20.462J/3.962J Molecular Principles of Biomaterials

Summary of course objective:

Develop a firm understanding of the **fundamental materials science & engineering principles** underlying synthetic/engineered materials used in **biology**, **biotechnology**, **and biomedical** applications—focusing on a subset of problems that can be quantitatively understood (and that we have time to cover!)

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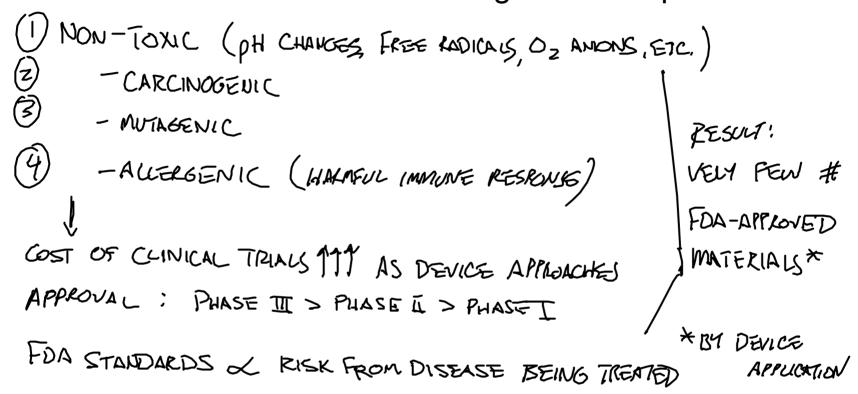
Please see:

Fig. 1(a) in Richardson T. P., M. C. Peters, A. B. Ennett, and D. J. Mooney. "Polymeric System for Dual Growth Factor Delivery." *Nature Biotechnology* 19, no. 11 (2001): 1029-34.

Prelude to degradable solid polymers: In vivo applications of Biomaterials

NON-TERIALS 'active' lifetime: **Implants** Artificial hips, artifical heart, pacemaker, 8-10 yrs Tissue engineering, cell therapy 了四个个 ≤ 1 year Delivery of cells Scaffolds for in vivo tissue guidance Drug delivery ≤ 6 months Injected or implanted devices Biosensors Hours - days In situ measurements of pH, analyte MATUS concentrations, etc.

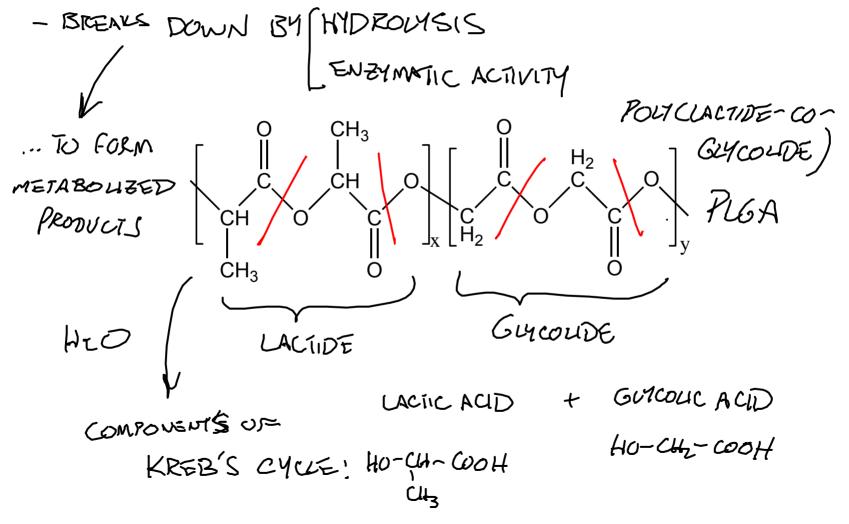
If a material is to be utilized *in vivo*, what characteristics must it have in addition to fulfilling device requirements?



CBS News | FDA Rejects Silicone Implants | January 8, 2004 09:38 ...

"Long-term safety, the concern that prompted the removal from the market 11 years ago, was clearly not demonstrated," Whalen wrote.

3 classes of materials used in vivo: (1) biodegradable materials



(2) Bioeliminable Materials

DO NOT DEGRADE!

HO-SOLUBLE, EXCRETABLE

EXAMPLES !

KIDNEY CLEARANCE;

≤ 2-3 nm

PEGYLATED)
PROTEIN
DRUG

Solo

cino

POLY (ETHYLENZ GLYCOL) PEG < 20KDQ (CH2-CH2-O+1) ETHERS GENERALLY STABLE IN VIVO POLY (ETHYLENE OXIDE) PEO > 20 KDQ

Dextrah

POUSACCHARDES

(NOT DEGRADABLE BY MAMMAUAN
ENZINES)

(3) Permanent/retrievable materials

NOT DEGRADABLE OR EXCRETABLE

REQUIRE SURGERY FOR REMOVAL

EXAMPLES:

POLYETHYLENZ (COP/SOCKET OF AMIFICIAL HIPS)

Extracellular environment

T: A WOYS ALTIFICIAL HIPS

DRUG DELIVERY MATRIX-VERY MILD INFLAMMMORY RESPONSE OF $O-C-CH_3$ $\left(-CH_2\ CH_2\ \frac{1}{x}\left(-CH_2\ CH_2\ \frac{1}{x}\right)_{x}\right)$

$$\left(-\mathsf{CH}_2\,\mathsf{CH}_2\,\frac{}{}\right)_{\mathsf{X}}\!\!\left(-\mathsf{CH}_2\,\mathsf{CH}_2\,\frac{}{}\right)_{\mathsf{Y}}\!\!\left(-\mathsf{CH}_2\,\mathsf{CH}_2\,\frac{}{}\right)_{\mathsf{Y}}$$

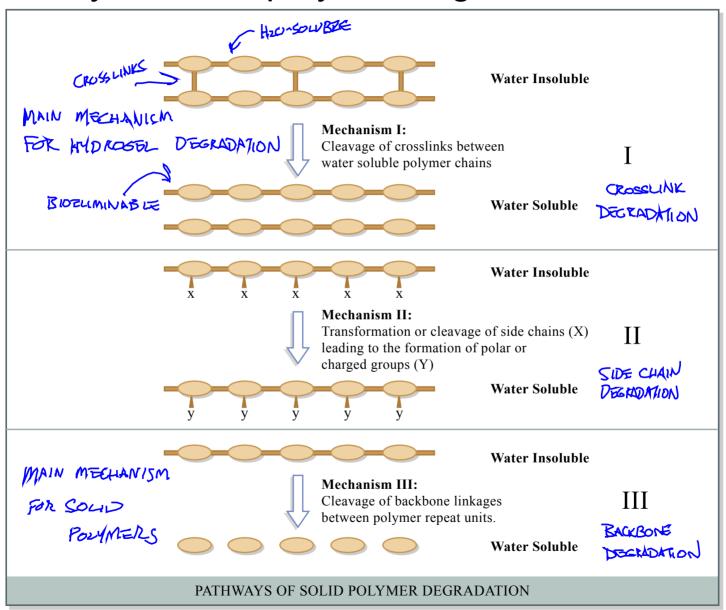
Poly(ethylene-co-vinyl acetate) (PEVAc)

Biodegradable solid polymers

- our definition of 'biodegradable' for this course: [NITIALLY SOUD OR GEL-PHASE MATERIAL REDUCED TO SOLUBLE FRAGMENTS THAT ARE METABOLIZED OR EXCRETED UNDER PHYSIOLOGICAL CONDITIONS (Shine ENVIRONMENT, ph 7.4, 37°C)
- Why use biodegradable materials?
 - TEMPORALY NEEDS

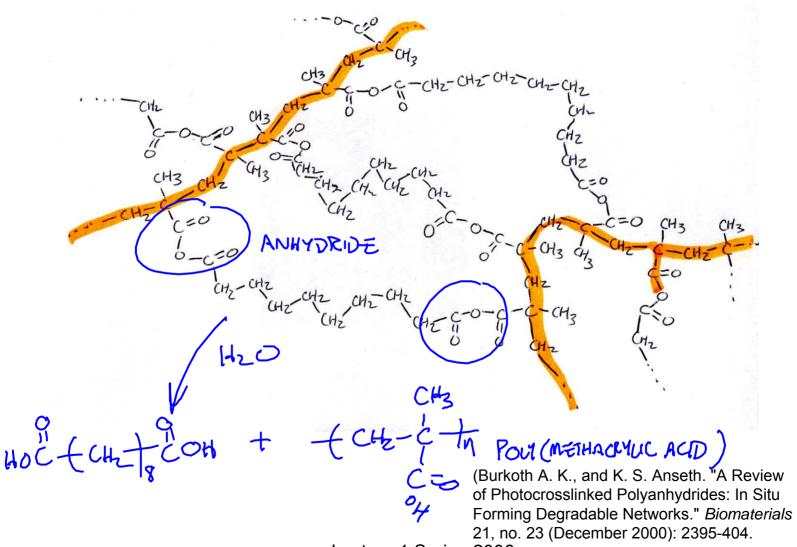
 GENERAL DESIRABILITY OF 1-TIME SUNGERIES
 - 2 AVOID CHRONIC INFLAMMATION & ITS ASSOCIATED COMPLICATIONS
 - (PEG, DEXTRAN, ALGINME, CHITOSAN, ...?)

Pathways of solid polymer degradation



Mechanism I example: polyanhydride networks

CROSSLINK DEGRADATION



Lecture 1 Spring 2006

Mechanism II

Poly(methyl vinyl ether-co-maleic anhydride)

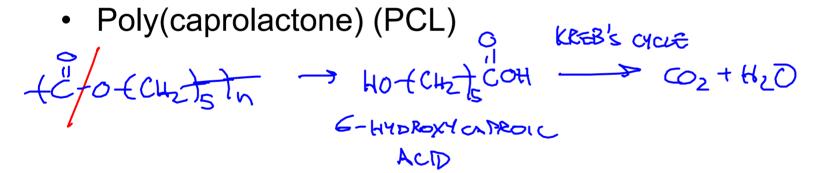
Mechanism III BACKBONE DEGRADATION

Example: Polyphosphazenes:

• Example: Polypnosphazenes:

$$(N = P) + 2H_2N-R$$
 $(N = P) + 2H_2N-R$
 $(N = P) + 2H_2N-R$

Medically-applied degradable polymers are chosen for metabolizable or excretable final breakdown products



• Poly(hydroxybutyrate)

CH3 O NORMAL CONSTITUENT

CH3 CH2 O HO-CH-CH2-COH OF BLOOD

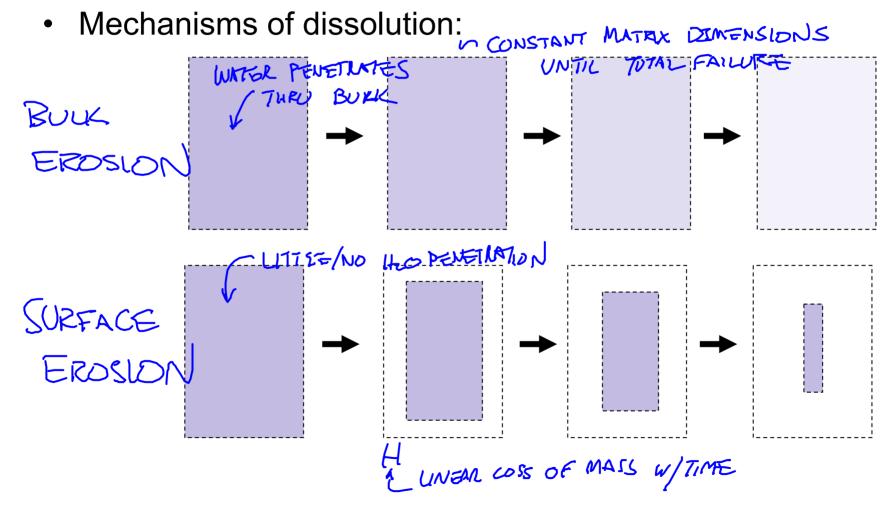
D-3-HYDROXI BUTYRATE

What doesn't work?

- Degradation too slow
- Breakdown products not clearable

Physical chemistry of hydrolysis

structure influences mechanism of erosion as well as overall rate



Bulk vs. surface erosion

Bulk erosion (Puga)

(PUMANHYDRIDE)
Surface erosion

Images removed for copyright reasons.

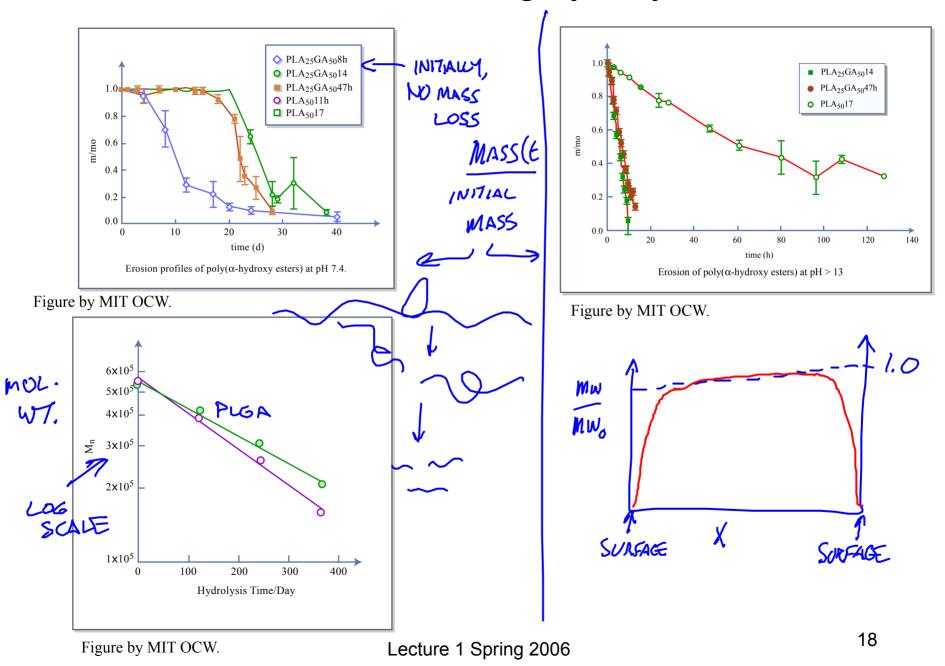
Please see:

Fig. 8(b) in Lu, L., C. A. Garcia, and A. G. Mikos. "In Vitro Degradation of Thin Poly(DL-lactic-co-glycolic acid) Films. *J Bio Med Mater Res* 46 (1999): 236-44.

Images of surface erosion removed due to copyright restrictions.

Fig. 6(d) in Agrawal, C. M., and K. A. Athanasiou. "Technique to Control pH In Vicinity of Biodegrading PLA-PGA Implants." *J Biomed Mater Res* 38 (1997): 105-14.

Dissolution during hydrolysis



Role of molecular structure in hydrolysis rate:

- " EFFECTIVE "
- (1) RELATIVE BOND STABILITY
- 2 HYDROPHOBICITY
- (3) STERIC EFFECTS
- (4) PRODUCTION OF AUTOCATALYTIC PRODUCTS
- 5 MICROSTRUCTURE CRYSTALINITY?
 PHASE SEPARATION?
 POROSITY?

Role of molecular structure in hydrolysis rate:

(1) Relative bond stability:

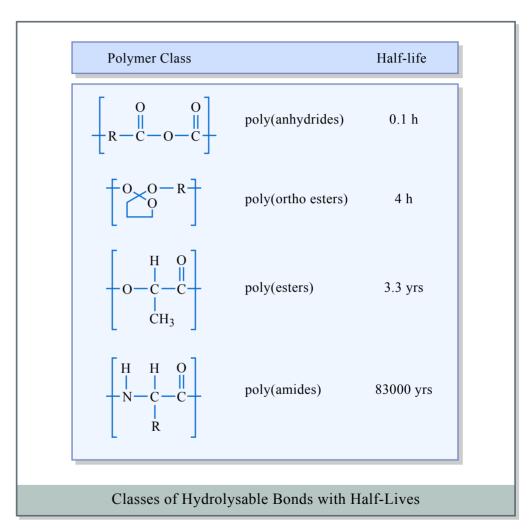
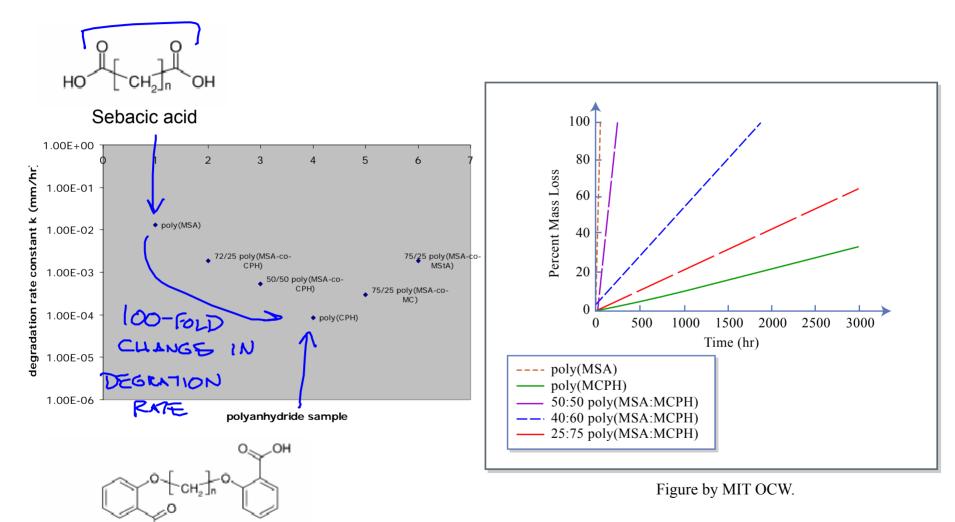


Figure by MIT OCW.

(2) Effect of polymer hydrophobicity on solid polymer erosion rate



OH

n = 6: 1,6-bis(o-carboxyphenoxy)hexane (o-CPH)

(3) Steric effects controlling polymer hydrolysis rates

Local structure

Glass transition (Tg)

(4) Production of autocatalytic products

Polyesters:

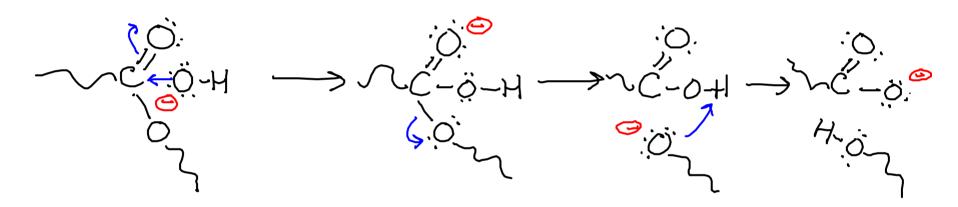
Mechanisms of hydrolysis: polyesters

acid-catalyzed hydrolysis:

Mechanisms of hydrolysis: polyesters

Base-catalyzed hydrolysis:

(saponification)



Nucleophilic substitution at acyl carbon

Physical properties

Semicrystalline polymers boxed

Polymer Transition (°C) Temperature (°C) Strength (MPa) Modulus (MPa) Modulus (MPa) Yield (%) Br (%) Poly(glycolic acid) (MW: 50,000) 35 210 n/a
Poly(lactic acids) L-PLA (MW: 50,000) 54 170 28 1200 1400 3.7 6 L-PLA (MW: 100,000) 58 159 50 2700 3000 2.6 3 L-PLA (MW: 300,000) 59 178 48 3000 3250 1.8 2 D, L-PLA (MW: 20,000) 50 - n/a
L-PLA (MW: 50,000) 54 170 28 1200 1400 3.7 6 L-PLA (MW: 100,000) 58 159 50 2700 3000 2.6 3 L-PLA (MW: 300,000) 59 178 48 3000 3250 1.8 2 D, L-PLA (MW: 20,000) 50 - n/a n/a n/a n/a n/a n/a D, L-PLA (MW: 107,000) 51 - 29 1900 1950 4.0 6 D, L-PLA (MW: 550,000) 53 - 35 2400 2350 3.5 5 Poly(β-hydroxybutyrate) (MW: 422,000) 1 171 36 2500 2850 2.2 2 Poly(ε-caprolactone) (MW: 44,000) -62 57 16 400 500 7.0 Polyanhydrides ^b Poly(SA-HDA anhydride) (MW: 142,000) n/a 49 4 45 n/a 14 Poly(ortho esters) ^c
L-PLA (MW: 100,000) 58 159 50 2700 3000 2.6 32
L-PLA (MW: 300,000) 59 178 48 3000 3250 1.8 2 D, L-PLA (MW: 20,000) 50 - n/a n/a n/a n/a n/a n/a D, L-PLA (MW: 107,000) 51 - 29 1900 1950 4.0 6 D, L-PLA (MW: 550,000) 53 - 35 2400 2350 3.5 5 Poly(β-hydroxybutyrate) (MW: 422,000) 1 171 36 2500 2850 2.2 2 Poly(ε-caprolactone) (MW: 44,000) -62 57 16 400 500 7.0 Polyanhydrides ^b Poly(SA-HDA anhydride) (MW: 142,000) n/a 49 4 45 n/a 14 Poly(ortho esters) ^c
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Poly(SA-HDA anhydride) (MW: 142,000) n/a 49 4 45 n/a 14 Poly(ortho esters) ^c
DETOSU: t-CDM:1,6-HD (MW: 99,700) 55 – 20 820 950 4.1 2
Polyiminocarbonates ^d
Poly(BPA iminocarbonate) (MW: 105,000) 69 – 50 2150 2400 3.5 4
Poly(DTH iminocarbonate) (MW: 103,000) 55 – 40 1630 n/a 3.5 7
Based on data published by Engelberg and Kohn (1991). n/a = not available, (-) = not applicable. ^b A 1:1 copolymer of sebcid (SA) and hexadecanedioic acid (HDA) was selected as a specific example. ^c A 100:35:65 copolymer of 3, 9-bis(ethylide, 4, 8, 10-tetraoxaspiro [5,5] undecane) (DETOSU), <i>trans</i> -cyclohexane dimethanol (t-CDM) and 1, 6-hexanediol (1,6-HD) elected as a specific example. ^d BPA: Bisphenol A; DTH: desaminotyrosyl-tyrosine hexyl ester.

Figure by MIT OCW.

Further Reading

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