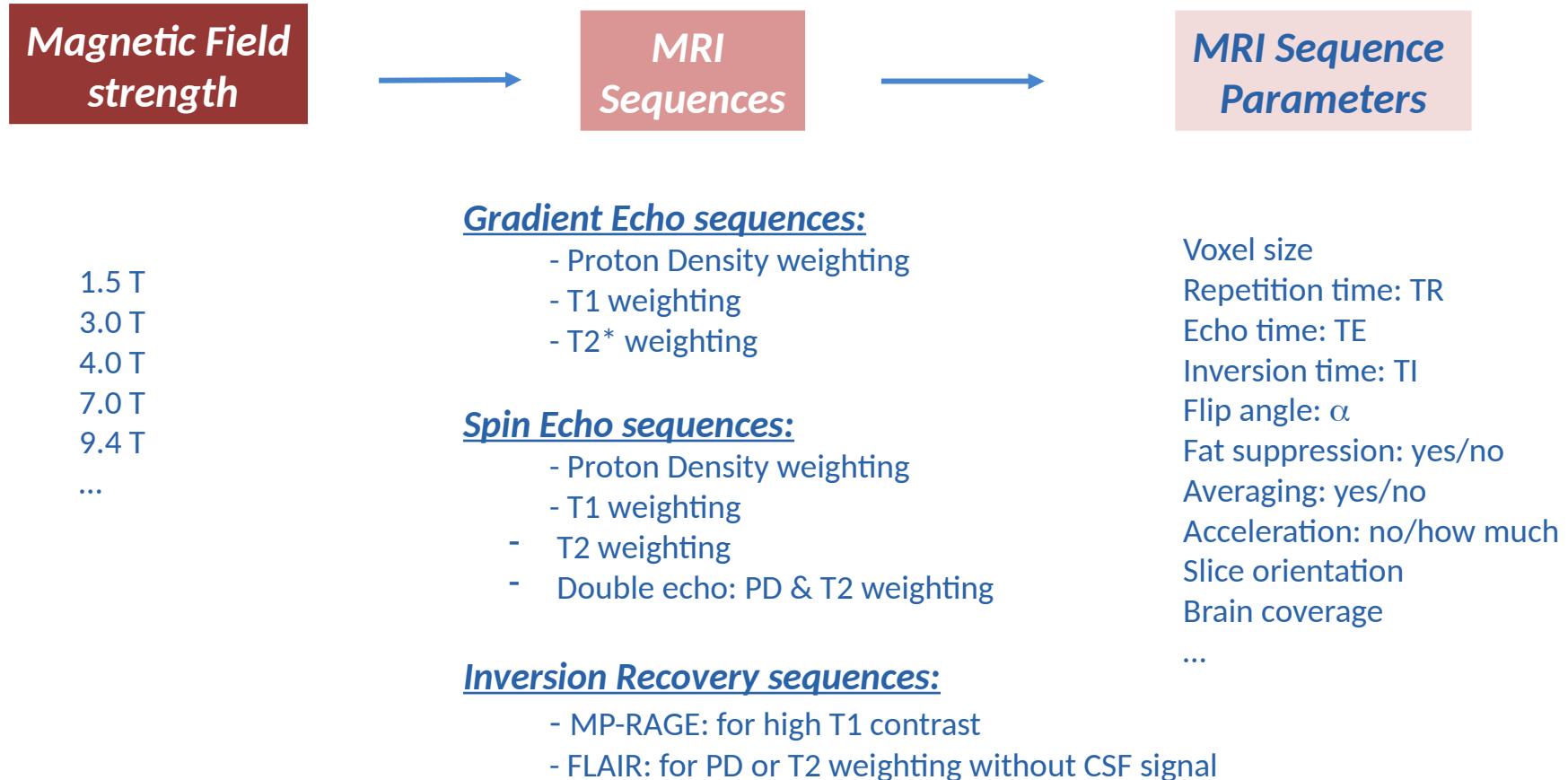
PD: Proton Density weighted MRI

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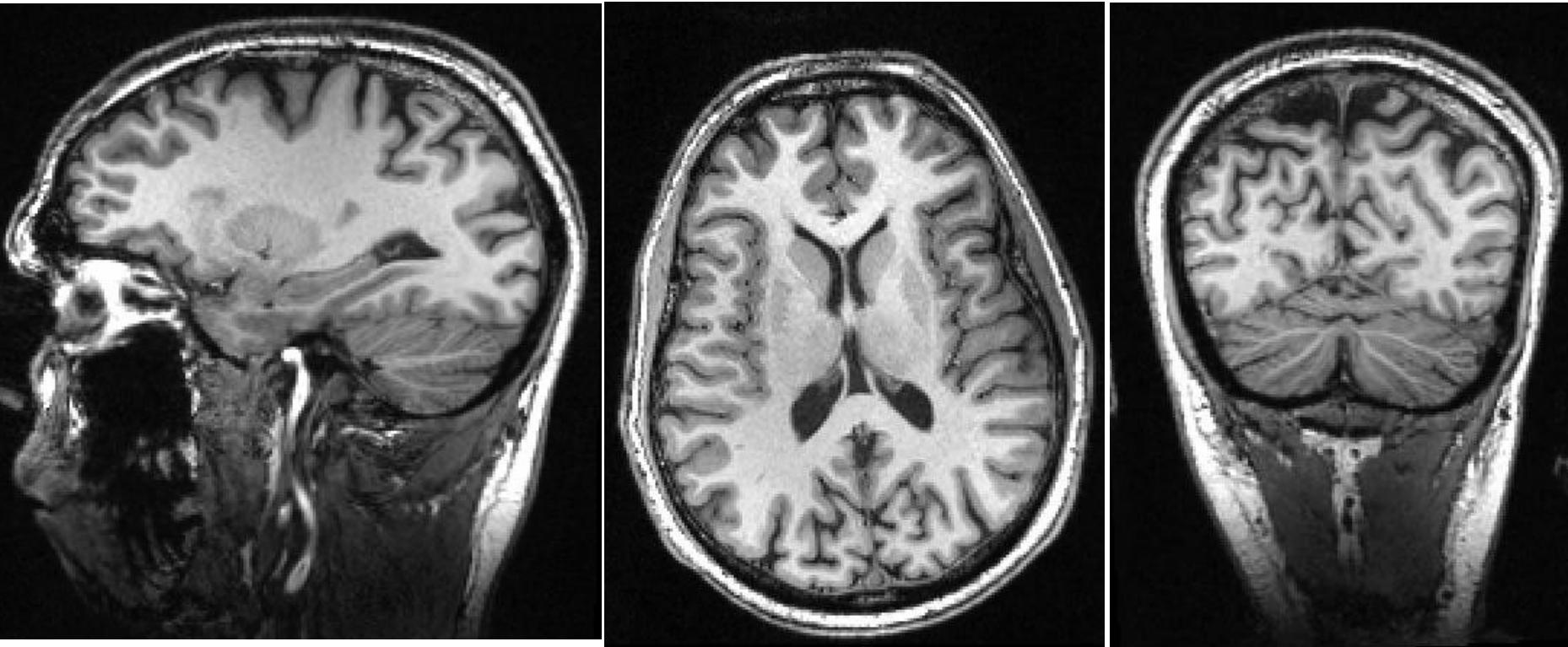
Multiple options to manipulate MRI contrast



The choice of a particular sequence & parameters depends on the metrics you want to derive and analyze from the images

Example: T1-weighted MRI

Most common brain structural MRI contrast used
in cognitive neuroscience studies

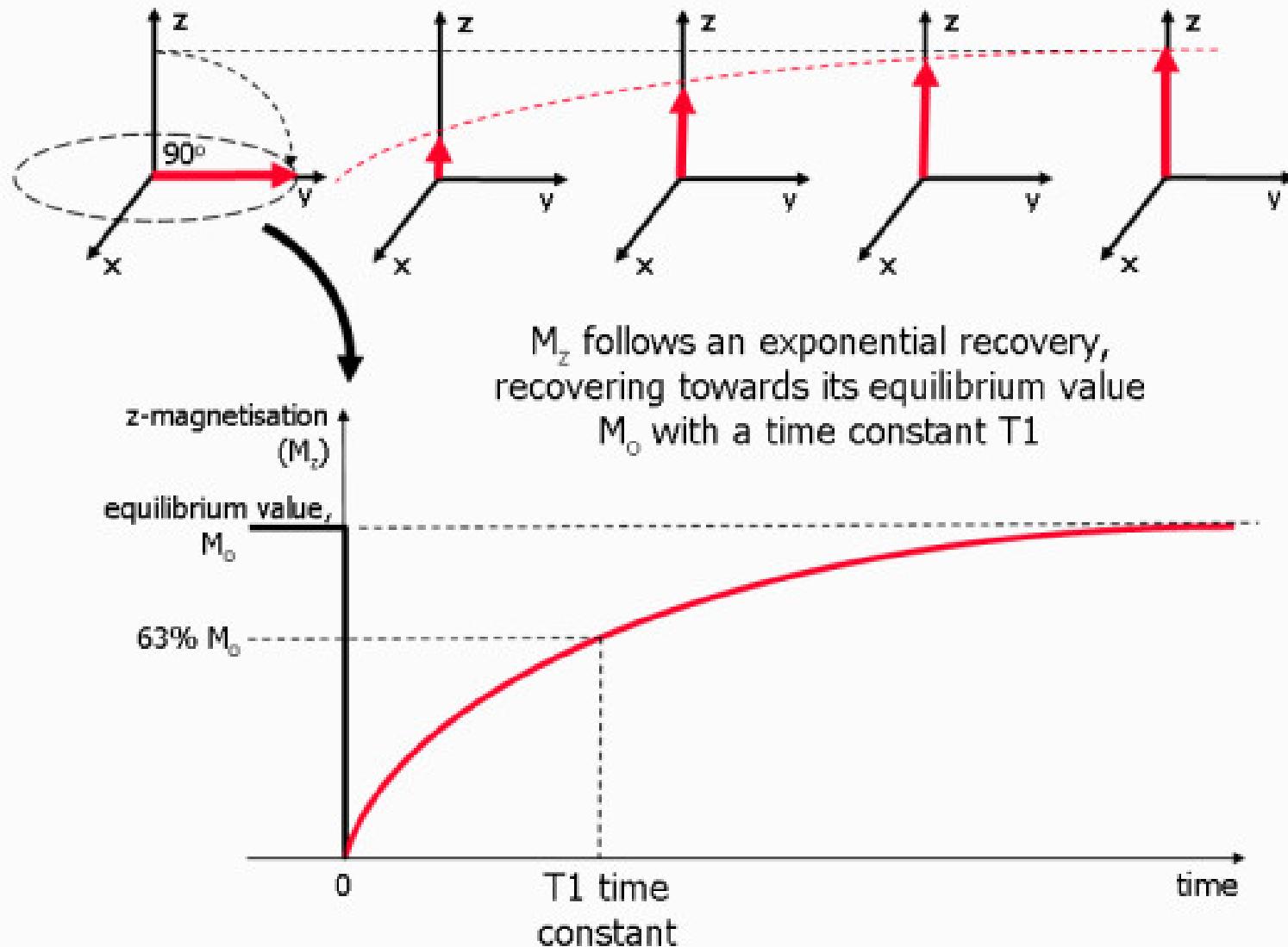


3D MP-RAGE (T1 contrast, 4T)

Spatial Resolution: $1 \times 1 \times 1 \text{ mm}^3$
Acquisition time: 5 minutes

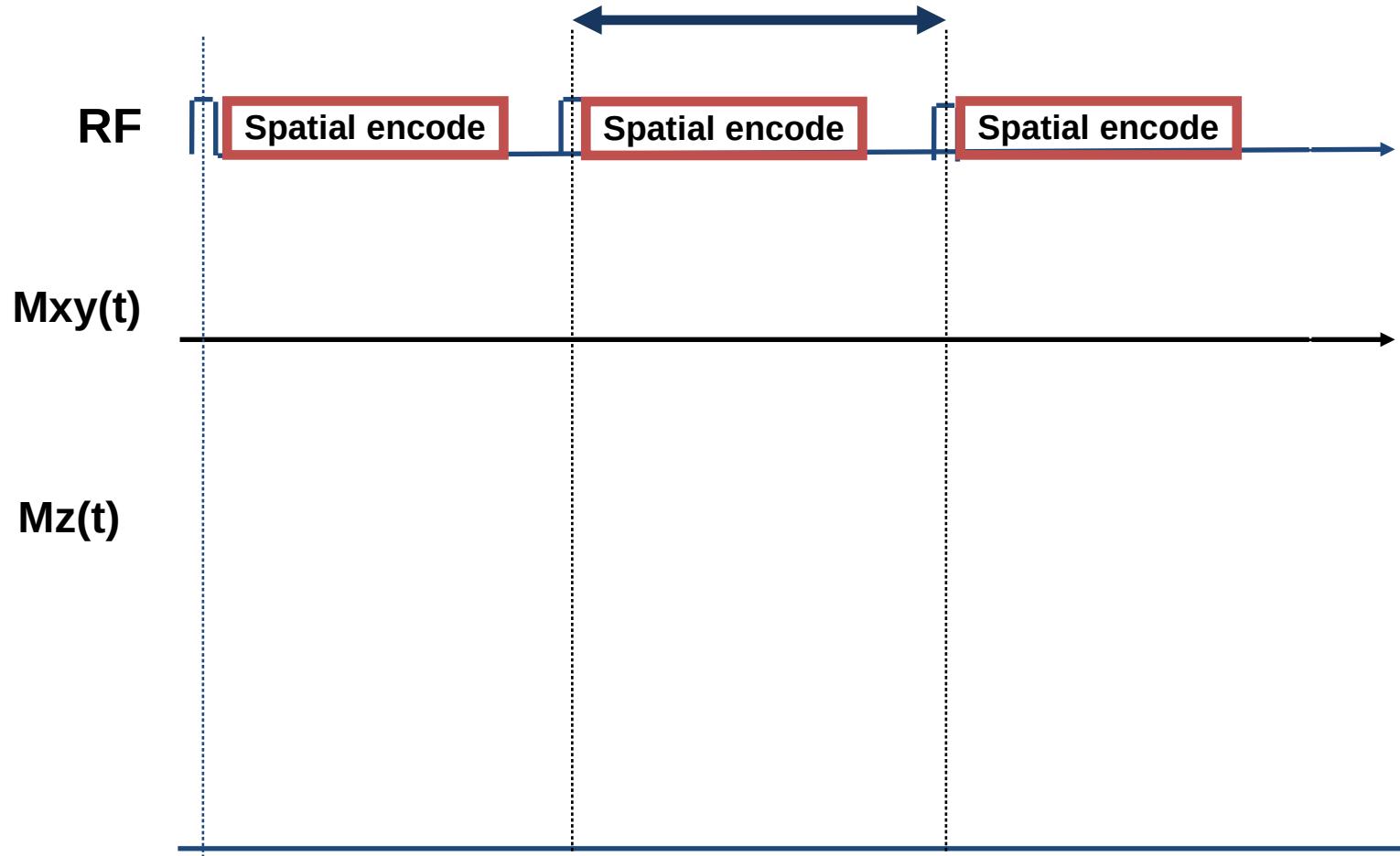
How is this contrast obtained?

Reminder of T1 relaxation



Example: changing contrast with TR

TR: Repetition Time (time between RF excitations of the magnetization)



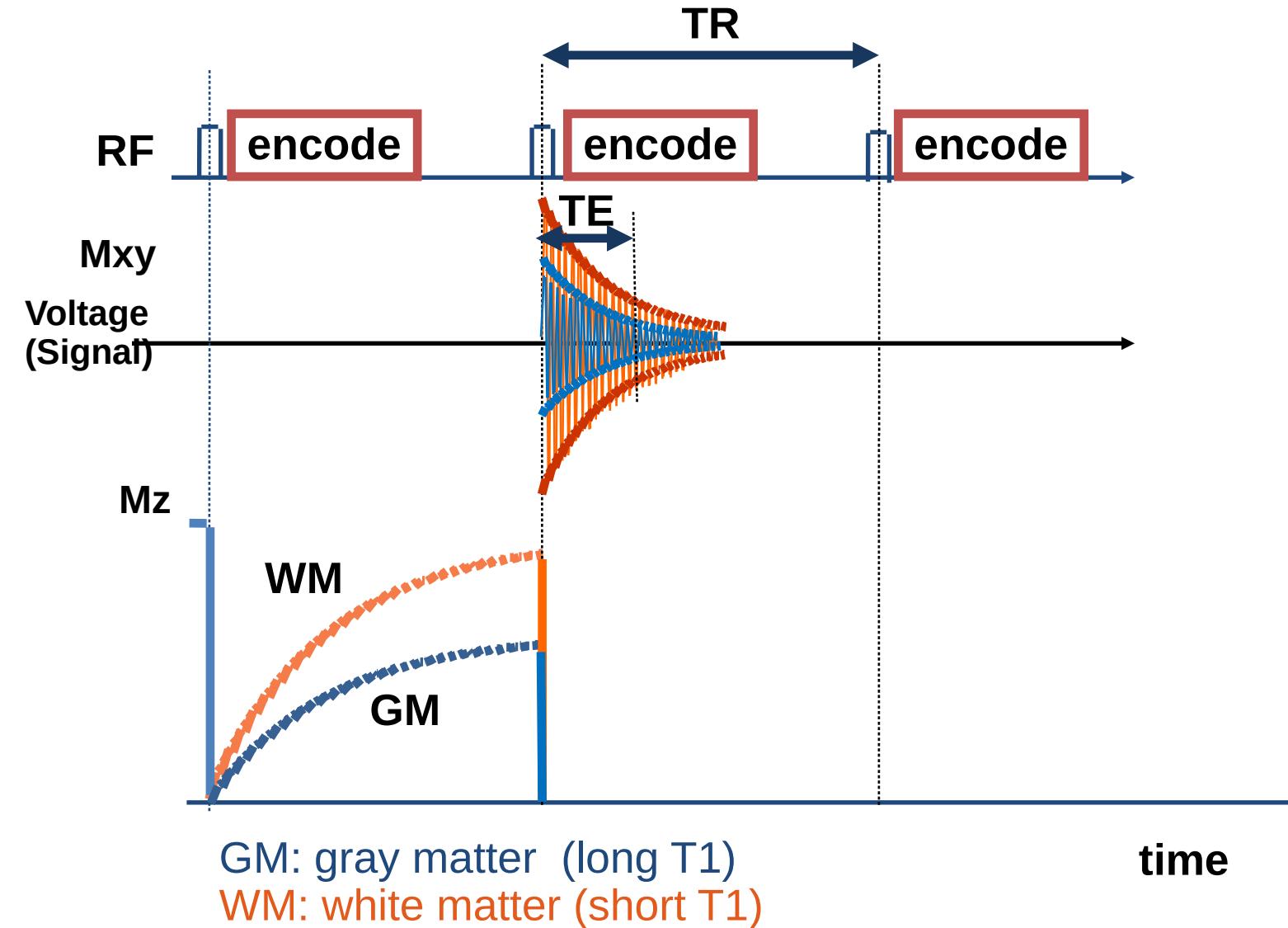
GM: gray matter (T1 long)

WM: white matter (T1 short)

Assume T2* similar and very short in both GM & WM

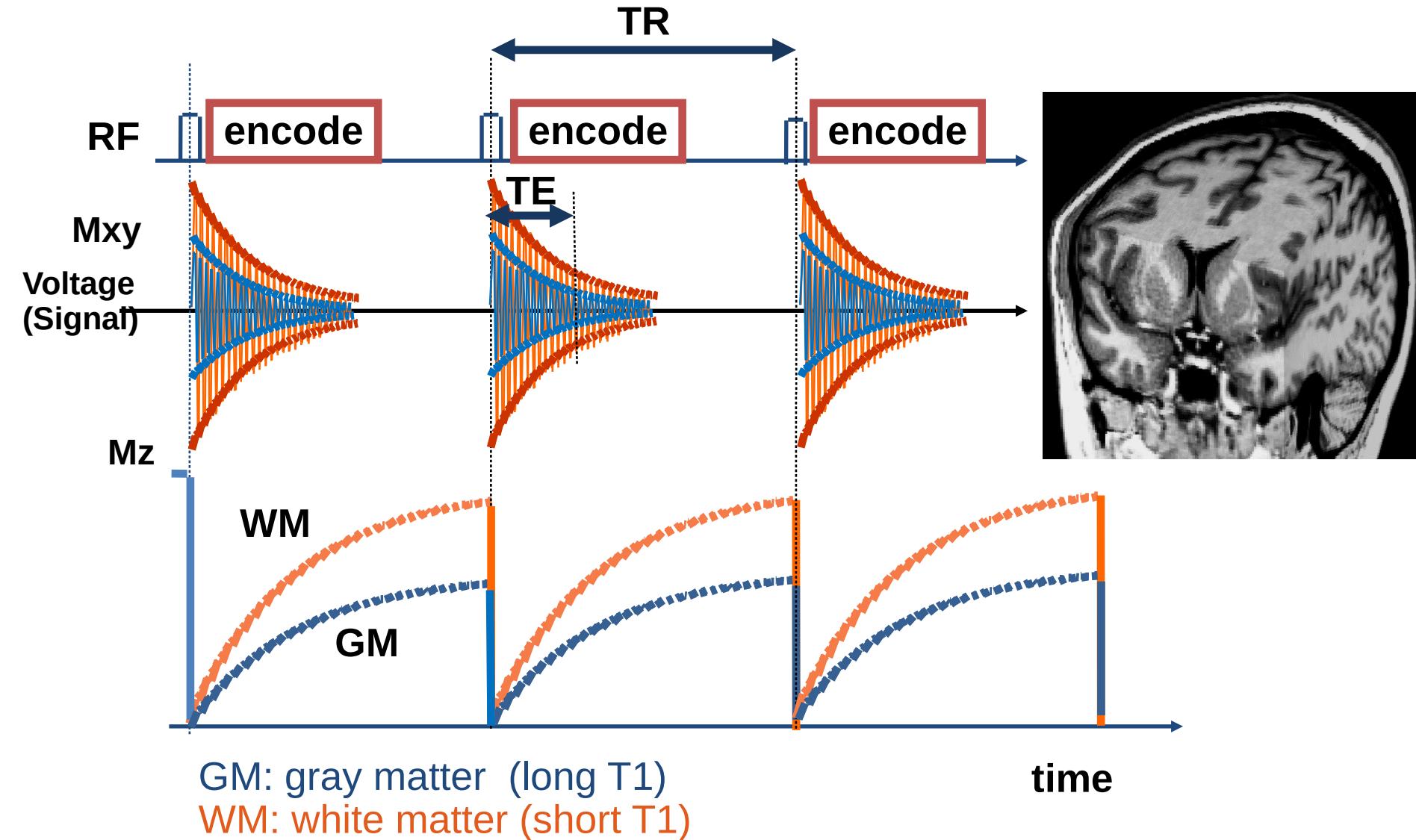
Example: changing contrast with TR

TR: Repetition Time (time between RF excitations of the magnetization)

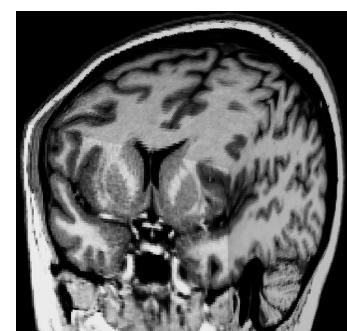
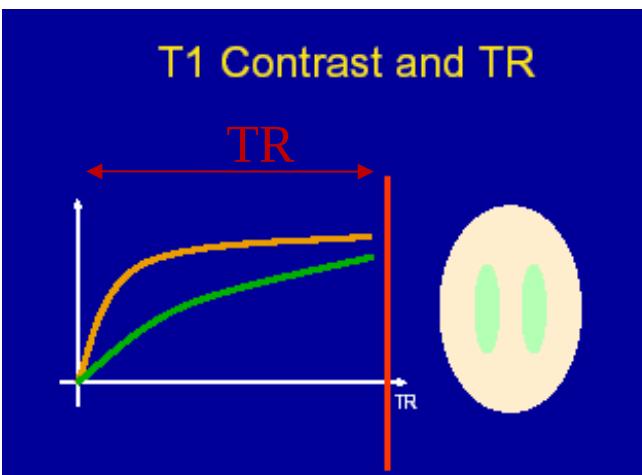
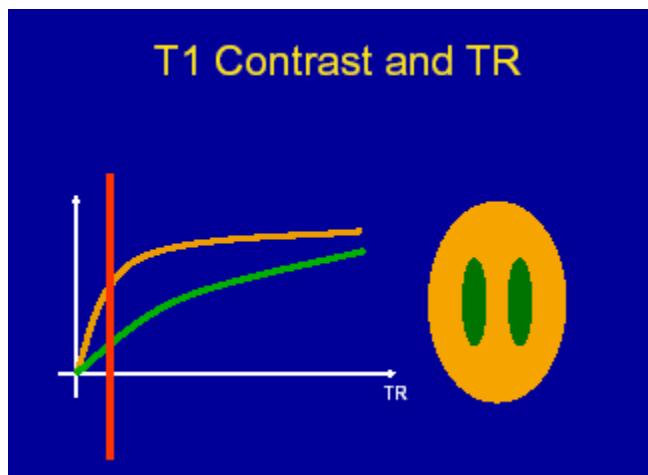
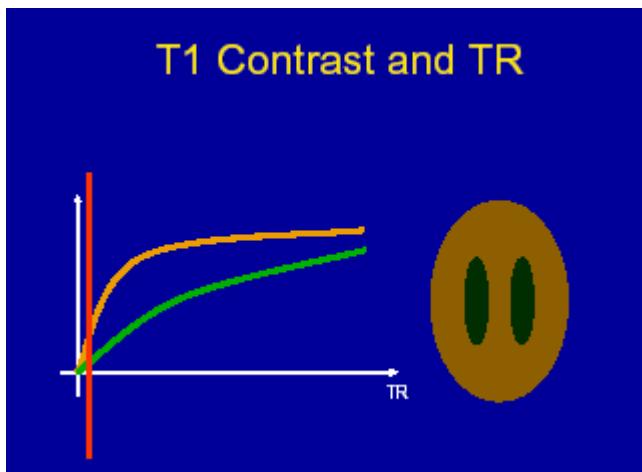
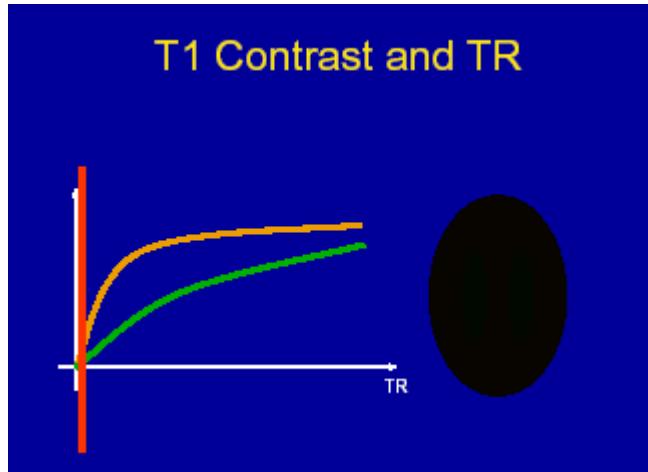


Example: changing contrast with TR

TR: Repetition Time (time between RF excitations of the magnetization)



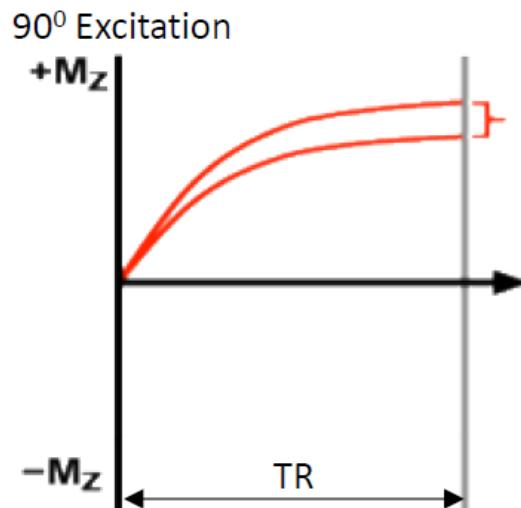
Example: changing contrast with TR



To optimize the contrast-to-noise ratio between tissues
we need to know T1 of the tissues of interest

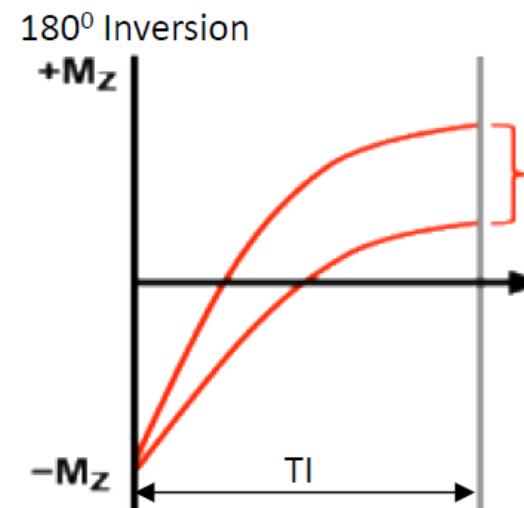
Better T1 contrast with «inversion pulse»

Behavior of Magnetization during T1 Relaxation



Saturation with a short TR

- TSE with TR = 400 – 700 ms
- GRE with TR = 3 – 200 ms



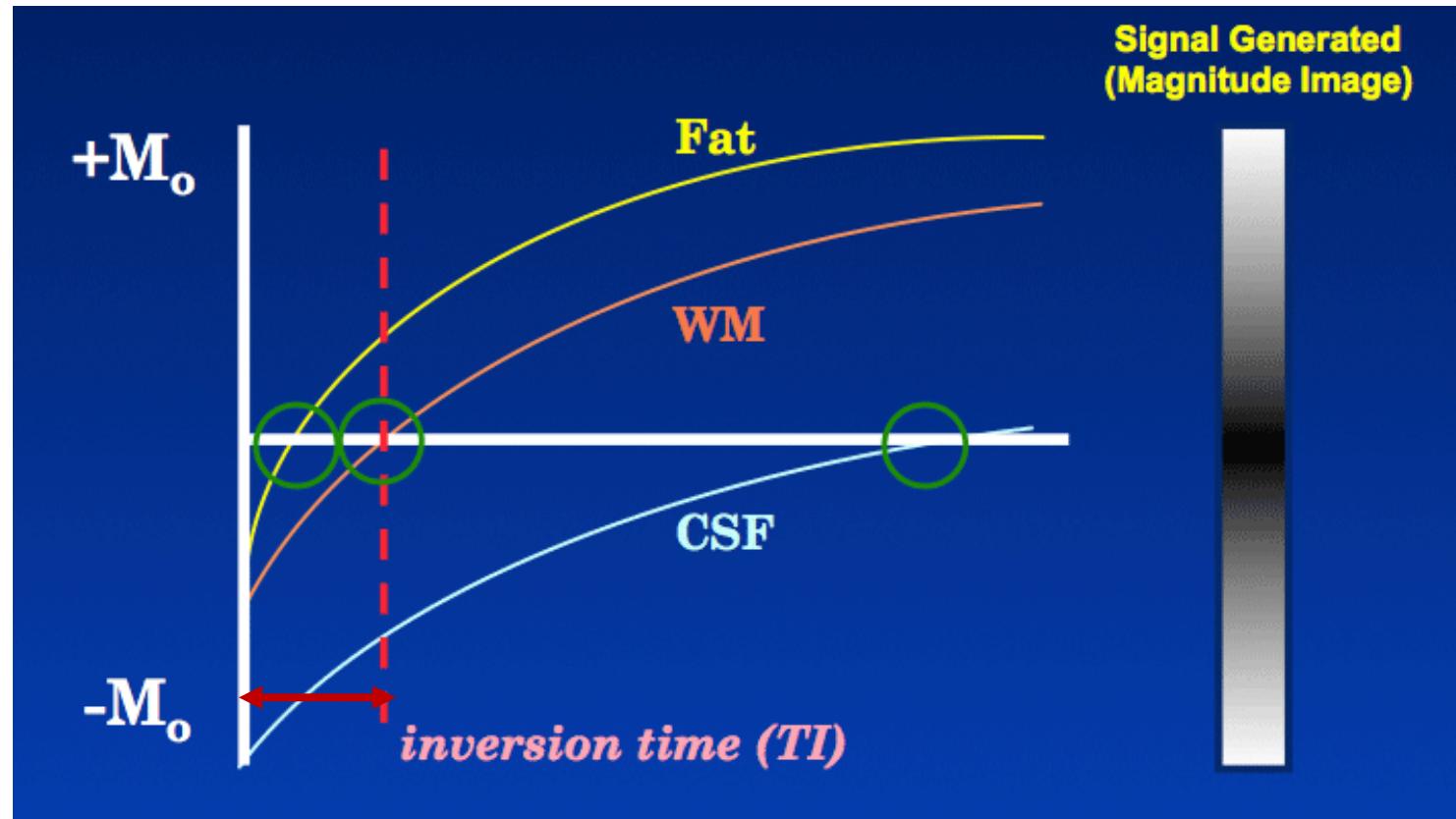
Preparation with IR

- T1 FLAIR
- IR-SPGR / MP-RAGE

Modified from: <http://mriquestions.com/why-use-ir.html>

Better T1 contrast with «inversion pulse»

Inversion time choice: selects tissue to «eliminate» from image

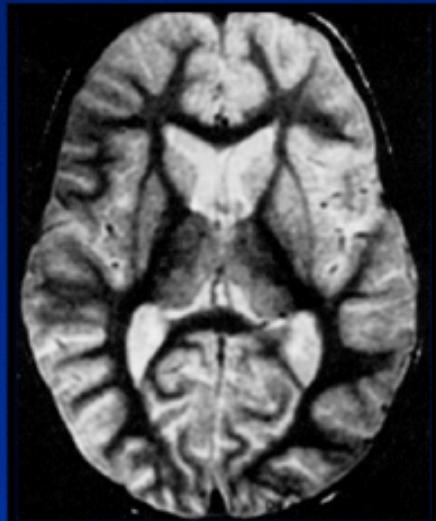


Longitudinal magnetization recovery after a
180° inversion pulse (WM: white matter, CSF: cerebral spinal fluid)

Source: <http://mriquestions.com/ti-to-null-a-tissue.html>

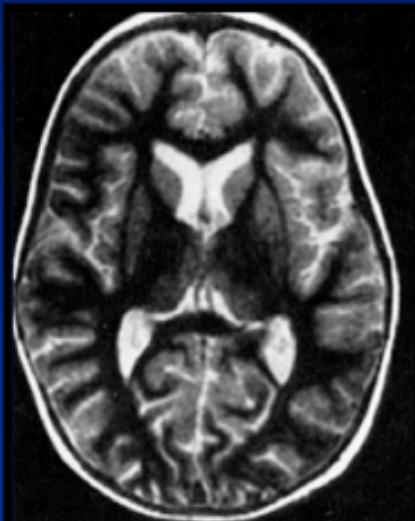
Better T1 contrast with «inversion pulse»

Choice of TI: selective suppression of tissue MRI signal



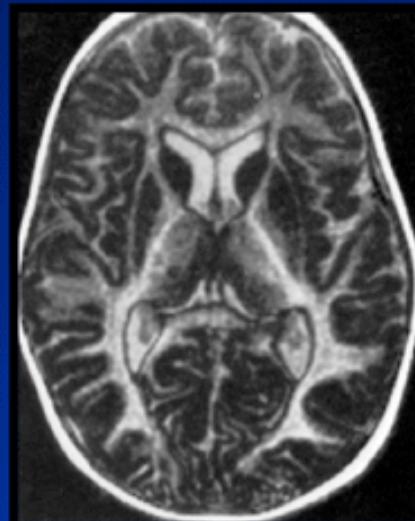
TI = 180 msec

Fat suppression
(STIR sequence)



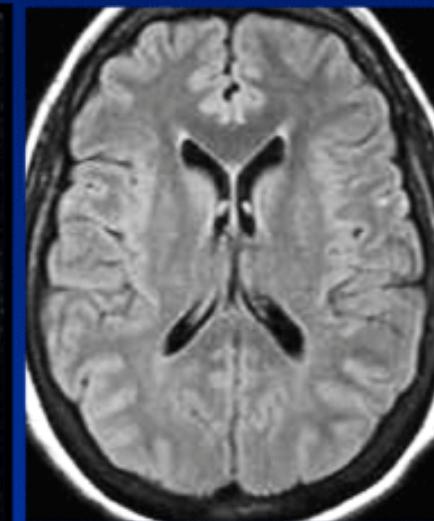
TI = 400 msec

White matter
suppression



TI = 650 msec

Gray matter
suppression



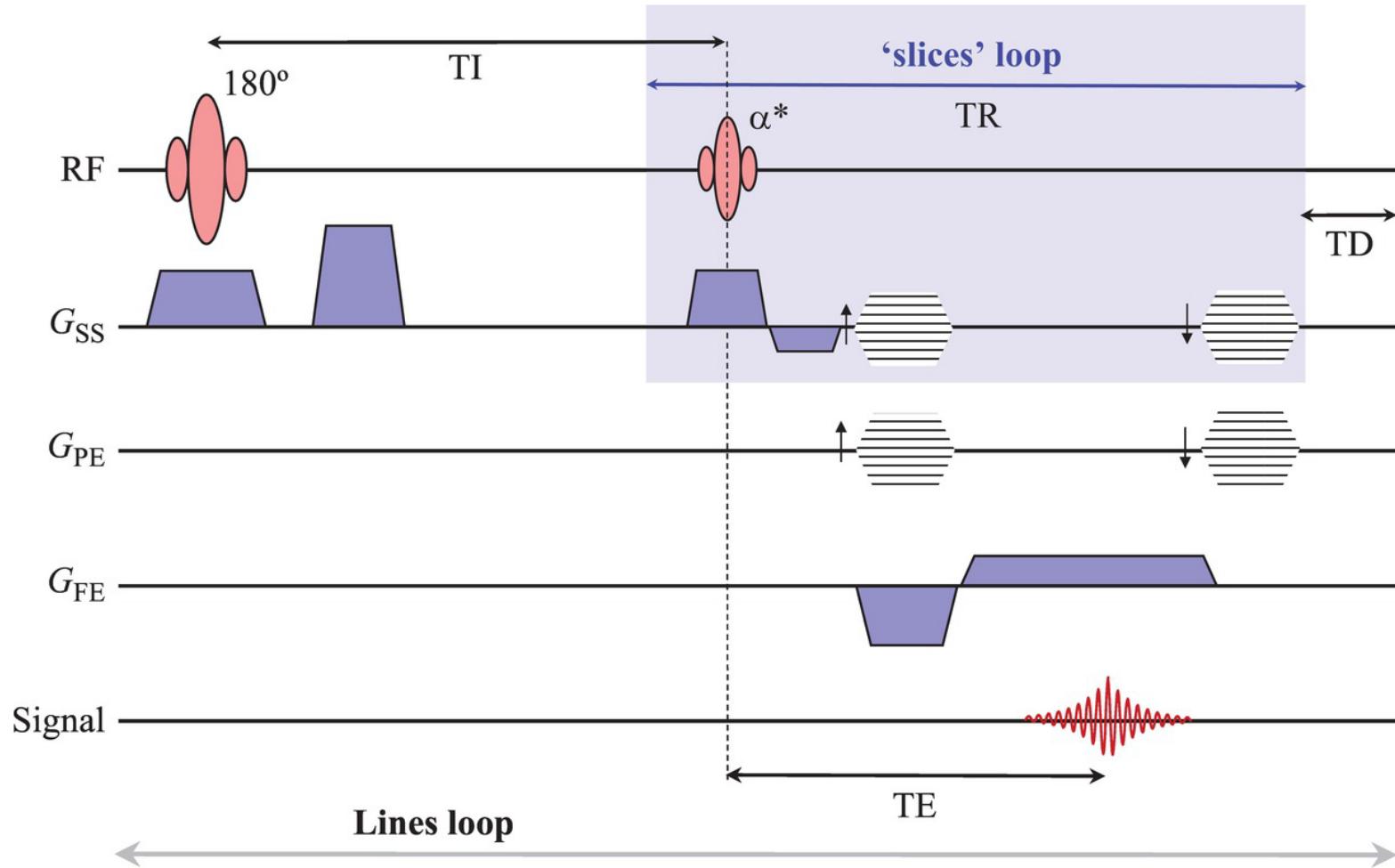
TI = 2500 msec

CSF suppression
(FLAIR sequence)

Source: <http://mriquestions.com/choice-of-ir-parameters.html>

Structural T1-weighted MRI: 3D MPRAGE

Magnetization Prepared Rapid Gradient Echo (MPRAGE)



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Before MRI data acquisition

0) Define what metrics do you need

Define your hypothesis testing criteria

This defines:

- acquisition protocol
- analyses strategies

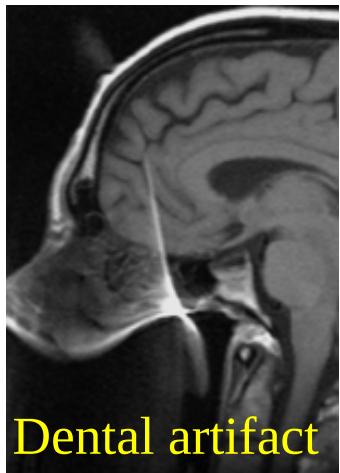
Structural analysis: first step

0) Define what metrics do you need

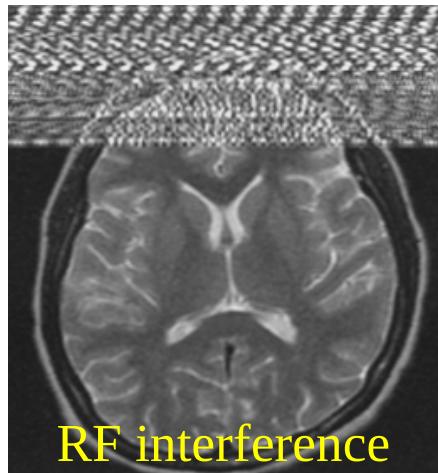
1) MRI quality control

- Problems with subject
 - Movement?
 - Inplants?
 - Lesions?
 - Position inside coil?
- Problems with sequence-parameters
 - Contrast good?
- Problems with MRI system
 - Inhomogeneities B0
 - Inhomogeneities B1
 - Instabilities
- Problems in laboratory
 - Interference with other equipment
- Etc.

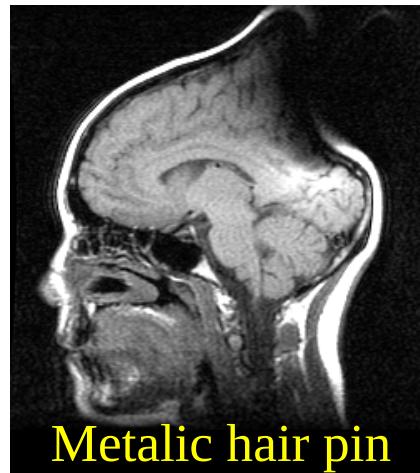
LOOK at images, LOOK for problems



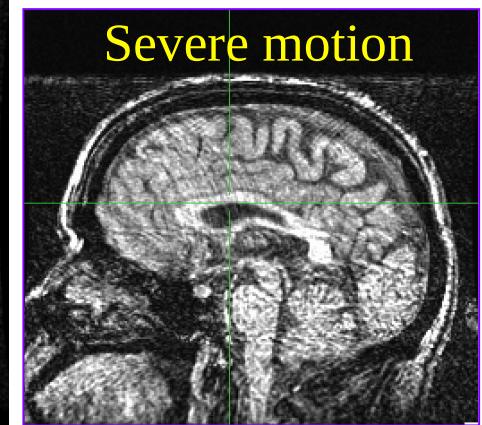
Dental artifact



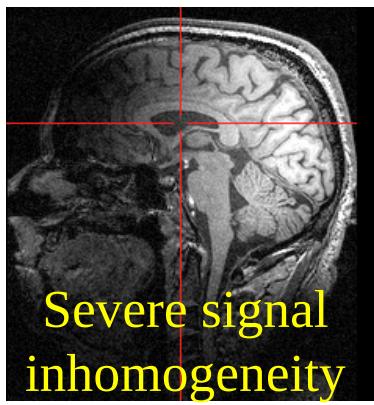
RF interference



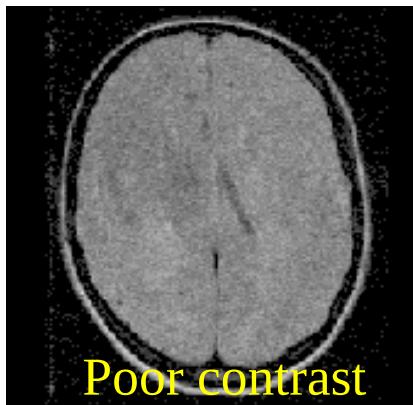
Metalic hair pin



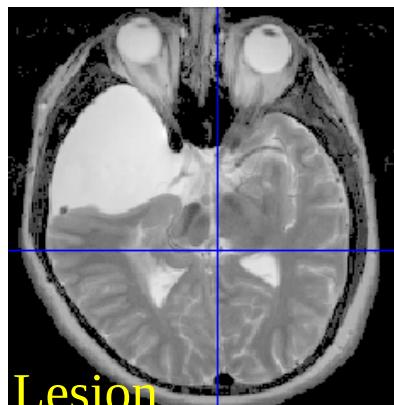
Severe motion



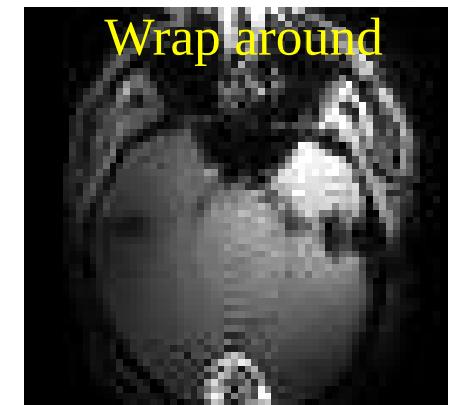
Severe signal inhomogeneity



Poor contrast

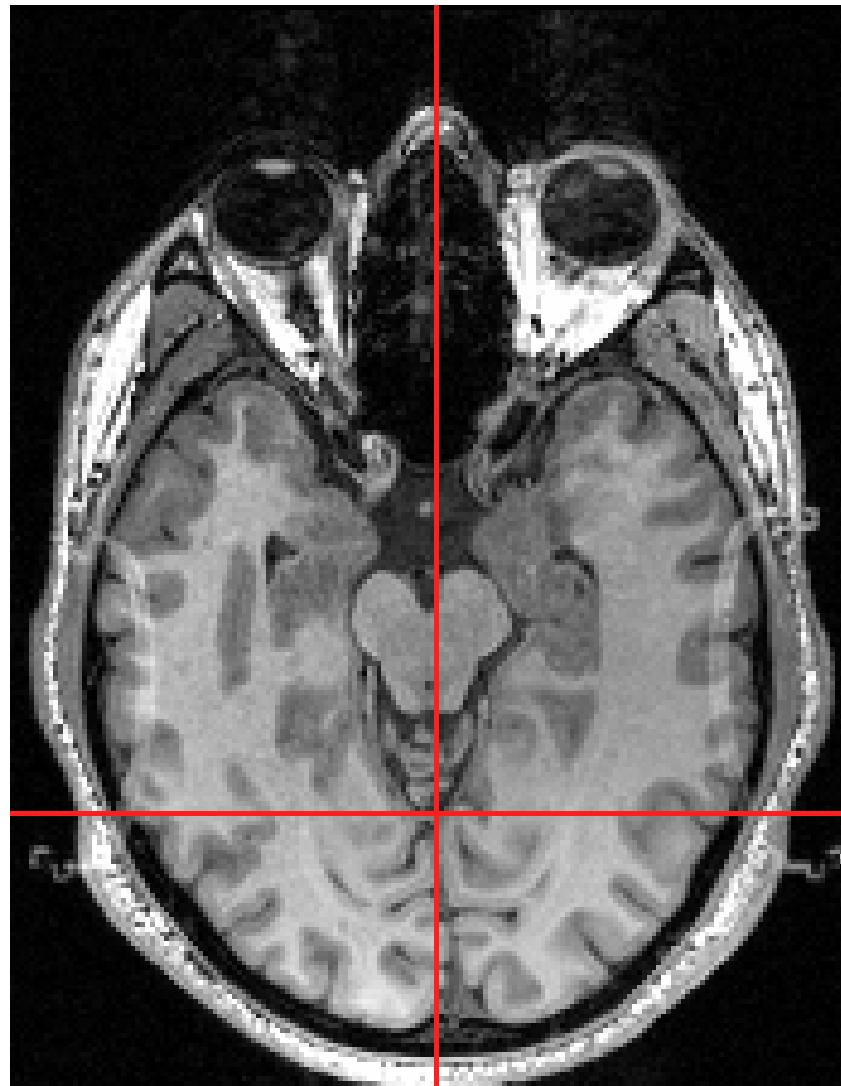


Lesion



Wrap around

Is this OK?



Structural MRI analysis

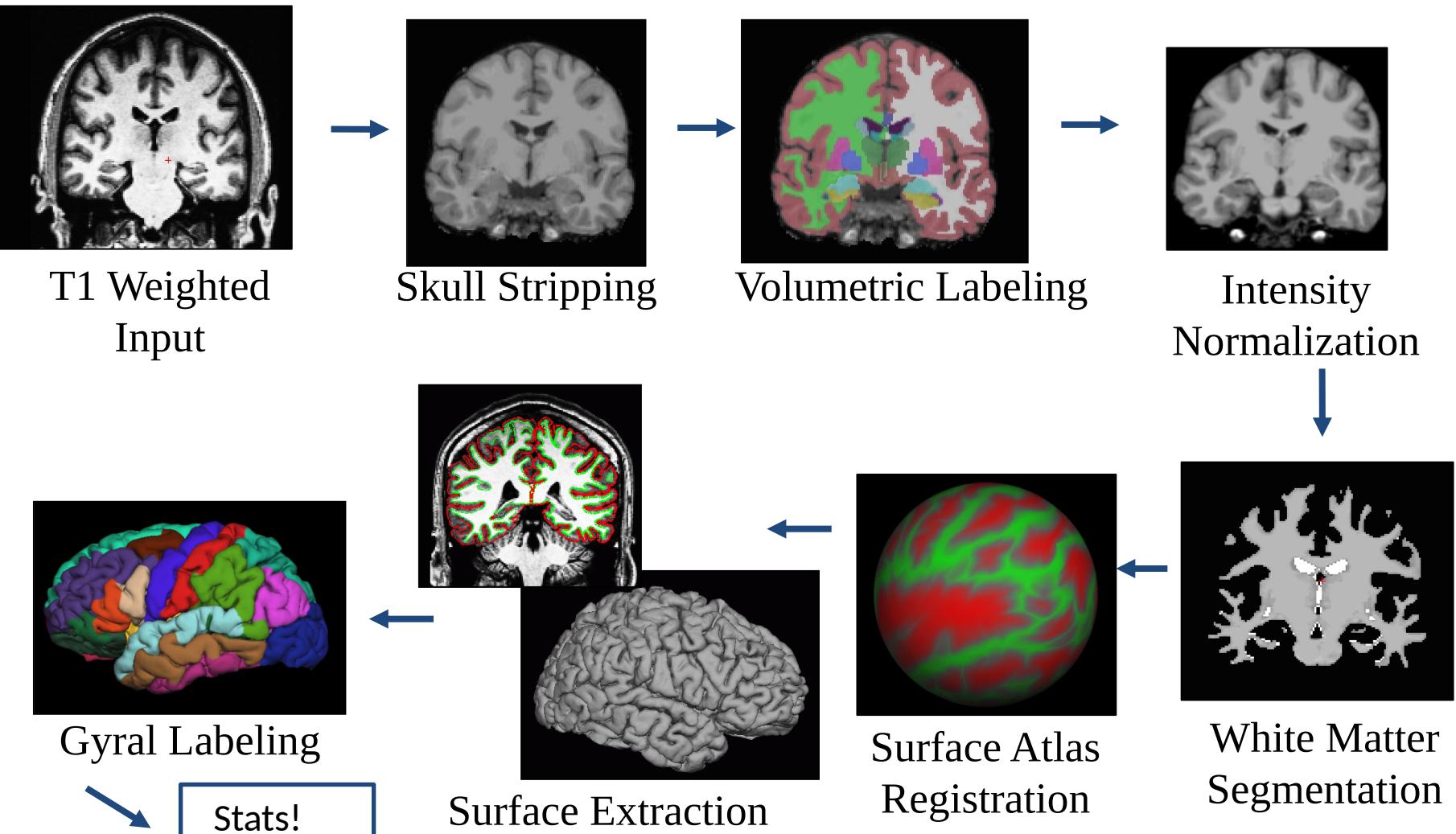
0. Define target metrics needed
1. MRI quality control
2. Metrics extraction will depend on experimental details

Examples:

- Segmentation of cortex, subcortical structures, ventricles
 - Acquire T1 (+ T2 for improved segmentation)
 - Brain morphometry (volumes, thickness, curvature, etc.)
- Lesion segmentation
 - Acquire T2* sequence for microvascular bleeding
 - Acquire FLAIR sequence for deep white matter lesions

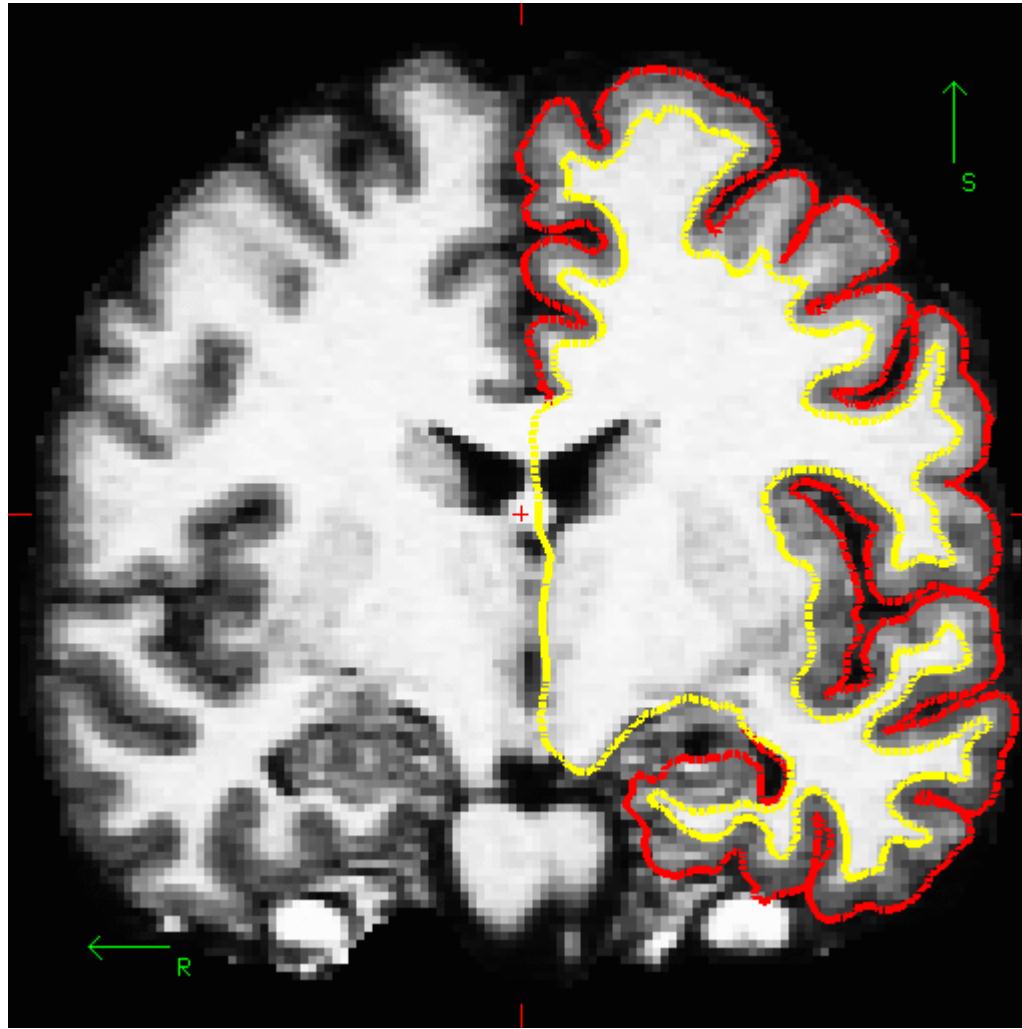
Example: Freesurfer segmentation

Fully automated segmentation of cortex, ventricles, subcortical structures



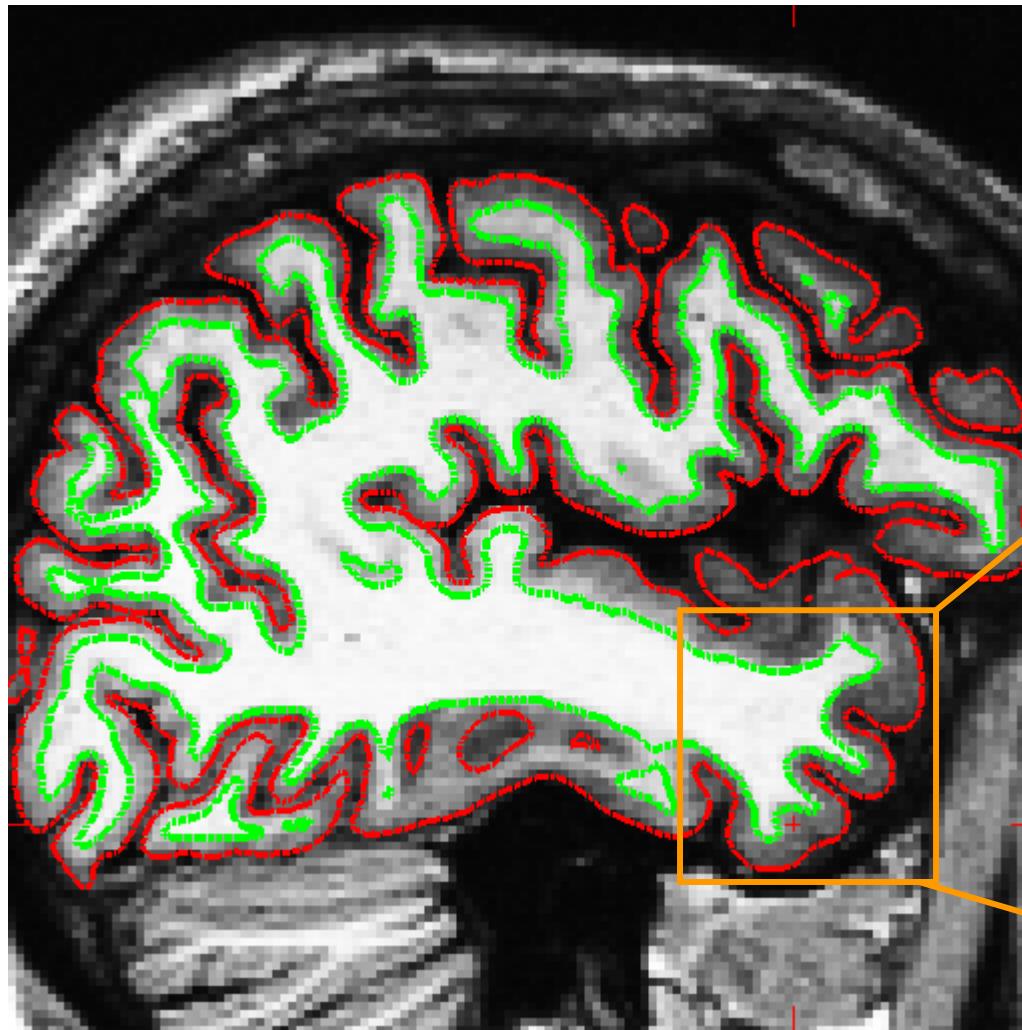
<https://surfer.nmr.mgh.harvard.edu/fswiki>

Freesurfer: WM/GM surface grows to pial surface

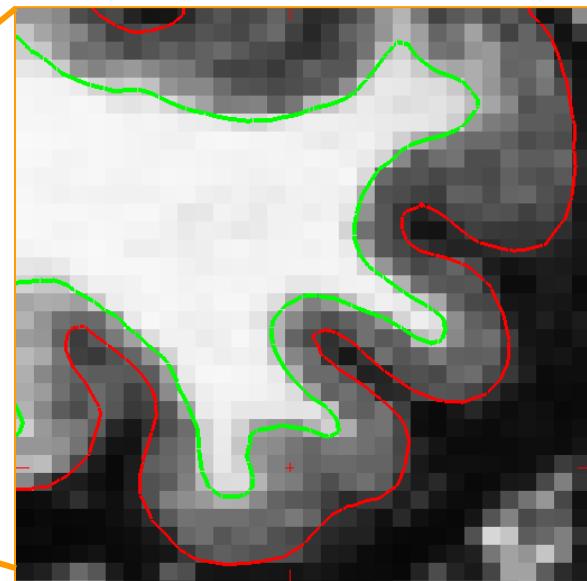


GM: gray matter
WM: white matter

Cortical segmentation needs good T1 contrast

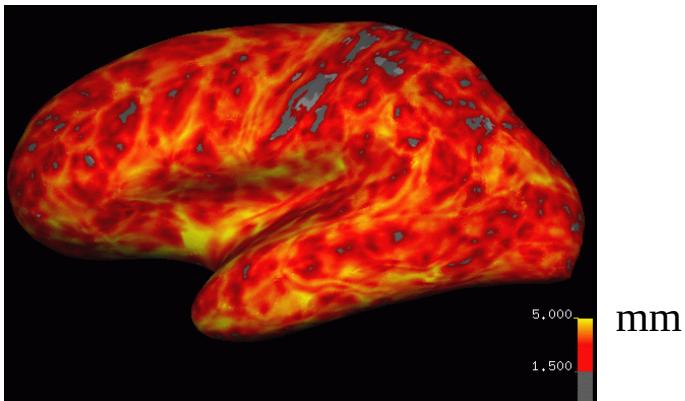


- Cortical surface models
- Cortical thickness estimates

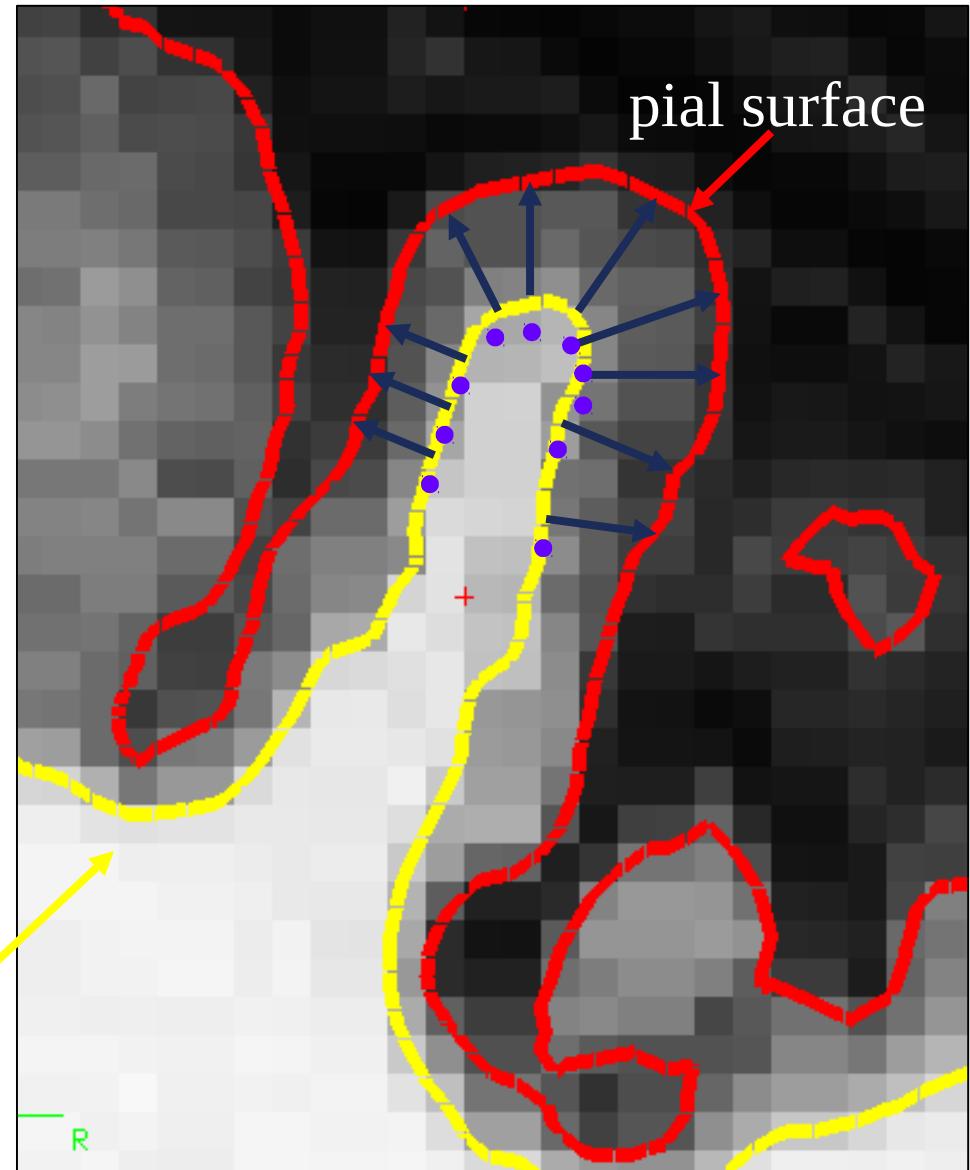


Cortical thickness estimations

- Distance between white and pial surfaces
- One value per vertex
- Surface-based more accurate than volume-based

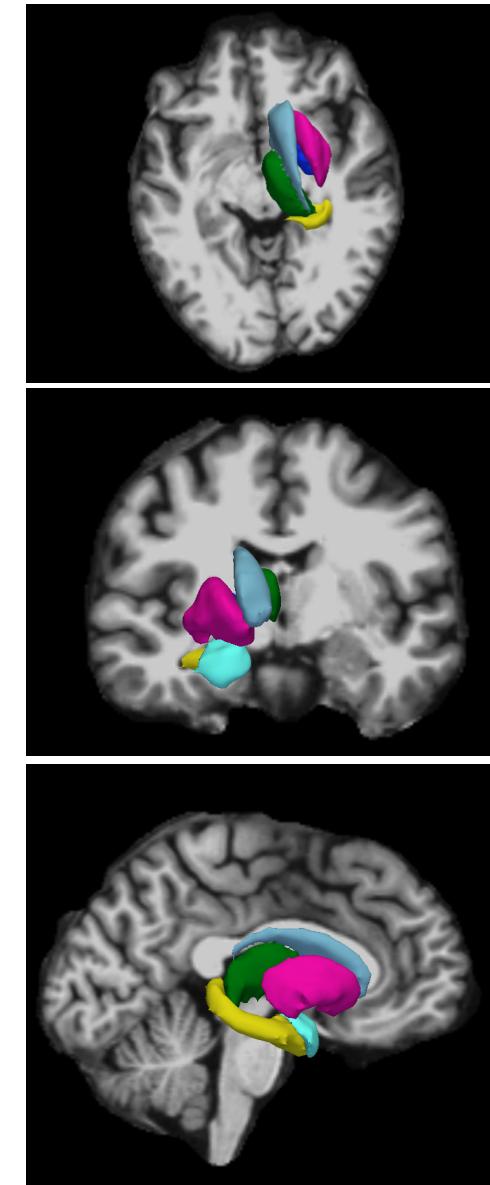
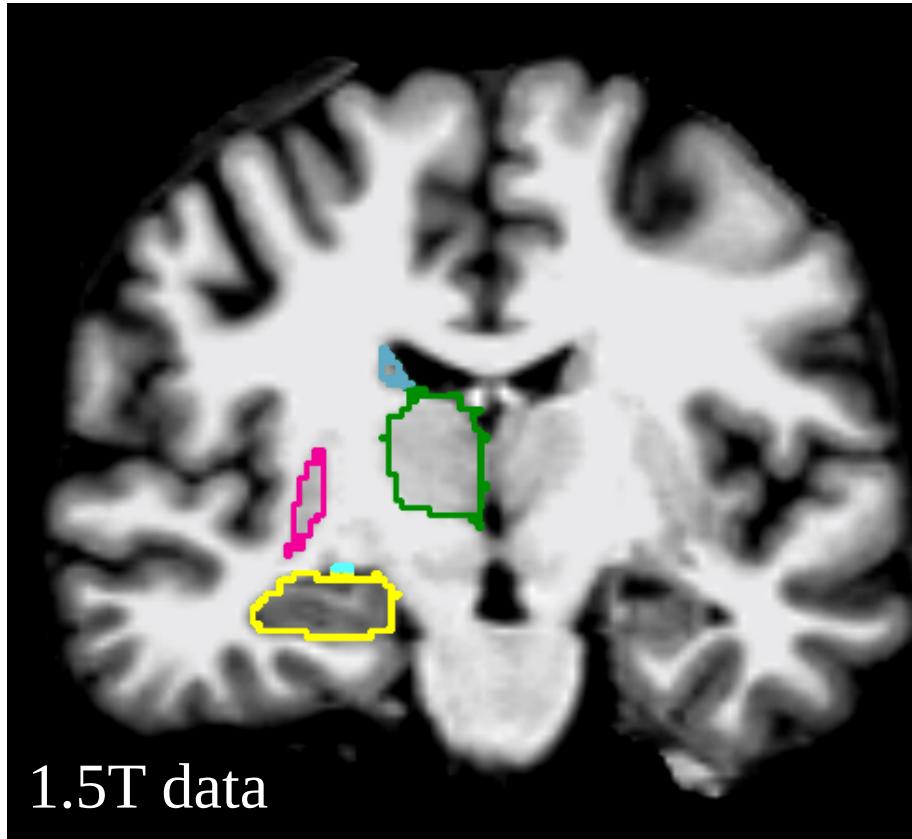


white/gray surface
lh.thickness, rh.thickness



Segmentation of subcortical structures

- Good gray/white contrast: subcortical structures segmentation
- Subcortical structures: ROIs for fMRI analyses
- Subcortical structures: Shape and volume characterization



Lecture 2 outline

Brain structure MRI

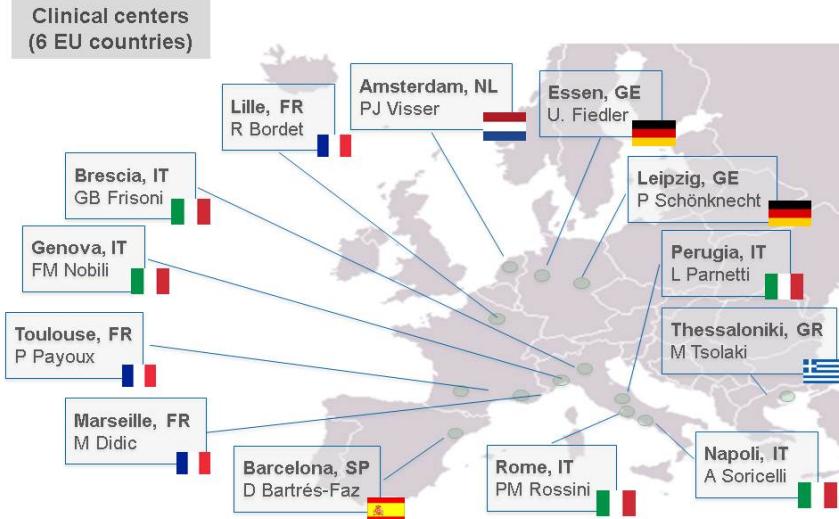
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Structural MRI: Application examples

- Medical anatomical information
- Anatomical information for functional studies
 - Registration with other MRI data
 - Same subject: other images, other acquisition sessions
 - Different subjects: group analyses
 - Registration with data from other modalities (PET, EEG, MEG)
 - Development of tissue models (dipoles for EEG, MEG)
- Morphometry analyses
 - Comparisons across populations (healthy or not)
 - Correlation with behavioural or demographics measures
 - Treatment effects (e.g., learning, therapeutical, etc.)
- Anatomical covariance (network analyses)
- Tissue mapping (T1, T2, T2*, myelin, etc.)

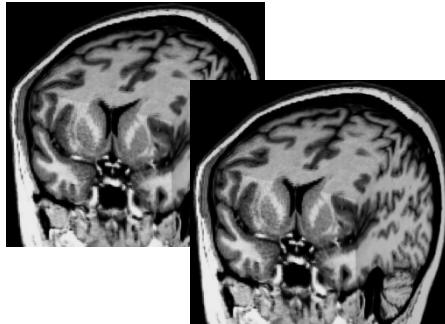
Structural MRI: multisite hippocampal segmentation to study Alzheimer's disease progression

Pharmacog Human MRI Consortium



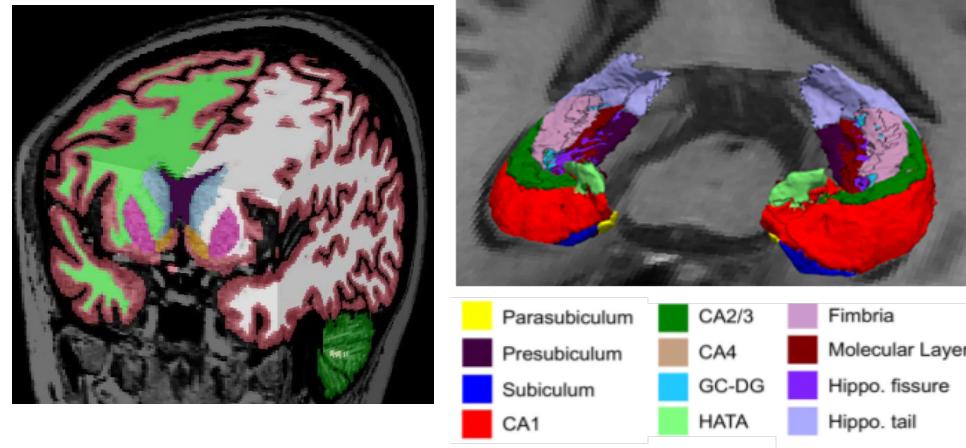
MR Vendor	Models	Sites (n=13)	Head RF Coils	Acceleration
Siemens (n=6)	Allegra	Verona	Birdcage	None
	TrioTim	Barcelona, Leipzig	8-ch	GRAPPA
	Skyra	Essen	20-ch	GRAPPA
	Verio	Marseille	12-ch	GRAPPA
	Biograph mMR	Napoli	12-ch	GRAPPA
Philips (n=4)	Achieva	Chieti, Peugia, Lille, Toulouse	8-ch	SENSE
GE (n=3)	HDxt	Genova, Amsterdam, Thessaloniki	8-ch	ASSET

Vendor
T1-weighted
3D MRI



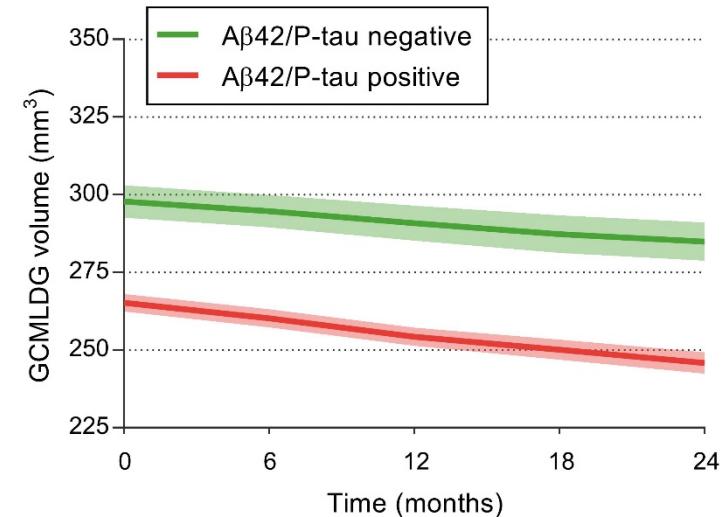
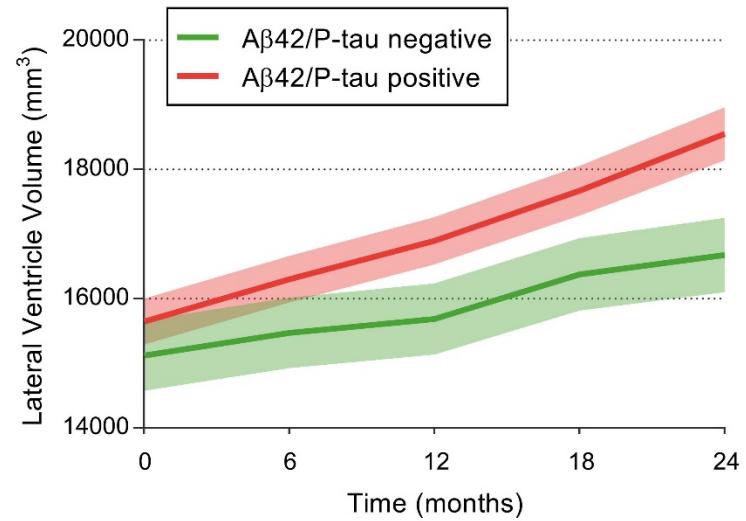
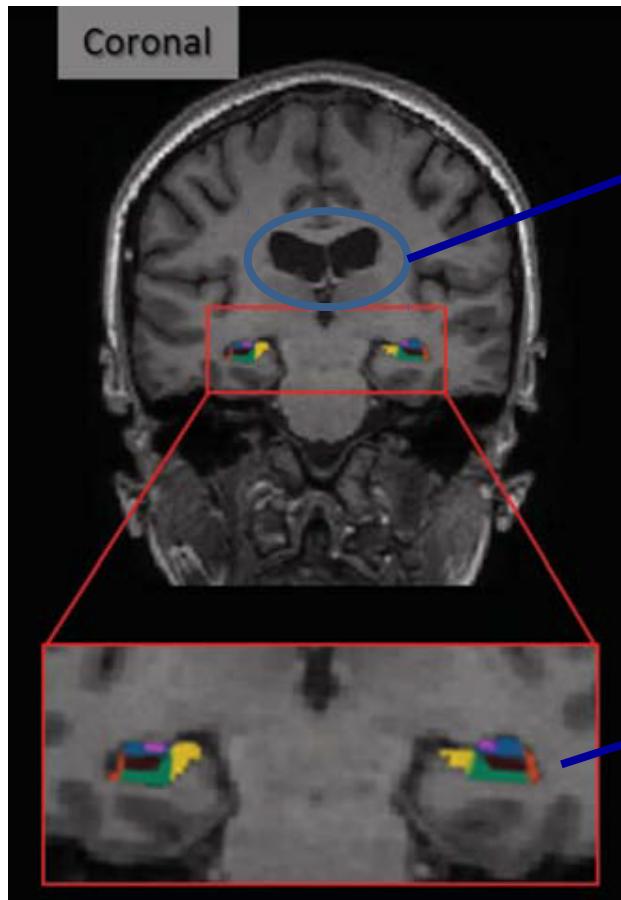
MPRAGE, 1x1x1 mm³

Two acquisitions (~5 min each)



Structural biomarkers with differential disease progression

- 150 amnestic Mild Cognitive Impaired patients
- Followed longitudinally: T0, T6, T12, T18, T24
- Separated in low risk (negative) and high risk (positive) based on CSF amyloid/p-tau levels



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3D MPRAGE: Most common brain T1

<https://www.ncbi.nlm.nih.gov/pubmed/?term=mprage+or+multiecho+mprage+or+mp2rage>

The screenshot shows a PubMed search results page. The search term 'mprage or multiecho mprage or mp2rage' is entered in the search bar. The results are sorted by 'Best Match'. There are 576 items, with the first 20 shown. The results include two articles:

1. Duché Q, Saint-Jalme H, Acosta O, Raniga P, Bourgeat P, Doré V, Egan GF, Salvado O. *Hum Brain Mapp.* 2017 Oct;38(10):5115-5127. doi: 10.1002/hbm.23719. Epub 2017 Jul 5. PMID: 28677254
Similar articles
2. Quantitative comparison of cortical surface reconstructions from MP2RAGE and multi-echo MPRAGE data at 3 and 7 T.

On the right side, there is a 'Results by year' chart showing the distribution of publications over time, with a 'Download CSV' button below it.

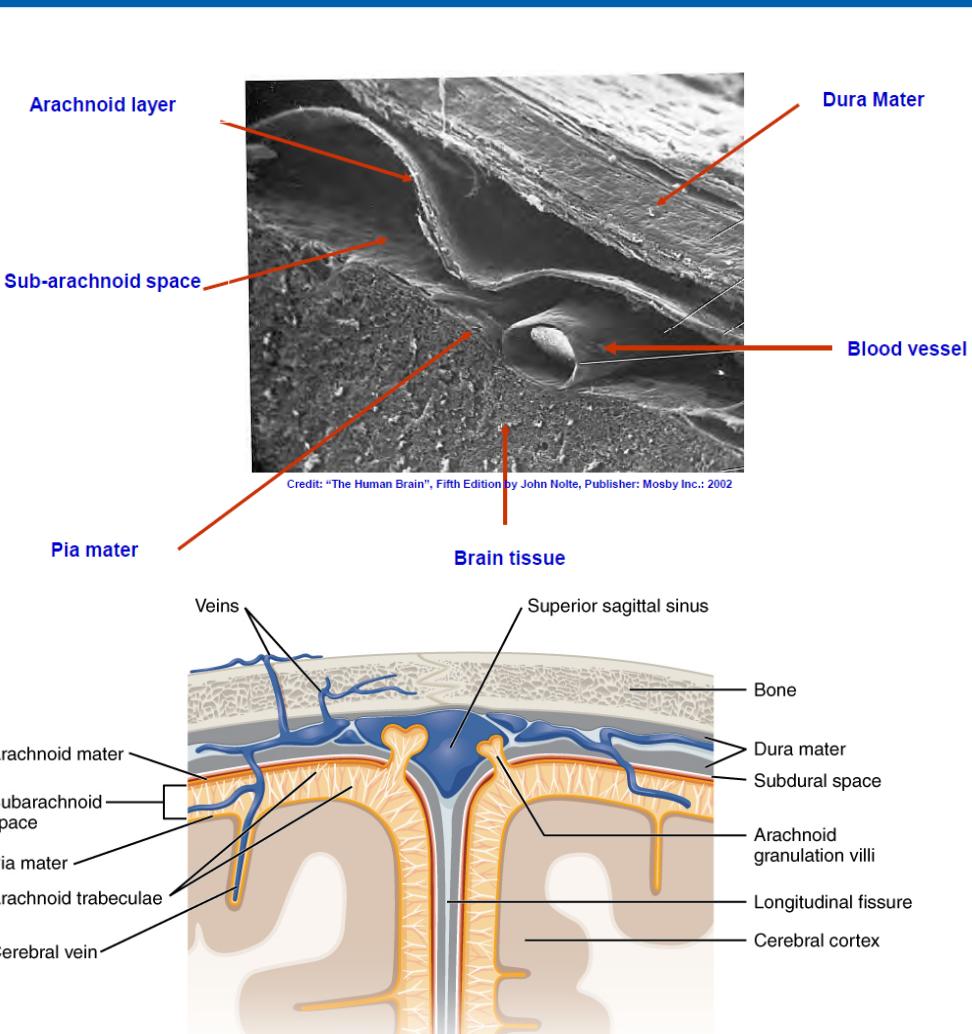
- **Lots of interest**
- **Lots of optimization work**

- Optimization criteria reflect challenges, and include:
 - Tissue contrast-to-noise ratio
 - Intensity non-uniformities
 - Image distortions
 - Spatial and temporal resolution
 - Strategies for motion correction
 - Reproducibility and accuracy of segmentations

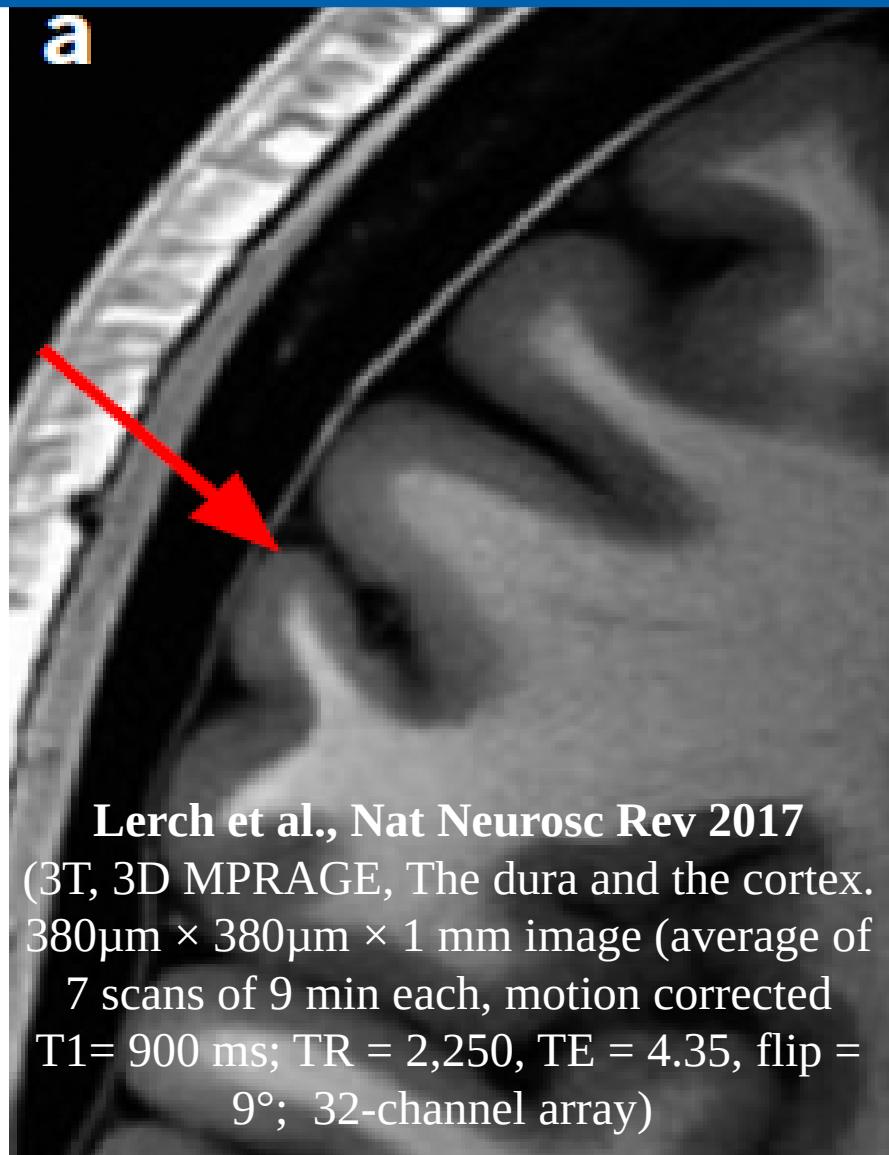
Structural MRI: Challenges

- **Optimization of image contrast**
- Head movement correction (retrospective, prospective)
- Optimization of spatial-temporal resolution
- Optimization of automated segmentations
- Validation of segmentations (histology)
- Multi-vendor protocol harmonization
- ...

Anatomical challenge: differentiate gray matter border (pial surface) from dura

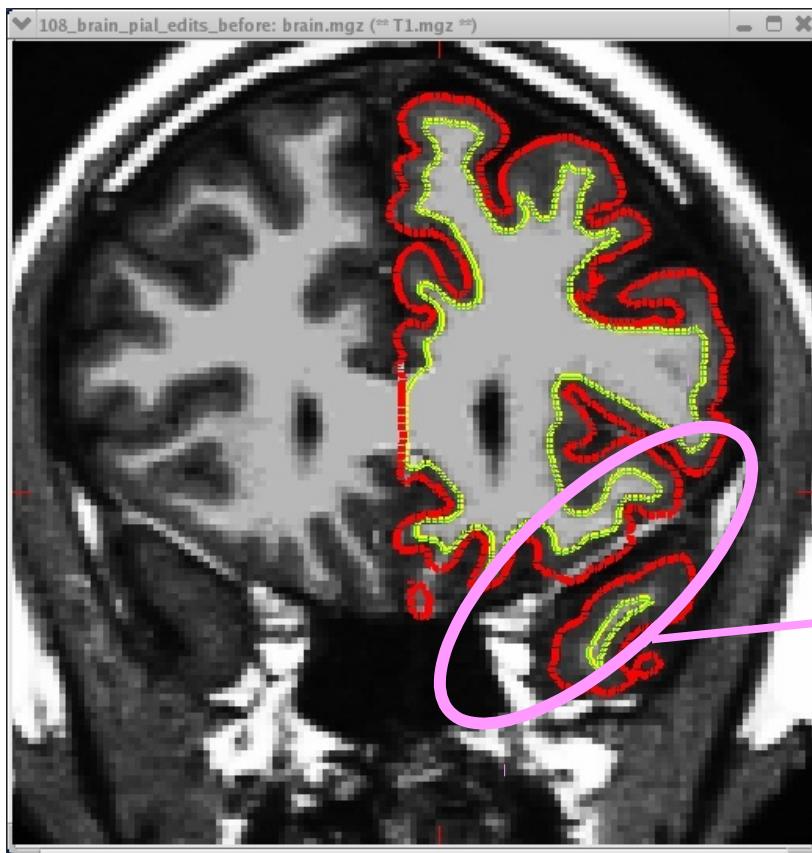


<https://en.wikipedia.org/wiki/Meninges>



Lerch et al., Nat Neurosci Rev 2017
(3T, 3D MPRAGE, The dura and the cortex.
380 μ m \times 380 μ m \times 1 mm image (average of
7 scans of 9 min each, motion corrected
T1 = 900 ms; TR = 2,250, TE = 4.35, flip =
9°; 32-channel array)

Pial misplacement



Segmentation errors:

Tissue that is neither white nor gray matter (like blood vessels, dura or pial), get wrongly classified as one of the two just because of similar image intensity values

Dura or Blood Vessel
White/Gray OK, but
Pial Inaccurate

Dura and GM have extremely similar intensity characteristics on most T1-weighted sequences (but different T2*!).

<https://surfer.nmr.mgh.harvard.edu/>

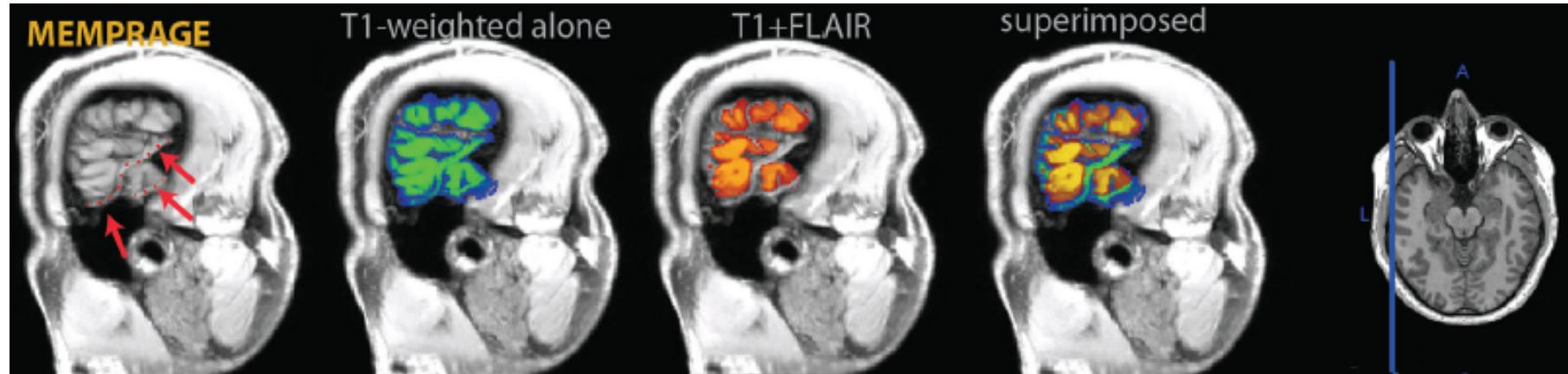
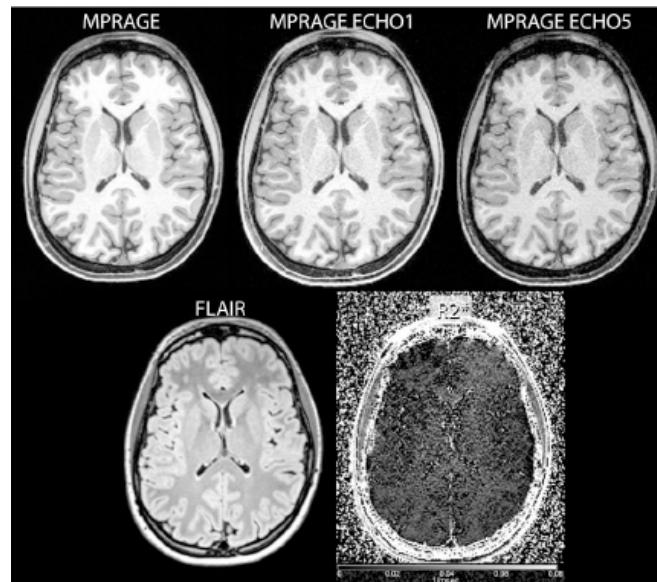
Gray matter segmentation errors



Multimodal MEMPRAGE, FLAIR, and R₂^{*} Segmentation to Resolve Dura and Vessels from Cortical Gray Matter

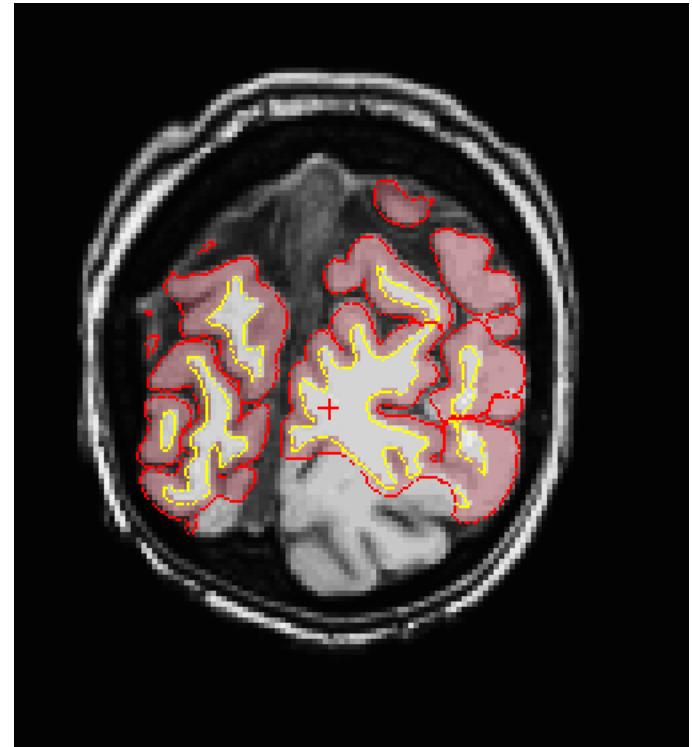
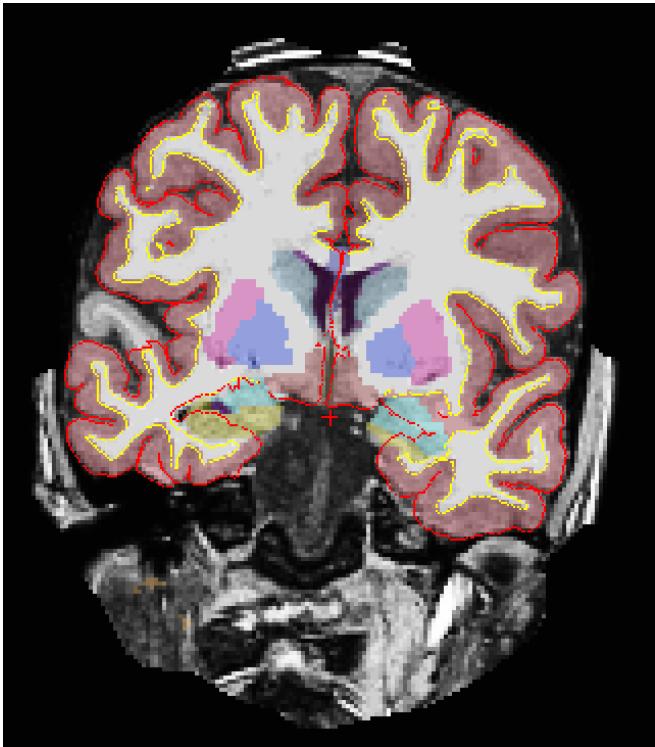
Roberto Viviani^{1,2*}, Eberhard D. Pracht³, Daniel Brenner³, Petra Beschoner⁴, Julia C. Stingl^{5,6} and Tony Stöcker^{3,7}

¹ Institute of Psychology, University of Innsbruck, Innsbruck, Austria, ² Psychiatry and Psychotherapy Clinic III, University of Ulm, Ulm, Germany, ³ German Center for Neurodegenerative Diseases (DZNE), Bonn, Germany, ⁴ Clinic for Psychosomatic Medicine and Psychotherapy, University of Ulm, Ulm, Germany, ⁵ Research Division, Federal Institute for Drugs and Medical Devices, Bonn, Germany, ⁶ Center for Translational Medicine, University of Bonn Medical School, Bonn, Germany, ⁷ Department of Physics and Astronomy, University of Bonn, Bonn, Germany



Missclassification of sulcal vessels as GM

Skull stripping errors



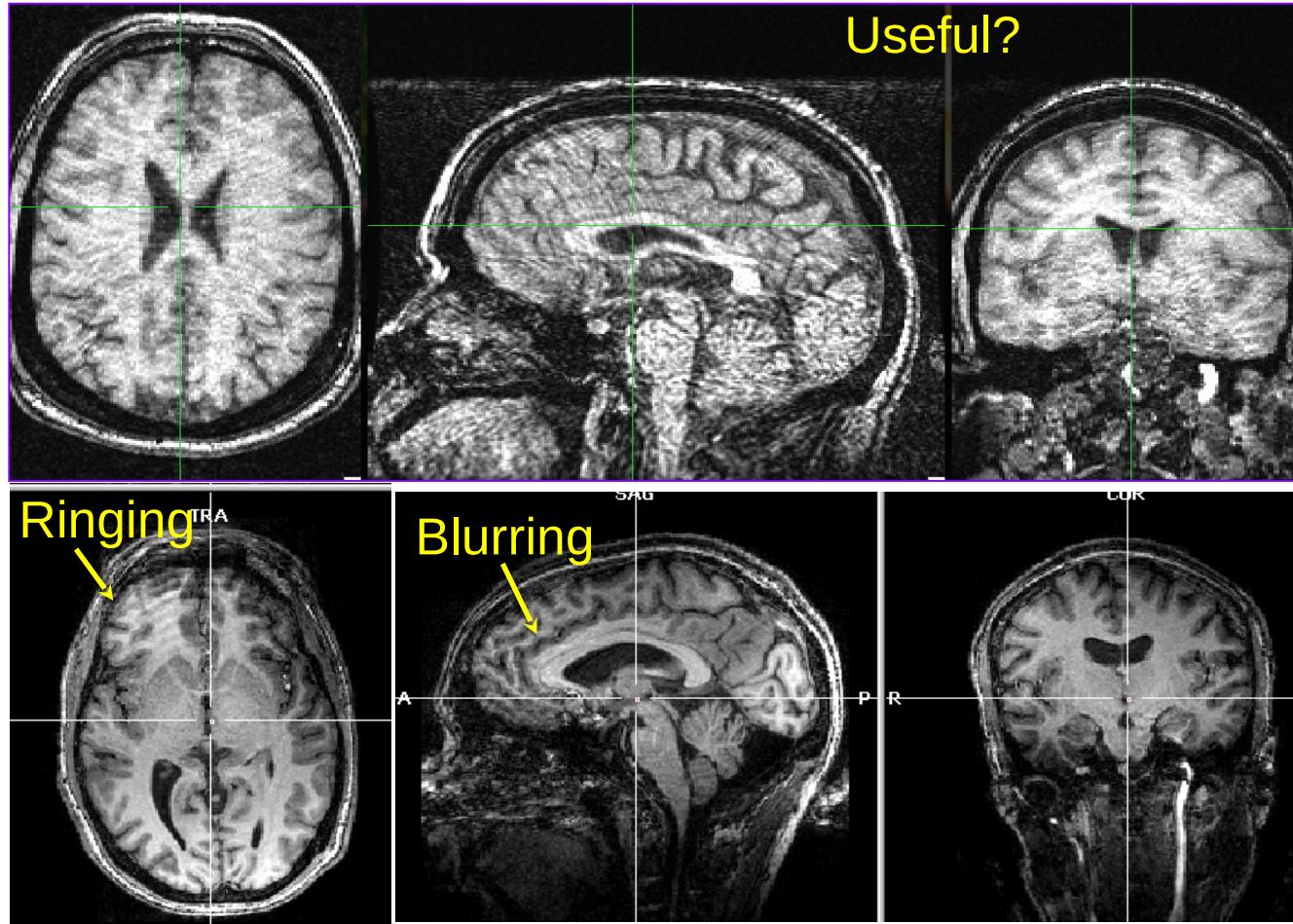
Parts of brain tissue removed
Such errors are ONLY detected by VISUAL quality assurance
YOU NEED TO LOOK AT THE DATA AND RESULTS

Structural MRI: Challenges

- Optimization of image contrast
- **Head movement correction (retrospective, prospective)**
- Optimization of spatial-temporal resolution
- Optimization of automated segmentations
- Validation of segmentations (histology)
- Multi-vendor protocol harmonization
- ...

Head motion in structural MRI

- Brain morphometry estimates are useful biomarkers
- Problem: head motion



Head motion biases morphometry data

NeuroImage 107 (2015) 107–115



Contents lists available at ScienceDirect

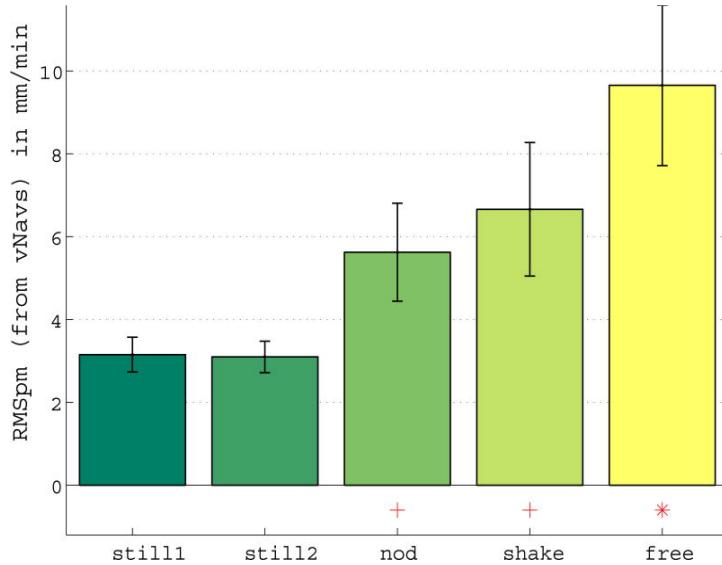
NeuroImage

journal homepage: www.elsevier.com/locate/ynimng

Head motion during MRI acquisition reduces gray matter volume and thickness estimates

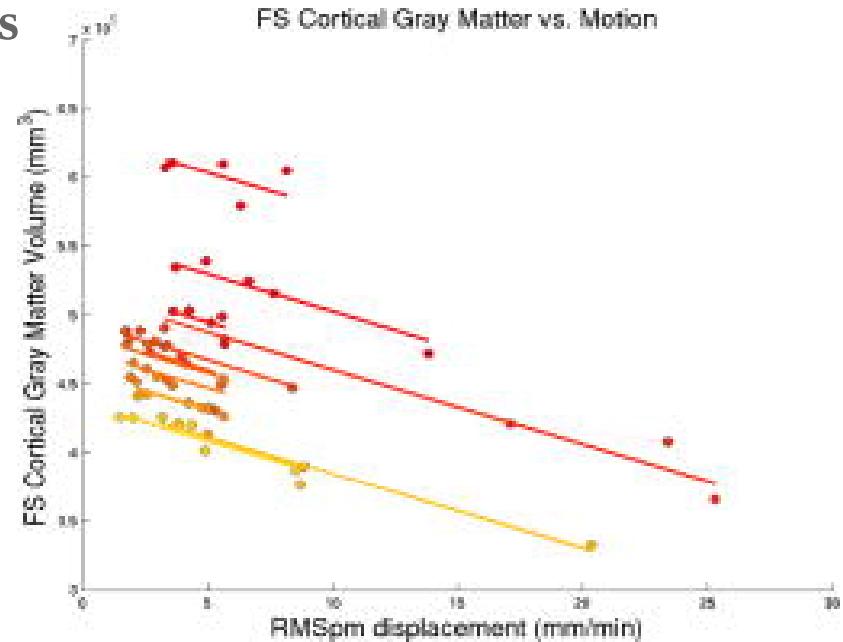
Martin Reuter ^{a,b,c,d,*}, M. Dylan Tisdall ^{b,d,1}, Abid Qureshi ^{a,d}, Randy L. Buckner ^{b,d}, André J.W. van der Kouwe ^{b,d}, Bruce Fischl ^{b,c,d}

Different Motion Levels across Motion Types



Experiment design:

- 12 healthy adults, 3T MRI
- For each subject:
 - Scan still
 - Scan during 3 motion conditions
- Segment both scans
- Quantify morphometry changes



Prospective motion correction reduces biases

NeuroImage 127 (2016) 11–22



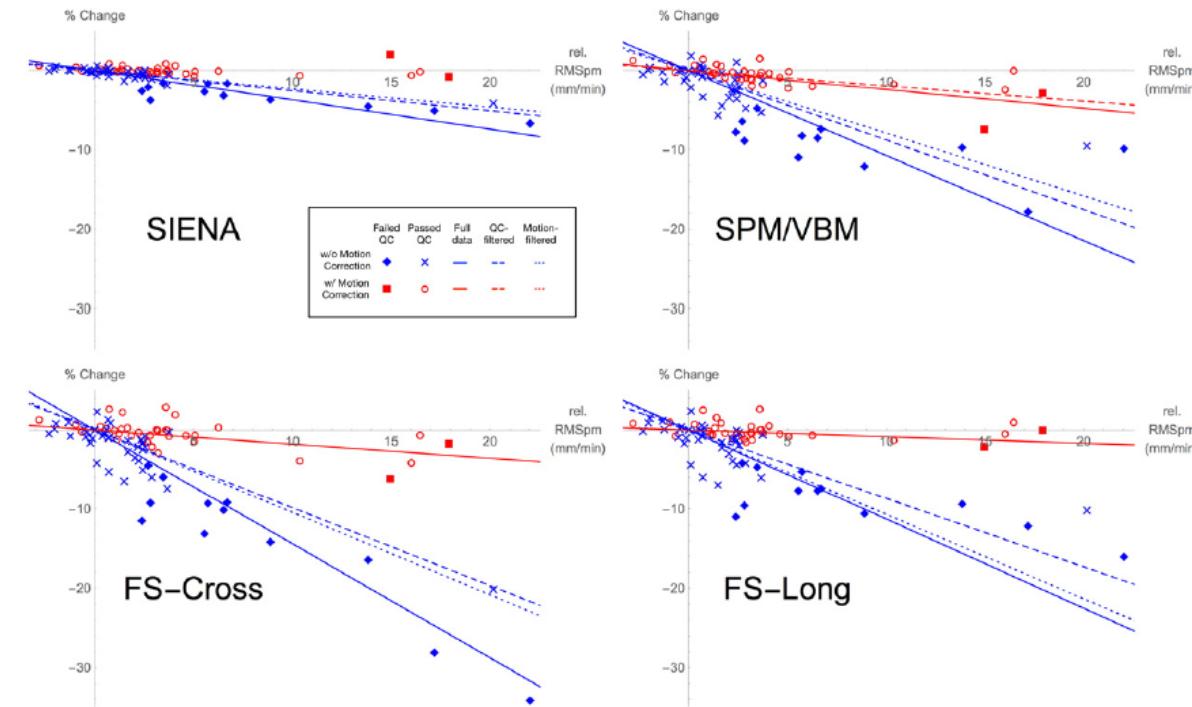
Contents lists available at ScienceDirect

NeuroImage

journal homepage: www.elsevier.com/locate/ynim

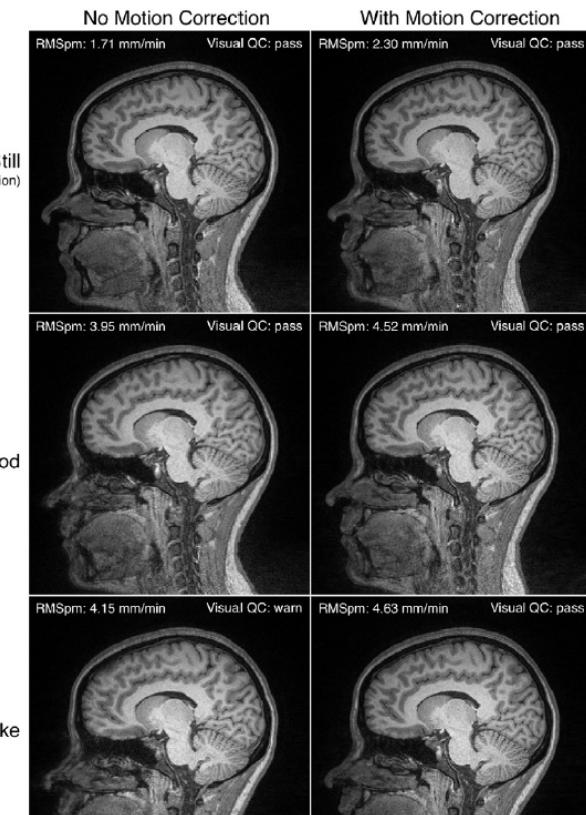
Prospective motion correction with volumetric navigators (vNavs) reduces the bias and variance in brain morphometry induced by subject motion

M. Dylan Tisdall ^{a,b,*}, Martin Reuter ^{a,c,g,1}, Abid Qureshi ^c, Randy L. Buckner ^{a,d,e,f}, Bruce Fischl ^{a,b,g}, André J.W. van der Kouwe ^{a,b}



Experiment design:

- 12 healthy adults, 3T MRI
- For each subject:
 - Scan still
 - Scan during 3 motion conditions (no mc)
 - Scan during 3 motion conditions (mc)
- Segment both scans
- Quantify morphometry changes



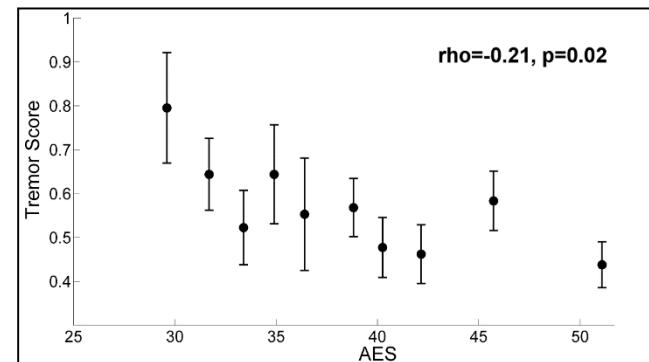
Estimation motion degree from MPRAGE

Method for Retrospective Estimation of Natural Head Movement During Structural MRI

Domenico Zacà, PhD,* Uri Hasson, PhD, Ludovico Minati, PhD, and

Jorge Jovicich, PhD

J. MAGN. RESON. IMAGING 2018;00:000–000.



3D MPRAGE: Parkinson's Progression Markers Initiative

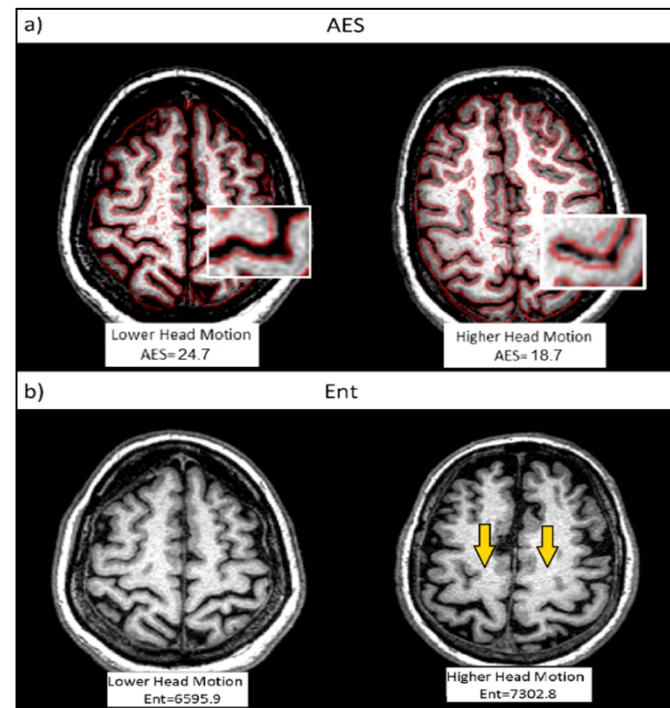
Groups	Age (years)	Gender
HC: n=84	59.6 ± 10.9	M 54/ F 30
PD: n=124	60.4 ± 9.8	M 77/F 47
Group differences	$T=-0.44, p=0.66$	$X^2=0.10, p=0.75$

Motion Metrics evaluated:

- Average Edge Strength (AES)
- Image entropy

$$AES = \frac{\sqrt{\sum_{i,j} E(I_{i,j}^k) [(G_x(I_{i,j}^k))^2 + (G_y(I_{i,j}^k))^2]}}{\sum_{i,j} E(I_{i,j}^k)}$$

$$Ent = - \sum_{p=1}^n \frac{I_p}{I_{tot}} \ln \left(\frac{I_p}{I_{tot}} \right) \quad I_{tot} = \sqrt{\sum_{p=1}^n I_p^2}$$



Structural MRI: Challenges

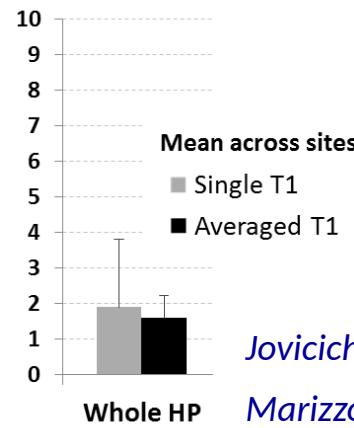
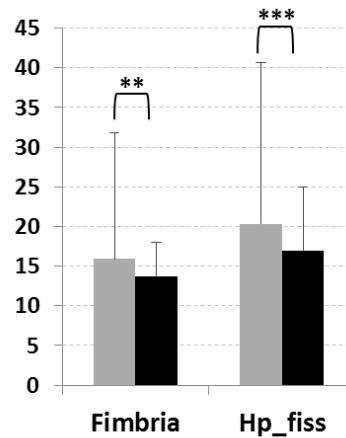
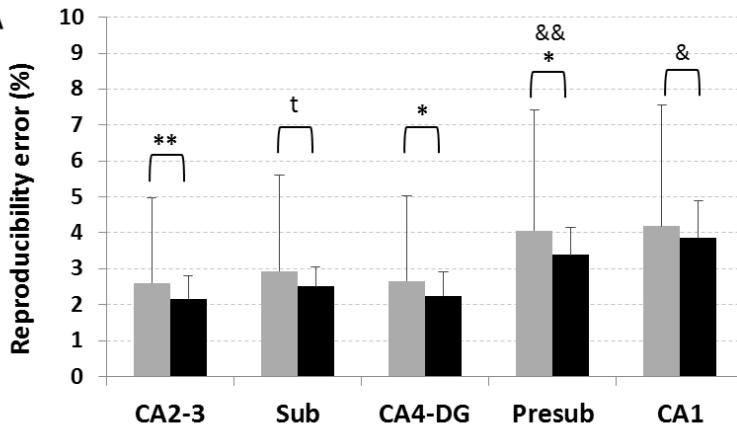
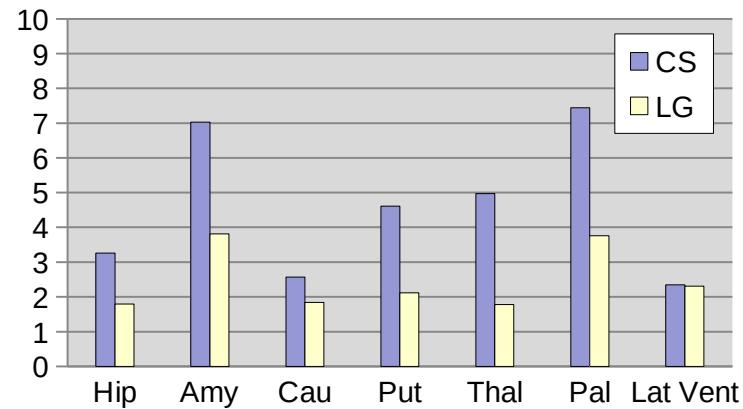
- Optimization of image contrast
- Head movement correction (retrospective, prospective)
- Optimization of spatial-temporal resolution
- Optimization of automated segmentations
- Validation of segmentations (histology)
- **Multi-vendor protocol harmonization**
- ...

Multicentric morphometry optimizations

Pharmacog study findings for structural T1 harmonization:

- Despite MR site variability, vendor sequences + harmonized protocol give good quality automated segmentations
- Accelerated MPRAGE \sim non-accelerated
 - Time efficient, lower head motion sensitivity
- Longitudinal Freesurfer (LG) more reliable than cross-sectional Freesurfer (CS)
- Averaging 2 MPRAGE improves hippo. subfields

Absolute % volume reproducibility error

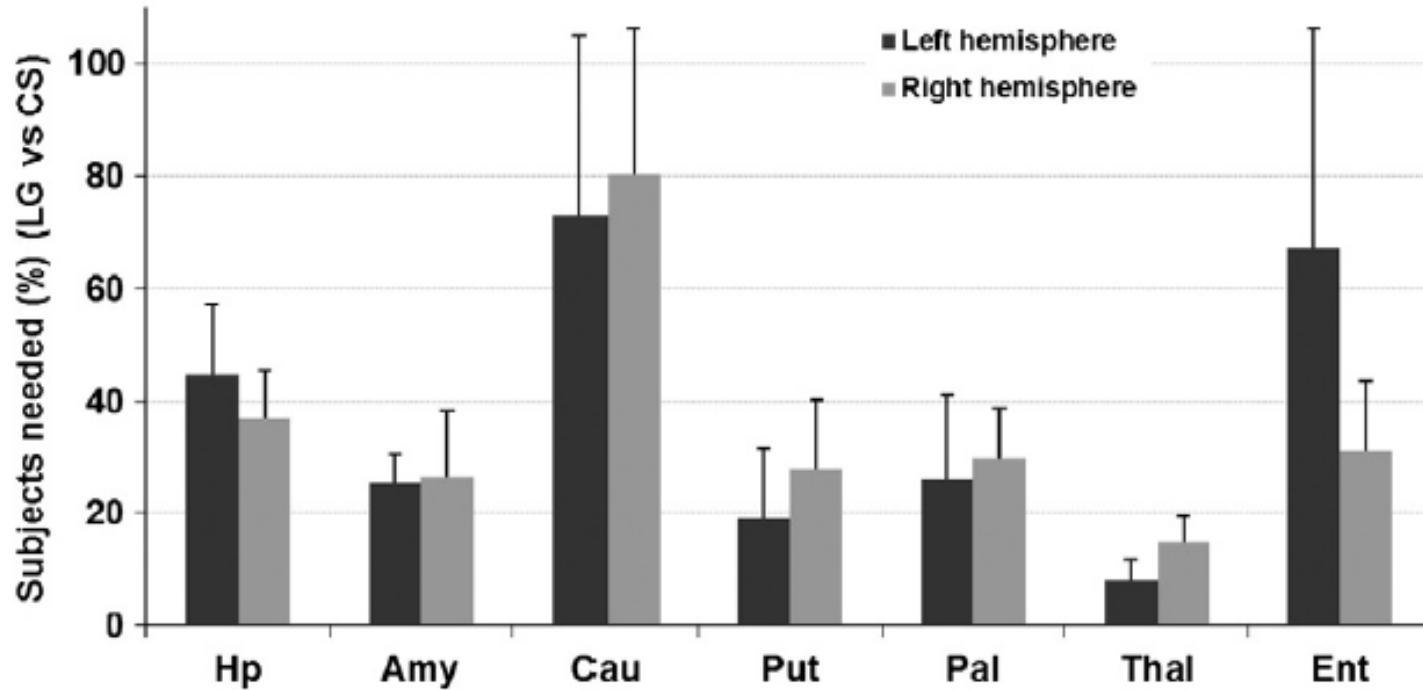


Jovicich et al., Neuroimage 2013

Marizzoni et al., Neuroimage 2015

Multicentric morphometry optimizations

Practical consequences of reproducibility improvements



Sample size ratio needed to have the same power analysis using LG instead of CS stream. The percentage of subjects needed is less than 50% for most of the structures considered.

Left and right hemispheric structure labels are: Hp = hippocampus, Amy = amygdala, Cau = caudate, Put = putamen, Pal = pallidum, Thal = thalamus and Ent = entorhinal cortex.

Lecture 2 outline

Brain structure MRI

- What is a structural MRI?
- What is image contrast?
- How can image contrast be manipulated?
- What image analyses are common from brain structural MRI?
- What are some structural MRI applications?
- What are some structural MRI challenges?

Complementary reading

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REVIEW

FOCUS ON HUMAN BRAIN MAPPING

nature neuroscience

Studying neuroanatomy using MRI

Jason P Lerch^{1,2}, André J W van der Kouwe^{3,4}, Armin Raznahan⁵, Tomáš Paus^{6–8}, Heidi Johansen-Berg⁹, Karla L Miller⁹, Stephen M Smith⁹, Bruce Fischl^{3,4,10} & Stamatis N Sotiroopoulos^{9,11}

The study of neuroanatomy using imaging enables key insights into how our brains function, are shaped by genes and environment, and change with development, aging and disease. Developments in MRI acquisition, image processing and data modeling have been key to these advances. However, MRI provides an indirect measurement of the biological signals we aim to investigate. Thus, artifacts and key questions of correct interpretation can confound the readouts provided by anatomical MRI. In this review we provide an overview of the methods for measuring macro- and mesoscopic structure and for inferring microstructural properties; we also describe key artifacts and confounds that can lead to incorrect conclusions. Ultimately, we believe that, although methods need to improve and caution is required in interpretation, structural MRI continues to have great promise in furthering our understanding of how the brain works.

314 VOLUME 20 | NUMBER 3 | MARCH 2017 **NATURE NEUROSCIENCE**

Free brain segmentation software tools include:

Freesurfer: <https://surfer.nmr.mgh.harvard.edu/fswiki>

SPM: <https://www.fil.ion.ucl.ac.uk/spm/>

ANTS: <http://stnava.github.io/ANTs/>

FSL: <https://fsl.fmrib.ox.ac.uk/fsl/fslwiki/FAST>



NeuroImage

SUPPORTS OPEN ACCESS

Articles in press Latest issue Sp

Segmenting the Brain

Edited by Cameron Craddock, Pierre Bellec, Saad Jbabdi
Volume 170, Pages 1-494 (15 April 2018)

<https://www.sciencedirect.com/journal/neuroimage/vol/170/suppl/C>

- Functional connectivity parcellation (9)
- Segmentation of different structures (9)
- Atlas of (sub)cortical cytoarchitectonics areas (3)
- White matter bundles (4)
- Quality of cortical models (3)
- Multi-modality (task) areal parcellation (5)
- Automated segmentation of structural MRI data (5)

Concept map for lectures

Lecture 1

NMR Signal origin

- Powerful magnet
- Radio frequency
- Magnetic field gradients

MR Image & Contrast

- Spatial encoding
- Magnetic gradients
- Pulse sequences

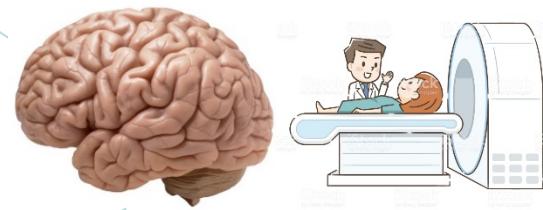
MR Safety

- Powerful magnet
- Radio frequency
- Magnetic field gradients

Lecture 2

Structural MRI

- Contrast, important parameters
- Sequences & artifacts
- Analyses & applications



Lecture 3

Diffusion MRI

- Contrast, important parameters
- Sequences & artifacts
- Analyses & applications

Lecture 4

Functional MRI

- Contrast, important parameters
- Sequences & artifacts
- Pre-processing