

Hit and Run and Stuff

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Abstract

The brain must select its control strategies among an infinite set of possibilities, thereby solving an optimization problem. While this set is infinite and lies in high dimensions, it is bounded by kinematic, neuromuscular, and anatomical constraints, within which the brain must select optimal solutions. We use data from a human index finger with 7 muscles, 4DOF, and 4 output dimensions. For a given force vector at the endpoint, the feasible activation space is a 3D convex polytope, embedded in the 7D unit cube. It is known that explicitly computing the volume of this polytope can become too computationally complex in many instances. We generated random points in the feasible activation space using the Hit-and-Run method, which converged to the uniform distribution. After generating enough points, we computed the distribution of activation across each muscle, shedding light onto the structure of these solution spaces- rather than simply exploring their maximal and minimal values. We also visualize the change in these activation distributions as we march toward maximal feasible force production in a given direction. Using the parallel coordinates method, we visualize the connection between the muscle activations. Once can then explore the feasible activation space, while constraining certain muscles. Although this paper presents a 7 dimensional case of the index finger, our methods extend to systems with up to at least 40 muscles. We challenge the community to map the shapes distributions of each variable in the solution space, thereby providing important contextual information into optimization of motor cortical function in future research.

²⁶ **1 Author Summary**

²⁷ **2 Introduction**

²⁸ Described in a mathematical way the feasible activation set is expressed as follows. For
²⁹ a given force vector $f \in \mathbb{R}^m$, which are the activations that satisfy

$$\mathbf{f} = A\mathbf{a}, \mathbf{a} \in [0, 1]^n?$$

³⁰ In our 7-dimensional example $m = 4$ and $n = 7$, typically n is much larger than m .
³¹ The constraint $\mathbf{a} \in [0, 1]^n$ describes that the feasible activation space lies in the n -
³² dimensional unit cube (also called the n -cube). Each row of the constraint $\mathbf{f} = A\mathbf{a}$ is a
³³ $n - 1$ dimensional hyperplane. Assuming that the rows in A are linearly independent
³⁴ (which is a safe assumption in the muscle system case), the intersection of all m equality
³⁵ constraints constraints is a $(n - m)$ -dimensional hyperplane. Hence the feasible activation
³⁶ set is the polytope given by the intersection of the n -cube and the $(n - m)$ -dimensional
³⁷ hyperplane. Note that this intersection is empty in the case where the force f can not
³⁸ be generated.

³⁹ **3 Materials and Methods**

⁴⁰ Exact volume calculations for polygons can only be done in reasonable time in up to
⁴¹ 10 dimensions [2, 6, 7]. We therefore use the so called Hit-and-Run approach, which
⁴² samples a series of points in a given polygon. Given the points for a feasible activation
⁴³ space, this method gives us a deeper understanding of its underlying structure.

⁴⁴ **3.1 Hit-and-Run**

⁴⁵ In this section we introduce the Hit-and-Run algorithm used for uniform sampling in a
⁴⁶ convex body K , was introduced by Smith in 1984 [10]. The mixing time is known to be
⁴⁷ $\mathcal{O}^*(n^2 R^2 / r^2)$, where R and r are the radii of the inscribed and circumscribed ball of K
⁴⁸ respectively [1, 8]. I.e., after $\mathcal{O}^*(n^2 R^2 / r^2)$ steps of the Hit-and-Run algorithm we are at
⁴⁹ a uniformly at random point in the convex body. In the case of the muscles of a limb,
⁵⁰ we are interested in the polygon P that is given by the set of all possible activations
⁵¹ $\mathbf{a} \in \mathbb{R}^n$ that satisfy

$$\mathbf{f} = A\mathbf{a}, \mathbf{a} \in [0, 1]^n,$$

where $\mathbf{f} \in \mathbb{R}^m$ is a fixed force vector and $A = J^{-T} RF_m \in \mathbb{R}^{m \times n}$. P is bounded by the
unit n -cube since all variables $a_i, i \in [n]$ are bounded by 0 and 1 from below, above
respectively. Consider the following 1×3 example.

$$1 = \frac{10}{3}a_1 - \frac{53}{15}a_2 + 2a_3$$
$$a_1, a_2, a_3 \in [0, 1],$$

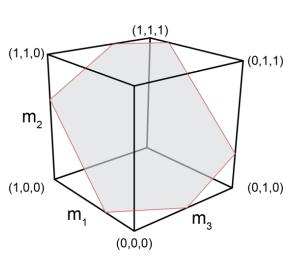


Figure 1: Feasible Activation

52 the set of feasible activations is given by the shaded set in Figure 1.

53 The Hit-and-Run walk on P is defined as follows (it works analogously for any convex
54 body).

- 55 1. Find a given starting point \mathbf{p} of P (Figure 2a) .
- 56 2. Generate a random direction through \mathbf{p} (uniformly at random over all directions)
57 (Figure 2b).
- 58 3. Find the intersection points of the random direction with the n -unit cube (Figure
59 2c).
- 60 4. Choose the next point of the sampling algorithm uniformly at random from the
61 segment of the line in P (Figure 2d).
- 62 5. Repeat from (b) the above steps with the new point as the starting point .

63 The implementation of this algorithm is straight forward except for the choice of the
64 random direction. How do we sample uniformly at random (u.a.r.) from all directions
65 in P ? Suppose that \mathbf{q} is a direction in P and $p \in P$. Then by definition of P , \mathbf{q} must
66 satisfy $\mathbf{f} = A(\mathbf{p} + \mathbf{q})$. Since $\mathbf{p} \in P$, we know that $\mathbf{f} = A\mathbf{p}$ and therefore

$$\mathbf{f} = A(\mathbf{p} + \mathbf{q}) = \mathbf{f} + A\mathbf{q}$$

67 and hence

$$A\mathbf{q} = 0.$$

68 We therefore need to choose directions uniformly at random from all directions in
69 the vectorspace

$$V = \{\mathbf{q} \in \mathbb{R}^n | A\mathbf{q} = 0\}.$$

70 As shown by Marsaglia this can be done as follows [9].

- 71 1. Find an orthonormal basis $b_1, \dots, b_r \in \mathbb{R}^n$ of $A\mathbf{q} = 0$.
- 72 2. Choose $(\lambda_1, \dots, \lambda_r) \in \mathcal{N}(0, 1)^n$ (from the Gaussian distribution).

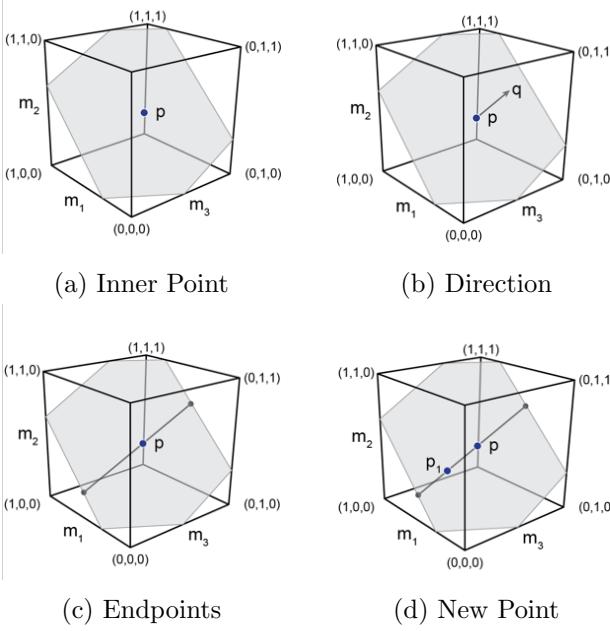


Figure 2: Hit-and-Run Step

73 3. $\sum_{i=1}^r \lambda_i b_i$ is a u.a.r. direction.

74 A basis of a vectorspace V is a minimal set of vectors that generate V , and it is
 75 orthonormal if the vectors are pairwise orthogonal (perpendicular) and have unit length.
 76 Using basic linear algebra one can find a basis for $V = \{A\mathbf{q} = 0\}$ and orthogonalize it
 77 with the well known Gram-Schmidt method (for details see e.g. [3]). Note that in order
 78 to get the desired u.a.r. sample the basis needs to be orthonormal. For the limb case we
 79 can safely assume that the rows of A are linearly independent and hence the number of
 80 basis vectors is $n - m$.

81 **3.2 Mixing Time**

82 How many steps are necessary to reach a uniformly at random point in the polytope?
 83 The theoretical bound $\mathcal{O}^*(n^2 R^2 / r^2)$ given in [8] has a very large hidden coefficient (10^{30})
 84 which makes the algorithm almost infeasible in lower dimensions.

85 These bounds hold for general convex sets. For convex polygons in higher dimensions,
 86 experimental results suggest that $\mathcal{O}(n)$ steps of the Hit-and-Run algorithm are sufficient.
 87 In particular Emiris and Fisikopoulos paper suggest that $(10 + 10 \frac{n}{r}) n$ steps are enough
 88 to have a close to uniform distribution [4]. In all cases tested, sampling more point did
 89 not make accuracy significantly higher.

90 Ge et al. showed experimentally that up to about 40 dimensions, ??? random points
 91 seem to suffice to get a close to uniform distribution [5].

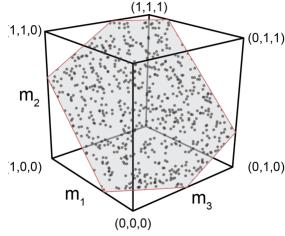


Figure 3: Uniform Distribution

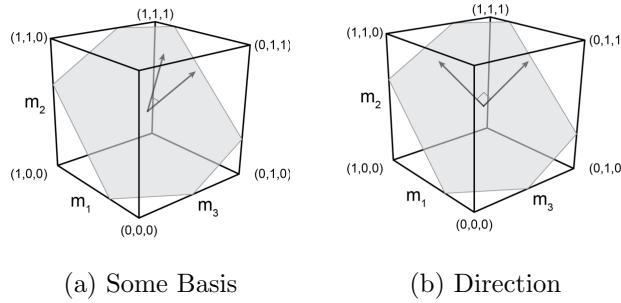


Figure 4: Find Orthonormal Basis

92 Therfore for given output force we execute the Hit-and-Run algorithm 1000 times
 93 on 100 points. The experimental results propose that those 1000 points are uniformly
 94 distributed on the polygon.

95 As a additional control, for each muscle we observe that the theoretical upper and
 96 lower bound of the feasible activation match the observed corresponding bounds (dif-
 97 ference max ??). To find the theoretical upperbound (lowerbound) of a given muscle
 98 activation we solve two linear programs maximizing (minimizing) a_i over the polytope.

99 3.3 Starting Point

100 To find a starting point in

$$\mathbf{f} = A\mathbf{a}, \mathbf{a} \in [0, 1]^n,$$

101 we only need to find a feasible activation vector. For the hit and run algorithm to mix
 102 faster, we do not want the starting point to be in a vertex of the activation space. We
 103 use the following standard trick using slack variables ϵ_i .

$$\begin{aligned} & \text{maximize} && \sum_{i=1}^n \epsilon_i \\ & \text{subject to} && \mathbf{f} = A\mathbf{a} \\ & && a_i \in [\epsilon_i, 1 - \epsilon_i], \quad \forall i \in \{1, \dots, n\} \\ & && \epsilon_i \geq 0, \quad \forall i \in \{1, \dots, n\}. \end{aligned} \tag{1}$$

104 This approach can still fail in theory, but this method has the choose $\epsilon_i > 0$ and therefore
 105 $a_i \neq 0$ or 1. Since for all vertices of the feasible activation space lie on the boundary
 106 of the n -cube, at least $n - m$ muscles must have activation 0 or 1. Documentation is
 107 included in our supplementary information.

108 3.4 Parallel Coordinates: Visualization of the Feasible Activation Space

109 Citation A common way to visualize higher dimensional data is using parallel coordinates.
 110 To show our sample set of points in the feasible activation space we draw n
 111 parallel lines, which representing the activations of the n muscles. Each point is then
 112 represented by connecting their coordinates by $n - 1$ lines.

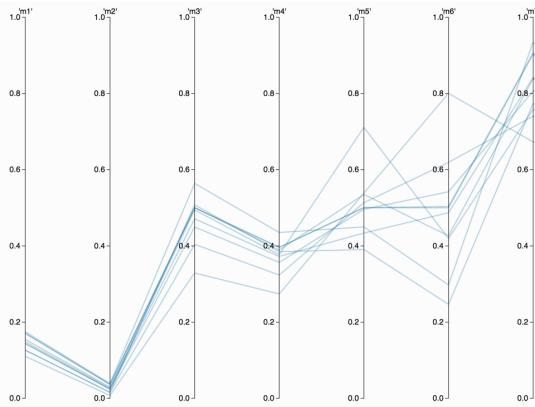


Figure 5: Feasible Activation

113 Using an interactive surface one can now restrict each muscle function to any desired
 114 interval, e.g., figure ??.

115 NICE FIGURE OF RESTRICTED PARALLEL COORDINATES

116 For the l_1 , l_2 and l_3 norm respectively, we added an additional line to represent
 117 the corresponding weight. E.g. for a given point $\mathbf{a} \in \mathbb{R}^n$ we are interested in $\sum_{i=1}^n a_i$,
 118 $\sqrt{\sum_{i=1}^n a_i^2}$ and $\sqrt[3]{\sum_{i=1}^n a_i^3}$. As for the muscles one can restrict the intervals of the weight
 119 functions, to explore the corresponding feasible activation space.

120 NICE PICTURE WITH WEIGHTS INCLUDED

121 4 Results

122 Many nice figures

123 1. Histograms

124 2. Histograms 3 directions

125 3. PC

126 **4.1 Activation Distribution on a Fixed Force Vector**

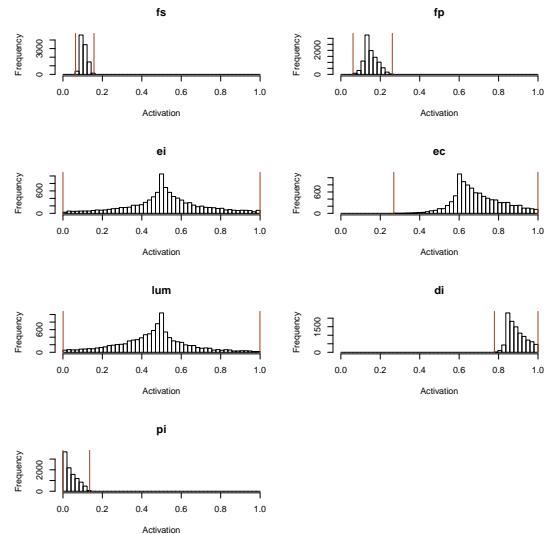


Figure 6: Histogram for Fixed Force

127 **4.2 Changing Output Force in 3 Directions**

128 We discuss different forces into three different directions, which are given by the palmar
129 direction (x -direction), the distal direction (y -direction) and the sum of them. The
130 maximal forces into each direction are given by ??, ?? and ?? respectively. For $\alpha =$
131 $0.1, 0.2, \dots, 0.9$, we give the histograms where the force is $\alpha \cdot F_{\max}$, where F_{\max} is the
132 maximum output force in the corresponding direction.

133 **4.3 Parallel Coordinates**

134 *Muscle 5 and 6 same direction and same strength \Rightarrow Does not matter which one we*
135 *activate for low cost*

136 **5 Discussion**

137 Mostly to be written by Brian

138 **5.1 Distributions**

- 139 • Bounding box away from 0 and 1 means muscle is really needed \rightarrow Already known
140 from the bounding boxes

- 141 • High density → most solutions in that area

142 **5.2 Parallel Coordinates**

- 143 • Parallel lines in PC indicate opposite direction of muscles
144 • Crossing lines indicate similar direction

145 **5.3 Running Time**

146 The step of the algorithm which are time consuming are finding a starting point, which
147 solves a linear program and can take exponential running time in worst case. For each
148 fixed force vector we only have to find a starting point and an orthonormal basis once,
149 and are hence not of concern for the running time.

150 Running one loop of the hit and run algorithm only needs linear time, therefore the
151 method will extend to higher dimesions with only linear factor of additinal running time
152 needed.

153 **6 Acknowledgments**

154 **References**

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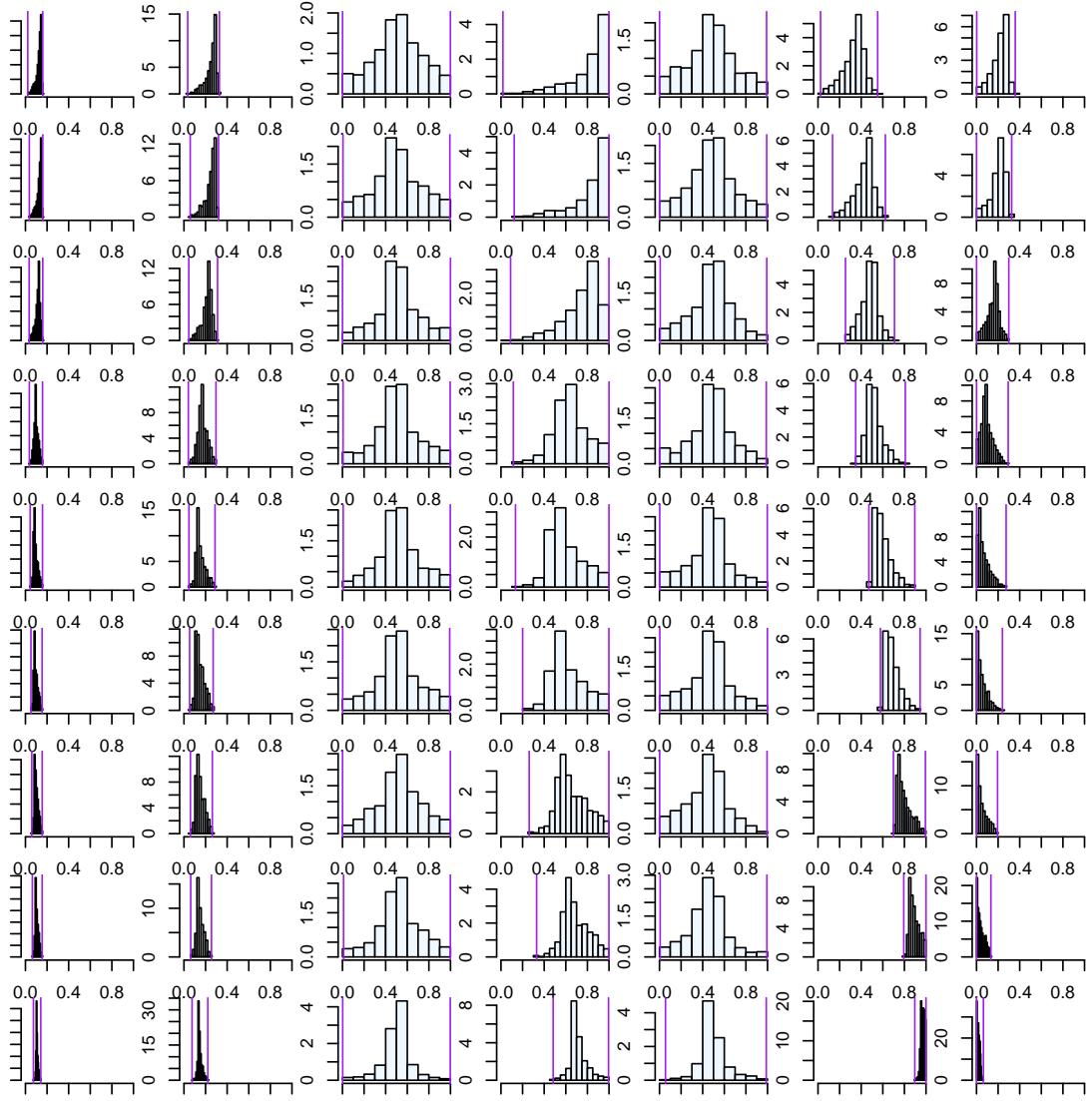


Figure 7: Histogram for x -Direction

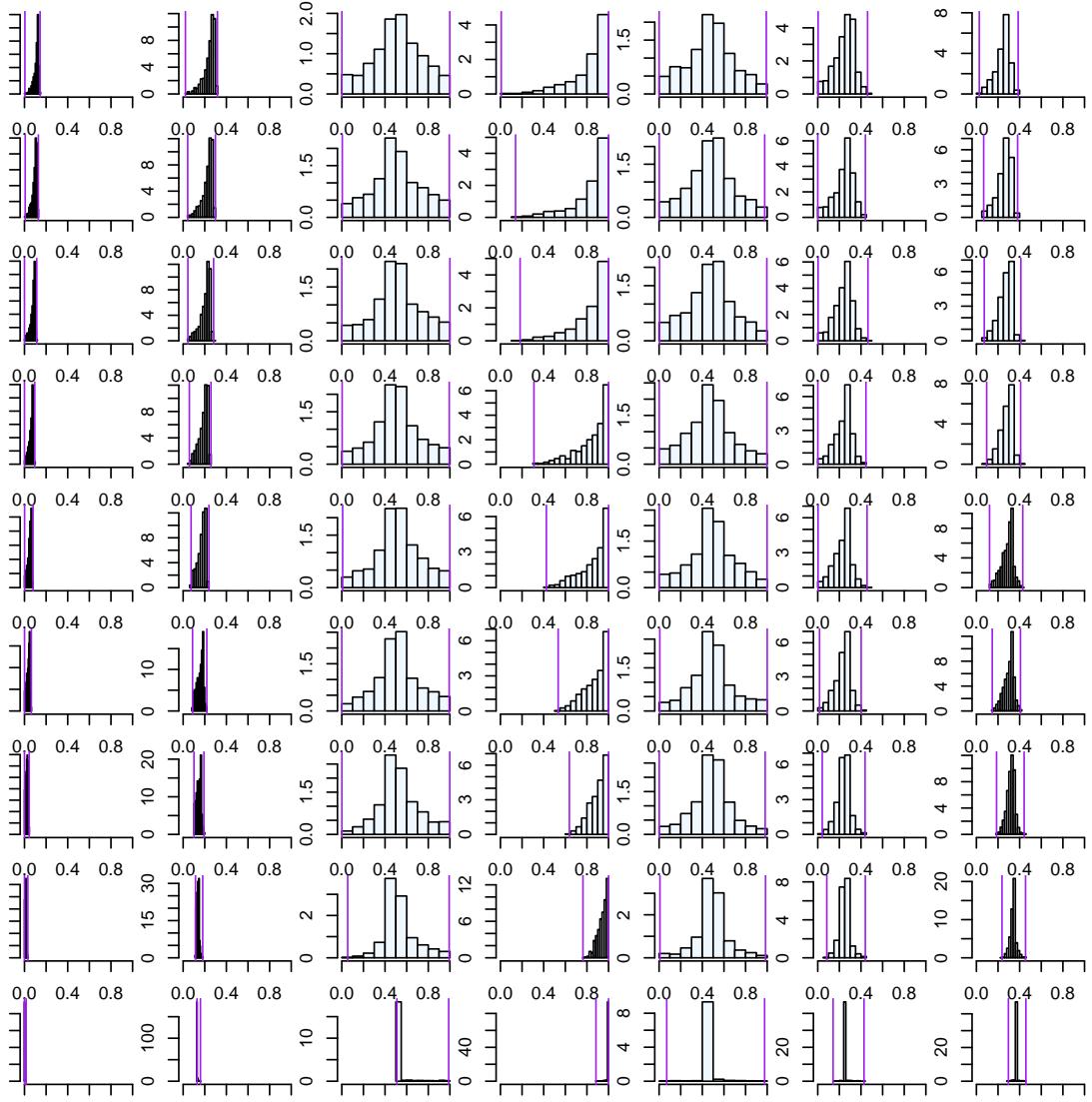


Figure 8: Histogram for xy -Direction

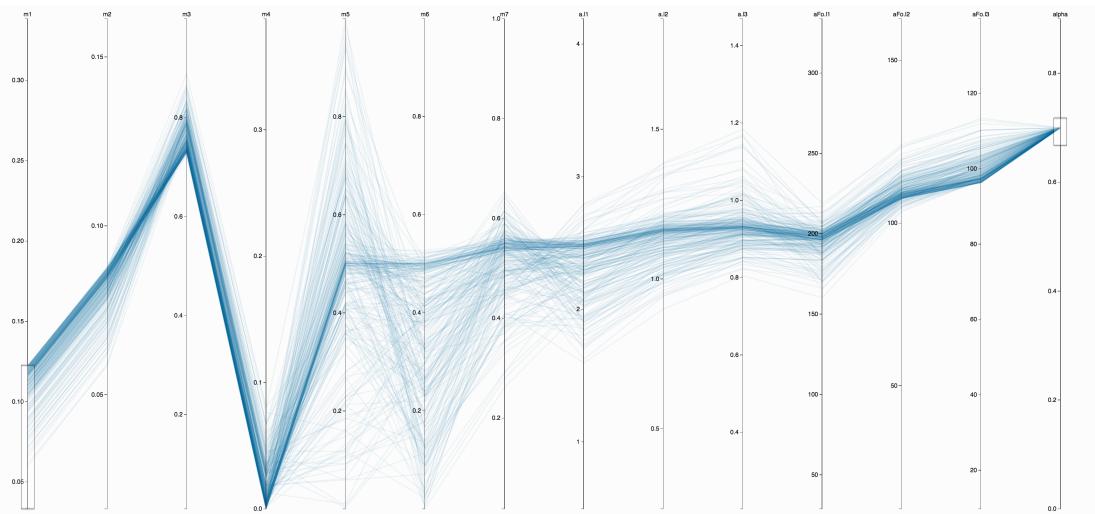


Figure 9: Low for Muscle 1

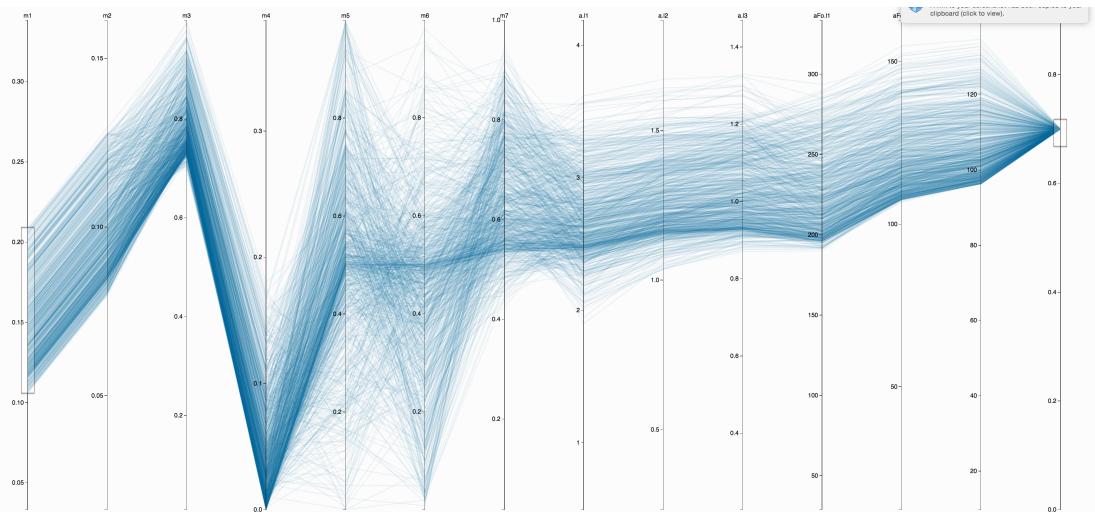


Figure 10: Middle for Muscle 1

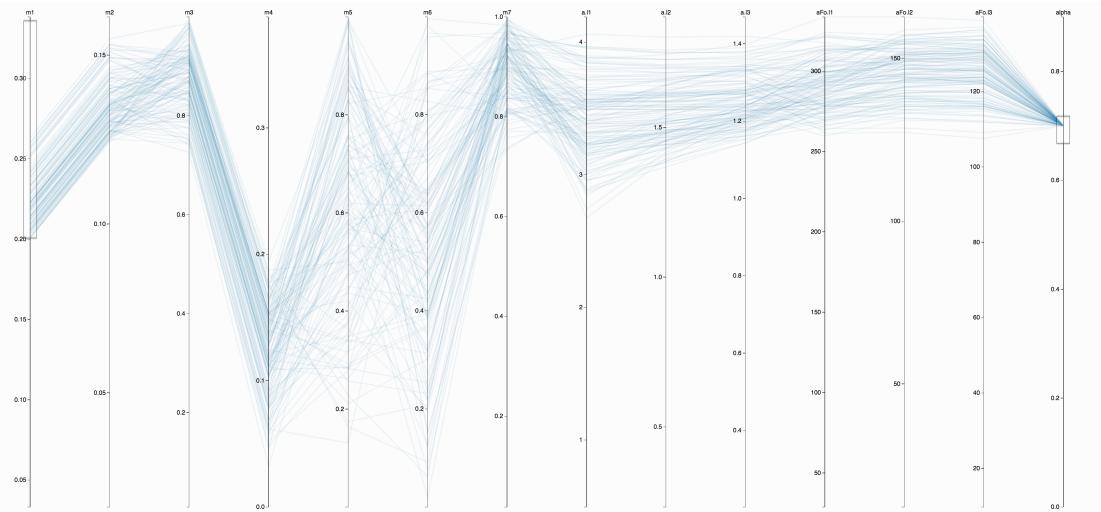


Figure 11: Upper for Muscle 1

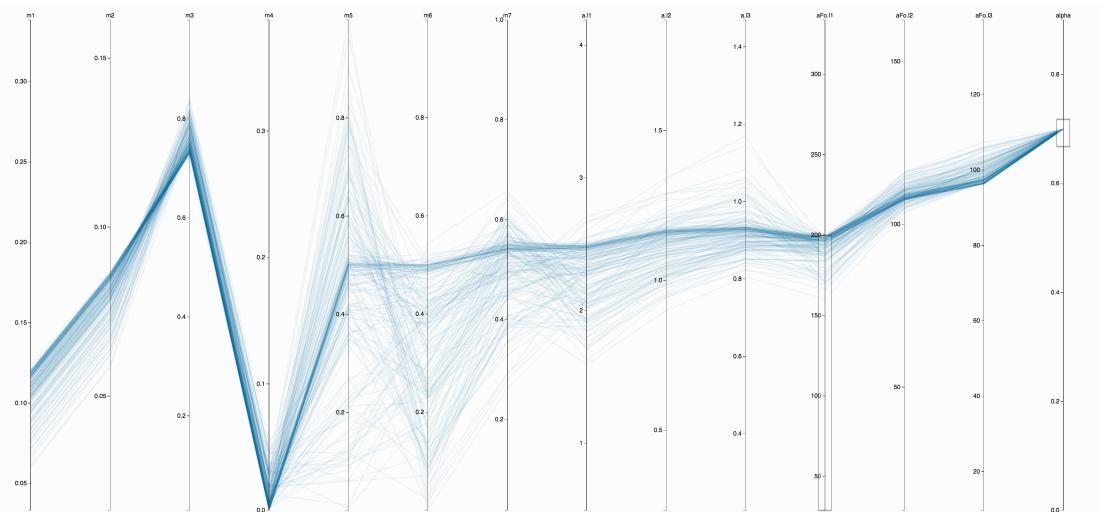


Figure 12: Weighted Cost