

Problem-1

 Implement the Pan-Tompkins method for QRS detection in MATLAB. You may employ a simple threshold-based method to detect QRS complexes as the procedure will be run off-line.

Apply the procedure to the signals in the files ECG3.dat, ECG4.dat, ECG5.dat, and ECG6.dat, sampled at a rate of $200 \ Hz$ (see the file ECGS.m). Compute the averaged heart rate and QRS width for each record. Verify your results by measuring the parameters visually from plots of the signals.

- Signal ECG3, ECG4, ECG6 are more stable than ECG5, but each with different heart rate.
- ECG5 contains power line interference.



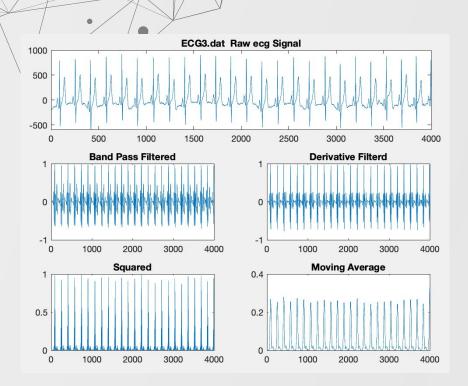
Use ECGS.m Read ECG Low Pass Filter (12Hz) High Pass Filter (5Hz)

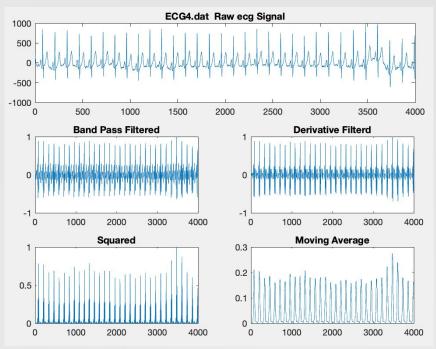
Derivat ive Filter

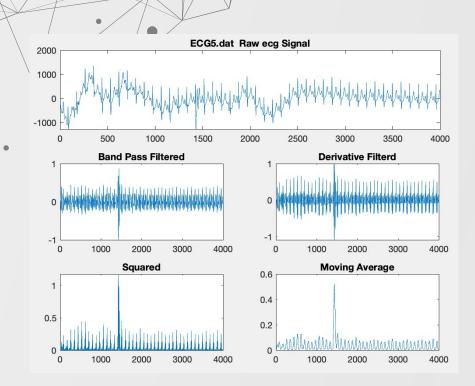
Square

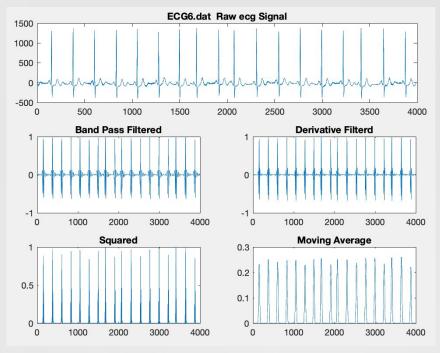
Moving Average (N=30 for 200Hz)

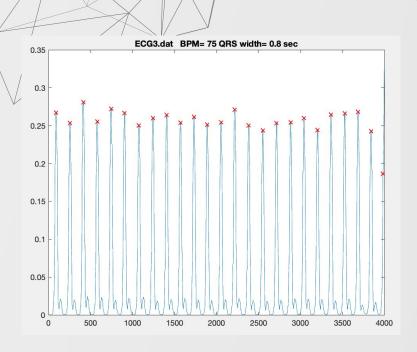
Find Peaks



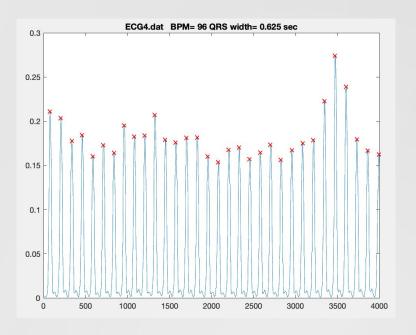




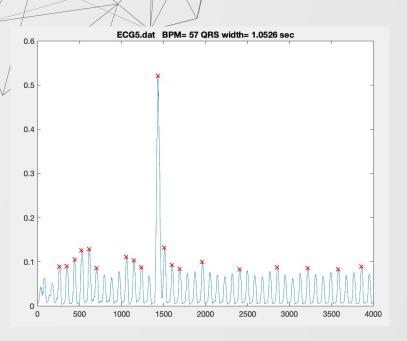




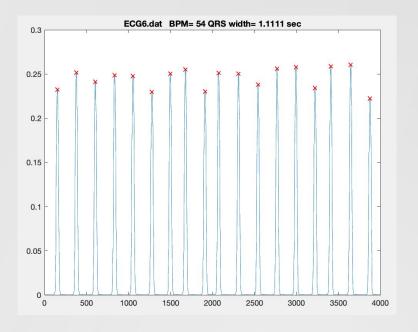
Visual Measure from Raw Data : BPM=75 Width=0.816sec



Visual Measure from Raw Data : BPM=96 Width=0.63 sec



Visual Measure from Raw Data: BPM=132 Width=0.45sec



Visual Measure from Raw Data: BPM=54 Width=1.11 sec



Discussion

- Using "findpeaks" function might have good performance in detection of regular peaks and calculate the correct BPM.
- But bad in QRS complex width evaluation and also bad in power line shifted, unusual ECG signal. (ECG5.dat)

Problem-2

Implement the Pan-Tompkins method for QRS detection in MATLAB. You may employ
a simple threshold-based method to detect QRS complexes as the procedure will be run
off-line.

Apply the procedure to the signals in the files ECG3.dat, ECG4.dat, ECG5.dat, and ECG6.dat, sampled at a rate of 200~Hz (see the file ECGS.m). Compute the averaged heart rate and QRS width for each record. Verify your results by measuring the parameters visually from plots of the signals.

2. Implement the adaptive thresholding and searchback procedure to your P-T method and redo problem 1.

Use ECGS.m Read ECG Low Pass Filter (12Hz) High Pass Filter (5Hz)

Derivati ve Filter

Square

Moving Average (N=30)

Initialize
Signal level
Noise level
Threshold

Thresholding and decision

Search Back (1.66 of averaged RR duration)

Initialize
Signal level
Noise level
Threshold

Thresholding and decision

Searchback (1.66 of averaged RR duration)

Initialize Signal level and Noise level as a percentage of the maximum and average amplitude of the integrated signal, respectively.

Initialize
Signal level
Noise level
Threshold

Thresholding and decision

Searchback (1.66 of averaged RR duration)

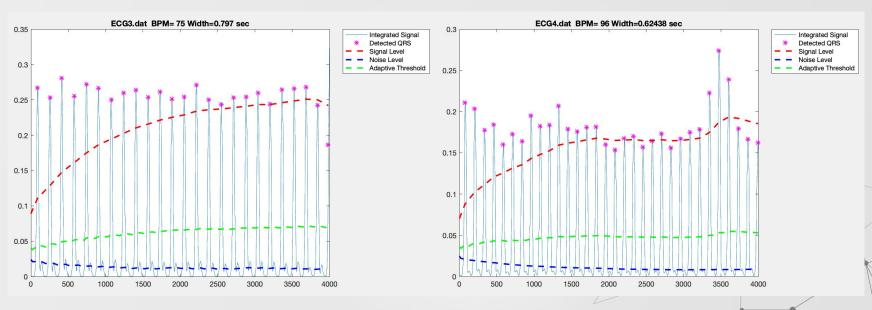
```
SPKI = 0.125 \, PEAKI + 0.875 \, SPKI if PEAKI is a signal peak; (4.15) NPKI = 0.125 \, PEAKI + 0.875 \, NPKI if PEAKI is a noise peak; THRESHOLD \, I1 = NPKI + 0.25 (SPKI - NPKI); \quad (4.16)
```

Initialize
Signal level
Noise level
Threshold

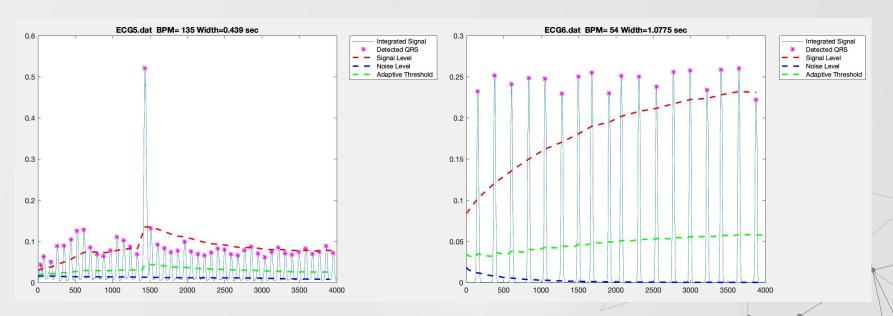
Thresholding and decision

Searchback (1.66 of averaged RR duration)

THRESHOLD I2 = 0.5 THRESHOLD I1.



Visual Measure from Raw Data : BPM=75 Width=0.816 sec Visual Measure from Raw Data : BPM=96 Width=0.63 sec



Visual Measure from Raw Data: BPM=132 Width=0.45 sec Visual Measure from Raw Data: BPM=54 Width=1.11 sec



Discussion

 Using adaptive threshold and searchback procedure will have a better result in processing signals with baseline shifted or unusual ECG signal.

Problem-3

3. Apply your P-T method to your personal ECG.

- Load .mat data type as a struct, get values as .data (fs=250Hz)
- Cut noise signal at the beginning
- A bit power line interference

Load ECG

Low Pass Filter (12Hz) High Pass Filter (5Hz)

Derivati ve Filter

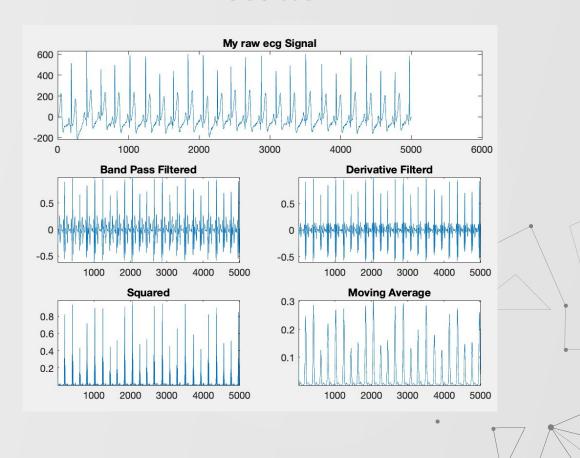
Square

Moving Average (N=30)

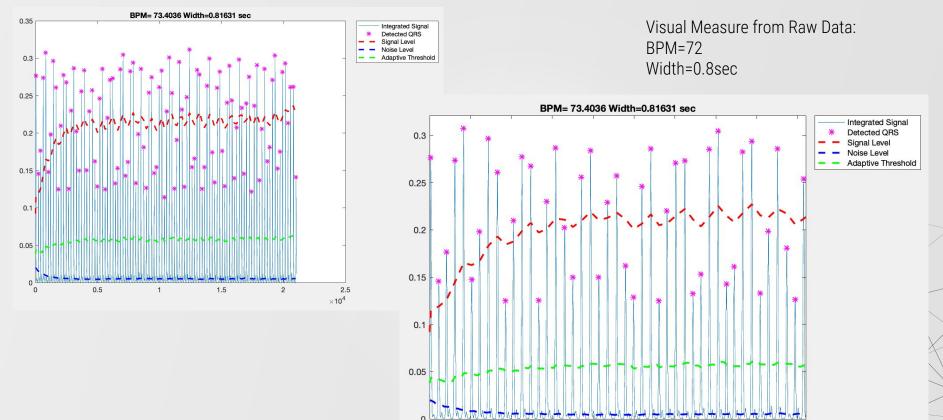
Initialize
Signal level
Noise level
Threshold

Thresholding and decision

Search Back (1.66 of averaged RR duration)



Results-Adaptive Thresholding





Discussion

- Although my signal contains a baseline shifting, adaptive thresholding can correctly measure my BPM.
- We can clearly observe the floating of the signal level and the threshold while doing adaptive thresholding.

