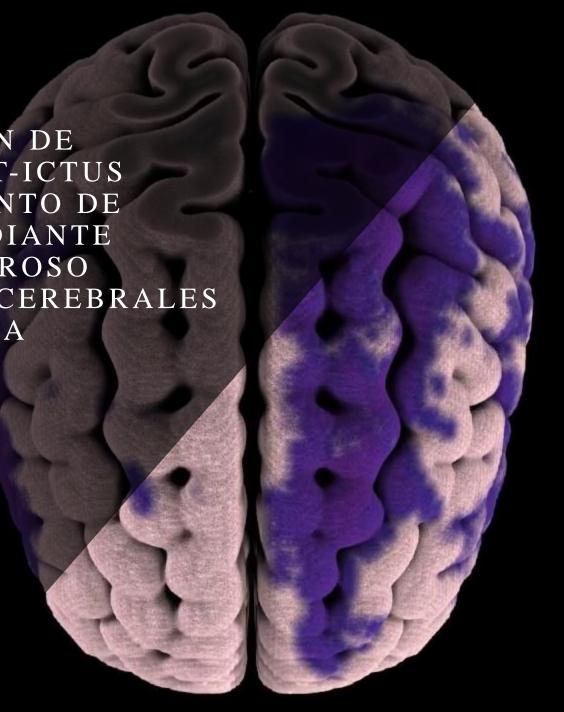


Mario Pascual González

Grado en Ingeniería de la Salud, mención en Bioinformática

Profesor Director del Proyecto: Dr. Enrique Nava Baro



ÍNDICE



1. Introducción



2. Trabajos Relacionados



3. Metodología



4. Resultados



5. Discusión



6. Conclusión



7. Investigación Futura



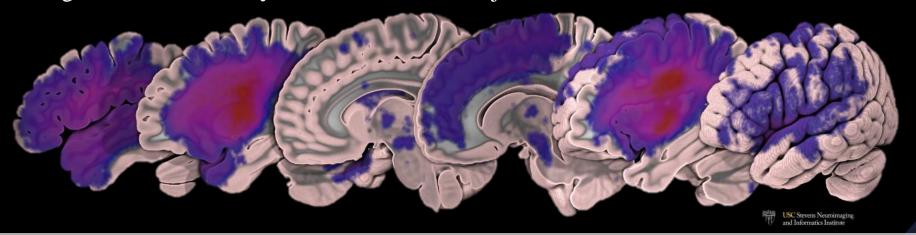
1. Introducción

Tejido objetivo: Lesión cerebral posterior a Accidente Cerebro-Vascular (ACV) o Ictus

Algoritmo: Crecimiento de Regiones empleando Lógica Borrosa (FISRG)

Modalidad de las imágenes: Resonancia Magnética Nuclear en pulso T1 (MRI-T1)

Código desarrollado en Python 3.9 usando el conjunto de datos ATLAS R2.





2. Trabajos Relacionados

Research Article

A Study on the Application of Fuzzy Information Seeded Region Growing in Brain MRI Tissue Segmentation

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Received 25 February 2014; Accepted 4 April 2014; Published 5 May 2014

Academic Editor: Her-Terng Yau

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... sino que son otro tipo de tejidos: GM, WM, CEF, Tumores, etc. En ninguno de estos el tejido objetivo son las lesiones post-ictus ...

TRANSACTIONS ON MEDICAL IMAGING, VOL. 18, NO. 9, SEPTEMBER 1999

Adaptive Fuzzy Segmentation of Magnetic Resonance Images

Dzung L. Pham, Student Member, IEEE, and Jerry L. Prince,* Member, IEEE

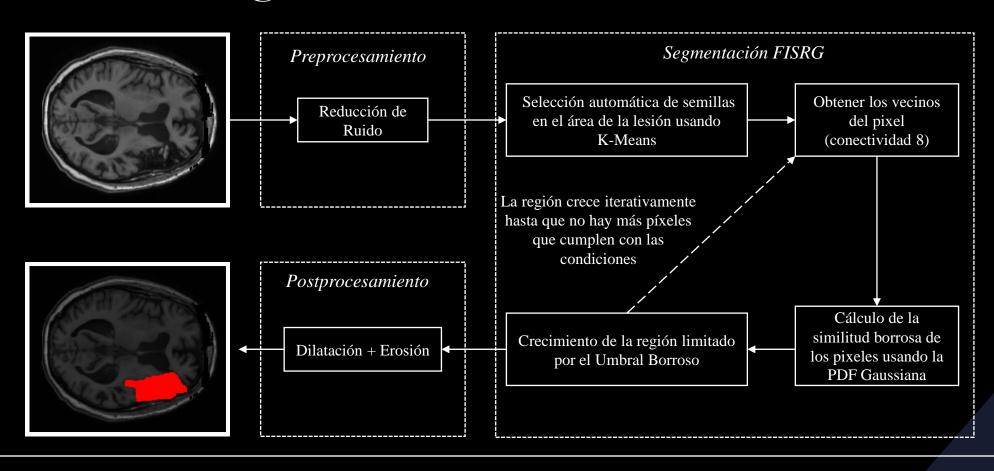
Abstract—An algorithm is presented for the fuzzy segmentation of two-dimensional (2-D) and three-dimensional (3-D) multispectral magnetic resonance (MR) images that have been corrupted by intensity inhomogeneities, also known as shading artifacts. The algorithm is an extension of the 2-D adaptive fuzzy C-means algorithm is an extension of the 2-D adaptive fuzzy C-means algorithm is an extension of the 2-D adaptive fuzzy C-means alfield that causes image intensity inhomogeneities as a gain field that causes image intensities to smoothly and slowly vary through the image space. It iteratively adapts to the intensity inhomogeneities and is completely automated. In this paper, we fully generalize 2-D AFCM to three-dimensional (3-D) multispectral images. Because of the potential size of 3-D image data, we also describe a new faster multigrid-based algorithm for its

In MR images, intensity inhomogeneities are typically caused by nonuniformities in the RF field during acquisition, although other factors also play a role [4], [5]. Similar artifacts also occur in computed tomography images, due to beam hardening effects, as well as in microscopy and light photography, due to nonuniform illumination. The result is a shading effect where the pixel or voxel intensities of the same tissue class vary over the image domain. It has been shown that the shading in MR images is well modeled by the product of the original image and a smooth slowly varying gain field [6], [7]. Typically, corrupted images are segmented

² Networks and Communications Group, Advantech Co., Ltd., Neihu 114, Taiwan

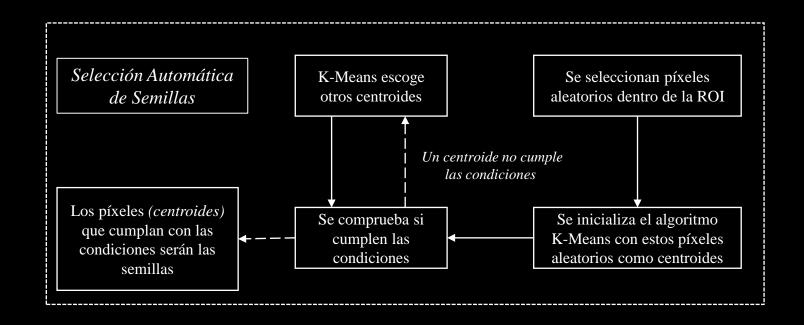


3. Metodología – I. Visión General





3. Metodología – II. Selección de semillas





3. Metodología – III. FISRG: Predicado

Función de Densidad de Probabilidad Gaussiana

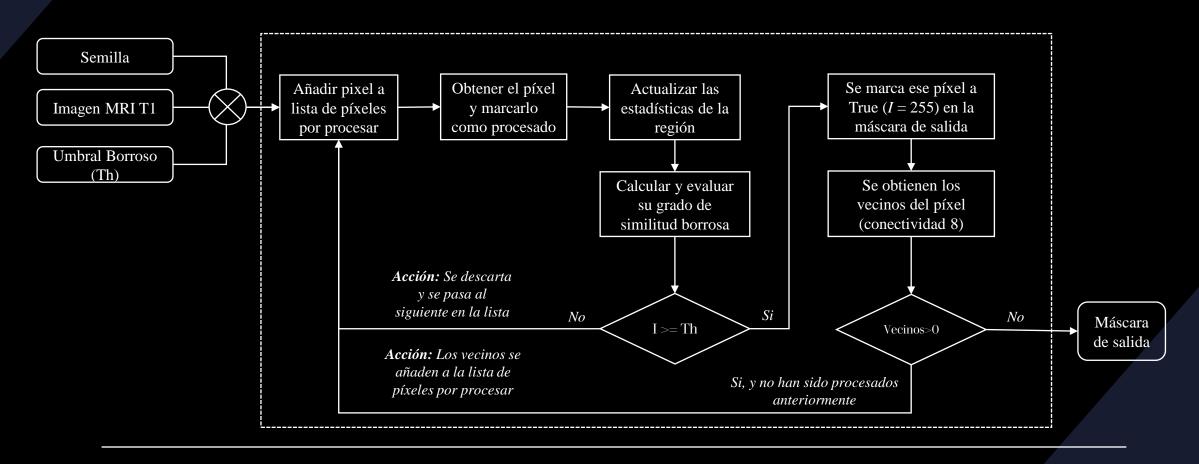
$$f(x) = \frac{1}{\sqrt{2\pi\sigma^2}} e^{\frac{-(x-\mu)^2}{2\sigma^2}}$$

La media y desviación estándar usadas para el cálculo de la similitud de un píxel con la función Gaussiana se actualizan dinámicamente a medida que la región crece

- El algoritmo es más robusto a texturas inusuales en la lesión.
- El algoritmo es capaz de adaptarse mejor a los cambios de intensidad.

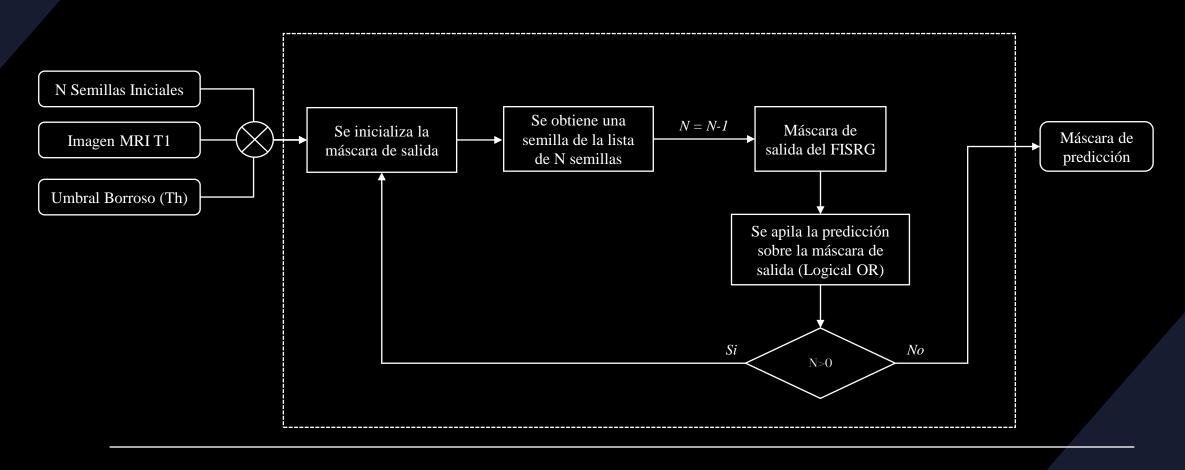


3. Metodología – III. FISRG: Algoritmo



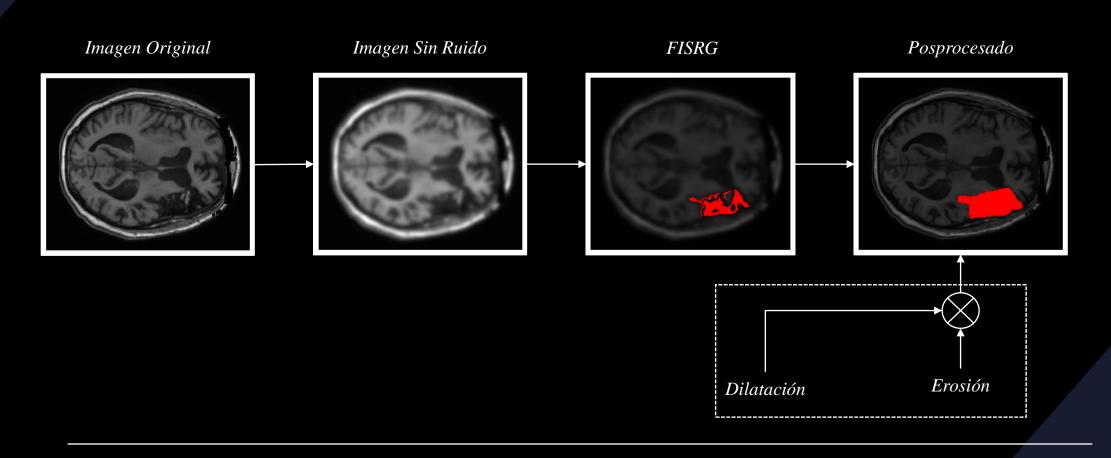


3. Metodología – III. FISRG: N semillas





3. Metodología – IV. Postprocesamiento

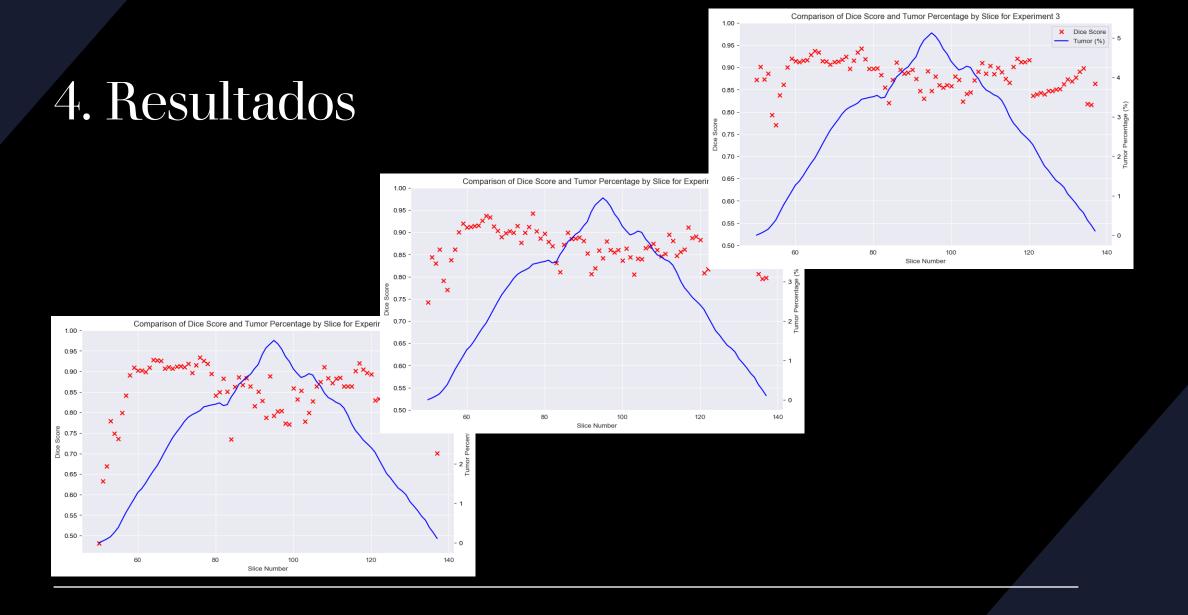




4. Resultados

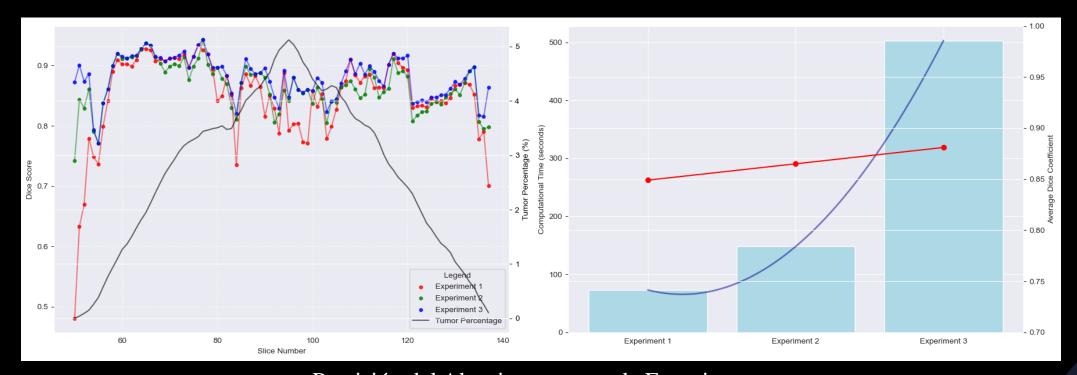
Experimento	Parámetros que se ajustan iterativamente
1	Umbral borroso, Número de semillas
2	Umbral borroso, Número de semillas, Sigma (σ)
3	Umbral borroso, Número de semillas, Sigma (σ), Tamaño del kernel de Dilatación







5. Discusión



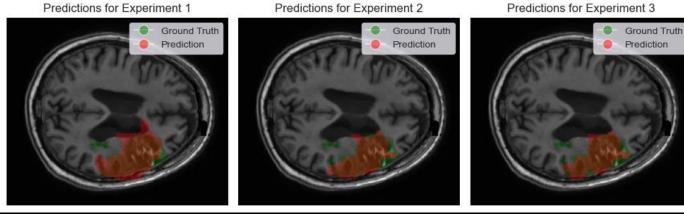
Precisión del Algoritmo para cada Experimento VS

Coste Computacional

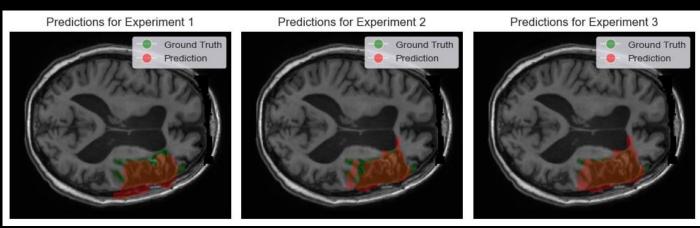


5. Discusión

Disminución de la eficacia del algoritmo para imágenes en las que la lesión es demasiado grande



Estas imágenes prueban la teoría de saltos entre estructuras anatómicas

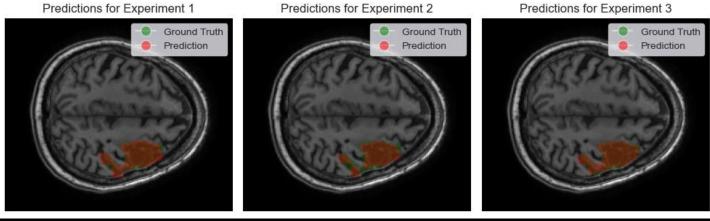


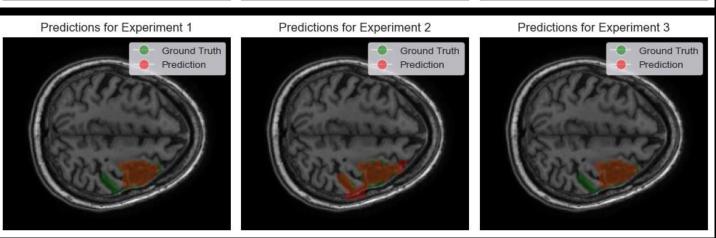


5. Discusión

Disminución de la eficacia del algoritmo a partir de la imagen 120 abruptamente, seguido de una recuperación

Estas imágenes prueban que el algoritmo no puede manejar cambios abruptos en la lesión, como su separación en dos regiones





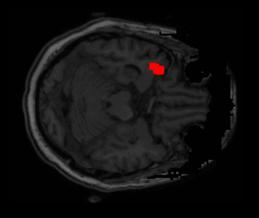
6. Conclusión

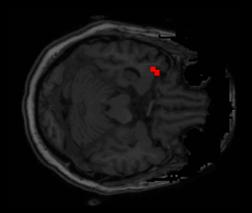
- Buenos resultados para un problema que no había sido abordado con este método antes.
- Robusto ante una segmentación complicada, ya que este tipo de lesiones ACV son muy poco homogéneas.
- Sensible a lesiones demasiado grandes que invadan otras regiones anatómicas cerebrales de intensidad parecida a la de la lesión post-ictus.
 - Sensible a cambios bruscos.

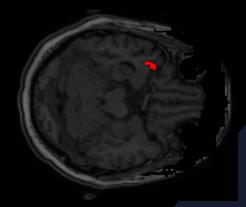
Experimento 1

Experimento 2

Experimento 3



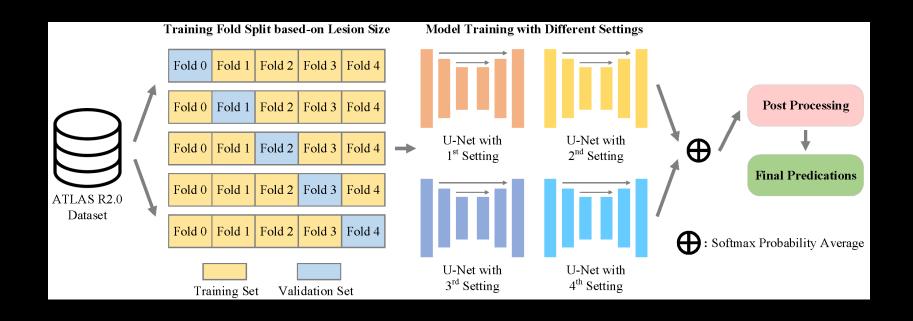






7. Investigación Futura

Proyecto por Huo et al. (2022): "MAPPING: Model Average with Post-processing for Stroke Lesion Segmentation"



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