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# A Review of Medical Image Segmentation Algorithms

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#### **Abstract**

INTRODUCTION: Image segmentation in medical physics plays a vital role in image analysis to identify the affected tumour. The process of subdividing an image into its constituent parts that are homogeneous in feature is called Image segmentation, and this process concedes to extract some useful information. Numerous image segmentation techniques have been developed, and these techniques conquer different restrictions on conventional medical segmentation techniques. This paper presents a review of medical image segmentation techniques and statistical mechanics based on the novel method named as Lattice Boltzmann method (LBM). The beauty of LBM is to augment the computational speed in the process of medical image segmentation with an accuracy and specificity of more than 95% compared to traditional methods. As there is not much information on LBM in medical physics, it is intended to present a review of the research progress of LBM.

OBJECTIVE: As there is no review paper on the research progress of the LB method, this paper presents a review with an objective to give some thought regarding the different segmentation for medical image and novel LB method to advance interest for future investigation and exploration in medical image segmentation.

METHODS: This paper in attendance a short review of medical image segmentation techniques based on Thresholding, Region-based, Clustering, Edge detection, Model-based and the novel method Lattice Boltzmann method (LBM).

CONCLUSION: In this paper, we outlined various segmentation techniques applied to medical images, emphasize that none of these problem areas has been acceptably settled, and all of the algorithms depicted are available for broad improvement. Since LBM has the benefits of speed and adaptability of modelling to guarantee excellent image processing quality with a reasonable amount of computer resources, we predict that this method will become a new research hotspot in image processing.

**Keywords:** Segmentation, Medical Physics, Radiation Therapy, Computed Tomography (CT), Magnetic Resonance Imaging (MRI), Radiotherapy treatment planning systems (RTPS), Image processing, Image analysis, Thresholding, Edge detection, Clustering, lattice Boltzmann method (LBM)

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#### 1. Introduction

Image processing techniques have become progressively significant in a wide assortment of applications with sophisticated techniques and instruments. Image segmentation is an exemplary subject in image processing

and further hotspot and focal point in image processing techniques. Image segmentation is a technique of partitioning an image into sub constituent parts, remarkably homogenous in feature and this process concede to extract some useful information. Image segmentation accepts a part prominent position in image analysis. Medical images take part in health care as the



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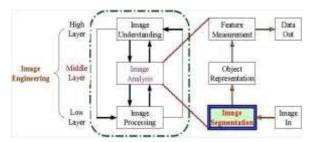
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medical image's quality influences the diagnosis and treatment. Segmentation is significant in medical image analysis and intends to draw out some details from the images. Those images can be utilized for high-level image understanding. Scientifically speaking, segmentation is a hypothetical middle-level vision task performed by neurons between low-level and high-level cortical areas, as schematically shown in figure 1[1]. Segmentation of clinical images intends to find anatomic structures and portray their limits on a computerized source. Especially in Radiotherapy (RT), Imaging is an essential part of the therapy routine since it utilizes to perceive the therapy target and ordinary structures to abstain from irradiation. Hence, Radiotherapy treatment planning systems (RTPS) require anatomical data to be portrayed on CT scans. The treatment target and ordinary structures are physically depicted on CT scans by clinicians. Segmented clinical images are moved to an RTPS for computing radiation dose. Hence, precise segmentation is crucial for the patient treatment result. For the reasons of radiotherapy treatment, segmentation quality incorporates spatial precession and dose computation exactness, which are firmly related [2, 3]. Image segmentation aims to partition the medical image into elemental parts or objects in the medical image with uniform and similar features. One of them is intensity, a colour that relates to anatomical structures, tumours, etc. The degree of segmentation is application dependent, and there is no universal theory of image segmentation. Distinct segmentation methods or algorithms have been proposed in the literature. These techniques conquer different restrictions on conventional medical segmentation techniques. Choice of specific techniques or algorithm over the other depends on the problem's image type and nature. Recent advances in image segmentation techniques have frequently been reviewed [4, 5]. These review articles are driven by classifying the methods utilized for processing pixel data voxel data and their applications in diagnosis, treatment planning and follow up studies; However, methods that have been applied in practice, a shortcoming still exists, an obvious one is a computational speed. This paper in attendance a short review of medical image segmentation techniques based on Thresholding, region-based, Clustering, edge detection, model-based, and the novel method Lattice Boltzmann method (LBM) to augment the computational speed, which is based on the microscopic description of the macroscopic physical process. As there is no review paper on the LB method's research progress, this paper presents a review to give some thought regarding the different segmentation for medical images and novel LB method to advance interest for future investigation and exploration in medical image segmentation.



**Figure 1.** Image Engineering and Image Segmentation [1]

# 2. Segmentation techniques

Of late, a lot of endeavours have been concentrating on the segmentation process. Distinct segmentation methods or algorithms have been discussed in the literature. These methods conquer different restrictions on conventional medical division techniques. Yet, there isn't so much as one single strategy to be considered a better technique for different kinds of images; those techniques are only suitable for particular images and applications. Image division techniques can be grouped into [6] Thresholding, Region growing & region merging and splitting, Clustering, Edge detection and Model-based methods. All segmentation techniques depend on two essential things of intensity values, discontinuity, and similarity. The discontinuity proceeds towards segment the image based on an instantaneous change in intensity levels in an image or grey levels of an image. In this technique, our interest predominantly focuses on the recognition of isolated points. The second approach is based on the pixels, which are similar in some range as per the preset criteria upon which images are segmented, includes approaches like Thresholding, Region growing, and region splitting and merging.

## 3. Thresholding approach

Thresholding is the primary method of image segmentation, in which one threshold value is used to change a greyscale image into a binary image. This procedure's important thing is to choose the threshold value (T), pixels with intensity over and above the foreground region's threshold value, and all other pixels in the background region [7]. A few famous strategies utilized in the industry are "The maximum entropy method" [8], Otsu's method (maximum) variance [9]. Kmeans clustering [9] can also be used in this regard. The presence of noise and obscure boundaries influences Thresholding segmentation and performs well for the images with sharp edges [9]. To invalidate the impact of Thresholding smoothing noise on Thresholding with Edge detection are two regular strategies.



# 4. Region-based methods

There are three essential techniques for Region-based Segmentation of the Image.

# Region growing

At the region growing algorithms beginning of the specific pixel, the region's growth will be dependent on the connectivity with the neighbouring cells depending on similarity criteria corresponding to the greyscale intensity, shape size, or colour defined by the thresholds to expand the growth [10]. The choice of the seed point and the similarity criteria reflects the segmentation results by region growing. Statistical information and prior knowledge assimilated in algorithms to depend on starting seed points and make the algorithm adaptive [11].

## Region split and Merge approach

The second method based on the region is the split and merge image segmentation. The said method depends on a quadtree information depiction where splitting of an image takes place into four quadrants with due consideration of the non-uniform feature of the original image segment. If splitting of neighbouring images is discovered as uniform, they are converged by a solitary image made out of the four neighbouring images [11]. The cycle ends when no further merges are conceivable. This technique wipes out the high recurrence artefacts with the seed point selection depend on nearby statistics, utilized for evaluating the breast and cyst mass [11]. These algorithms predominantly depend on the image intensity information to deal with the partial volume effects and control the leakage.

### Watershed approach

The other technique that depends on the region is the Watershed method. It views the image as a topographic surface. The idea is that low-intensity pixels are interpreted as valleys of the surface, while high-intensity pixels appear as hills or peaks [12]. The algorithm starts by filling the valleys from local minima if we have seeds that are water sources. Every seed can colour with different coloured water. Those seeds are used to flood such local minima to increase the water in each part. When different water in terms of colour meets, a barrier is built to prevent them from merging from one region to another, the watershed lines [13]. This process of filling with water and barrier construction continues until all peaks are underwater, then the barrier they were found during the process represents the segmentation. In such a way, this algorithm integrates the information of the gradient and grey levels of the image. The gathering of water towards the neighbourhood of local lowest called catchment basins. The pixels in the greyscale images are clone to water beads, and the outcome of the catchment basins are the part of the locale of the image having a like class of pixels. There are two basic algorithm processes to deal with the image using watershed: (a) rainfall and (b)

In the process of rainfall algorithm neighbourhood, lowest is established all over the image. Every neighbourhood lowest is given a distinctive marking, close to neighbourhood lowest is joined with this distinctive marking. A theoretical water drop is kept at each unmarked pixel. The drop makes headway, its negligible sufficiency neighbour until it comes to a marked pixel, where it presumes a marked value. In the process of flooding, single theoretical pixels are kept at each neighbourhood lowest. An ocean of pixels continues to drench the neighbouring area of the pixel located at the neighbourhood lowest. If there is a flood of pixels, the additional pixels are disposed of, and later one is speedier than earlier. Yet, it isn't reasonable for frail boundaries images for the segmentation. Standard watershed methods are vulnerable to excessive segmenting of the images when it contains noise or the objects themselves having a low signal to noise ratio [14]. Excessive segmentation can be minimized by selecting a suitable filtering technique, thereby eliminating the unrelated neighbourhood lowest [15, 16]. The power watershed algorithms unravel the issues in regular watershed algorithms, thereby delivering the ideal outcome [17]. Incorporates the benefits of unsupervised neural network (NN) classification and morphological watershed segmentation to draw out the exact contours of breast tumours from ultrasound images [18]. The new variant stochastic watershed was applied to increase the accuracy of the selected contour [19]. Optimal parameters of the method are tuned utilizing training. Afterwards, they were applied to 17 data sets, and the demonstrated results show that it is a robust tool for automatic liver segmentation compared to the other methods. Extraction of tumour in brain MR images was done using marker-controlled watershed algorithms and distinctive feature combinations [20].

#### Clustering approach

A gathering of homogeneous data into clusters depend on analogy criteria is called Clustering. "K-means clustering (hard clustering)" is the fundamental clustering segmentation algorithms in which the dataset's components belong to only one cluster at a time. Soft clustering approach (FCM) in which the pixel can have a place with greater than one group and the fuzzy community function value is the decisive power to fit in with a pixel in the group, and the value lies in the span of 0 to 1. The pixel position is exceptionally near the centroid, and it very well may be obliged in that class if the community function value is one. The summation of the squared Euclidean separation connecting to each input sample and relating to the cluster centre with the fuzzy community's distances is called the objective function [21]. FCM algorithm is used to partition both grey and colour images; we can set the number of clusters in advance. A difference from the anticipate value may assist us in finding out any shortcomings in the segmentation. In FCM, the objective function can be balanced and stretched out according to the necessities. convenience of the variability of the objective function makes FCM appropriate for various types of images. The FCM algorithm itself has the facility for the validity



measure, thus minimize the computational exertion yields palatable outcomes. Refinement of the FCM algorithms was in practice. The outcome of the customary FCM algorithms is subtle to noise in compensating MR images' intensity heterogeneities. It replaces the Euclidean separation with the kernel induced separation called Kernelized fuzzy C-means (KFCM)[22]. The dimensional penalty was added to the objective function. Presented Fast generalized fuzzy, c-means (FGFCM) clustering algorithm by assimilating the local spatial and grey data in conjunction to suppress the noise and detail preserving for an image [23]. A portion of the upgrades in the regular FCM algorithms was made. It was tested these algorithms in the presence and absence of noise on CT brain images to identify the abnormality region and with a bacteria image to separate the bacteria from the background. They concluded that T2FCM (TYPE-II FUZZY C-MEANS) has efficiently removed the noise with the cost of an increase in the object's size. IFCM (INTUITIONIST FUZZY C-MEANS) was efficient in segmenting the images in contrast to other methods. Proposed "Fuzzy based artificial bee colony (FABC)", where they combined "Artificial bee colony optimization (ABC) "with the "Fuzzy C-Means (FCM)"[24]. They used the Fuzzy community function to search an optimum cluster centre using ABC and tested on synthetic and medical images; the efficiency results were shown in contrast with the other methods. Proposed ARKFCM, a customizable regularized kernel-based algorithm for brain MRI segmentation, upgrades the robustness to preserve image subtleties with the advent of the regularised kernel adaptability [26].

# 6. Edge detection

It is the most traditional methodology for the detection of irregularity in an image. The separation between two areas having distinct intensity levels or grey level is called Edge. The edges are remarkable in any applications and image enhancement to enhance the details of the image. Derivative operations are used for the Edge's existence in an image, and primarily a convolution function is done on a picture with an appropriate mask [11]. The canny is an efficient edge detector that enhances the Edge; it uses the gradient extent threshold to locate the possible Edge. It stifles them through the system of non-maximal suppression and hysteresis thresholding [27]. Noise in the Image strongly influences edge detections leads to the identified edges comprised of discrete pixels, might be inadequate or irregular; hence before the edge detection, the image has to smooth using the Gaussian operator. The images pre-processing may erstwhile lead to fallacious edge detection and can get rid of multi-resolution Edge detection and Edge tracing techniques [28].

### 7. Model-based algorithms

Model-based approaches have been set up as probably the best strategies for picture analysis to go with a model. This model contains information about the look forward of the shape and existence of the structure. This technique is sturdier against the artefacts associated with the images than the conventional algorithms.

### Markov Random field models

It is a simple stochastic process in which future states' distribution relies only on the current state and not how it arrived in the current state. A random sequence with the Markov property if its present status dictates its distribution is called Markov random fields (MRF), inspired by the Ising model [29]. MRF methods have been broadly utilized to segmentation the images, and the image's revamped since they can protect the edges by parameter approximation [30]. Presented Hidden Markov random field (HMRF) [31], based on a random process created by MRF model whose state of arrangement cannot be watched straightforwardly, which can be seen through an examination. It can be shown mathematically "FM model" is a decadent version of the "HMRF model". By incorporating the HMRF model and an "Expectationmaximization (EM)" algorithm into an "HMRF-EM framework", precise and sturdy segmentation achieved and was exhibited by correlation experiments with the model-based segmentation". Discussed combination of MRF and SOFM (self-organizing feature map) by incorporating the spatial constraints, which improves the smoothness of partitioning regions [32]. Discussed mass breast segmentation using proclaimed PRF (Pickard random fields), an "Unsupervised MRF model". The PRF model was discovered to be productive compared to the regular MRF in terms of computational complexity [33].

# Atlas-based approach

Atlas consists of images, including anatomical subtleties to join earlier data for partitioning and outcome changes depending on the Atlas' particulars. The informational indexes of clinically debilitated subjects and ordinary subjects are used to advance an atlas. Atlas can be a physically marked picture; it possesses a close connection with the picture to be partitioned. The image enrolment takes part in an essential job, and numerous atlases enhance the partition precession [34]. In the image enrolment course, the physically marked Atlas was changed by a mapping strategy frequently named "LABEL PROPAGATION" to precise partitioning the earmark object. The exactness of enrolment is essential since mistakes might happen if there is a topographic distinction between the Atlas and the examination object [35]. Choice of source images for an Atlas development was made by either deciding the population's true mean or collecting the sample closer to the mean. Depending upon several parameters, variable numbers of iterative algorithms could diminish the atlas development's bias effect. On account of numerous atlas partitions, an enormous database is required, and the determination of a proper atlas of the query image is to be done [36]. Labels of Atlas for the earmark depiction was confined by dimensionally changing the fusion weights obtained from neighbourhood evaluation of the enrolment activity [37].



They presented average -shape atlas-based segmentation strategy makeover the preferred outcome over a single atlas-based strategy of cardiac and aortic Segmentation in CT scan images [37]. In this study, authors utilized ribbone atlases to automatically take out the patient rib bone on conventional chest x-ray (CXR) utilizing the physically alongside the mimicked models from CT and bone images acquired from the dual-energy x-ray machine [38]. During the enrolment, they compute the transformation mapping between the model x-ray and the patient x-ray by the regional similarities between the x-rays, and they apply the result mapping to the rib masks. The average of enrolled models establishes the rib bone likelihood map for the patient-X-ray.

#### Artificial neural networks

It is a mathematical model of neurons, just like human brain cells inspired by biological neural networks. The node is nothing but a replica of neurons, which may be implemented with specific functional units. These nodes are connected through communication links with synaptic weights. The inputs of these synaptic weights are processed to classify or identify the object with the activation function's help [39]. Training and learning are the two significant features of neural networks. Neural networks are prepared with attributes, perhaps statistical in a feature like mean, standard deviation, kurtosis, skewness, or transfer, depending upon the attributes with the application of Wavelet transform or Curvelet transform. During the training phase, the introductory phase of neural networks is named a speculating phase and progresses until the study state achieved. Moreover, the neural network's training, the more acceptable the outcome related to the examination image. Learning is a customizable activity in which the weights related to the interlinking neurons changed to give appropriate feedback. The Learning process involves neural networks grouped as supervised learning and Unsupervised learning [40]. Neural network algorithms have significant difficulty determining the architecture, network size, type, number of layers, architecture, network size and geographies. The choice of the above said components influence the exhibition of dealing with the problem. Identification of the lungs from the clinical images was described by the "Group Method of Data Handling (GMDH)" [41]. Fuzzy neural networks yield better segmentation result, which was insensitive to noise [42]. Proposed separation measurements utilized by the SVM classifier and also investigated the importance of hyperparameter selection [43]. This method proved that the segmentation accuracy is good apart; it takes less processing time and less memory usage. Worked on segmentation of liver malignancy out of MR images utilizing a combination of "3D fast marching algorithm" and the "Single hidden layer "feed-forward neural network. The results are validated with those physically delineated by a radiologist utilized as ground truth [44]. The time unpredictability was extraordinarily decreased, and precise outcomes were acquired with other semiautomatic segmentation techniques [44]. A deep convolution Neural network (DCNN) was used to identify the brain MR images' glioblastomas [45].

### Graph cut approach

The graph cut algorithm's fundamental idea is to borrow tools from the graph theory to partition the image into foreground and background. In graph theory, every pixel will be a node, and the edges are the links that connect those nodes. Connecting links are the probability of that node being foreground or background to connect the source (S) or sink (T) with the weight correlated to the probability, i.e., the Edge's weight. The weight that promotes the pixels that are similar to stay together in the same segment and the different pixels promotes them to become different segments [46]. After constructing the graph, partition that graph by creating a minimal cut with the least effort that partition the foreground and background. With some hard constraints, the cost function represents the boundary and region properties considered as soft constraints for the segmentation. When the hard constraints are changed, the global optimization recomputed as per the new constraints when the cost function is mentioned. In the graph, cut pixels represent the nodes, and edges are the weighed connecting nodes. They compute the global optimal minimum cut to obtain the object & background from the image. They demonstrated this technique with photo, video editing and Medical image processing [46]. They proposed two algorithms to minimize the energy function, which is based on the graph cuts. In the first, the labelling is done among the arbitrary set of pixels so that there is a movement among the labelled pixels so that energy is minimized. The second algorithm requires smoothing. They used three quadratic energy functions first one is with truncated quadratic energy function. The second and third energy functions correspond to the Potts model, and truncated distance as the penalty of smoothness and the results are compared with the different annealing variants. [47]. The graph cut algorithm gives an optimum outcome than the conventional graph cut algorithms with earlier information about the foreground's shape. Multiregional graph cut partitioning is done through kernel mapping of the image data, and the objective function contains original data to assess the deflection of the changed The optimization algorithm iterated two consecutive steps: graph cut optimization and fixed point iterations for refreshing the region's parameters. This strategy bears a powerful option in contrast to the complex modelling of the original data while exploiting the computational advantages of graph cut images. This method was quantified and comparatively validated with synthetic, natural, and medical images. Kernel mapping yields good results in the multi-region partition of brain MR images [48].

#### Lattice Boltzmann method (LBM)

They are powerful techniques with a high degree of accuracy. Lattice Boltzmann method (LBM) is one such simulation technique that depends on the microscopic elucidation of the macroscopic physical process, which has applied widely in kinetic theory to simulate various systems [49]. In LBM, an attempt has been made to close the gap between the macroscopic and microscopic scales by taking the behaviour of a group of particles supposed



to behave similarly, rather than a single particle behaviour. Each such collection of particles is given as a distributive function, which represents the collection of particles. In LBM, the solution area is separated into lattices. At every lattice node, the dissemination of particle resides. Some of these particles advance along a specific direction to the adjacent node. The number of directions, linkage relies upon the lattice alignment. The normal phrasing utilized in LBM DnQm, where 'n' speaks the dimension of the problem, 'm' alludes to the speed model, the number of linkages. The crucial element in LBM is the equilibrium distributive function (few) with a relaxation time  $(\tau)$  ascertaining the sort of issue that should have to be tackled. LBM has an alternate tool to the conventional mathematical methods for solving partial differential equations (PDE). LBM is faster, easier, and it has the facility to assimilate large parallel computation and has the advantage of occupying less memory during the simulations as it considers the distribution of particles rather than tagging each particle. The general LBM comprises of two stages as follows: a streaming stage in which particles (or particle densities) moves from one node to another node on a lattice and a collision stage in which particles (or particle densities) are reorganized at each node [50].

The two stages are governed by the LBM evolution equation, where parameter relaxation time( $\tau$ ) and source term (α) decide the particles' movement. The state of each node at the next moment is only related to the state of its neighbouring nodes because the particles move along the links, and the lattice number and lattice speed govern the links. LBM can be efficiently used in image analysis techniques such as (i)image smoothening [51-53], (ii) image inpainting [54], (iii) image segmentation [55-60]etc. In image processing, each pixel value is considered as particle densities, and changes in pixel value can be considered as a redistribution of particles that are decided by relaxation time  $(\tau)$  source term  $(\alpha)$  in which image information such as gradient and curvature are embedded. LBM in image processing is done, which can be applied easily to complex domains and could be used to serve multiphase and multicomponent flows. Introduced an anisotropic diffusion model dependent on LBM for picture division and showed the adequacy of the calculation in clinical pictures [55], [61-65]. Proposed a novel LBM method using the D2Q19 lattice arrangement model for the Segmentation of MR and clinical images, which is similar to anisotropic diffusion as shown in figure 2 [56], [66-71].



Figure 2. Segmentation of MR image by LBM [56].

(a) MR Image

(b) LBM

Utilized LBM to tackle the Level Set Equation (LSE), they proposed a Region-based stop function [71-76]. Unsigned Pressure Force (UPF) in light of regional attribute can adequately and effectively stop the contour at feeble obscured edges [57]. They utilized the parallelizable lattice Boltzmann method (LBM) to solve the level set equation(LSE). This technique is quicker since it is unravelled in histogram space instead of pixel domain [77-81]. The time problem is extensively diminished since the quantity of grey levels is commonly a lot littler than the size of the picture. The strategy is productive, profoundly parallelizable, and quicker than those dependent on the LSM [58]. Edge of object division can be obtained by the Lattice Boltzmann Anisotropic Diffusion Model (LBADM) and indicated calculation could precisely fathom the convection and diffusion condition [59]. The algorithm incredibly lessens the calculation of division. They proposed a new variation multiphase level set approach to clinical segmentation, calculated multiphase level set conditions and entropy for the LBM model for D2Q9[60]. Demonstrated their method for MR breast images reveals it is more efficient and faster [81-84]. The LBM's merit is a pixel-based algorithm. It deals with the particles, and the pixels are the replica of particles, therefore at any resolution, we can tune the algorithm using various kinds of lattice points. With the increase of lattice points, computational load also will be increasing, and it may be a demerit of the LBM in the view of computation. Since it is particlebased in the microscopic domain, all the macro parameters can be redefined, but since LBM is dealt with, density has to define in a regular structure. In a medical image, getting a regular structure is very difficult; therefore, it may have the LBM's demerit.

#### 8. Conclusion

This paper presents a review to explain the different segmentation for medical images and novel LB method to advance interest for future investigation and exploration in medical image segmentation. Emphasize that none of these problem areas has been acceptably settled, and all of the algorithms depicted are available for broad improvement. Segmentation of medical images is a yet complicated issue in real-time applications like diagnosis and radiotherapy treatment where segmentation algorithm can accurately recognize different tissues encompassing the tumour site and tumour boundaries, henceforth more inventive work is required augment the computational speed. LBM has the benefits of speed and adaptability of modelling to guarantee excellent image processing quality with a reasonable amount of computer resources. The LBM has an exact physical meaning in image processing, the image's pixel value is considered particle densities, and changes in the pixel value can be considered redistribution of particles. It is governed by the relaxation time, which decides the kind of problem needed to be addressed, and the addition of source term is straight



forward. The quality of the image segmentation and the computational speed utilizing LBM with high dimensionality and more lattice vectors are expected to comprehend, so we predict that the LB method will become a new research hotspot field Medical image segmentation.

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