

Automating
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Planning in
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MRI-LINACs
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Futures

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Automating Treatment Planning in Radiation Therapy

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Presented by **Lekan Molu** (Lay-con Moh-lu)

March 10, 2021

Acknowledgments

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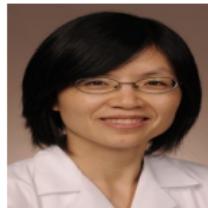
Steve Jiang, UTSW



Nick Gans, UTARI



Xuejun Gu, UTSW



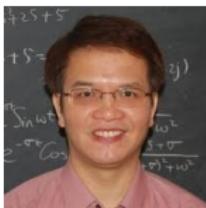
Dan Nguyen, UTSW



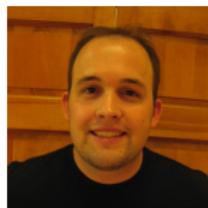
Rod Wiersma, Penn



Xinmin Liu, Penn



Tyler Summers, UTD



Yonas Tadesse, UTD



Funding Sources

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Talk Outline

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- Beam Orientation Optimization (BOO)
 - Monte Carlo Tree Search and Neuro-Dynamic Programming for BOO
 - Column Generation as Pretraining for MCTS for BOO
- Patient Head Motion Correction in External Beam Radiation Therapy (RT)
 - Intensity-Modulated RT (IMRT): Earlier PhD Work
 - Magnetic Resonance Imaging and Linear Accelerator Systems (MRI-LINACs)
- Robustness Margins and Robust Deep Policies for Nonlinear Control

Research Significance

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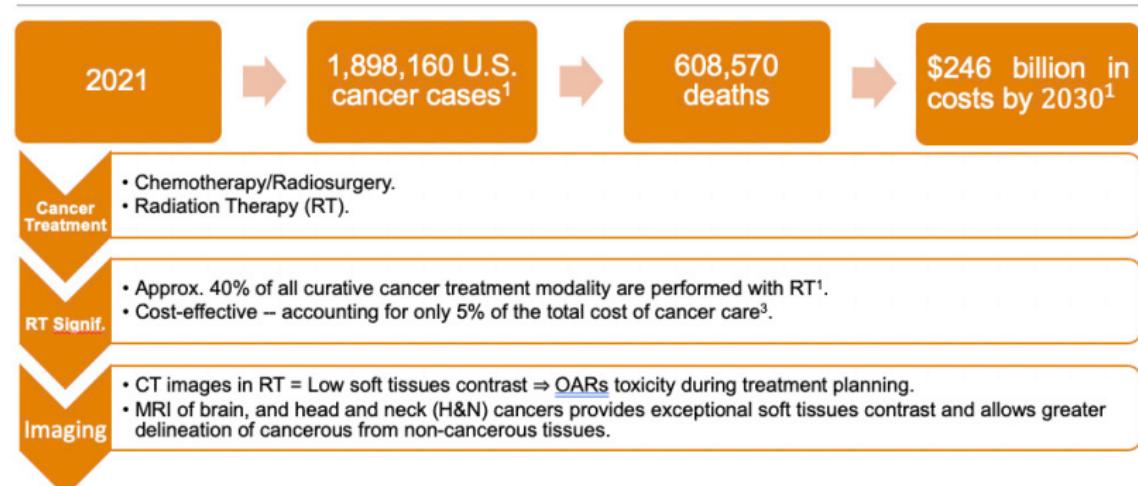
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IMRT Treatment Planning (Beam Delivery)

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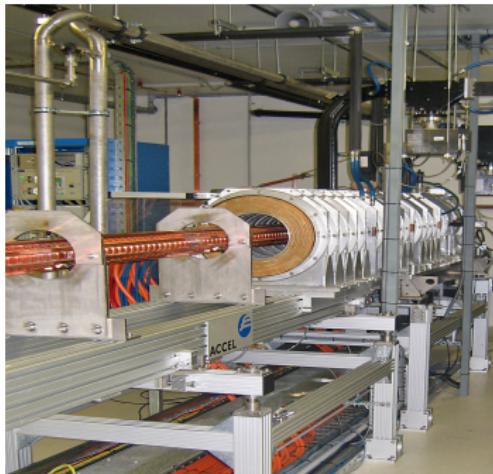
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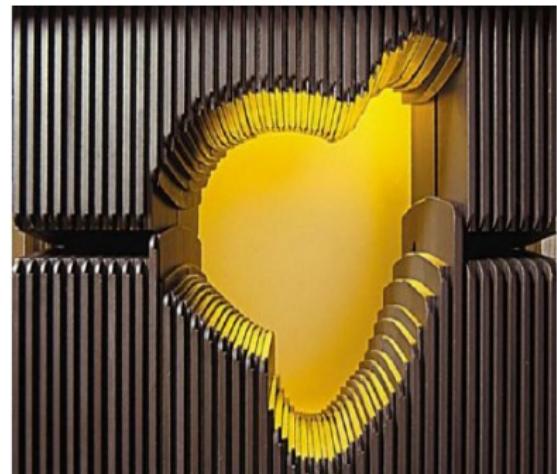
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The Australian Synchrotron.



A Multi-leaf collimator, ©Varian.

Radiation Delivery Couch and Gantry

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Varian's TrueBeam Radiotherapy System.

Part I.A: Beam Orientation Optimization (BOO)

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■ Beam Orientation Optimization (BOO)

- Monte Carlo Tree Search and Neuro-Dynamic Programming

Contributions

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Relevant Publications

Ogunmolu, Olalekan, Michael Folkerts, Dan Nguyen, Nicholas Gans, and Steve Jiang. "Deep BOO! Automating Beam Orientation Optimization in Radiation Therapy." In *Algorithm Foundations of Robotics XIII*, Merida, Mexico. Published in *Springer's Proceedings in Advanced Robotics (SPAR) Book*, 2020.

- A sparse tree lookout strategy for games with large state spaces guides transition between beam angle sets
- Tree lookout strategy guided by a deep neural network policy

Prostate Cancer Example

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Stage I Prostate Cancer

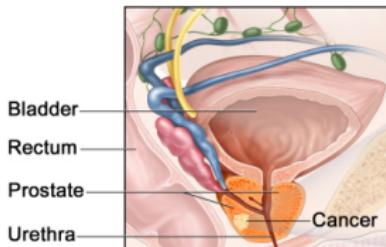


Found by: Needle biopsy

Grade Group: 1

PSA level: Less than 10

OR



Found by: Digital rectal exam

Grade Group: 1

PSA level: Less than 10

Cancer in: 1/2 or less of
one side

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BOO Process: Fluence Map Optimization

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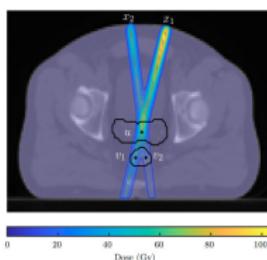
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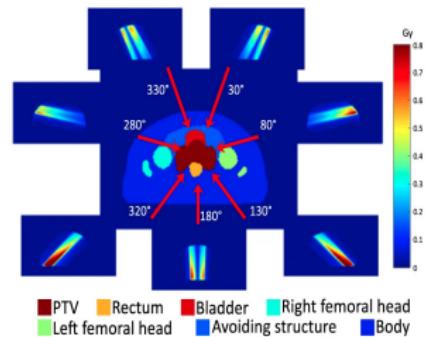
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Prostate CT slice



Prostate before BOO



Fluence Map

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Manually Selection/Protocols Adoption

Laborious process; could take up to 5 days for head and neck cancer treatment.

Pre-solve Large Sparse Dose Influence Matrix

Takes hours to solve for a single patient. Days/months for multiple patients.

Solve Fluence Map Optimization

Time-consuming. Often takes minutes.

Treatment Plan Flowchart

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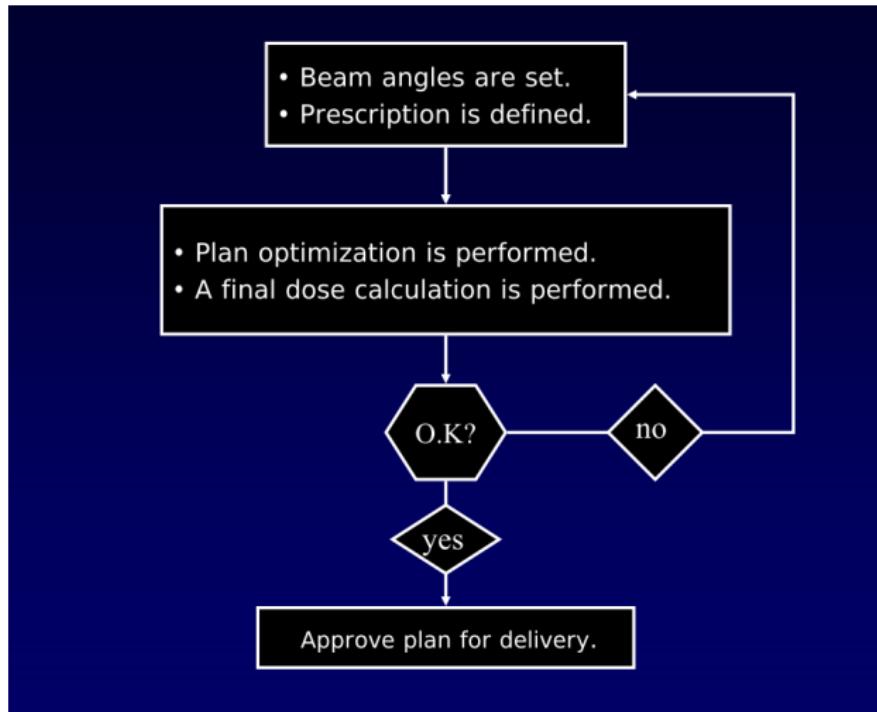
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Reprinted from "IMRT Optimization Algorithms. David Shepard. Swedish Cancer Institute. AAPM 2007."

Current Approaches and Limitations

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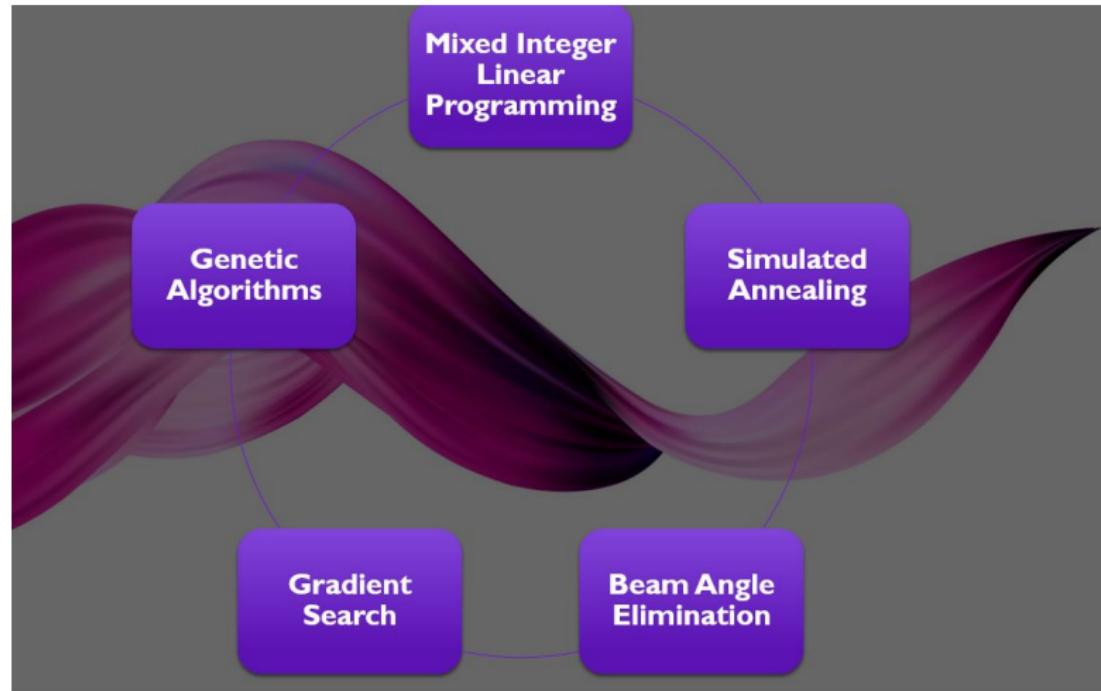
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- A Tower Neural Network generates a policy that guides MCTS simulations for two players in a zero-sum Markov game
 - Produces a *utility (value) function* & a subjective *probability distribution*
- Each player in a two-player Markov game finds an alternating best response to the current player's average strategy
 - driving the neural network policy's weights toward an approximate **saddle equilibrium** [Heinrich et al. (2015)].
 - aids network in finding an *approximately optimal* beam angle candidate set that meets a dosimetric requirements.

State Encoding: Prostate Organ Masks

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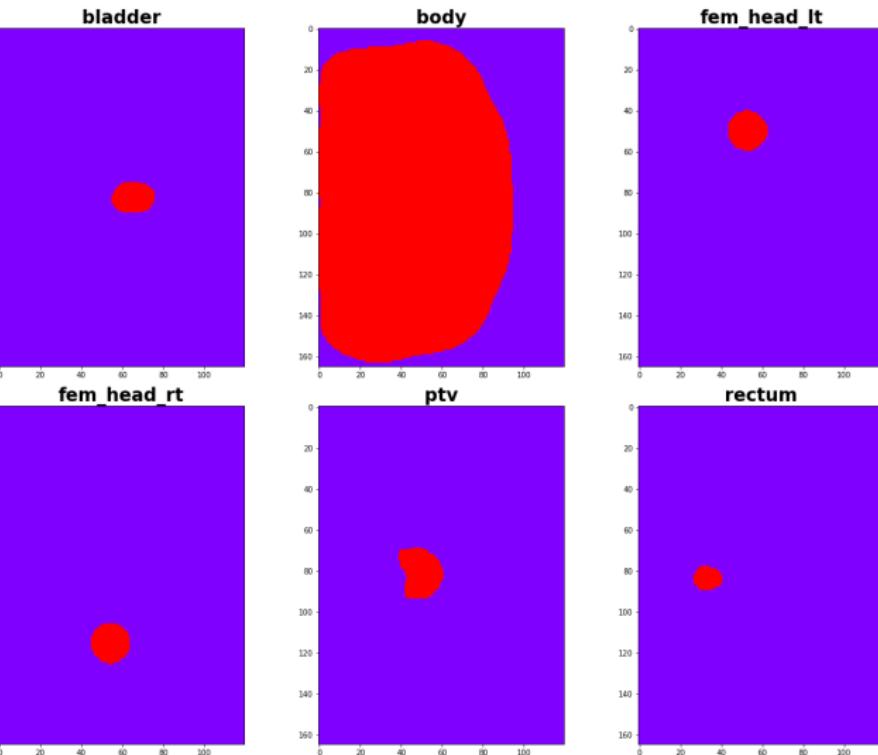
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State Representation: Beam Angles

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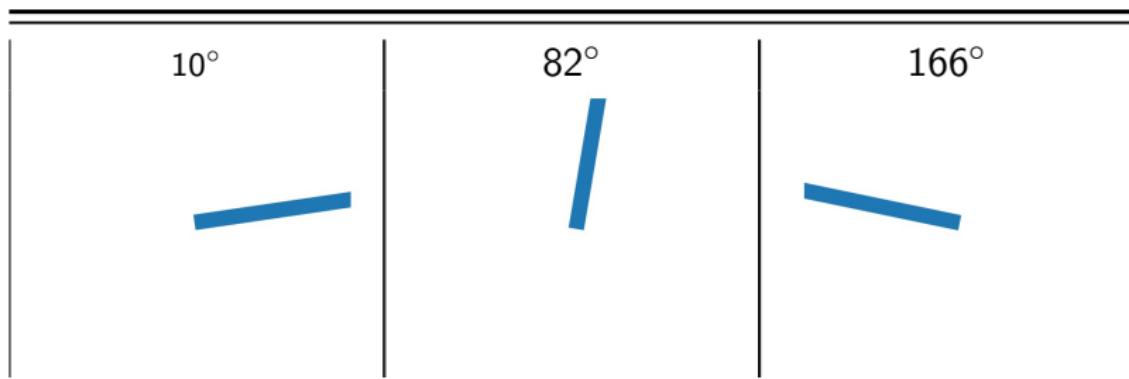
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State Representation

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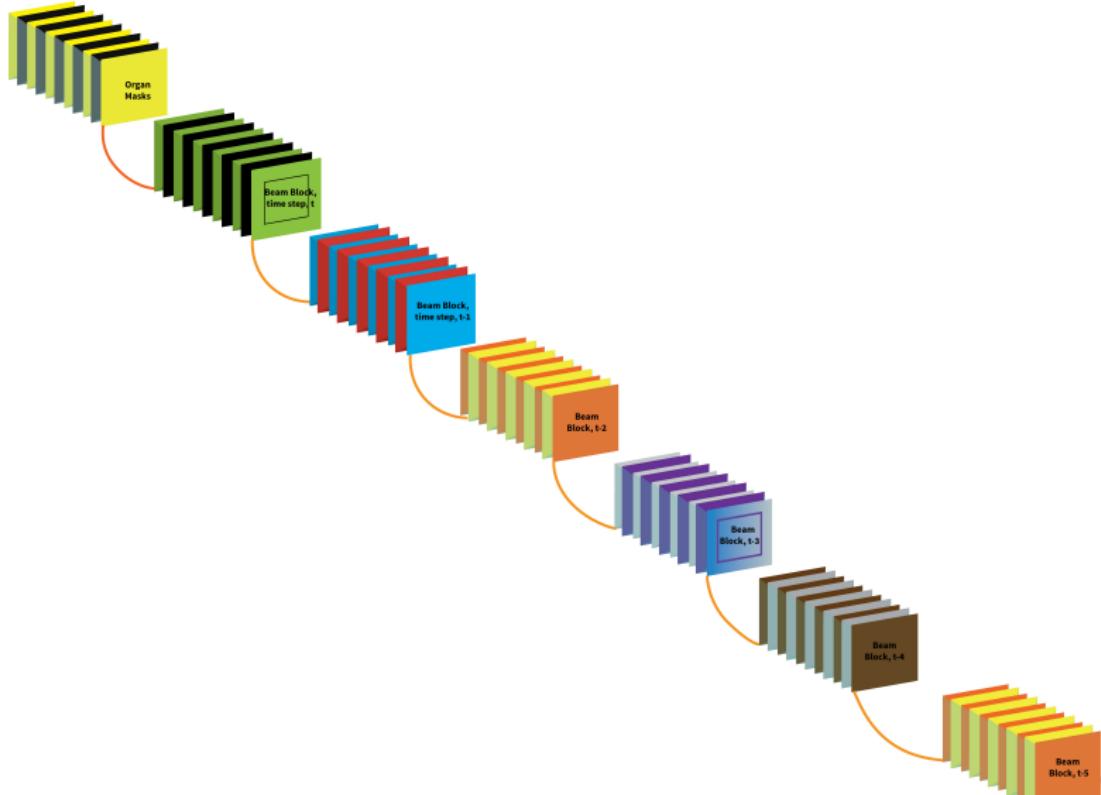
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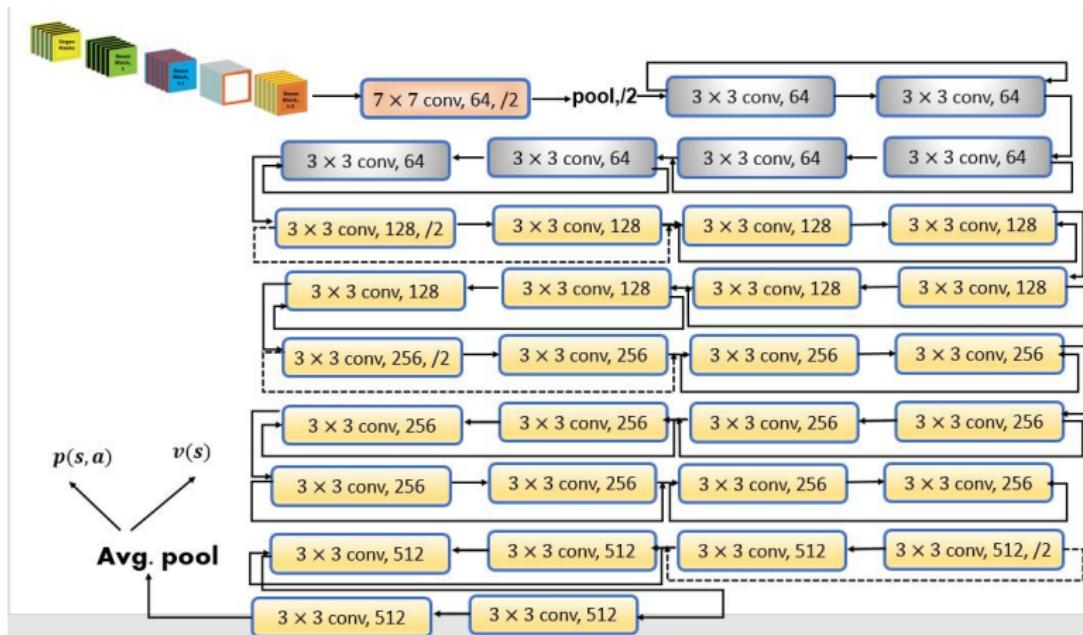
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Two-player Fictitious network play with ResNet



Tree Representation and Game Simulation

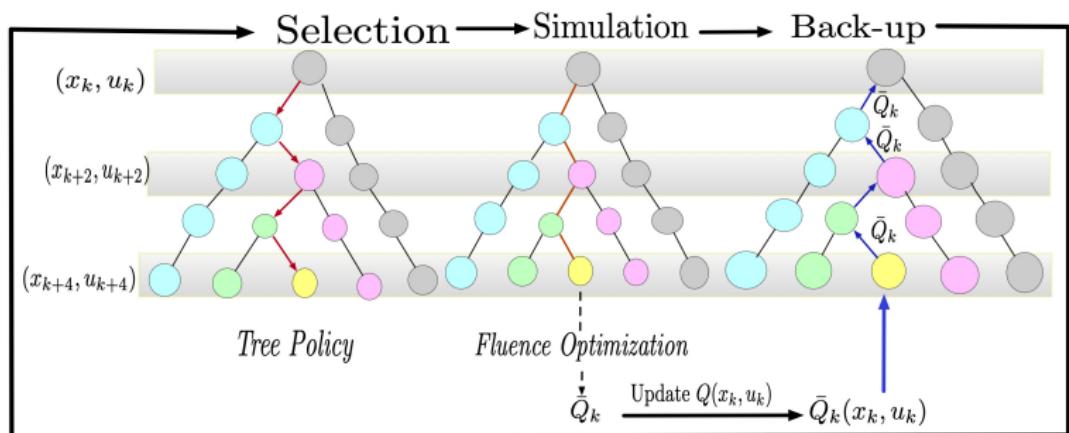
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Tree Composition

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Every **node** of the tree, x , has the following fields:

- a pointer to the parent that led to it, $x.p$;
- the beamlets, x_b , stored at that node; $b = \{1, \dots, m\}$;
- a set of move probabilities prior, $p(s, a)$;
- a pointer $x.r$, to the reward r_t , for the state x_t ;
- a pointer to the state-action value $Q(s, a)$ and its upper confidence bound $U(s, a)$;
- a visit count $N(s, a)$, that indicates the number of times that node was visited; and
- a pointer $x.child$; to each of its children nodes.

Saddle Point Strategy Formulation

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- **Saddle point strategies** for optimal control sequence pair $\{a_t^{p_1^*}, a_t^{p_2^*}\}$ recursively obtained by optimizing, $V_t(s, a)$

$$V_t^*(s) = Q_t^*(s_t, \pi_t^{p_1}, \pi_t^{p_2}) = \min_{\pi^{p_1} \in \Pi^{p_1}} \max_{\pi^{p_2} \in \Pi^{p_2}} Q_t^*(s_t, \pi^{p_1}, \pi^{p_2})$$
$$\forall s_t \in \mathcal{S}, \pi^{p_1} \in \Pi^{p_1}, \pi^{p_2} \in \Pi^{p_2}.$$

such that

$$v_{p_1}^* \leq v^* \leq v_{p_2}^* \quad \forall \{\pi_t^{p_1}, \pi_t^{p_2}\}_{0 \leq t \leq T}.$$

- p_1, p_2 respectively generating a **mixed strategy** via **averaging the outcome** of individual plays.

Training and Validation Loss

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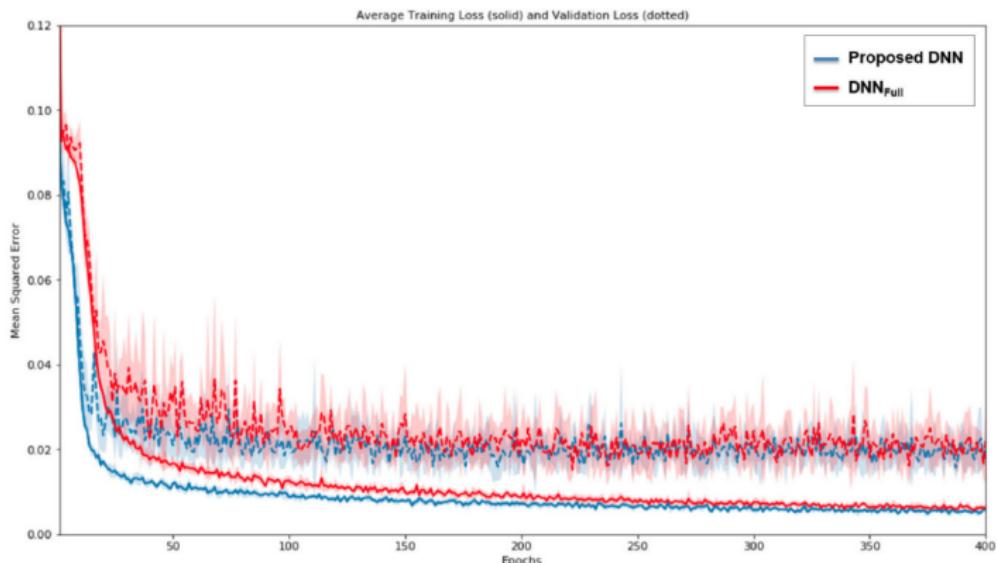
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Average training (solid) and validation (dotted) loss function (MSE) values across six cross-validation folds for the network (blue) and full network.

BOO Results: Testing of self-play network

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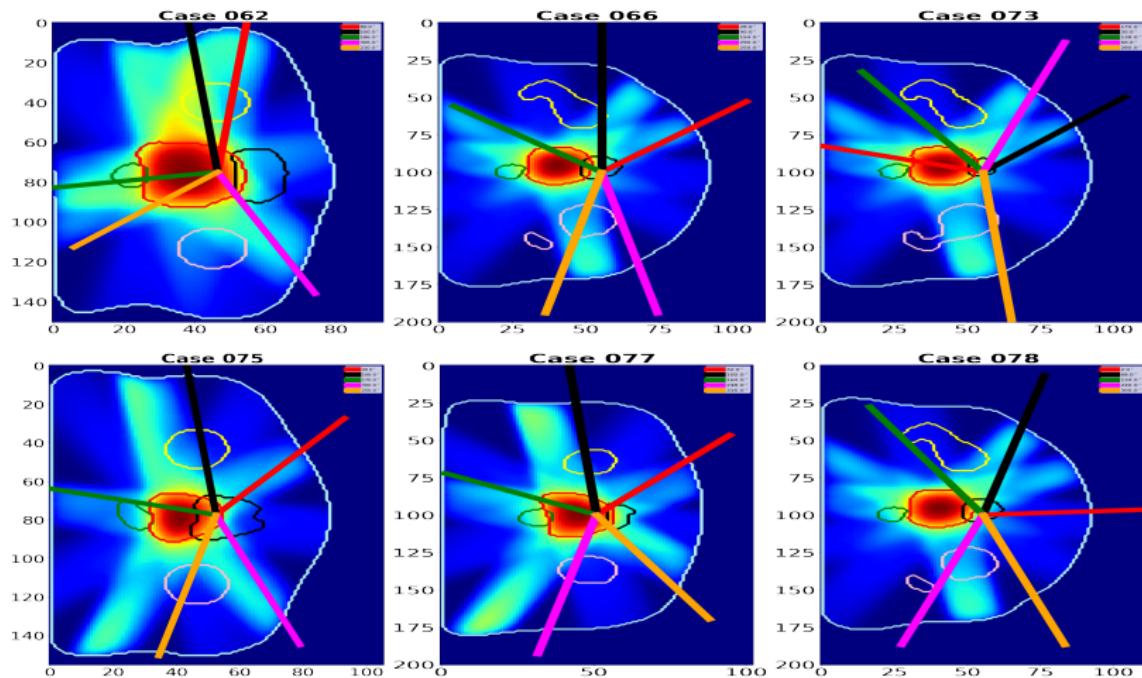
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Column Generation vs Neural Network

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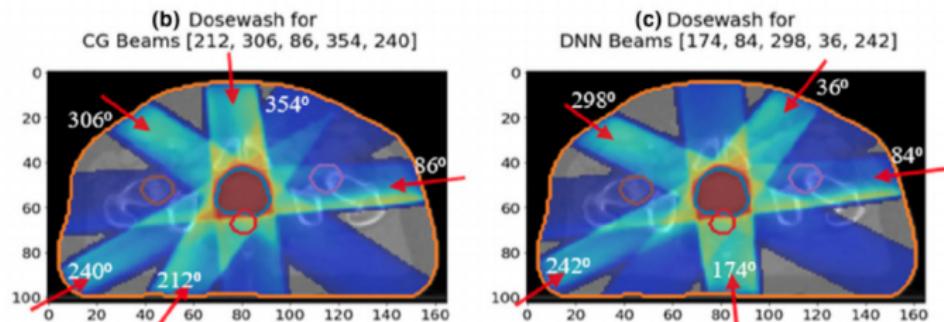
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Dose-Volume Histogram of CG vs DNN architectures [Sadeghnejad Barkousaraie, Azar and Ogunmolu, Olalekan and Jiang, Steve and Nguyen, Dan (2019)].

Conclusions

- Deep Neural Network optimizes network weights in a separate multiprocessing thread; Network outputs probabilities used to guide search;
- Sparse lookahead search builds tree with nodes labeled by state-action pairs in an alternating manner; sample rewards stored on edges connecting state-action with state nodes;
- Beam angles prediction takes between 2-3 minutes with MCTS vs. ~ 60 seconds with Column Generation Pre-training.

Head Stabilization in Radiation Therapy (RT)

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- Head Stabilization in Cancer Radiation Therapy
 - Intensity-Modulated RT (IMRT)

Robotic Radiosurgery

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A Patient Head Motion-Correction Mechanism for MRI-LINAC RT

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DEPARTMENT OF RADIATION ONCOLOGY, PENN SCHOOL OF MEDICINE

- Current Collaborators: Rodney Wiersma & Xinmin Liu (UChicago → UPenn)
- Past Collaborators: Steve Jiang, Xuejun Gu, (UT Southwestern); Nick Gans (UT Dallas, UT Arlington)

Correcting Head Motion: RT and MRI-LINACs

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(a) The BRW SRS Frame [Chelvarajah et al. (2004)]



(b) Thermoplastic masks



(c) Frame With MRI Coils (PSOM)

4-D Motion Correction Stage

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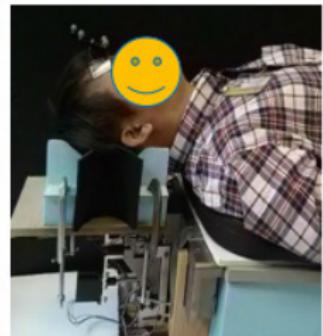
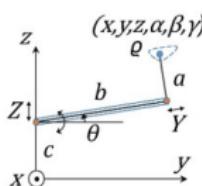
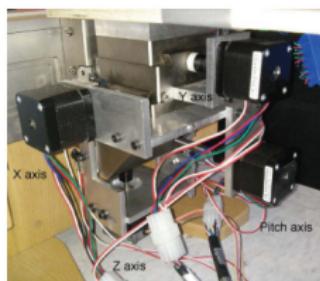
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Liu et al. (2015)

4-DOF Motion Controller Block Diagram

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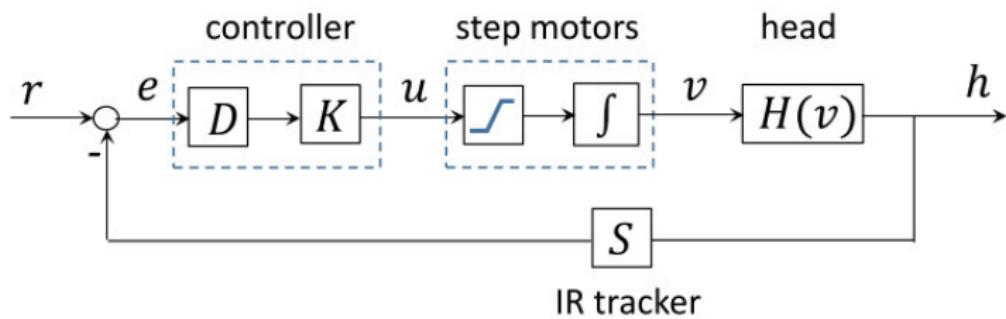
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Liu et al. (2015)

Phantom Feedback Motion Correction Results

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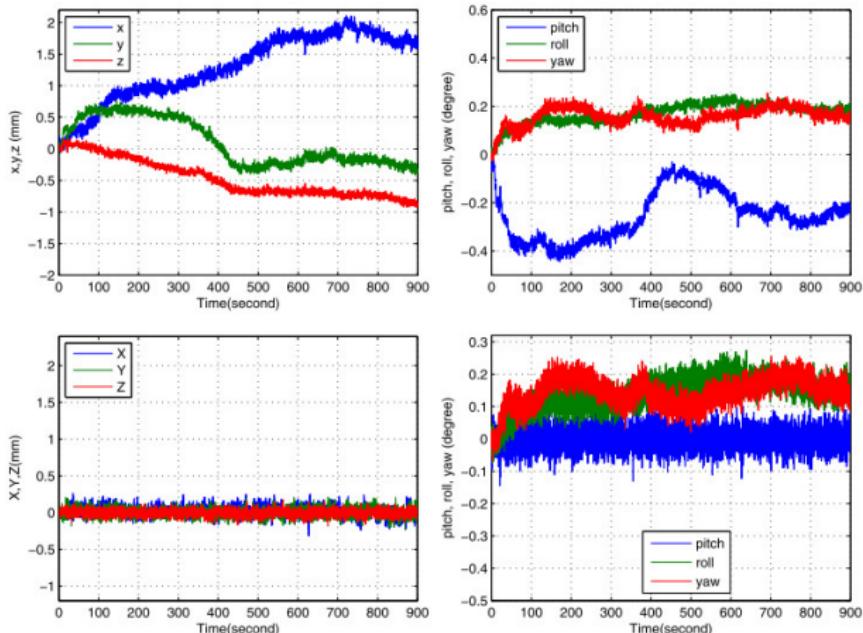
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Time response of feedback control without (left) and with (right) decoupling control [Liu et al. (2015)].

Human Volunteer Feedback Motion Correction Results

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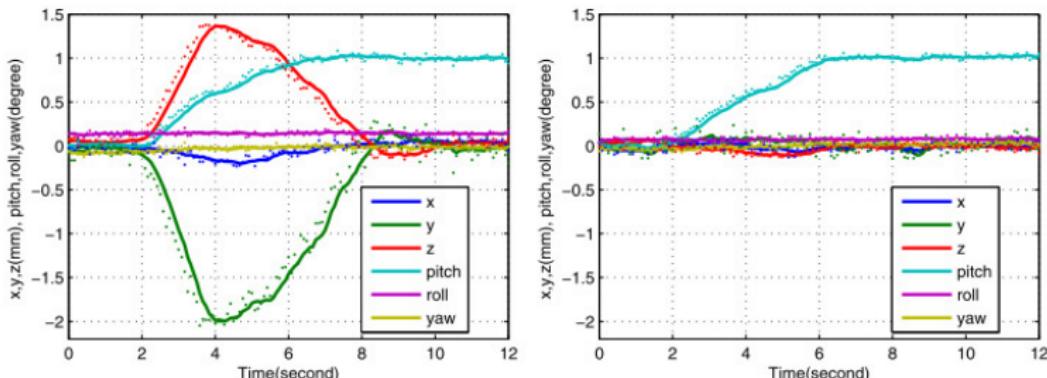
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Head Motion Without and With Motion Correction. Left: Coupled Axes; Right: Decoupled Axes.

SRS: Wiersma Stewart-Gough Platform

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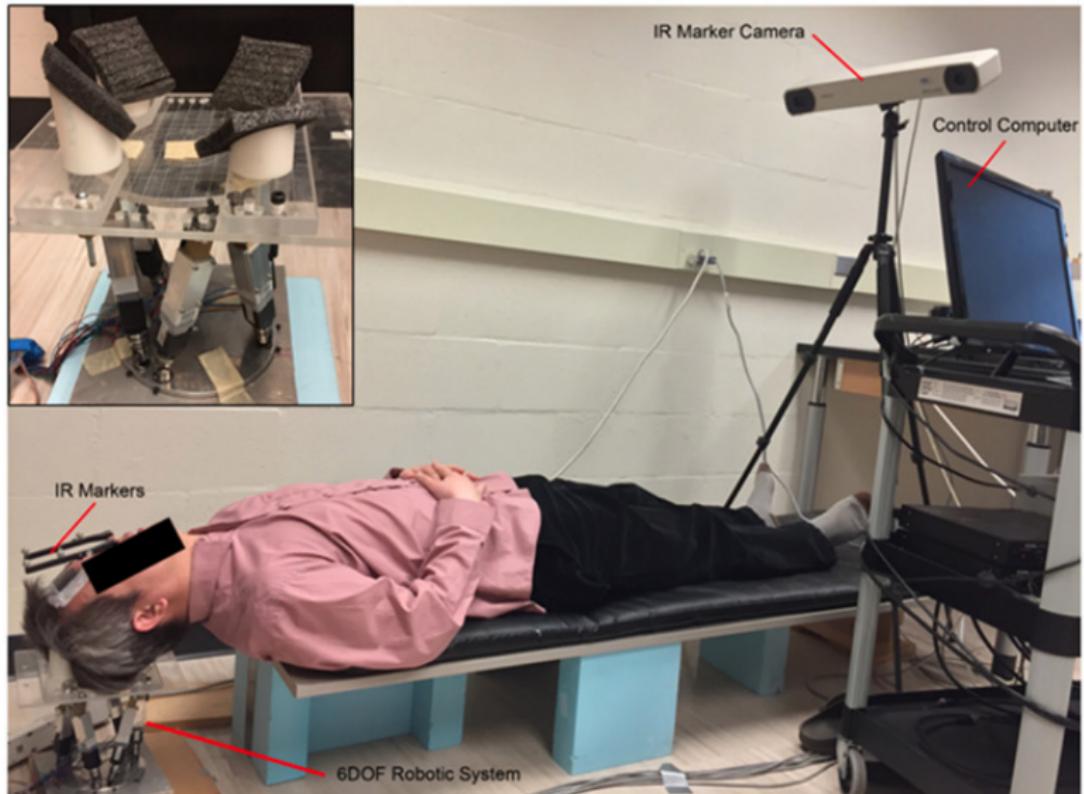
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6-DOF Motion Correction Results

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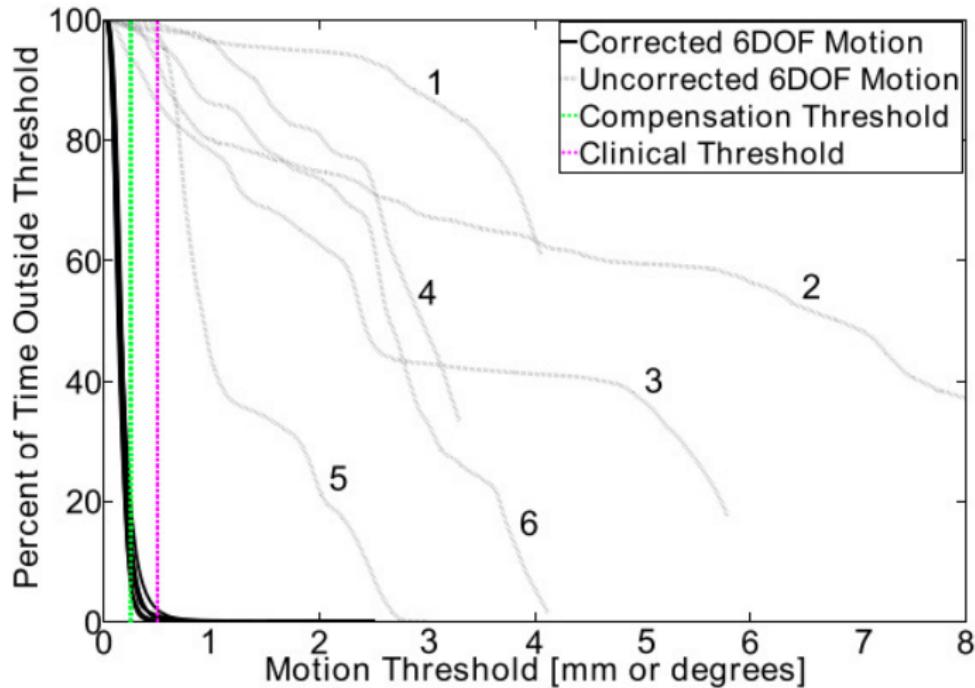
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Drawbacks of current solutions

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- Rigid patient's body assumption
- Non-compliant immobilization devices
- Invasiveness during radiosurgery/RT
- Attenuation of photon beams

Radiation Delivery Couch and Gantry

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Varian's TrueBeam Radiotherapy System.

Next-Gen RT Treatment with MRI-LINACs

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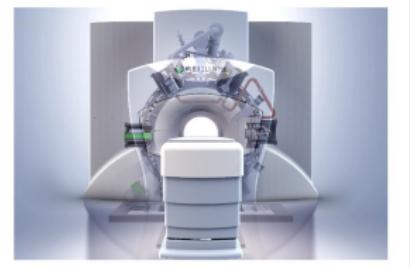
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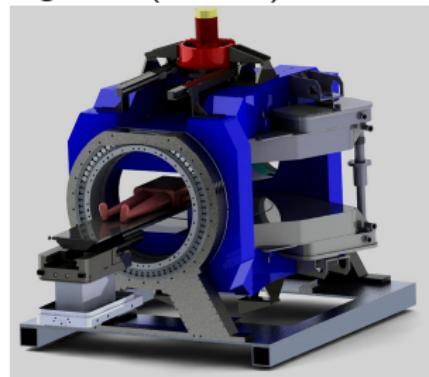
Elekta AB's (Sweden)



ViewRay's MRIdian



MagnetTx (Canada) Aurora RT



Soft Robots for Head Motion Compensation

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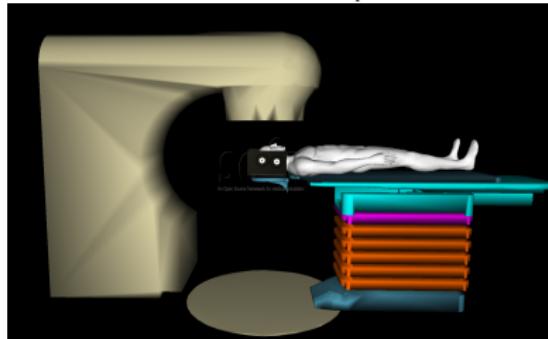
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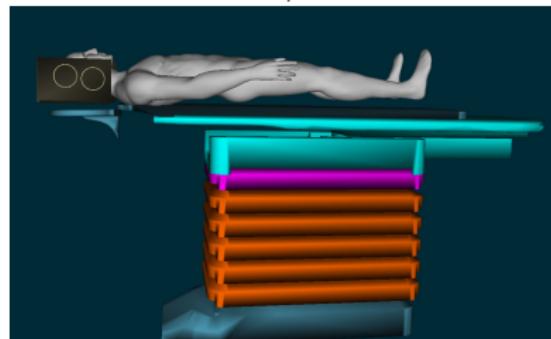
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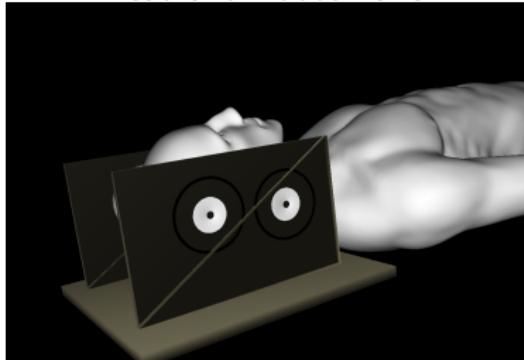
IMRT Setup



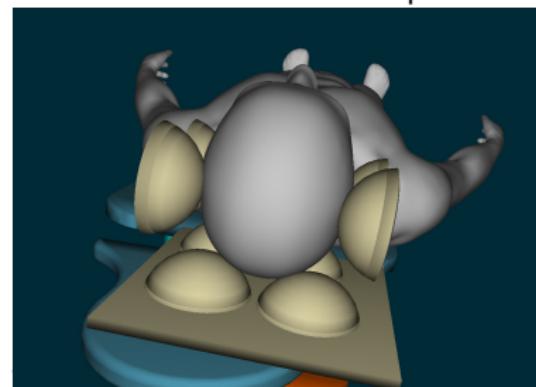
IMRT/MRI



Head and Robot Panel



Head-Robot Closeup



Morphing in Cephalopods

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Morph Stage 1



Morph Stage 2



Morph Stage 3



Morph Stage 4



Morph Stage 5



Morph Reversal

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Cephalopods Neural-Controlled Physical Texture

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Raises Periscope



Papillae



Papillae Up



Papillae × Papillae



Cuttlefish' Morphin ©Roger Hanlon, YouTube.

Cephalopods-inspired Actuator Design

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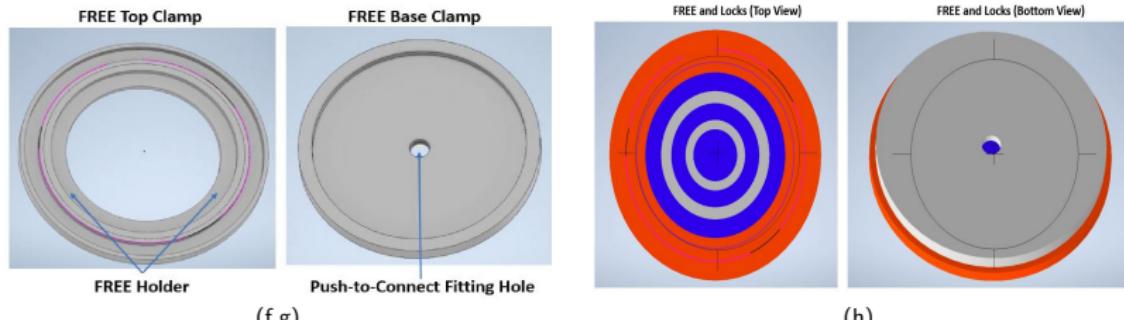
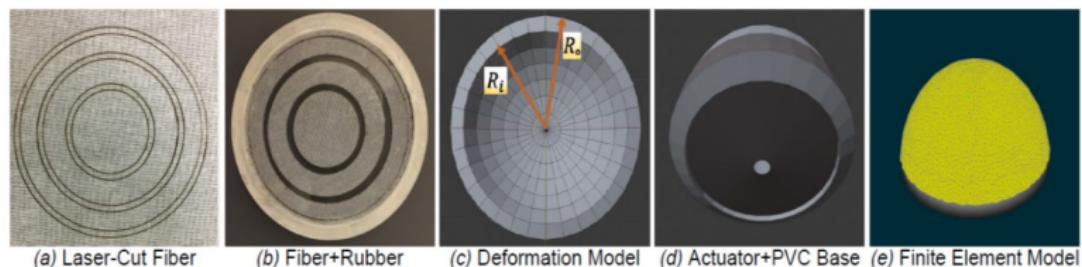
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Circumferentially Constrained And Radially Symmetric Elastomers (CCOARSE).



[Pikul et al. (2019)]

Nonlinear Elastic Deformation Analysis

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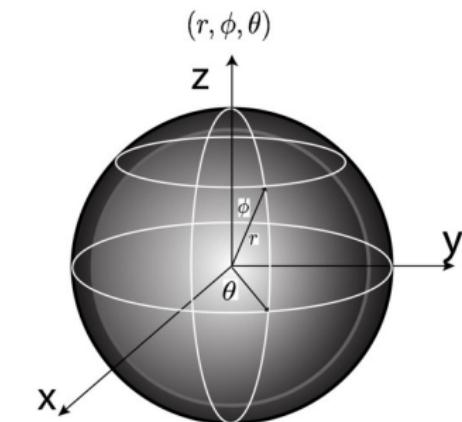
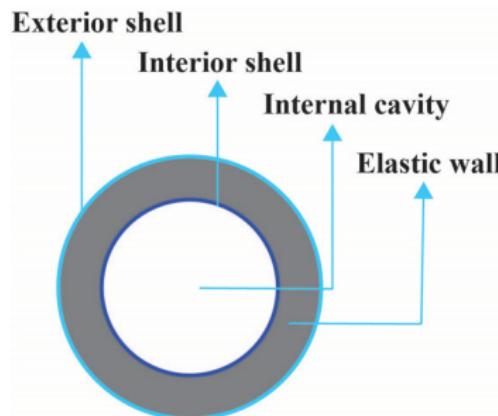
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IAB SHELLS AND AIR CAVITY/DEFORMATION ANALYSIS



$$r_i \leq r \leq r_o, \quad 0 \leq \theta \leq 2\pi, \quad 0 \leq \phi \leq \pi$$

Soft IK via Boundary Value Problem

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- With Cauchy's laws of motion, solve boundary value problem of traction, and find that

$$P(r) = \int_{r_i}^{r_0} \left[2C_1 \left(\frac{r}{R^2} - \frac{R^4}{r^5} \right) + 2C_2 \left(\frac{r^3}{R^4} - \frac{R^2}{r^3} \right) \right] dr \quad (1)$$

- i.e. Given a prescribed radius, find pressure to deform actuator between configurations

Volumetric Deformation Results (Simulation)

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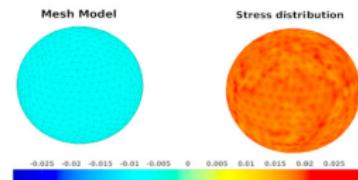
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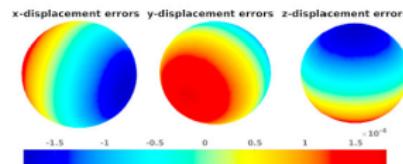
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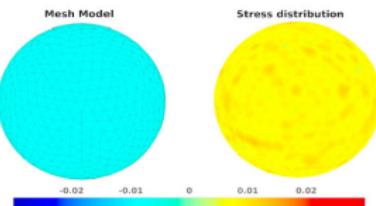
(a) Left: Mesh model. Right: Stress distribution on outer skin.



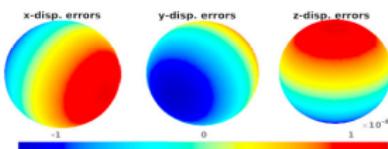
(b) Displacement errors along x, y, z coordinates.

Inputs				Outputs			
C_1	C_2	R_i	r_i	R_o	r_o	P	ΔV
1.1e4	2.2e4	.027	.03	.03	.033	.76	≈ 0

Fig. 6: Volumetric Deformation (Expansion).



(a) Left: Mesh model. Right: Stress distribution on outer skin.



(b) Displacement errors along x, y, z coordinates.

Inputs				Outputs			
C_1	C_2	R_i	r_i	R_o	r_o	P	ΔV
1.1e4	2.2e4	.025	.03	.03	.028	-.34	≈ 0

Fig. 7: Volumetric Deformation (Compression).

Pneumatic Control and Deformation Scheme

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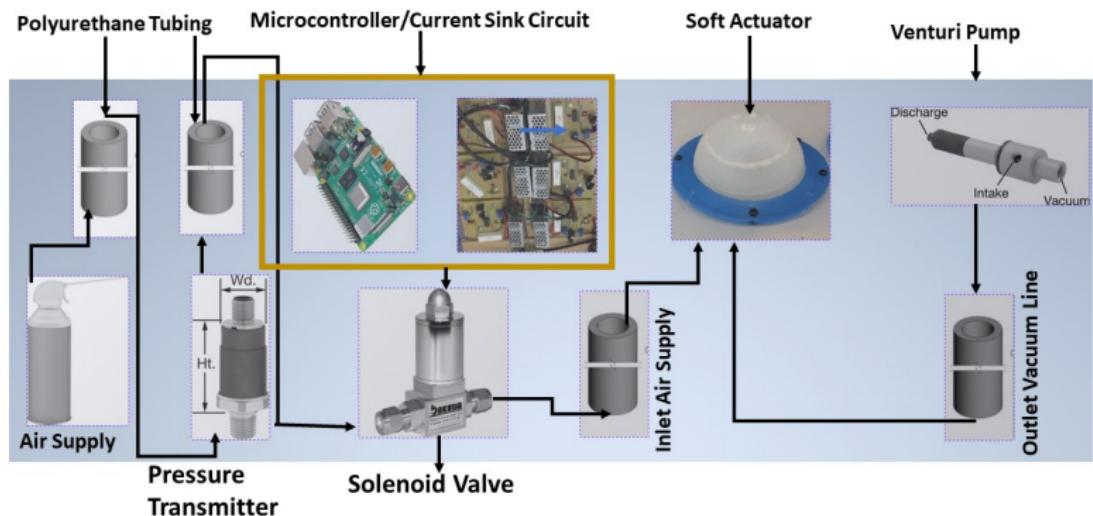
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Volumetric Deformation Results (Actual)

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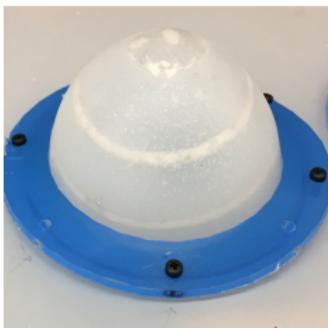
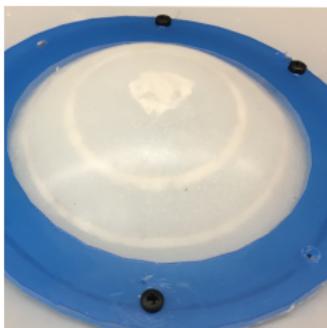
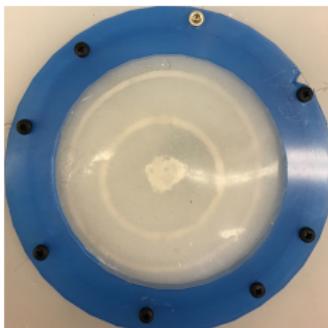
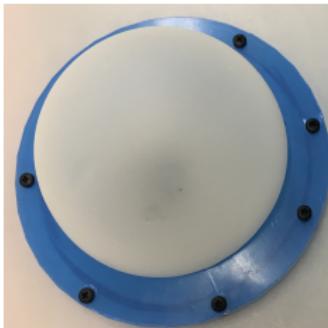
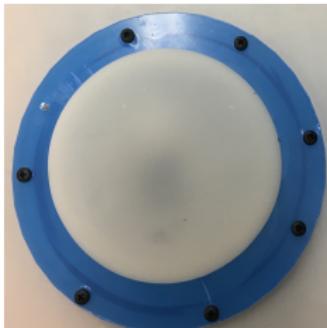
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Actuator and Overall Mechanism with Phantom

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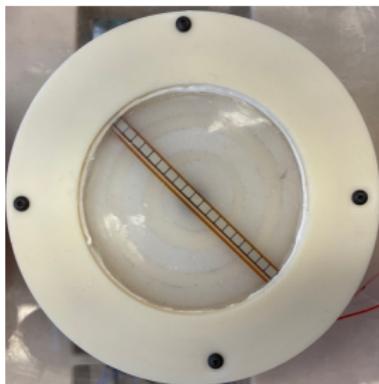
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Head Motion Open Loop Control

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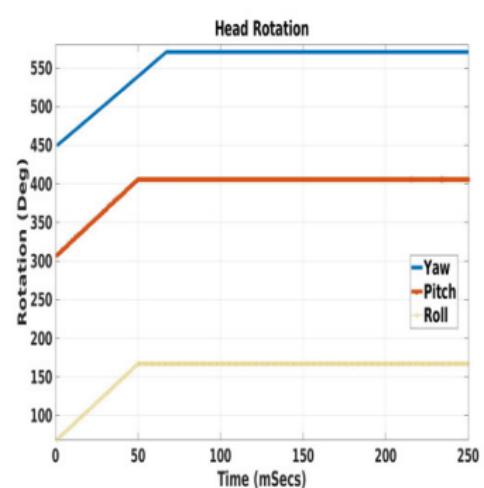
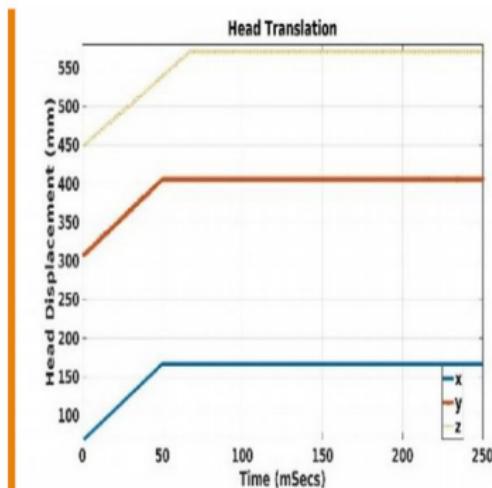
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Independent Actuation



Head Translation along x, y, z for a task of raising the head by a certain threshold above the table

Head rotation in Euler angles for a task of tilting the head about the x, y, z axes on the treatment table.

Ongoing Work: 6-DOF Closed-loop Control

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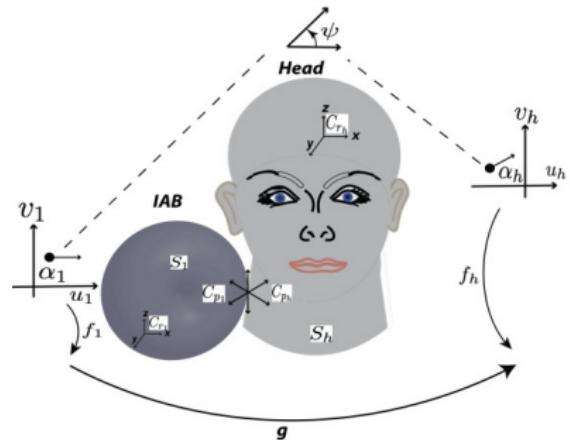
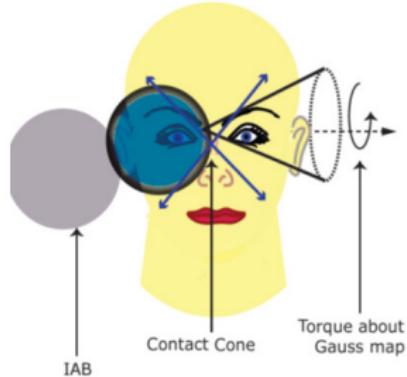
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Continuum Mechanical Model Validation/Differential Geometry/Newton-Euler Dynamics



3-DOF Simulation Testbed

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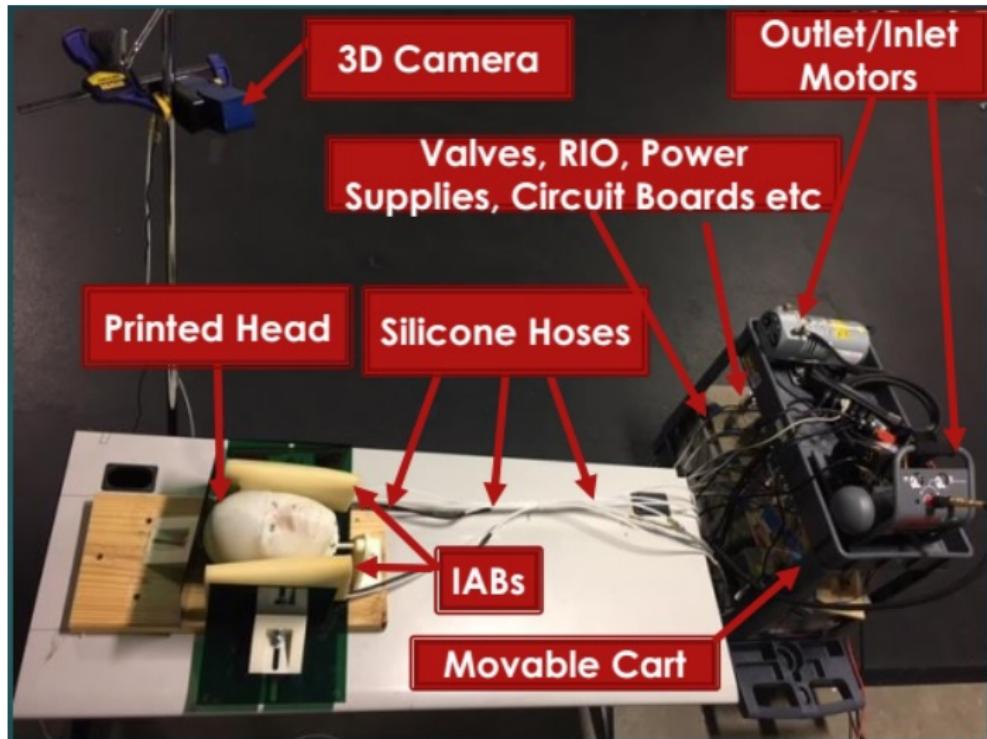
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Model Reference Adaptive Control

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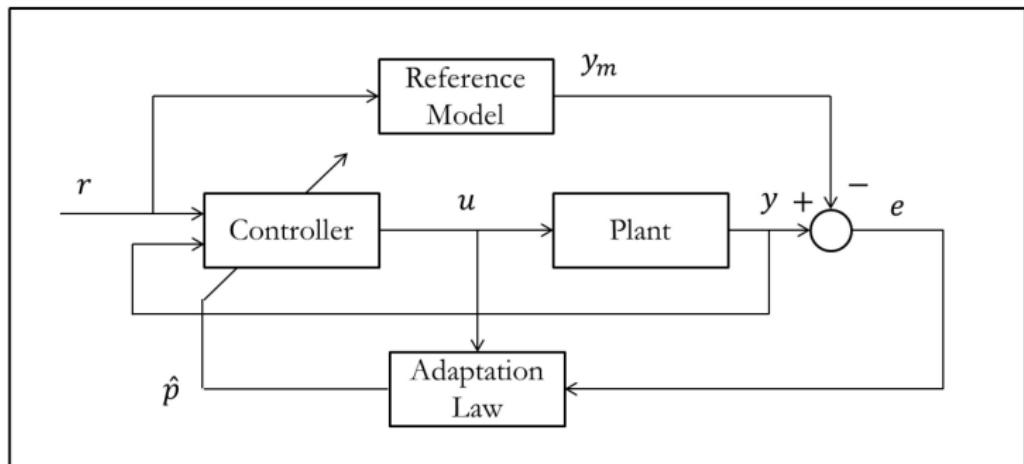
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Indirect MRAC system. (Source mdpi.com)

3-DOF Model Reference Adaptive Control

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- Model head and bladder dynamics as
 - $\dot{x} = Ax + B\Lambda(u - f(x, u)) + w(k)$
- Approximate $f(x, u)$ by a neural network with continuous memory states
- Derive adaptive adjustment mechanism from Lyapunov analysis for Adaptive Control Parks (1966)
 - $u = \underbrace{\hat{K}_x^T x}_{\text{state feedback}} + \underbrace{\hat{K}_r^T r}_{\text{optimal regulator}} + \underbrace{\hat{f}(x, u)}_{\text{approximator}}$

Neural Network Architecture

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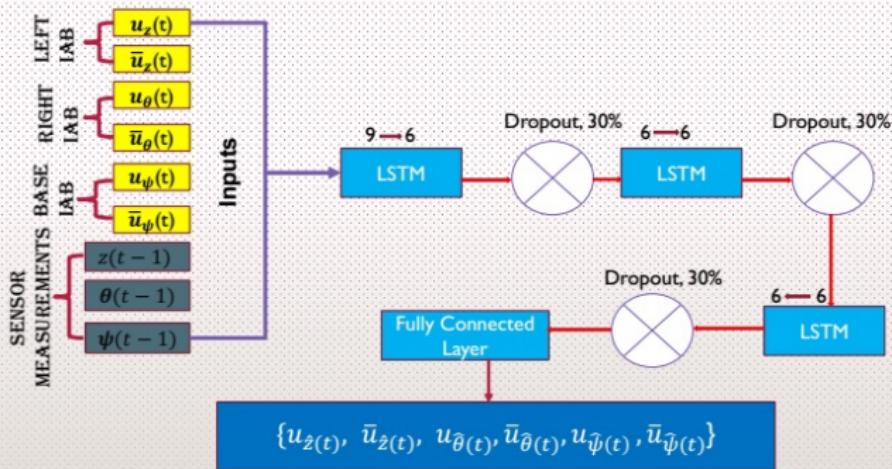
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Neural Net Architecture



Lyapunov Redesign: Theorem

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- For correct adaptive gains, $\hat{\mathbf{K}}_x$ and $\hat{\mathbf{K}}_r$, $\mathbf{e}(k)$ is ***uniformly ultimately bounded***, and the state \mathbf{x} converges to a neighborhood of \mathbf{r} .
- Choose a \mathbf{V} in terms of \mathbf{e} ; $\tilde{\mathbf{K}}_x^T$, $\tilde{\mathbf{K}}_r^T$; and parameter error $\varepsilon_f(\mathbf{x}(k))$ space

$$\mathbf{V}(\mathbf{e}, \tilde{\mathbf{K}}_x, \tilde{\mathbf{K}}_r) = \mathbf{e}^T \mathbf{P} \mathbf{e} + \text{tr}(\tilde{\mathbf{K}}_x^T \Gamma_x^{-1} \tilde{\mathbf{K}}_x | \Lambda |) + \text{tr}(\tilde{\mathbf{K}}_r^T \Gamma_r^{-1} \tilde{\mathbf{K}}_r | \Lambda |)$$

Results: Z and Pitch Motions

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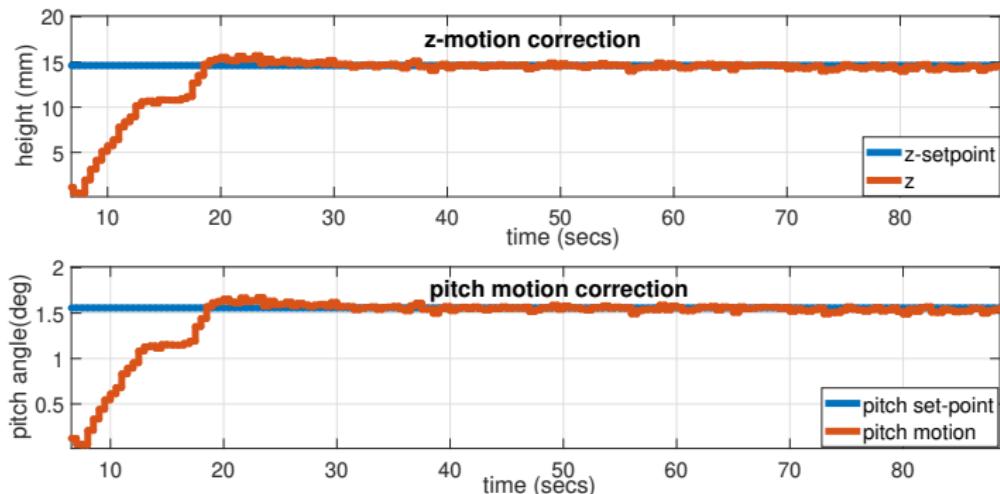
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Goal command: $(z, \theta, \phi) = (14\text{mm}, 1.6^\circ, 45^\circ)^T$.

Results: Roll Motion

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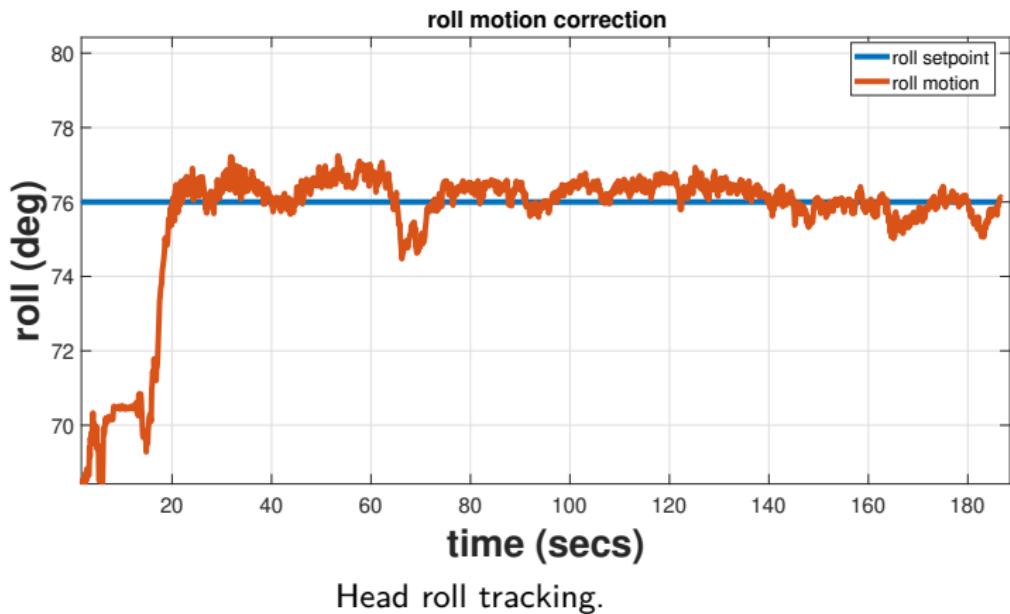
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- Non-invasive soft robot for head motion compensation ✓
- Photons-transparent as opposed to rigid/electro-mechanical devices/robots ✓
- Adaptable under MRI coils for newer MRI-LINACs ✓

Part III: Robustness Margins and Robust Deep Policies

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- Robustness Margins and Robust Deep Policies for Nonlinear Control

The robustness conundrum

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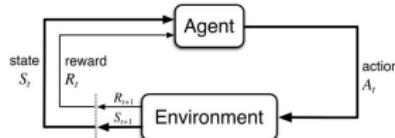
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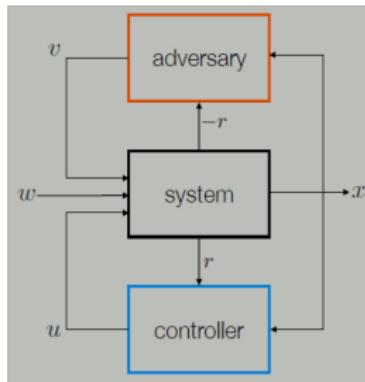
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- How to know *a priori* a policy's robustness limits?



- How to inculcate robustness into multistage decision policies?



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- To quantify the brittleness, we optimize the stage cost

$$\max_{\mathbf{v}_t \sim \psi \in \Psi} \left[\sum_{t=0}^T \underbrace{c(\mathbf{x}_t, \mathbf{u}_t)}_{\text{nominal}} - \gamma \underbrace{g(\mathbf{v}_t)}_{\text{adversarial}} \right]$$

- To mitigate lack of robustness, we optimize the *cost-to-go*

$$\mathcal{J}_t(\mathbf{x}_t, \pi, \psi) = \min_{\mathbf{u}_t \sim \pi} \max_{\mathbf{v}_t \sim \psi} \left(\sum_{t=0}^{T-1} \ell_t(\mathbf{x}_t, \mathbf{u}_t, \mathbf{v}_t) + L_T(\mathbf{x}_T) \right),$$

- and seek a saddle point equilibrium policy that satisfies

$$\mathcal{J}_t(\mathbf{x}_t, \pi^*, \psi) \leq \mathcal{J}_t(\mathbf{x}_t, \pi^*, \psi^*) \leq \mathcal{J}_t(\mathbf{x}_t, \pi, \psi^*),$$

Results: Brittleness Quantification

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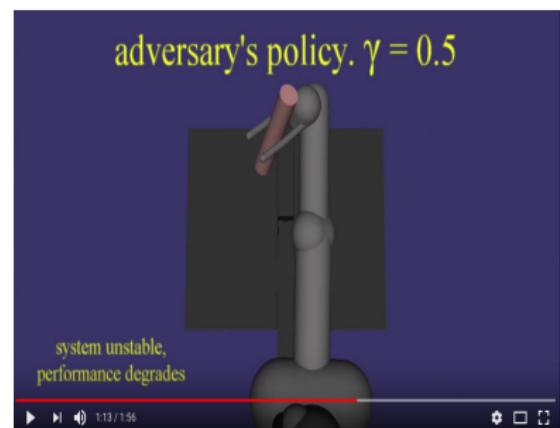
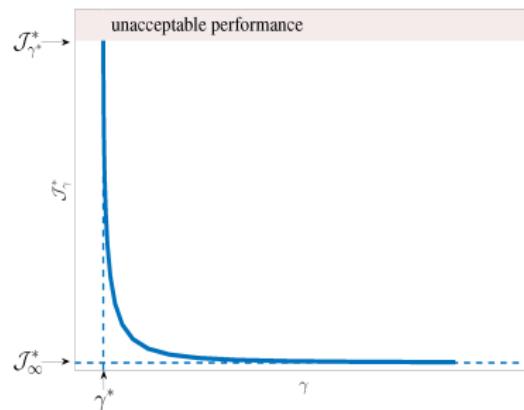
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Results: Iterative Dynamic Game

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Future Work: MRI/RT Immobilization

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- Explore multiple parallel robot mechanisms for head motion correction.
- Adopt iterative dynamic game approach [Ogunmolu et al. (2018)] for solving robust controller for head stabilization.
- Build on Freeman and Kokotovic's point-wise min-norm robust control lyapunov function to realize a meaningful value function in deep policies [Freeman and Kokotovic (1996)].

Constrained Robust Control Lyapunov Function (RCLF) Motion Planning

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Problem Definition

Find RCLF collision-free path $\sigma^* : [0, 1] \rightarrow \mathcal{M}_{free}$ given a path planning problem $(\mathcal{Q}_{free}, \xi_i, \mathcal{Q}_{goal})$, manipulation constraint, G , and cost function V such that $V(\sigma^*) = \min_{\sigma \in \Sigma_{\mathcal{M}_{free}}} V(\sigma)$ if one exists.

- Leverage [Freeman and Kokotovic (1996), Ogunmolu et al. (2018)].
- Greedy approach using L-BFGS optimization algorithm with box constraints, in contrast to the quadratic nonlinear constrained optimization e.g. Khansari-Zadeh and Billard (2014).

Reproducing a Nonlinear Motion with GMM

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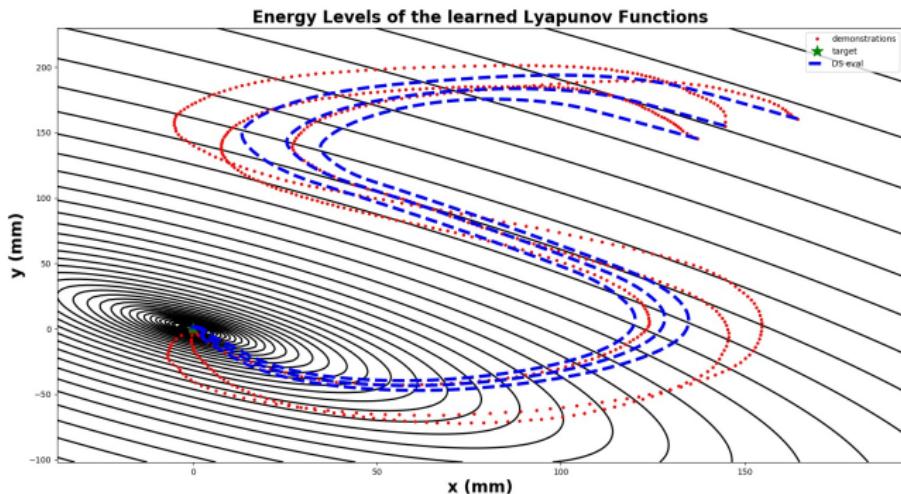
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A CLF motion executor (red curves) that shows convergence to local attractors (green asterisks) and follows 3 different set trajectories (blue curves) for 2D nonlinear motion-trajectory problems on the WAM robot
[Reproduced from Ogunmolu et al. (2020)].

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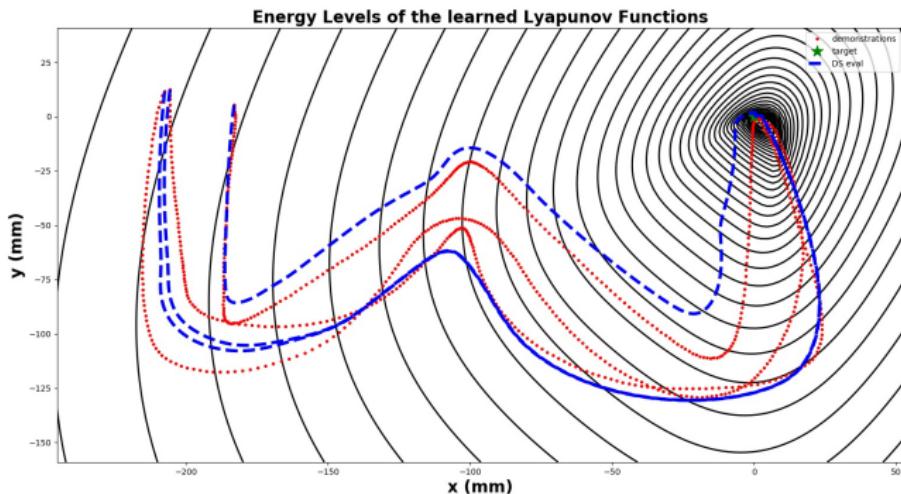
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A CLF motion executor (red curves) that shows convergence to local attractors (green asterisks) and follows 3 different set trajectories (blue curves) for 2D nonlinear motion-trajectory problems on the WAM robot
[Reproduced from Ogunmolu et al. (2020)].

Conclusions

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- Designed a non-invasive soft robot for head motion compensation in IMRT/emerging MRI-LINACs ✓
- Photons-transparent; Adaptable under MRI coils for newer MRI-LINACs ✓
- Fast inference of beam orientations in treatment planning:
Approx 60 secs beams prediction time✓
- Adapted H_{∞} control methods for quantifying the brittleness of deep policies✓
- Devised a min-max-trained deep saddle policy for mitigating model mismatch, transfer errors, and policy sensitivity e.t.c. ✓

End of Slides/More Acknowledgments

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Head
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LINACs RT

MRI-LINACs

Innovation

iDG

Robustness issues

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iDG Results

Futures

References

James Pikul, Asst.
Prof. Penn



Kevin Turner, Prof.
Penn



Audrey Sedal, Res.
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Rachel Thompson,
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Publications

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BOO: Search

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- Formulated as a bandit search that imposes a regret term on the Q -value
- During the planning process, we estimate a *value*, $v(\mathbf{y}_t)$, that estimates the optimality of a beam block;
- In parallel, we refine the deep neural network policy by optimizing its weight in a separate thread.
 - Network parameters updated by a **mixed strategy** which combines its **pure strategy**,
 - It is a best response to the fictitious opponent's **average pure strategy**.

BOO: Fluence Map Optimization

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- Q -value defined as

$$\bar{Q}(s, a) = Q_j(s, a) + c \sqrt{\frac{2 \ln n(s)}{N(s, a)}}, \quad (2)$$

$$a^* = \arg \max_a \bar{Q}(s, a) \quad (3)$$

Fluence Map Optimization

- $\mathcal{X} \implies$ total discretized voxels of interest (VOI 's) in a target volume
- $\mathcal{B}_1 \cup \mathcal{B}_2 \cup \dots \cup \mathcal{B}_n \subseteq \mathcal{B} \implies$ beam partition subset
- $\mathcal{D}_{ij}(\theta_k) \implies$ matrix that describes each dose influence, d_i
 - delivered to a discretized voxel, i , in a volume of interest, VOI_h ($h = 1, \dots, \mathcal{X}$), from a beam angle, θ_k , $k \in \{1, \dots, n\}$

BOO: Fluence Map Optimization

- Suppose further that $\mathcal{D}_{ij}(\theta_k)$ is the matrix that describes each dose influence, d_i
 - delivered to a discretized voxel, i , in a volume of interest, VOI_h ($h = 1, \dots, \mathcal{X}$), from a beam angle, θ_k ,
 $k \in \{1, \dots, n\}$
 - We compute the matrix $\mathcal{D}_{ij}(\theta_k)$ by calculating each d_i for every bixel, j , at every φ° , resolution, where $j \in \mathcal{B}_k$

BOO: FMO problem definition

- The fluence problem is to find the values of decision variables, x_j , for which d_i to the tumor is maximized, while simultaneously minimizing the d_i to critical structures
- For the voxels in a target volume,
 - let a weighted quadratic objective minimize the l_2 distance between a pre-calculated dose \mathbf{Ax} , and a doctor's prescribed dose, \mathbf{b}
 - let a weighted quadratic objective maximizes the l_2 distance between \mathbf{Ax} (where \mathbf{x} represents the vectorized bixels, x_j) and \mathbf{b}

BOO: FMO problem definition

- Cost

$$\frac{1}{v_s} \sum_{s \in \text{OARs}} \|(\underline{w}_s \mathcal{D}_{ij}^s \mathbf{x}_s)_+ - b_s\|_2^2 + \frac{1}{v_s} \sum_{s \in \text{PTVs}} \|(\bar{w}_s \mathcal{D}_{ij}^s \mathbf{x}_s - b_s)_+\|_2^2 \quad (4)$$

- Pre-calculated dose term:

$\mathbf{Ax} = \left\{ \sum_s \frac{w_s}{v_s} \mathcal{D}_{ij}^s \mathbf{x}_s \mid \mathcal{D}_{ij} \in \mathbb{R}^{n \times l}, n > l \right\}$, which is a combination of the dose components that belong to OARs and those that belong to PTVs.

- Let $w_s = \{\underline{w}_s, \bar{w}_s\}$ be the respective underdosing and overdosing weights for the OARs and PTVs

- v_s represents the total number of voxels in each structure.

BOO: FMO

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- Rewriting the objective

$$\min \frac{1}{2} \|Ax - b\|_2^2 \quad \text{subject to } x \geq 0.$$

- With Lagrangian:

$$L(x, \lambda) = \min \frac{1}{2} \|Ax - b\|_2^2 - \lambda^T x.$$

- Introducing an auxiliary variable z , we have

$$\min_x \frac{1}{2} \|Ax - b\|_2^2, \quad \text{subject to } z = x, \quad z \geq 0,$$

BOO: FMO by way of ADMM

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- Solving either the \mathbf{x} and \mathbf{z} sub-problems, we have

$$\mathbf{x}^{k+1} = (\mathbf{A}^T \mathbf{A} + \rho \mathbf{I})^{-1} (\mathbf{A}^T \mathbf{b} + \rho \mathbf{z}^k - \boldsymbol{\lambda}^k). \quad (5)$$

- And using the soft-thresholding operator, $S_{\boldsymbol{\lambda}/\rho}$, we find that

$$\mathbf{z}^{k+1} = S_{\boldsymbol{\lambda}/\rho} (\mathbf{x}^{k+1} + \boldsymbol{\lambda}^k), \quad (6)$$

where $S_{\boldsymbol{\lambda}/\rho}(\tau) = (\mathbf{x} - \boldsymbol{\lambda}/\rho)_+ - (-\tau - \boldsymbol{\lambda}/\rho)_+$. $\boldsymbol{\lambda}$ is updated as

$$\boldsymbol{\lambda}^{k+1} = \boldsymbol{\lambda}^k - \gamma (\mathbf{z}^{k+1} - \mathbf{x}^{k+1}), \quad (7)$$

where γ is a parameter that controls the step length.

App A: 3-DOF Closed-loop Control

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Closed-loop Phantom motion control along 3 DoFs with an adaptive neuro-controller.

3-DOF Simulation Testbed

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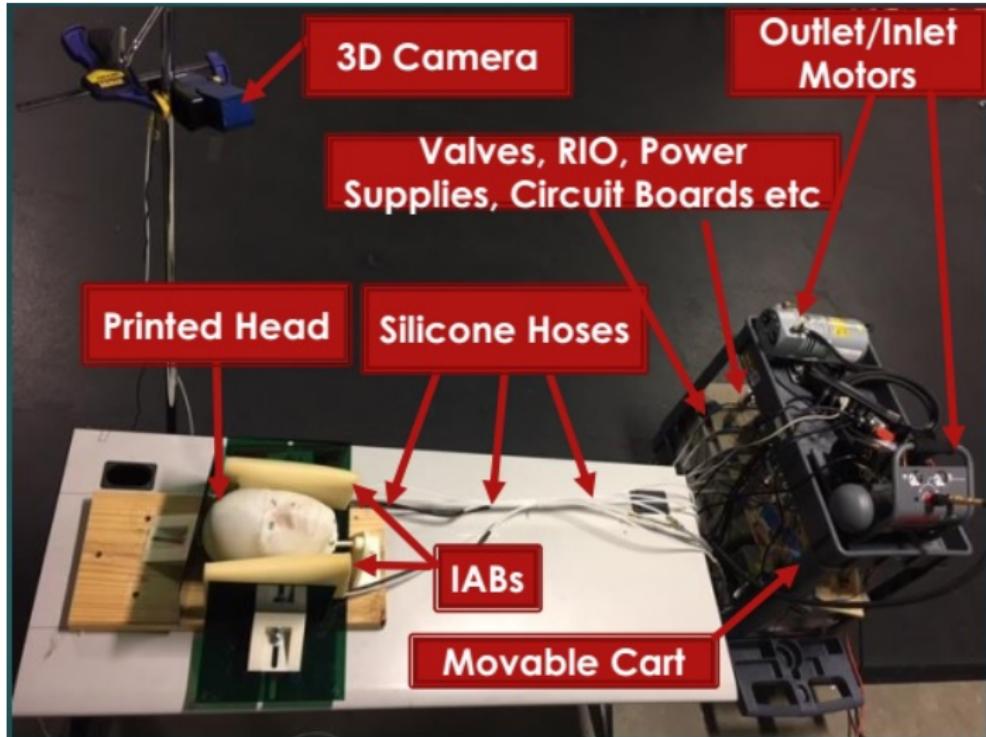
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Hardware Description

Control Design Goals

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- Stabilize z , pitch, and roll states, *i.e.*

$$\mathbf{x} = \begin{pmatrix} z \\ \theta \\ \phi \end{pmatrix}$$

- By solving an adaptive state feedback controller, optimal regulation, and minimize parametric uncertainties

Control Design Goals

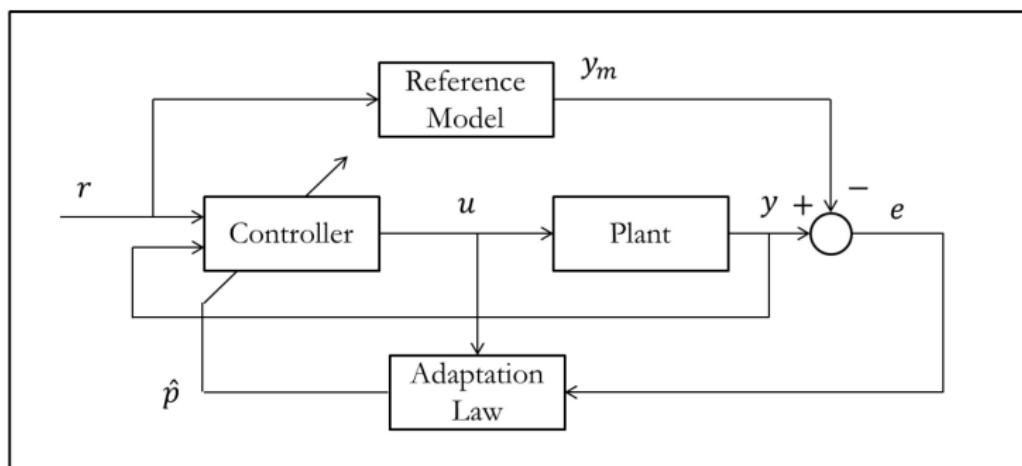
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- Provide closed loop tracking given a desired trajectory, r
- Robustify system to (non-)parametric uncertainties



Indirect MRAC system. (Source mdpi.com)

Lyapunov Redesign: Theorem

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- For correct adaptive gains, $\hat{\mathbf{K}}_x$ and $\hat{\mathbf{K}}_r$, $\mathbf{e}(k)$ is ***uniformly ultimately bounded***, and the state \mathbf{x} converges to a neighborhood of \mathbf{r} .
- Choose a \mathbf{V} in terms of \mathbf{e} ; $\tilde{\mathbf{K}}_x^T$, $\tilde{\mathbf{K}}_r^T$; and parameter error $\varepsilon_f(\mathbf{x}(k))$ space

$$\mathbf{V}(\mathbf{e}, \tilde{\mathbf{K}}_x, \tilde{\mathbf{K}}_r^T) = \mathbf{e}^T \mathbf{P} \mathbf{e} + \text{tr}(\tilde{\mathbf{K}}_x^T \Gamma_x^{-1} \tilde{\mathbf{K}}_x^T |\Lambda|) + \text{tr}(\tilde{\mathbf{K}}_r^T \Gamma_r^{-1} \tilde{\mathbf{K}}_r^T |\Lambda|)$$

Stability proof

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$$\dot{V}(\mathbf{e}, \tilde{\mathbf{K}}_y, \tilde{\mathbf{K}}_r) = \dot{\mathbf{e}}^T \mathbf{P} \mathbf{e} + \mathbf{e}^T \mathbf{P} \dot{\mathbf{e}} + 2\text{tr}(\tilde{\mathbf{K}}_y^T \Gamma_y^{-1} \dot{\tilde{\mathbf{K}}}_y | \Lambda |) \\ + 2\text{tr}(\tilde{\mathbf{K}}_r^T \Gamma_r^{-1} \dot{\tilde{\mathbf{K}}}_r | \Lambda |)$$

$$= [\mathbf{A}_m \mathbf{e} + \mathbf{B} \Lambda [\Delta \hat{\mathbf{K}}_r^T \mathbf{r} + \Delta \hat{\mathbf{K}}_x^T \mathbf{x}]]^T \mathbf{P} \mathbf{e} + \dots$$

$$\mathbf{e}^T \mathbf{P} [\mathbf{A}_m \mathbf{e} + \mathbf{B} \Lambda [\Delta \hat{\mathbf{K}}_r^T \mathbf{r} + \Delta \hat{\mathbf{K}}_x^T \mathbf{x}]] + \dots$$

$$2\text{tr}(\Delta \mathbf{K}_x^T \Gamma_x^{-1} \dot{\hat{\mathbf{K}}}_x | \Lambda |) + 2\text{tr}(\Delta \mathbf{K}_r^T \Gamma_r^{-1} \dot{\hat{\mathbf{K}}}_r | \Lambda |)$$

Stability Analysis

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$$= \mathbf{e}^T (\mathbf{P} \mathbf{A}_m + \mathbf{A}_m^T \mathbf{P}) \mathbf{e} + 2\mathbf{e}^T \mathbf{P} \mathbf{B} \boldsymbol{\Lambda} \left(\tilde{\mathbf{K}}_y^T \mathbf{y} + \tilde{\mathbf{K}}_r^T \mathbf{r} \right)$$

$$+ 2\mathbf{tr} \left(\tilde{\mathbf{K}}_y^T \boldsymbol{\Gamma}_y^{-1} \dot{\tilde{\mathbf{K}}}_y | \boldsymbol{\Lambda} | \right) + 2\mathbf{tr} \left(\tilde{\mathbf{K}}_r^T \boldsymbol{\Gamma}_r^{-1} \dot{\tilde{\mathbf{K}}}_r | \boldsymbol{\Lambda} | \right)$$

$$= -\mathbf{e}^T \mathbf{Q} \mathbf{e} - 2\mathbf{e}^T \mathbf{P} \mathbf{B} \boldsymbol{\Lambda} \boldsymbol{\varepsilon}_f(\mathbf{y}) + 2\mathbf{e}^T \mathbf{P} \mathbf{B} \boldsymbol{\Lambda} \tilde{\mathbf{K}}_y^T \mathbf{y}$$

$$+ 2\mathbf{tr} \left(\tilde{\mathbf{K}}_y^T \boldsymbol{\Gamma}_y^{-1} \dot{\tilde{\mathbf{K}}}_y \right) + 2\mathbf{e}^T \mathbf{P} \mathbf{B} \boldsymbol{\Lambda} \tilde{\mathbf{K}}_r^T \mathbf{r} + 2\mathbf{tr} \left(\Delta \mathbf{K}_r^T \boldsymbol{\Gamma}_r^{-1} \dot{\tilde{\mathbf{K}}}_r \right)$$

Notice $x^T y = \mathbf{tr} (y x^T)$ from trace identity

Stability Analysis Cont'd

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Therefore,

$$\begin{aligned}\dot{\mathbf{V}}(\cdot) = & -\mathbf{e}^T \mathbf{Q} \mathbf{e} - 2\mathbf{e}^T \mathbf{P} \mathbf{B} \boldsymbol{\Lambda} \varepsilon_f \\ & + 2 \mathbf{tr} \left(\tilde{\mathbf{K}}_y^T (\boldsymbol{\Gamma}_y^{-1} \dot{\tilde{\mathbf{K}}}_y + \mathbf{y} \mathbf{e}^T \mathbf{P} \mathbf{B} \text{sgn}(\boldsymbol{\Lambda})) \right) |\boldsymbol{\Lambda}| \\ & + 2 \mathbf{tr} \left(\tilde{\mathbf{K}}_r^T (\boldsymbol{\Gamma}_r^{-1} \dot{\tilde{\mathbf{K}}}_r + \mathbf{r} \mathbf{e}^T \mathbf{P} \mathbf{B} \text{sgn}(\boldsymbol{\Lambda})) \right) |\boldsymbol{\Lambda}|\end{aligned}$$

where for a real-valued x , we have $x = \text{sgn}(x)|x|$.

- first two terms will be negative definite for all $\mathbf{e} \neq 0$
 - since \mathbf{A}_m is Hurwitz
- other terms will be identically null if we choose the adaptation laws

$$\dot{\tilde{\mathbf{K}}}_y = -\boldsymbol{\Gamma}_y \mathbf{y} \mathbf{e}^T \mathbf{P} \mathbf{B} \text{sgn}(\boldsymbol{\Lambda}), \quad \dot{\tilde{\mathbf{K}}}_r = -\boldsymbol{\Gamma}_r \mathbf{r} \mathbf{e}^T \mathbf{P} \mathbf{B} \text{sgn}(\boldsymbol{\Lambda})$$

Stability Results: Ogunmolu et al. (2017)

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$$\begin{aligned}\dot{\mathbf{V}}(\cdot) &= -\mathbf{e}^T \mathbf{Q} \mathbf{e} - 2\mathbf{e}^T \mathbf{P} \mathbf{B} \boldsymbol{\Lambda} \boldsymbol{\varepsilon}_f \\ &\leq -\lambda_{low} \|\mathbf{e}\|^2 + 2\|\mathbf{e}\| \|\mathbf{P} \mathbf{B}\| \lambda_{high}(\boldsymbol{\Lambda}) \boldsymbol{\varepsilon}_{max}\end{aligned}$$

- $\{\lambda_{low}, \lambda_{high}\} \equiv \min/\max \text{ eigenvalues of } Q \text{ and } \boldsymbol{\Lambda}$.
- $\dot{\mathbf{V}}(\cdot)$ is thus negative definite outside the compact set:
$$\chi = \left(\mathbf{e} : \|\mathbf{e}\| \leq \frac{2\|\mathbf{P} \mathbf{B}\| \lambda_{high}(\boldsymbol{\Lambda}) \boldsymbol{\varepsilon}_{max}(\mathbf{y})}{\lambda_{low}(\mathbf{Q})} \right)$$
 - i.e. \mathbf{e} is uniformly ultimately bounded, or $\mathbf{y}(t) \rightarrow 0$ as $t \rightarrow \infty$.

Appendix C: 1-DOF Closed-Loop Control

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Head Pose Estimation: Sensor Fusion

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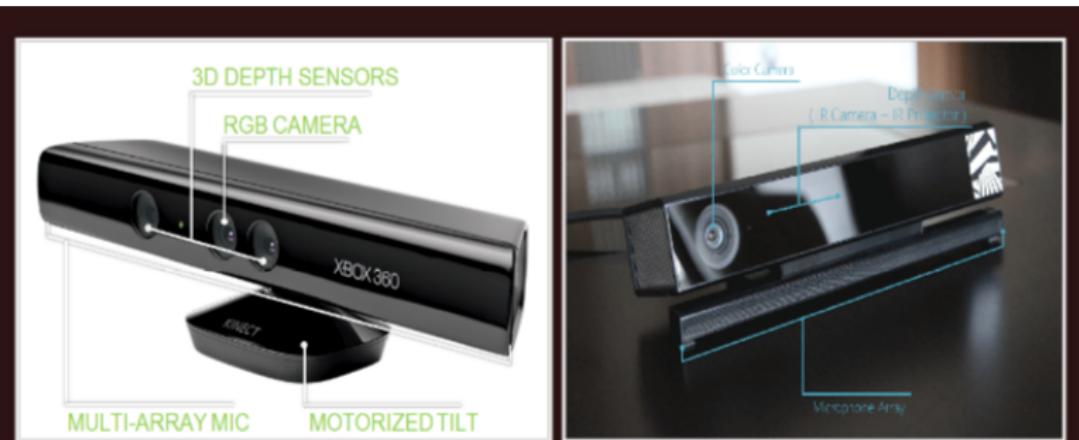
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Kinect Xbox

Kinect v1

Sensors' Noise Floor

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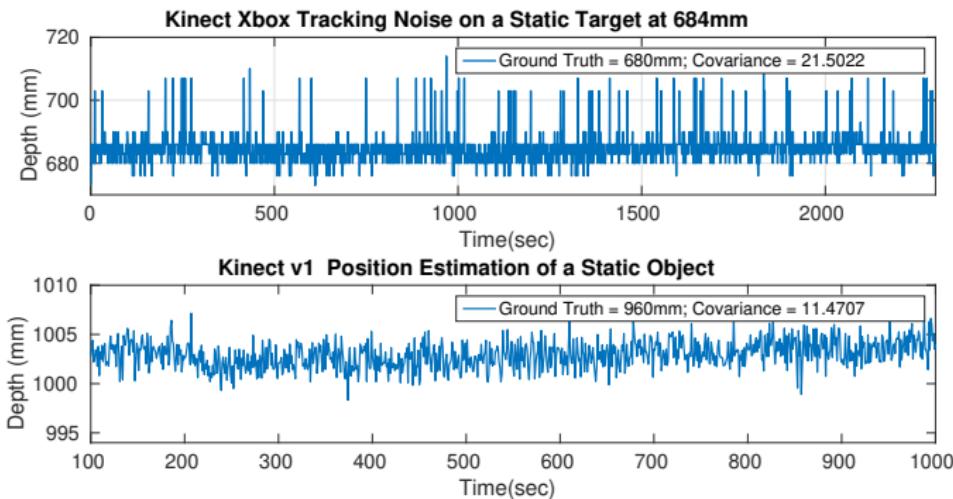
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Case for Sensed Observation Filtering

Optimal head state estimation and sensor fusion

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- Find the observation estimates $\hat{\mathbf{x}}(i)$ that minimize the mean-square error from true measurement, i.e. ,

$$\hat{\mathbf{x}}(i|j) = \arg \min_{\hat{\mathbf{x}}(i|j) \in \mathbb{R}^n} \mathbb{E}\{(\mathbf{x}(i) - \hat{\mathbf{x}})^T (\mathbf{x}(i) - \hat{\mathbf{x}}) | z(1), \dots, z(j)\}$$

- Define the estimate error's covariance as

$$\mathbf{P}(i|j) \triangleq \mathbb{E}\{(\mathbf{x}(i) - \hat{\mathbf{x}}(i|j))^T (\mathbf{x}(i) - \hat{\mathbf{x}}(i|j)) | Z^j\}. \quad (8)$$

State estimation with Kalman filters

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- Assume state model, $\mathbf{F}(k)$
- For a discretized time interval ΔT between measurements, we define the state

$$\mathbf{x}(k) = \mathbf{F}(k)\mathbf{x}(k-1) + \mathbf{B}(k)\mathbf{u}_k + \mathbf{G}_k\mathbf{w}_k \quad (9)$$

- with

$$\mathbf{F} = \begin{bmatrix} 1 & \Delta T \\ 0 & 1 \end{bmatrix} \quad (10)$$

Kalman filters

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- (9) $\Rightarrow \mathbf{x}_k = \mathbf{F}_k \mathbf{x}_{k-1} + \mathbf{G}_k \mathbf{w}_k$
- \mathbf{G}_k := uncontrolled forces accelerating on head
- Head's acceleration, $a_k \sim \mathcal{N}(0, \sigma_a)$
- Setting $\mathbf{G}_k = \mathbf{I}_{2 \times 2}$ and $\mathbf{w}(k) \sim \mathcal{N}(0, \mathbf{Q}(k))$
 - set $\mathbf{Q}(k)$ to a random walk sequence, $\mathbf{W}_k = [\frac{\Delta T^2}{2}, \Delta T]^T$

Kalman Filters Design

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- Such that

$$\mathbf{Q} = \mathbf{W}\mathbf{W}^T \sigma_a^2 = \begin{bmatrix} \frac{\Delta T^4}{4} & \frac{\Delta T^3}{2} \\ \frac{\Delta T^3}{2} & \Delta T^2 \end{bmatrix} \sigma_a^2. \quad (11)$$

- Set the transfer matrix from the estimates, $\mathbf{x}(k)$, to observations, $z_1(k)$ and $z_2(k)$ according to

$$z_s = \mathbf{H}_s(k)\mathbf{x}(k) + v_s(k) \quad s = 1, 2 \quad (12)$$

- where $\mathbf{H}_s(k) = [1, \ 0]^T$ and $v_s(k) \sim \mathcal{N}(0, \sigma_{rs}^2)$

KF Priori and Posteriori State Estimates

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■ Prediction Phase:

$$\hat{\mathbf{x}}_{k|k-1} = \mathbf{F}\hat{\mathbf{x}}_{k-1|k-1} + \mathbf{B}_k \mathbf{u}_k$$

$$\mathbf{P}_{k|k-1} = \mathbf{F}_k \mathbf{P}_{k-1|k-1} \mathbf{F}_k^T + \mathbf{Q}_k \quad (13)$$

■ Update Phase:

$$\mathbf{K}(k) = \mathbf{P}(k|k-1) \mathbf{H}(k)^T [\mathbf{H}(k) \mathbf{P}(k|k-1) \mathbf{H}(k)^T + \mathbf{R}(k)]^{-1}$$

$$\hat{\mathbf{x}}(k|k) = \hat{\mathbf{x}}(k|k-1) + \mathbf{K}(k)(\mathbf{z}(k) - \mathbf{H}(k)\hat{\mathbf{x}}(k|k-1))$$

$$\mathbf{P}(k|k) = (\mathbf{I} - \mathbf{K}(k)\mathbf{H}(k))\mathbf{P}(k|k-1) \quad (14)$$

Xbox Filtering Results

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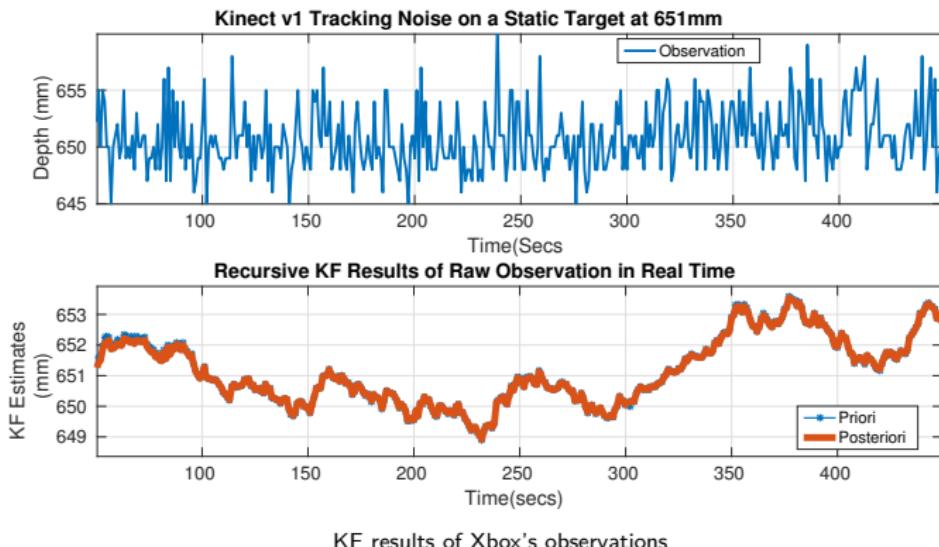
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Kinect 2 Filtering Results

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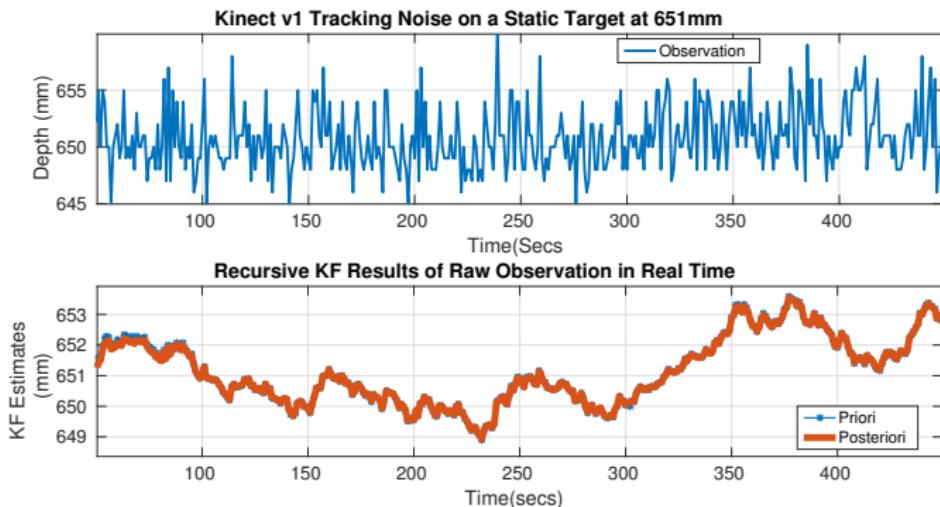
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KF results of Kinect v1's observation

Filtering Results

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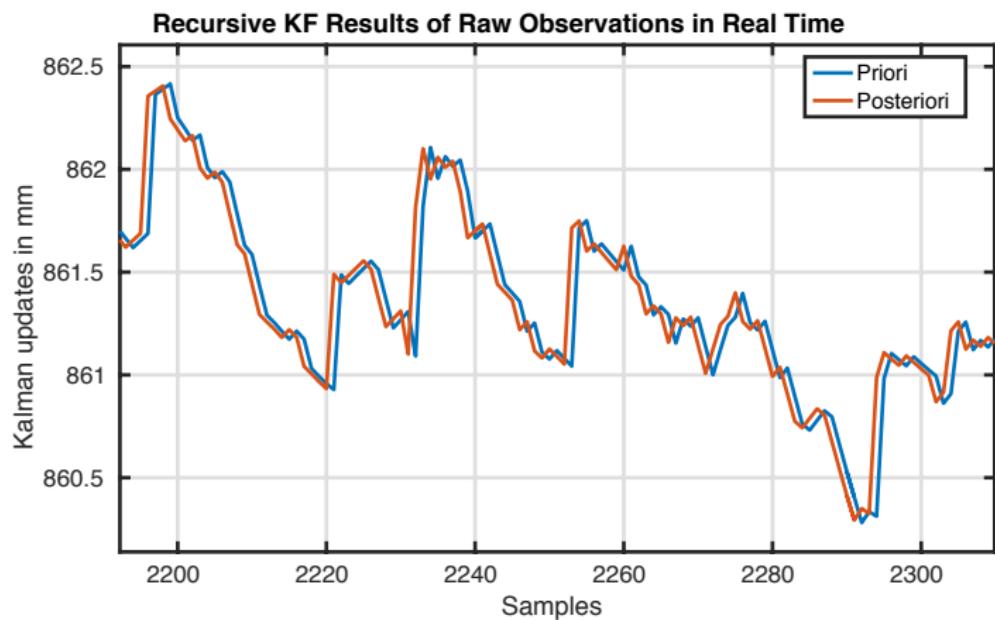
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Global fusion of local tracks

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- Fuse both updates with a variance-weighted average of each local track as follows,

$$\hat{\mathbf{x}}(F)(k|k) = \mathbf{P}(F)(k|k) \sum_{s=1}^N \left[\mathbf{P}(s)^{-1}(k|k) \hat{\mathbf{x}}(s)(k|k) \right]$$

$$\text{where } \mathbf{P}(F)(k|k) = \left[\sum_{s=1}^N \mathbf{P}(s)^{-1}(k|k) \right]^{-1}.$$

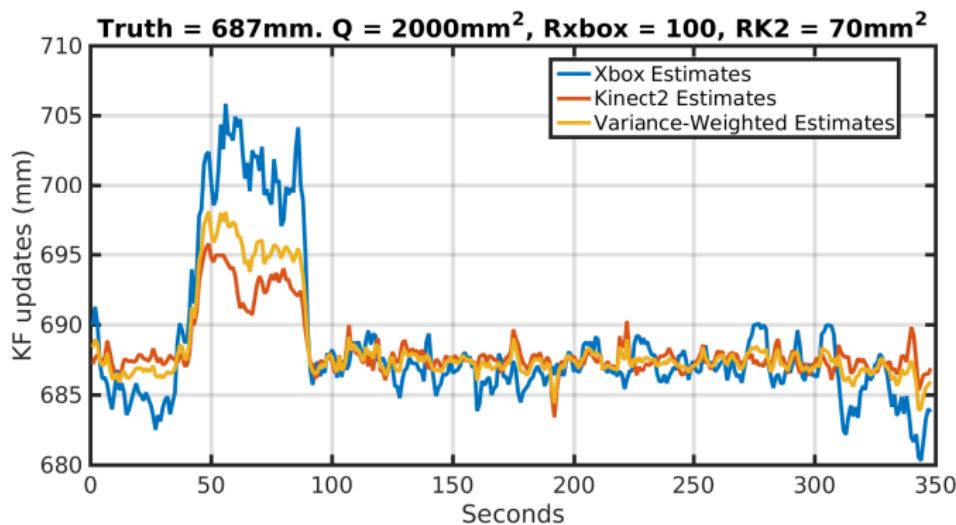
Track-to-track Fusion

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Track-to-track fusion of both sensors' local track estimates.

Vision-based Control

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- From I/O data, estimate a model
- Find set of optimal model parameters via the minimization,

$$G(t) = \arg \min_{\theta} V_N(\theta, Z^N)$$

- where $V_N(\theta, Z^N) = \sum_{k=1}^K \sum_{i=1}^n \frac{1}{2} (\hat{y}_i(k) - y_i(k))^2$,
- and $Z^N = \{u(1) \cdots u(N), y(1) \cdots y(N)\}$
- After a least squares minimization, we derive a state-space realization,

$$\begin{aligned} \mathbf{x}(k + Ts) &= \mathbf{Ax}(k) + \mathbf{Bu}(k) + \mathbf{Ke}(k) \\ \mathbf{y}(k) &= \mathbf{Cx}(k) + \mathbf{Du}(k) + \mathbf{e}(k) \end{aligned} \quad (15)$$

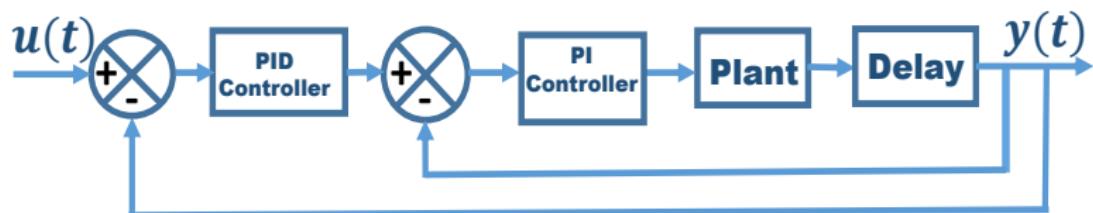
PID-PI Cascaded Controller

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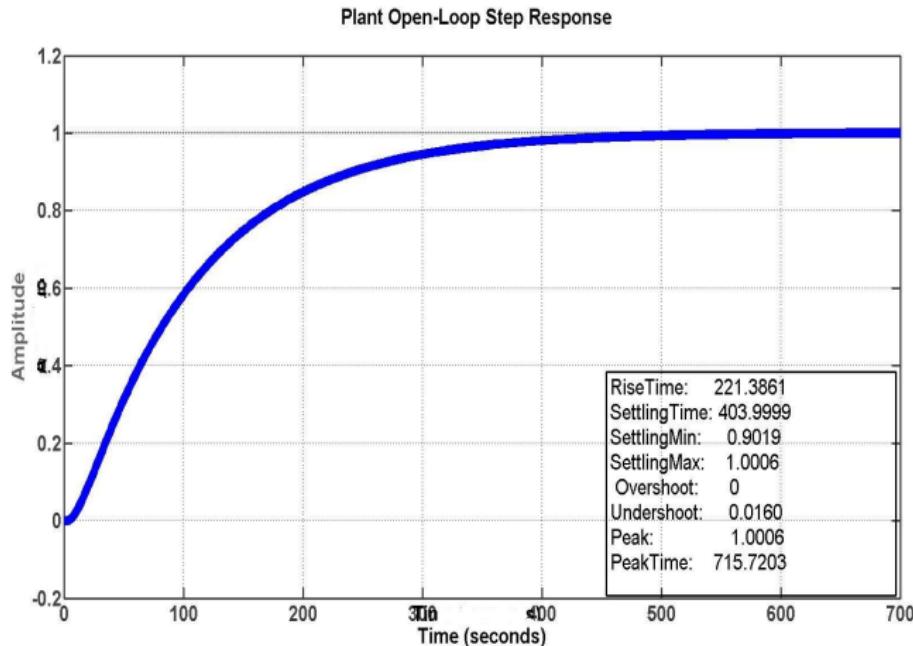
Open Loop Step Response

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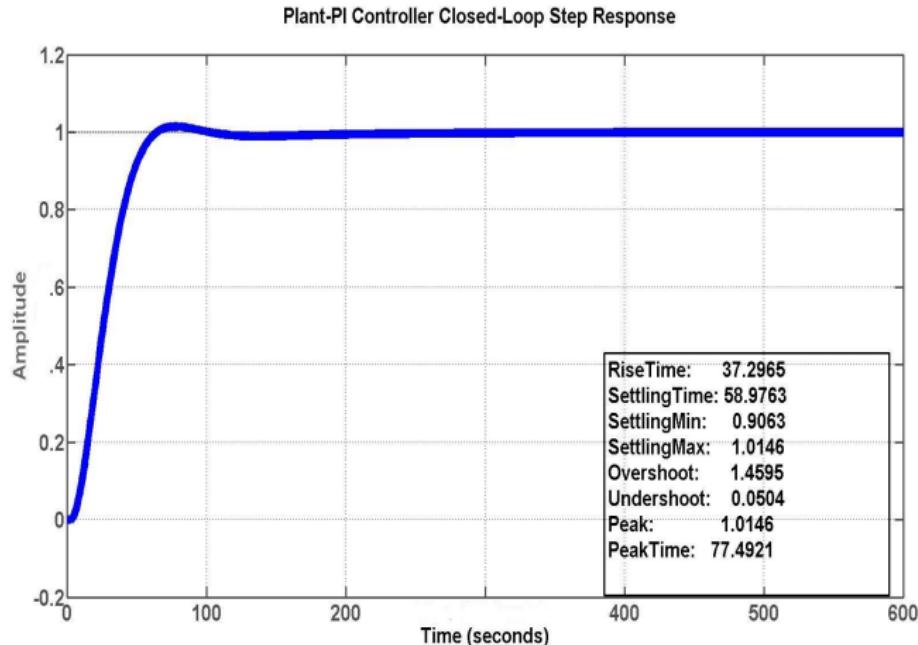
PI Closed-loop Step Response

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Cascaded PID-PI Closed-loop Step Response

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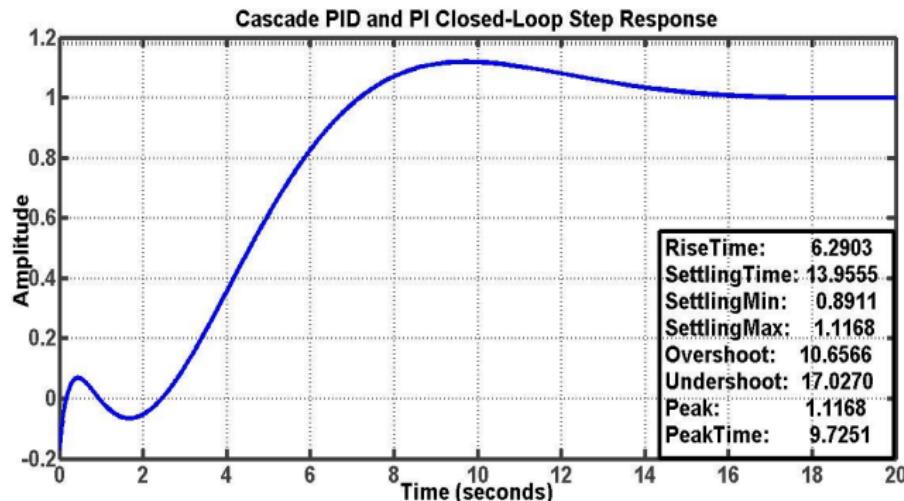
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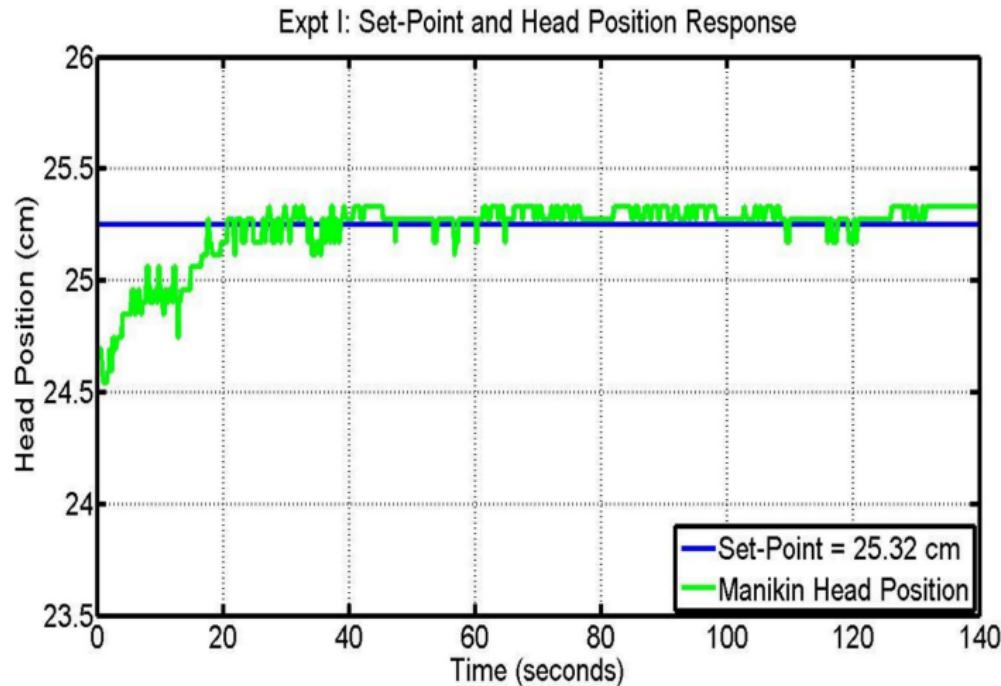
PI-PD Cascaded Controller Experimental Results

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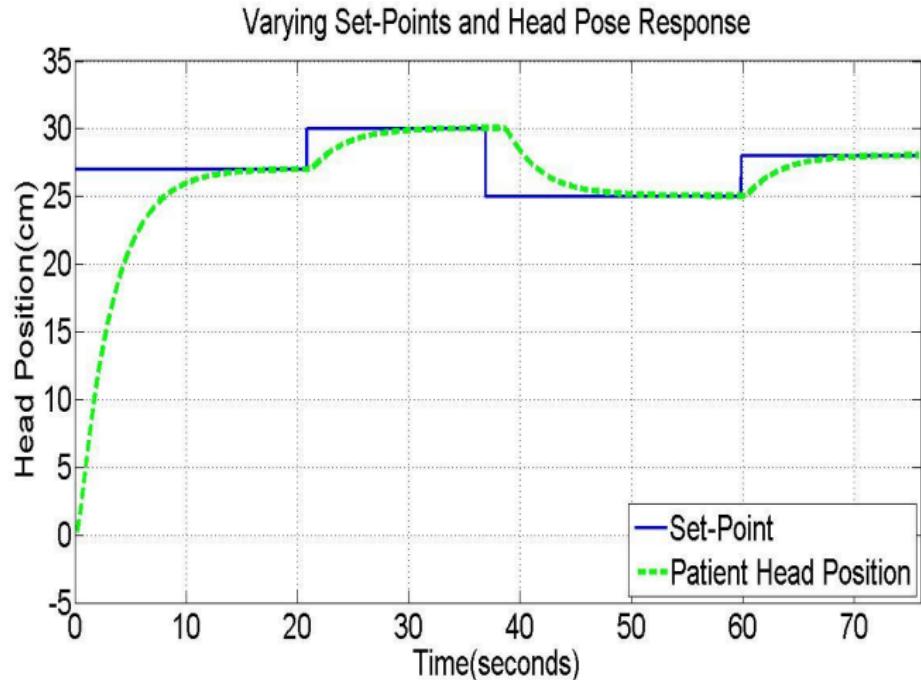
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Varying Setpoint Experiment

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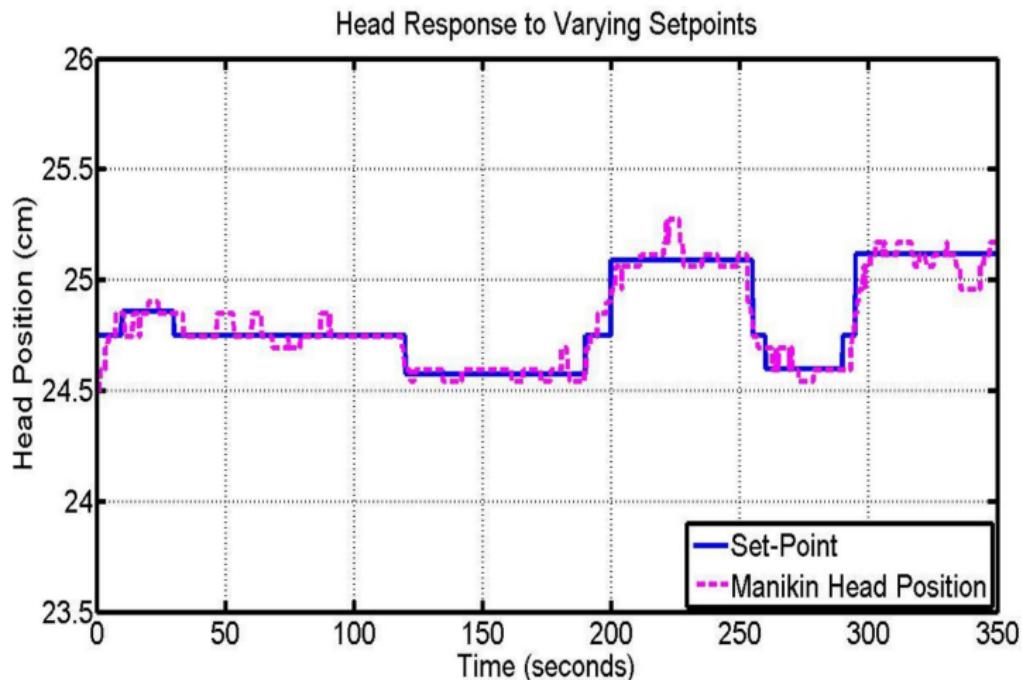
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3-DOF Controller Design (IROS 2017)

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■ Posing the cost

$$J = \sum_{k=0}^K x(k)^T Q x(k) + u(k)^T R u(k) + 2x(k)^T N u(k)$$

- we can obtain u as $\Delta u = \arg \min_{\Delta u} J$
- Δu is a future control sequence

Closed-loop control (Full state observer).

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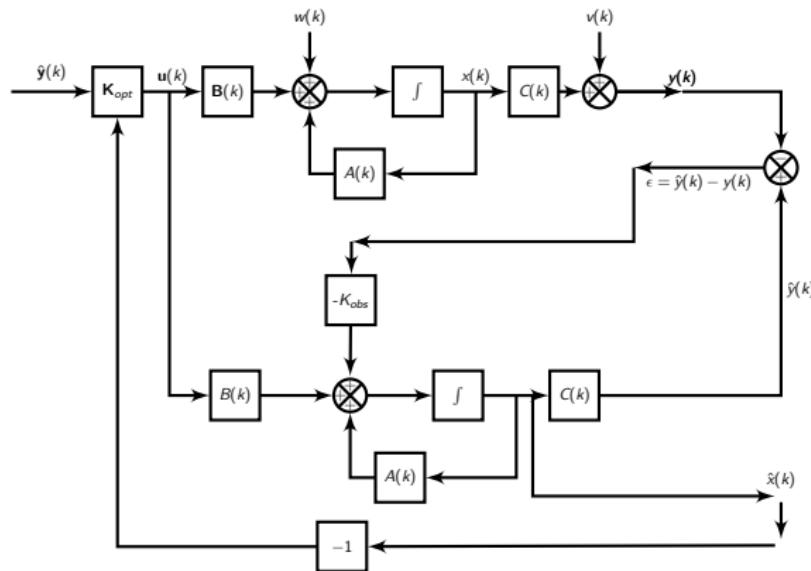
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$$\hat{x}(k+1) = A(k)\hat{x}(k) - K_{obs}[C(k)\hat{x}(k) - y(k)] + B(k)u(k).$$

1-DOF Control Results

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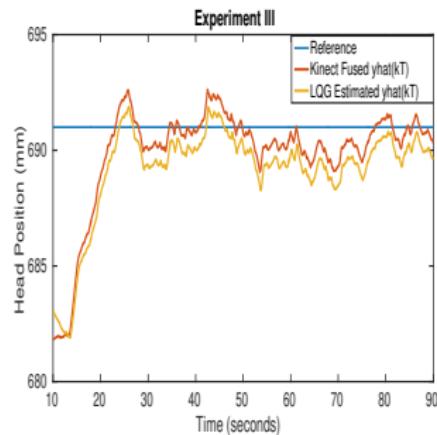
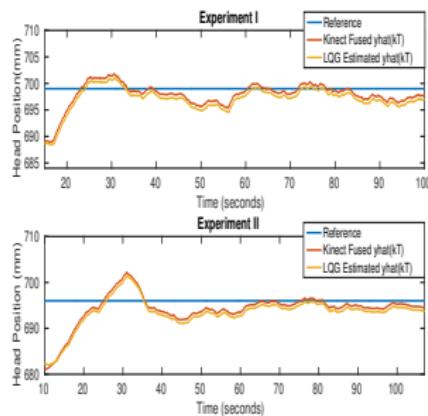
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LQG Controller on mannequin head.

Appendix D: CCOARSE Actuator Schematic

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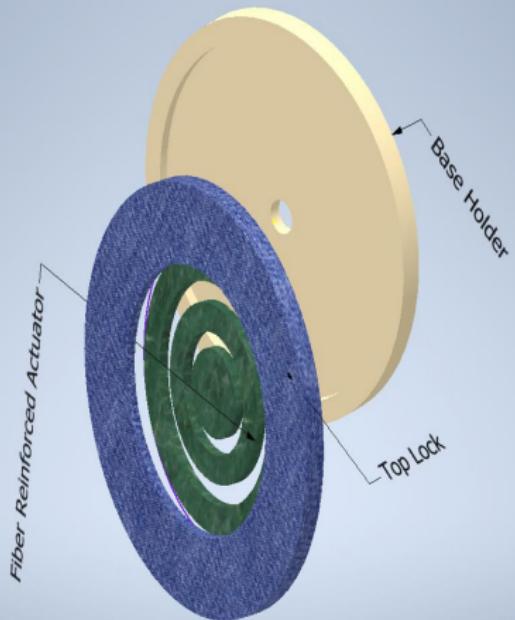
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Soft IK via Boundary Value Problem

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- With Cauchy's laws of motion, solve boundary volume problem of traction
- Using the following boundary conditions for the Cauchy Stress,
 - $\sigma_{rr}|_{R=R_0} = -P_{atm}, \sigma_{rr}|_{R=R_i} = -P_{atm} - P$
- And together with Cauchy's first law, we find that
 - $\sigma_{rr}(r) = - \int_{r_i}^{r_o} [2C_1\left(\frac{r}{R^2} - \frac{R^4}{r^5}\right) + 2C_2\left(\frac{r^3}{R^4} - \frac{R^2}{r^3}\right)] dr$
 - $\sigma_{rr}(r) = \int_{R_i}^{R_o} [2C_1\left(\frac{1}{r} - \frac{R^6}{r^7}\right) - 2C_2\left(\frac{R^4}{r^5} - \frac{r}{R^2}\right)] dr$
- With $\sigma_{rr}|_{R=R_i} = -P_{atm} - P$ and setting $P_{atm} = 0$, we find
 - $P(r) = \int_{r_i}^{r_o} [2C_1\left(\frac{r}{R^2} - \frac{R^4}{r^5}\right) + 2C_2\left(\frac{r^3}{R^4} - \frac{R^2}{r^3}\right)] dr$
 - $P(r) = \int_{R_i}^{R_o} [2C_1\left(\frac{1}{r} - \frac{R^6}{r^7}\right) - 2C_2\left(\frac{R^4}{r^5} - \frac{r}{R^2}\right)] dr$