

# FLUOROSNNAP

User Guide  
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Fluorescence Single Neuron and Network Analysis  
Package

**Tapan Patel, PhD**  
University of Pennsylvania  
[tapan.p.patel@gmail.com](mailto:tapan.p.patel@gmail.com)

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## Getting Started

### General comments

We created a set of MATLAB routines and graphical user interfaces to facilitate the analysis of calcium fluorescence imaging experiments of neuronal activity. The Fluorescence Single Neuron and Network Analysis Package (FluoroSNNAP) directly accepts .tif stacks of image activity or pre-processed .csv files containing fluorescence vs. time data.

The main steps of the analysis are segmentation, event detection, and network inference. Segmentation is the process of identifying individual neurons in the field of view. Event detection includes methods to detect when each neuron displays a calcium transient that is distinct from noise fluctuations in fluorescence. The network inference is an assortment of techniques to estimate several network connectivity metrics from a video segment. All of these tasks are automated and the user can interactively work on different steps of the pipeline with the GUI.

The only software requirement is MATLAB 2013b or MATLAB 2014a (no additional toolboxes other than the basic toolboxes are required). Note: GUI layout maybe different and unusable in MATLAB 2014b. Image processing is inherently memory intensive and we recommend having at least 8GB RAM (ideally >16GB). To date, we have tested this software on Mac OS/X (10.9), Windows 7 (64bit) and Linux (Ubuntu 14.04) machines. If MATLAB is running correctly on these machines (full install, including the available analysis packs), the software should run through the example data without any problems.

If there is motion artifact in your experiments, use ImageJ plugins prior to using this software to help correct for motion artifacts. We provide a set of rigid image registration routines that prove to be useful for small motion artifacts and sudden stage shift. We have not tested these algorithms on *in vivo* dataset with cardiac/pulmonary motion artifacts however.

We provide sample experiments as a .tif stack and a .csv file for you to try the software (available on [www.seas.upenn.edu/~molneuro/fluorosnnap.html](http://www.seas.upenn.edu/~molneuro/fluorosnnap.html)). Download the baseline.tif file or baseline.csv file and place them in separate folders. We recommend placing all .tif files in one folder and all .csv files in another folder.

For questions or comments for improvement, please email [tapanp@mail.med.upenn.edu](mailto:tapanp@mail.med.upenn.edu) and refer to the accompanying manuscript.

### Installation

- Download the calcium image analysis software source code FluoroSNNAP from <http://www.seas.upenn.edu/~molneuro/fluorosnnap.html>
- Unzip the FluoroSNNAP.zip package and navigate to FluoroSNNAP folder in MATLAB.
- The software package has been tested on MATLAB 2013b and MATLAB 2014a.

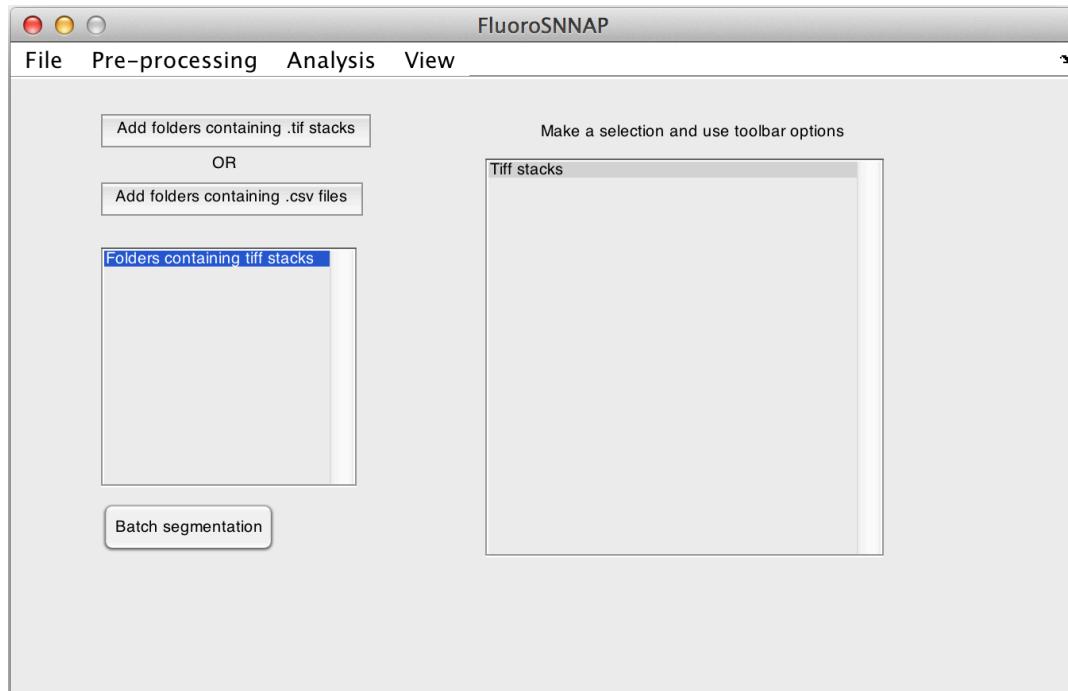
## Sample Pipeline

Follow these overall steps to process your .tif image stack of calcium activity. Details for each tool option are provided in later sections.

1. Run “FluoroSNNAP” at the MATLAB command prompt from FluoroSNNAP directory.
2. Add folders containing .tif stacks or .csv files.
3. Batch segmentation (Pre-processing menubar).
4. Set Preferences for analysis.
5. Launch Segmentation GUI and load the segmented image. Modify it as needed and save to return to the CalciumAnalysis GUI.
6. Process either the single file or batch process all files (Analysis menubar).
7. View results – raster plot, calcium events, network structure etc. (View menubar).

## Detailed descriptions of each menubar item

- Run MATLAB and change the working directory to FluoroSNNAP
- Enter the command **FluoroSNNAP** at the MATLAB command prompt.
- We recommend placing all the image files for a given experiment in one folder. This software can process multiple folders in batch mode.
- You will be prompted whether to use parallel processing routines. Select “Enable” if parallel processing toolbox is properly installed on your computer, otherwise select “Disable”.
- You should have a window like below.

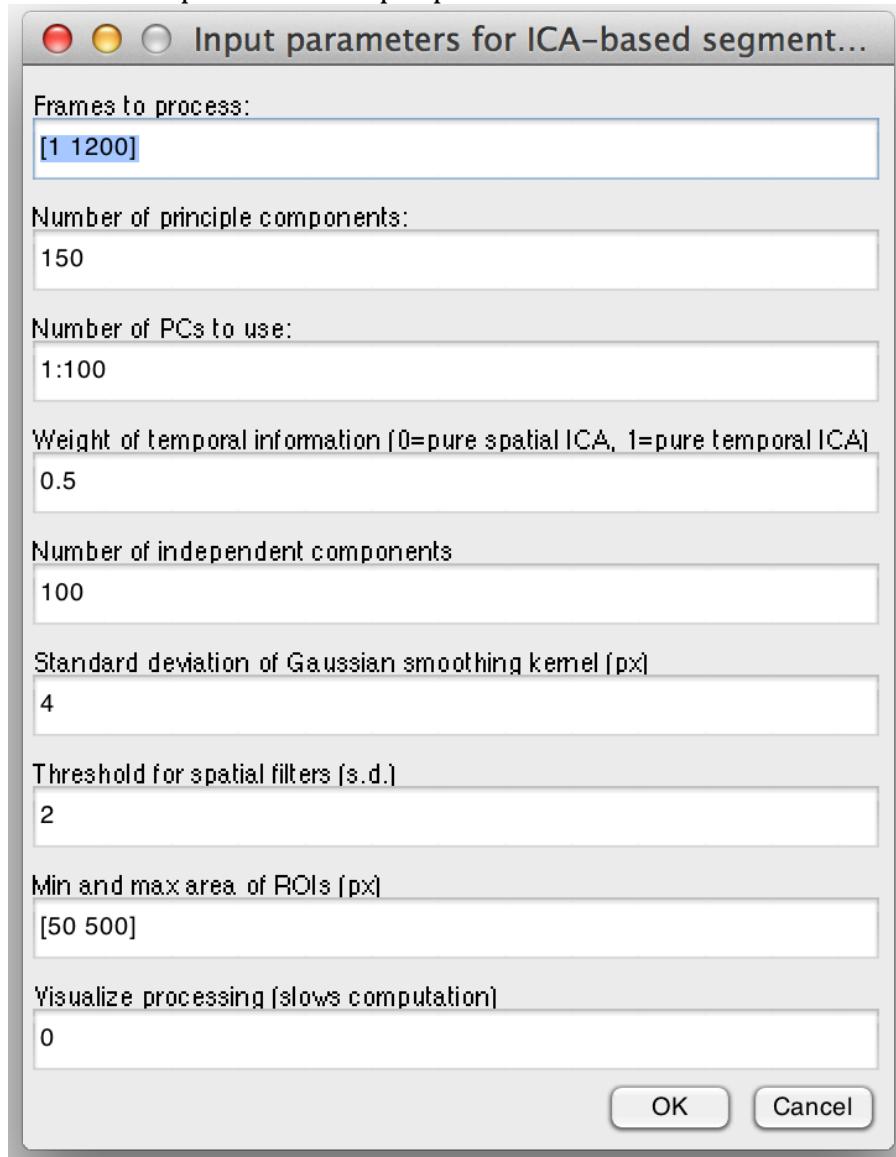


**File menubar:**

- *New*: clears the list boxes and resets the GUI.
- *Open folder containing .tif stacks*: Select folder containing .tif stack of calcium activity. Repeat this process to add multiple folders. Folder names should be populated in the left list box.
- *Open folder containing .csv files*: To make this software more versatile, we allow the users to import .csv files that may have been generated using an external program such as Igor. Although, .tif stack is ideal. The .csv file must be formatted in the following way: a) no headers are permitted, b) the file should contain only numerical entries, separated by commas, c) each row corresponds to a single frame and each column corresponds to an ROI, d) a value of, for example, 100.34 in row 3, column 5 means that the average fluorescence intensity of neuron # 5 in frame # 3 was 100.34. After selecting the folder, the software will generate a “mock” image stack so you can interactively work with the data by selecting different ROIs and visualizing their time-varying trace. Please refer to the sample “baseline.csv” file for formatting.
- *Merge files*: When streaming imaging data for long durations (> 5 minutes at 10Hz), many commercially available software such as Metamorph split the image stack into multiple tiff files. It is desirable to stitch these files together into a single larger file so that subsequent analysis can be performed on the full time-series. After selecting this option, you will be prompted to enter file indices in order that you want to stitch. For example, suppose the listbox on right has the following files: “baseline.tif, baseline-file001.tif, baseline-file002.tif, stim.tif”. If you want to stitch the first 3 files together, you would enter “[1,2,3]” in the input dialog box. This will append all the images from baseline-file001.tif to the end of baseline.tif and then append baseline-file002.tif to the now larger baseline.tif. Once merging is complete, baseline-file001.tif and baseline-file002.tif will be automatically recycled and the listbox will be updated to show only baseline.tif and stim.tif.

**Batch segmentation pushbutton:**

- After loading folders, we recommend doing batch segmentation by clicking the “Batch segmentation” button on the bottom left or Pre-processing -> Batch segmentation.
- There are two methods for automated segmentation and you will be prompted to select either “ICA” based approach or “Active contour” method. The active contour method is fast and does not require lot of RAM, but may require manual touch-ups. The ICA approach is based on (Mukamel, Nimmerjahn et al. 2009) and is significantly more memory intensive, however, it is likely more accurate than active contour. Select the option that best suits your hardware configuration.
- If you choose the ICA method, you will have the option to adjust parameters or accept default parameters. Scroll to the Segmentation GUI description below for more description on the input parameters.

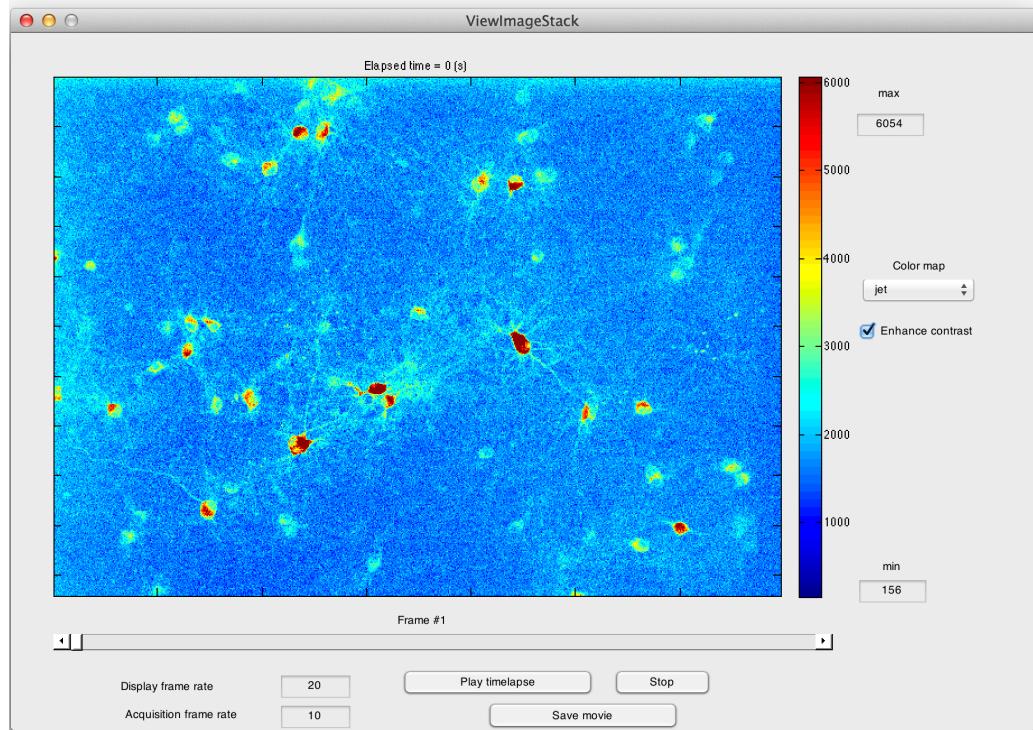


- Once batch segmentation is complete, proceed by making a folder selection on the left listbox. The right listbox will be populated with .tif files from the selected folder. Make a file selection in the right listbox.

## Pre-processing menubar

### *View image stack*

- You will be prompted to enter start and end frames. The default is to load all image frames. You should have a new figure like below:



- In the View Image Stack figure, you can quickly scroll through the image stack with playback controls and a frame slider bar. Colormap can be adjusted with a dropdown menu to either jet, grayscale, or green. Check the “Enhance contrast” checkbox for better visualization or adjust the colorbar limits by entering new values. You can also save the image stack (as it appears in the figure) to an .avi file for later playback. Exit this window to return to the main CalciumAnalysis figure.

### *Remove bad frames:*

Enter a range of frames to remove from the image stack. Enter the range as start:end, for example 200:300 will remove frames 200 to 300 from the image stack.

### *Motion correction*

We have incorporated several tools for assessing and removing motion artifact. Use the “View Image stack” tool to quickly scroll through the set of images and determine if there is any motion that could degrade ROI-based analysis. Download the file “stream1.tif” from our lab website to test our motion correction tools. During acquisition of this experiment, the user accidentally bumped the microscope stage, introducing a shift in focus. If you quickly scroll through this stack, you will get that the field of view shifts at frame #557.

### *Check for motion artifact:*

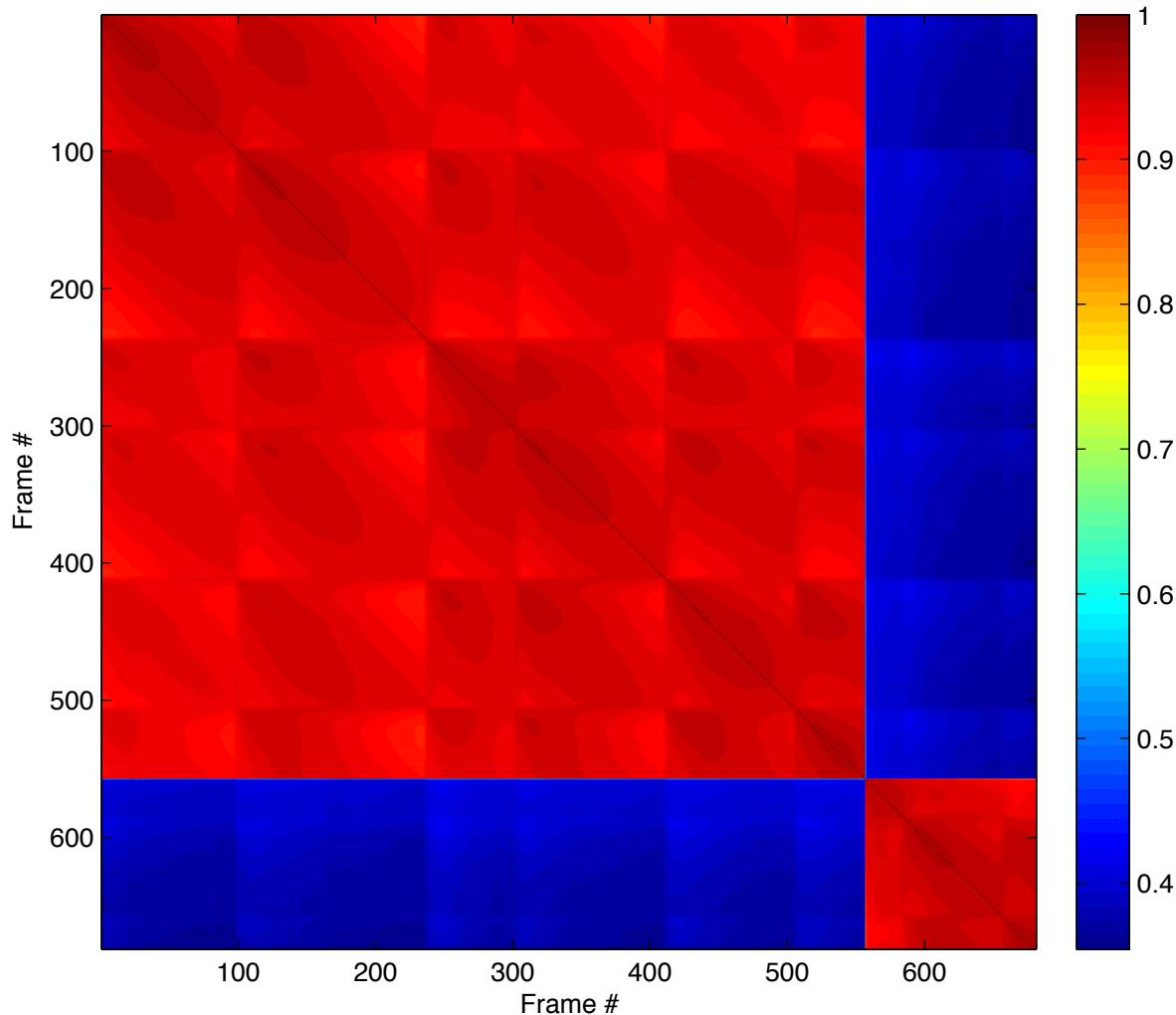
Computes a 2D correlation coefficient,  $r$ , between the first and the last frame of the image stack. Also randomly selects 100 frames from the image stack and computes pair-wise  $r$ . If

any of these  $r$  is less than 0.7, the user is warned that it is likely the image stack contains motion artifact.

#### [View correlation matrix](#)

Computes pair-wise 2D correlation coefficient between all image frames and displays the results of the matrix. Low values (blue) indicate possible misalignment, i.e. motion artifact. Note: computing the full correlation matrix is computationally intensive and may take up to 15 minutes for a stack containing 600 frames. The correlation matrix for the demo file, "steam1.tif" is shown below:

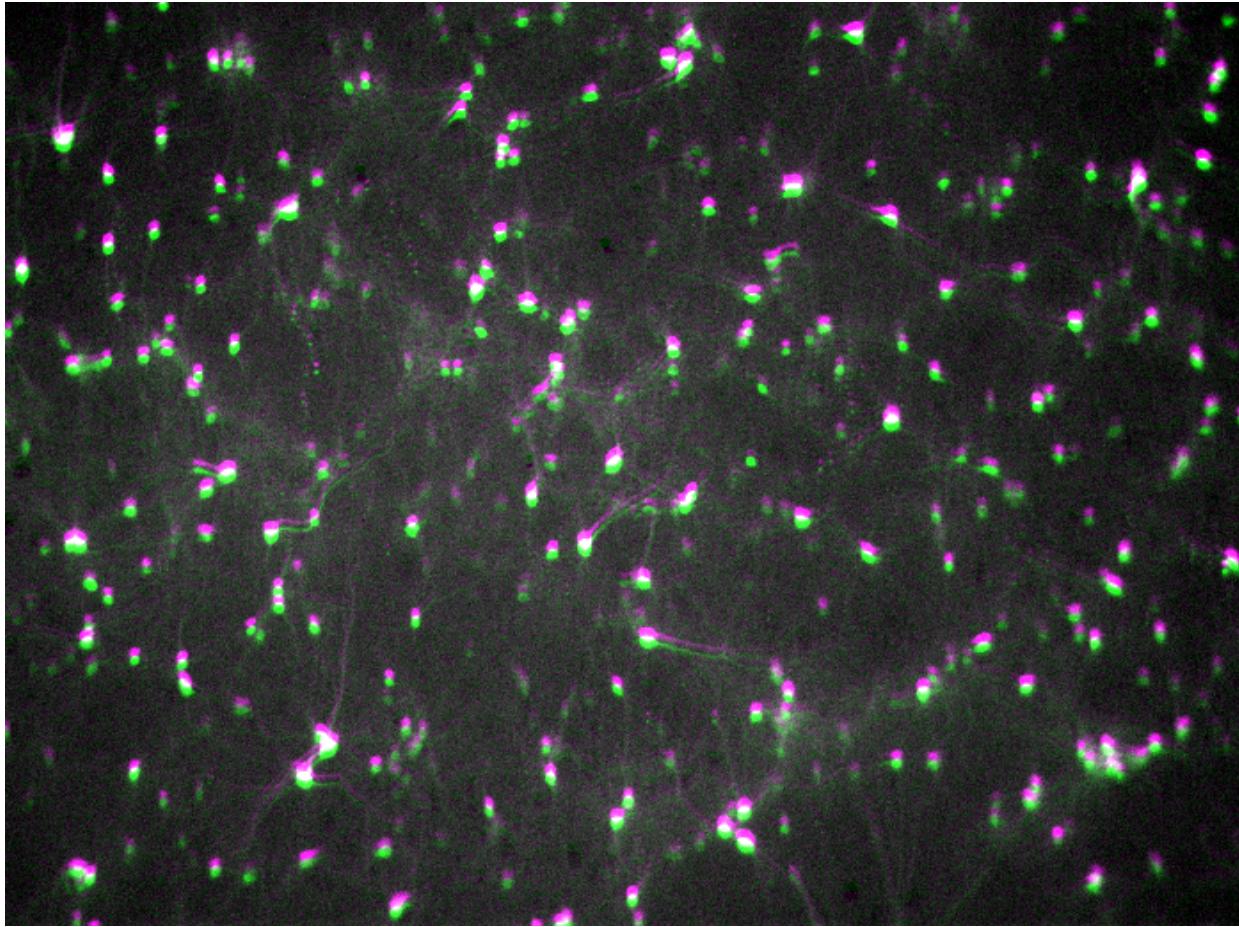
Pair-wise image frame correlations. Low values indicate possible misalignment (motion artifact)



#### [Overlay pair-wise frames:](#)

The user is prompted to enter two frame numbers. These two frames are overlaid and displayed in pseudocolor, where pink or green represent misalignment in pixel intensities between the frames. Overlay between the first and last frames of "stream1.tif" is shown below. Note how the image appears blurred due to a stage shift and the correlation coefficient is small (0.37).

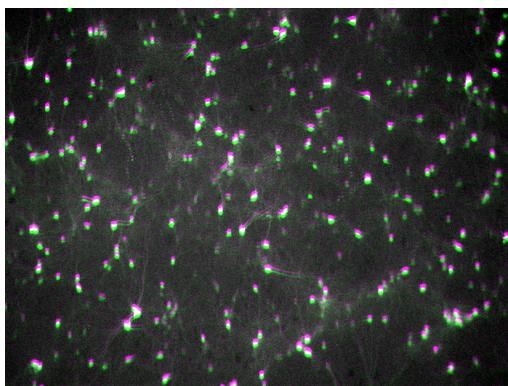
2-D correlation between frames 1 and 681 = 0.374211



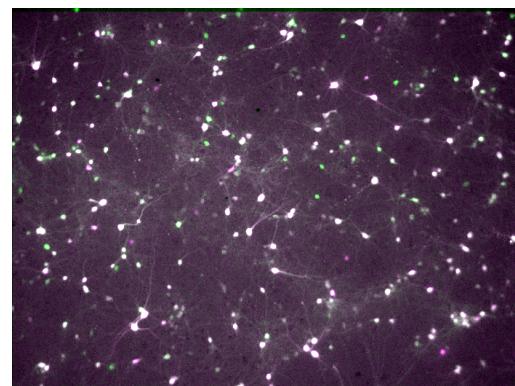
#### Align pair-wise frames

The user is prompted to enter two frame numbers, [frame1 frame2]. Frame1 represents the template frame and frame2 is the input frame which will be deformed/warped to align with the template frame1. An alignment between the first and last frames is shown below (compare with the original overlay).

ORIGINAL overlay between frames 1 and 681.  
2-D correlation = 0.374211



REGISTERED overlay between frames 1 and 681.  
2-D correlation = 0.772255



### Align all frames to a template

Uses image registration to warp a range of frames to a template. In this example, since we know that the field of view shifted at frame #557, we will align frames 557 to 681 (last frame in the stack) to the template frame # 556.

### View corrected stack

Displays a GUI to quickly scroll through the entire updated image stack, containing registered frames. If motion artifact has been removed, proceed to save the updated image stack. Otherwise, go to preferences and choose a different method of image registration transformation.

### Save image stack

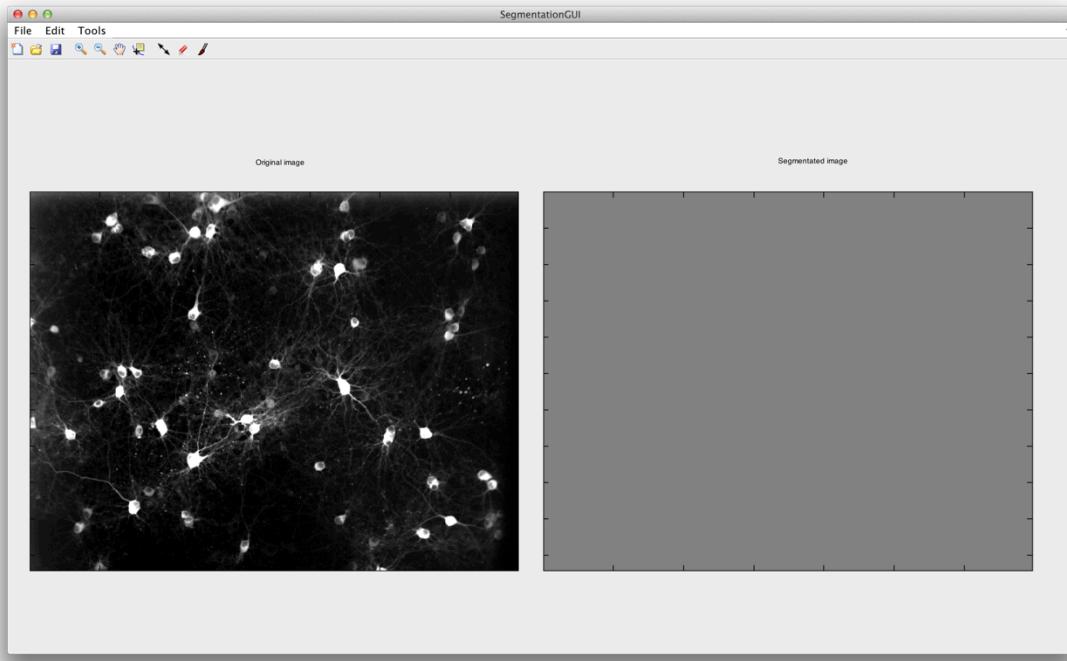
Overwrites the original file with the updated, motion-corrected file.

### Preferences

Select the transformation type for image registration and maximum number of iterations. Options are translation, rigid, similarity and affine. In most cases, the “translation” transformation should work best.

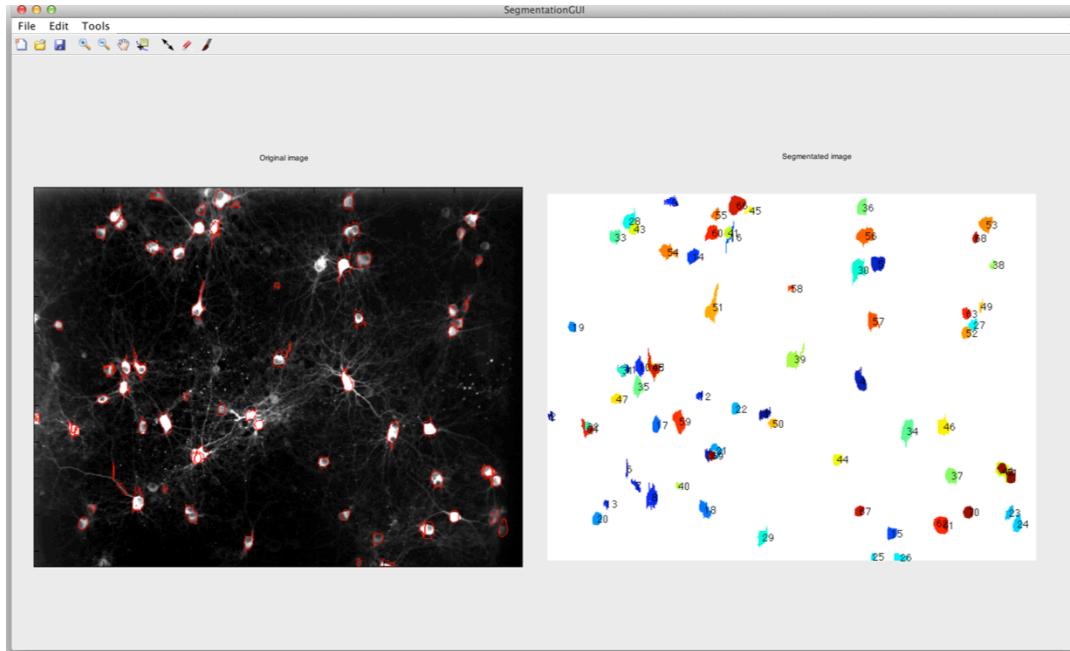
### *Segmentation GUI.*

This will bring up a window like below.



- The blank screen on the right will be populated with segmented regions per the analysis selected. This will change as you select different methods, and also as you edit the identified ROIs.
- There are many ways to segment the image to delineate neuronal cell bodies from background. We recommend using the demo data to develop a comparison of the different methods included in the software, and how each of these may present advantages or disadvantages when you begin analyzing your own data.

- If you already did the Batch segmentation, you can simply load the segmentation file using [File -> Open Segmentation](#). The segmentation files are saved with a “Segmentation-“ prefix and a “.mat” extension.
- The labeled segmentation is shown on the right and the boundaries of ROIs displayed in red.



- Here are several ways to work with the Segmentation GUI, listed by menu options:

#### [File menubar \(in the Segmentation GUI\)](#)

- New Segmentation: deletes the current segmentation
- Open Segmentation: open a previously saved segmentation. It is best to select a .mat file, but a .tif file generated with an external program such as ImageJ or Photoshop will work as well.
- Save Segmentation: saves the current segmentation to a .mat file. By default, segmentation for a file names “example.tif” will be saved as “Segmentation-example.mat”.
- Quit: exit and return to the parent CalciumAnalysis window

#### [Edit menubar \(in the Segmentation GUI\)](#)

- Undo: Undo the most recent (last) step.
- Select ROI: click anywhere inside the red boundary to select an ROI. Make your selection on the left image (not the right). The selected ROI will be highlighted in blue and you can change its shape and boundaries as desired to either remove neurites or incorporate more of the cell body.
- Update ROI: once you are satisfied with the selected ROI, this selection will update the segmented image.
- Delete ROI: the selected ROI will be completely deleted from the segmentation image

- **Freehand delete:** Select a region in the left image via freehand draw. Any objects within the freehand region will be removed from the segmented image. This is a great way to remove neurites without entirely deleting an ROI or to remove large portions of erroneously labeled segments.
- **Remove neurites:** As the name suggests, this option will remove neurites from the segmented image. For each labeled ROI, we compute a circularity factor, defined as  $4\pi \text{area}/\text{perimeter}^2$ . A perfectly circular ROI will have circularity factor = 1 and non-circles < 1. The user is prompted for a threshold value, default is 0.2. Any ROI whose circularity factor is less than 0.2 will be removed from the segmented image.

#### Tools menubar (in Segmentation GUI)

- **Threshold:** Use the datatip to estimate background intensity. Then enter a pixel intensity threshold such that values > threshold are part of the foreground. Enter limits on minimum and maximum area of segmented objects. This is a very crude method of segmentation and will likely be a good start, although not the final product.
- **Active contours** Active contour segmentation is based on a method where you select a “seed” point within the ROI that you would like to segment. This seed point then grows until there is no further change in the image gradient at the contour.
  - **Seed points:** To use this tool, simply click anywhere within the cell body. You can keep clicking as many cell bodies as you want. This function is in a continuous *while* loop.
  - **Stop:** Once you are done, go to Tools -> Active contours -> Stop to exit out of the *while* loop and return.
- **ICA:** Automated segmentation using independent component analysis. This is the serial equivalent of “Batch segmentation” in the CalciumAnalysis figure. If you did not choose the Batch segmentation option, you can choose to do an ICA based segmentation using this tool. You will be prompted with a set of parameters. The default should work well in most cases. To enumerate the parameters:
  - Frames to process: range of frames to process. Default is to process all frames in the image stack. Enter as [start\_frame end\_frame]
  - Number of principle components: The number of principle components to derive. This value should be greater than the expected number of neurons in the field of view
  - Number of PCs to use: Provide a list of principle components to retain for further analysis. This should be equal to or less than the number of principle components.
  - Weight of temporal information: Enter a number between 0 and 1. 0 = pure spatial ICA, 1 = pure temporal ICA
  - Number of independent components: This should be roughly the number of neurons in the field of view. More ICs will in general generate a better segmentation but will be slower in computation.

- Standard deviation of Gaussian smoothing kernel: Enter a value for smoothing the independent component filters.
- Threshold: Number of standard deviations above mean to threshold an object
- Min and max area: Enter as two element array, the minimum and maximum area of segmented objects
- Visualize processing: 0 = no, 1=yes.
- Manual
  - *Set radius*: enter a radius (in pixels) of neuronal cell body. This information will be used in the Tools -> Manual -> Ellipse callback.
  - *Ellipse*: Click on the center of a neuronal cell body. This will place a circle of a preset radius (above tool) centered at the point selected. Continue to click and select more ROIs. To stop, select Tools -> Manual -> Stop.
  - *Freehand*: Freehand draw an ROI. Use the zoom tools to better visualize the image.

### *View Segmentation*

- Displays the segmented image in separate figures.

### *Batch segmentation*

- Performs either active contour or ICA-based segmentation on each file within each folder listed in the left list box. ICA segmentation will take some time (15- 30 minutes). This is equivalent to pressing the “Batch segmentation” button in the GUI.

### *Time-averaged image*

- Working file is the one selected in the right list box. This option will load the image stack and compute the mean fluorescence of each pixel across time.

### *Maximum projection*

- Working file is the one selected in the right list box. This option will load the image stack and compute the maximum projection image across time. That is, in the final image, a pixel at (i,j) will be the maximum of the set {(i,j)} from frame 1, (i,j) from frame 2, ... (i,j) from frame N}.

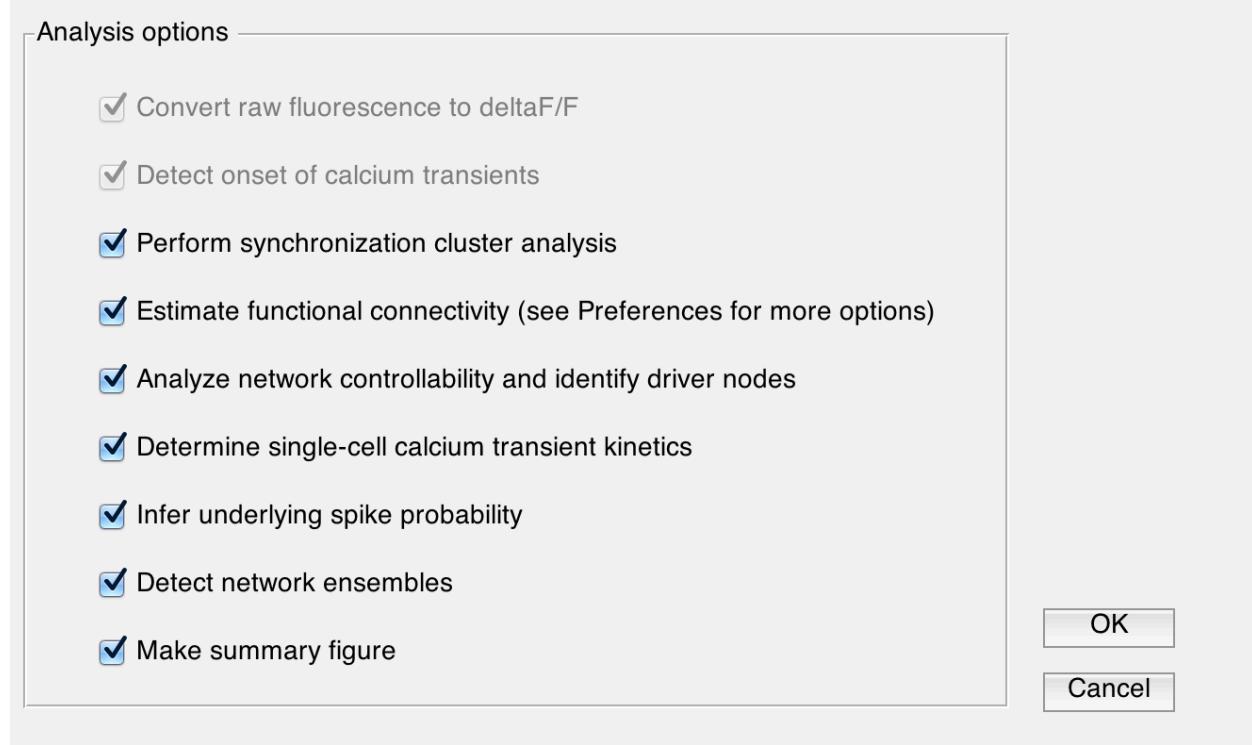
## Analysis menubar

### Preferences

There are several parameters that can be adjusted in the automated analysis of single-cell and network descriptors. These parameters are saved as FluoroSNNAP\_code/params.mat. The default parameters should work in most cases, but you have the option to change them from within the GUI. To enumerate:

### Choose analysis modules

FluoroSNNAP includes multiple modules to analyze single-cell and network-level features. You have the option to select all methods or pick and choose. For example, you may only be interested in synchronization analysis, but not inferring functional connectivity. Use the checkboxes to select the modules to include in the analysis. Note: deselecting “infer functional connectivity” will automatically deselect couple other modules that rely on knowing the underlying functional connectivity, e.g. controllability analysis.



### Parallel computing

Allows the user to either enable or disable parallel computing routines for the analysis. Default is to enable parallel computing.

### Acquisition frame rate

Enter the acquisition frame rate in frames per second. Default is 10 fps (i.e. 100ms exposure time).

### Baseline fluorescence ( $F_0$ )

In computing  $\Delta F/F$ , all pixels within each ROI are first averaged to give a single time course (raw fluorescence trace).  $\Delta F/F$  is calculated by subtracting each value of raw fluorescence with the mean of the lower 50% of previous 10-s values and dividing by the mean of the lower 50% of previous 10-s values. The parameters 50% and 10-s can be adjusted here.

### Calcium event detection

- Template-based method is the default. This method compares a short moving window of input fluorescence trace against a library of calcium transient waveforms. (provided with the source-code, spikes.mat) A similarity metric is computed and thresholded to determine whether the short input window “matches” a waveform in the library. Alternative option is based on fast spike deconvolution method.
- Calcium event detection threshold: threshold value above which a calcium event is detected. For template-based method, the threshold is a normalized correlation coefficient between a short input window and a calcium waveform from the library.
- Minimum deltaF/F0: The minimum change in fluorescence above baseline required for a putative event to be detected as a calcium transient.

### Synchronization Analysis

- Synchronization cluster analysis method: Several ways to determine synchronization exist. Default is to determine instantaneous phase for each fluorescence trace and compute circular variance across pair-wise neurons. Other options are event and equal-time correlation. See references in accompanying manuscript for description. Lastly, the mutual information between pair-wise neuronal calcium fluorescence trace is inversely related to synchronization.
- Minimum size of synchronization cluster: Minimum number of neurons that make up a synchronized assembly
- Number of surrogate resampling: For statistical comparison, we use surrogate data to resample the calcium fluorescence trace (amplitude adjusted fourier transform). The number of times surrogate resampling is performed affects accuracy of the synchronization cluster analysis.
- Significance level: An alpha-level to determine functional connectivity.

### Functional connectivity

We have implemented 5 different methods for inferring functional connectivity. They are, cross-correlation, partial-correlation, instantaneous phase, Granger causality and transfer entropy. Select which method you would like to use for inferring function connectivity using the drop-down menu. The appropriate panel of parameters will be highlighted in red. Refer to the View -> Functional connectivity section for more description of these methods.

Cross-correlation: N resampling = number of times to reshuffle the dataset for statistical significance. Max time lag = time lag for cross-correlation, default is to compute normalized cross-correlation between pair-wise fluorescence traces between -0.5 to 0.5s time lag.

Partial-correlation: alpha-level for significance

Instantaneous phase: N sampling: number of times to resample for statistical significance (default 100), alpha-level for significance (default 0.001)

Granger causality: Max model order (default 20), alpha-level for significance (default 0.05), number of iterations: manually enter a number (100 default) or automatically determine (will take a very long time).

Transfer entropy: N resampling (default 100): number of times to reshuffle to statistical significance, lags: default 1:10

### [Spike Inference](#)

$\Delta F/F$  trace is used to infer spike probability using the algorithms described in (Vogelstein, Packer et al. 2010). Parameters for inferring underlying spikes can be changed here.

### [Network Ensemble](#)

Groups of statistically significant co-active neurons are determined by binarizing spike probability trace at 3 standard deviations and reshuffling active neurons 1000 times per (Miller, Ayzenshtat et al. 2014).

### [Revert to default](#)

Reset all parameters to default values

### [Process single file](#)

- Working file is the one selected in the right list box. This option will load the segmentation for the selected file and compute the mean fluorescence intensity for each ROI at each frame. Results are stored in a new matlab file in the same folder as the selected file. The raw fluorescence intensities are stored in a file prefixed by "CaSignal-". In addition, the raw data is output to a comma delimited text file, where each row is an ROI and commas separate the mean fluorescence across frames.
- Next, it will determine the onset of calcium transients using parameters set in Analysis -> Preferences.
- Next, it will determine single cell calcium transient descriptors such as the onset of calcium transient, amplitude, rise and fall time.
- Next, it will determine the level of synchronization in the calcium activity and infer a functional connectivity matrix using the method selected in Preferences.
- Next, determine network ensembles
- The results of this analysis are stored as a matlab .mat file and plain text .txt file. Prefix "analysis-" denotes the matlab .mat file and post-script \_summary.txt denotes the plain text file. Also a summary figure is generated as .eps and .tiff files and stored in the directory "Figures".

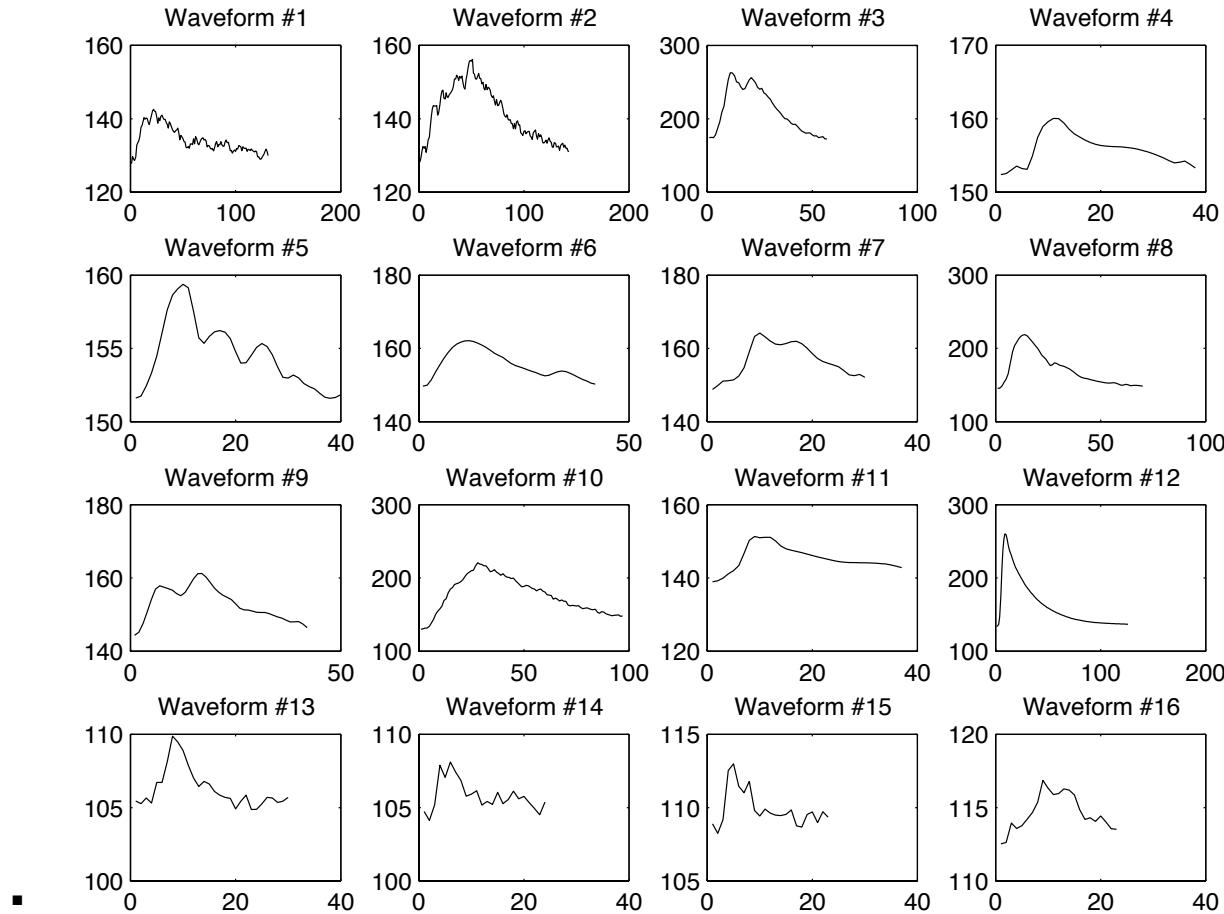
### [Batch single and network-analysis](#)

- This option batch processes all the files within each of the folder that have been added to the list box on left.
- Note, a segmentation file needs to exist for each tiff file to be processed. Run "Batch Segmentation" if you don't have segmentation files.
- See above for description of the analysis.

### *Template library*

#### **View calcium waveforms:**

- Generates a figure displaying the calcium waveforms that make up the library of “true” calcium events. An example is shown below:



#### **Add a calcium waveform to library:**

- For this option to work, you need to have processed the selected file. If you haven't done so already, select a file from the list box on right and select Analysis -> Process single file.
- Then enter a neuron ID to display its fluorescence trace.
- Select a start and end points to mark the beginning and end of a calcium transient that you would like to add to the library. After selecting the second point, hit <Enter> on your keyboard to return.

#### **Delete a waveform from library**

- All the waveforms from the library are first displayed in a multi-panel figure. Enter a number corresponding to the waveform that you would like to remove from the library.
- The new (reduced by one) library is displayed again to verify.

#### **Recompute synchronization and functional connectivity**

Use this tool to recompute synchronization and functional connectivity analysis if you made changes to calcium transient onset times or Preferences. This analysis does not

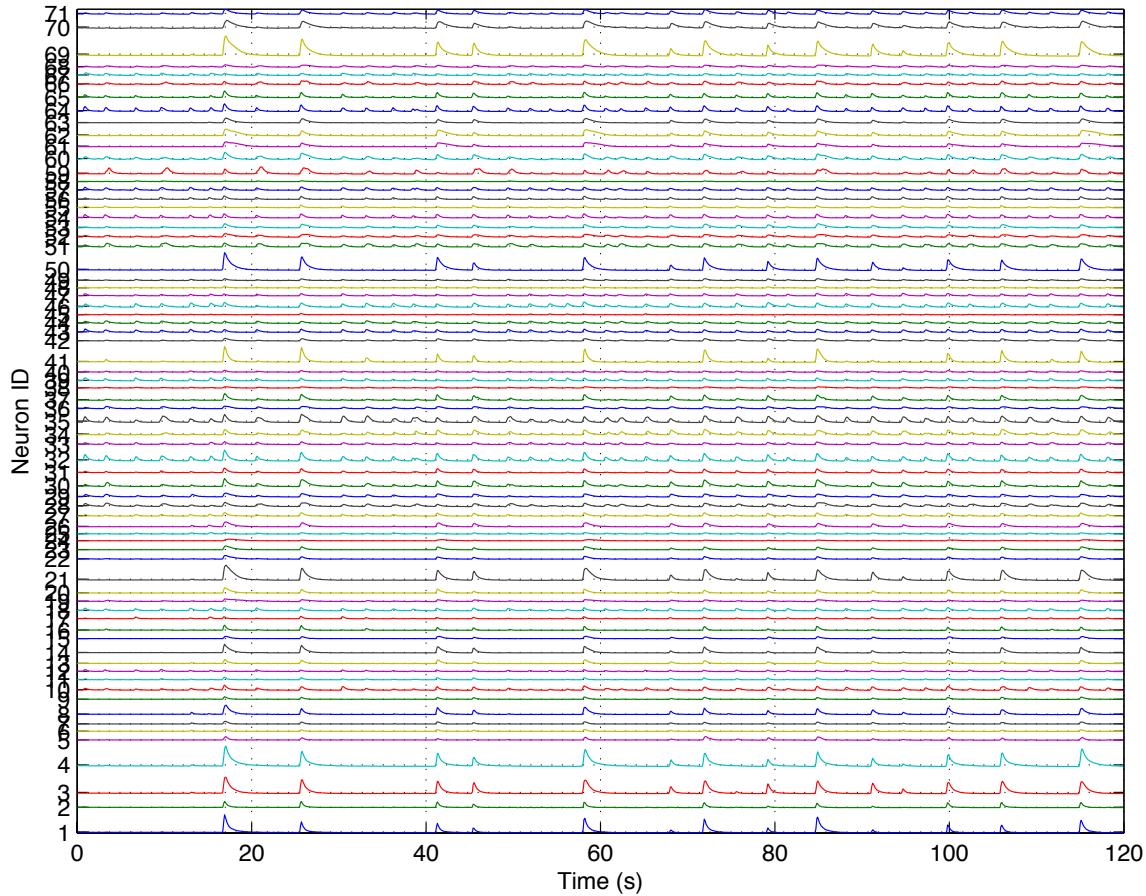
require the use of original tiff stack so it can be useful to reanalyze or visualize pre-processed data.

### View menubar:

Use this menubar after you have done either single file or batch analysis. Make a filename selection before using this menubar.

### *Fluorescence traces:*

- The time-varying fluorescence trace for each ROI is plotted on a single figure, scaled and separated for visual clarity. Example shown below:



### *deltaF/F0 traces*

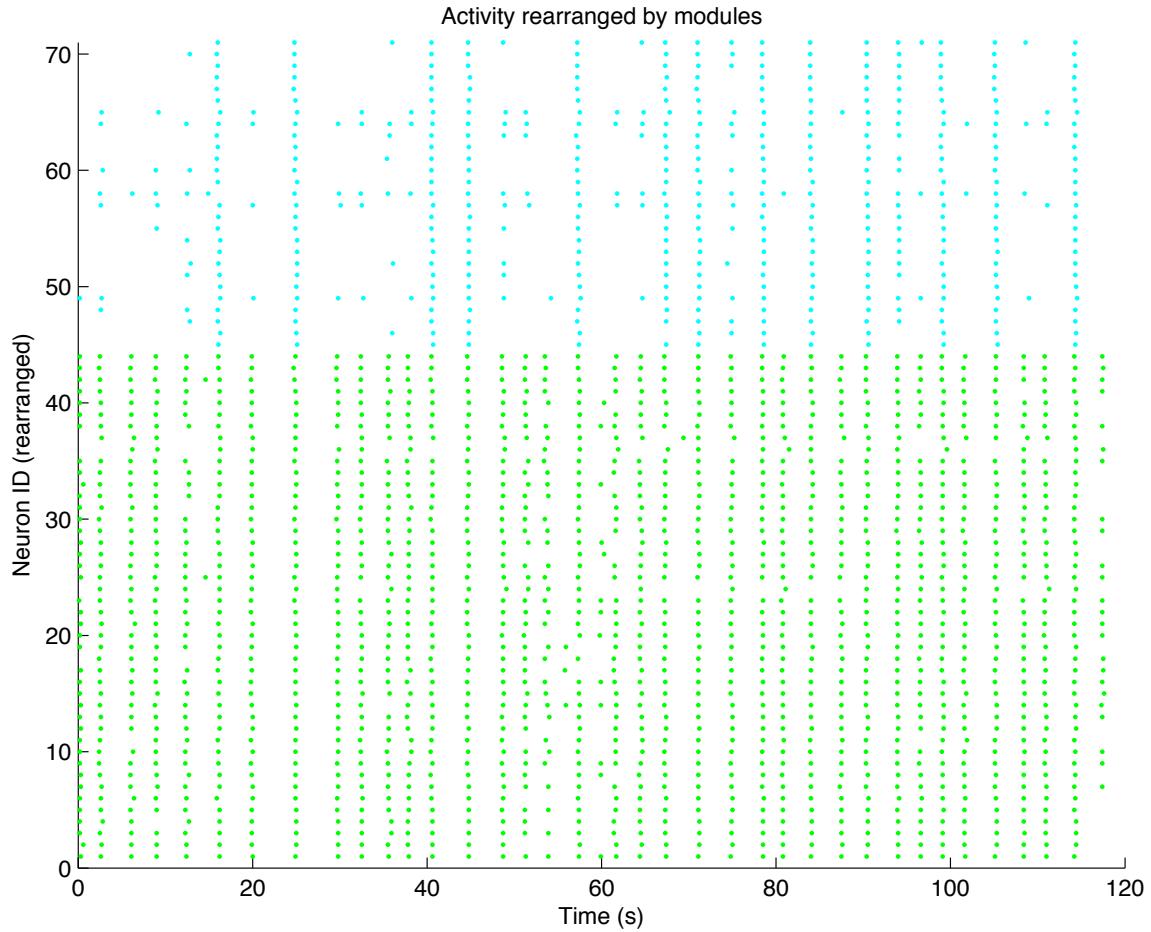
Displays the time-varying  $\Delta F/F_0$  trace for all ROIs.  $\Delta F/F_0$  value of at frame  $i$  of the  $j$ -th ROI is computed by subtracting the mean fluorescence intensity of the  $j$ -th ROI in frame  $i$  with the mean of the lower 50% of previous 10-s values of fluorescence intensities and dividing it by the same number.

### *Raster plot (calcium):*

- Plots the calcium activity as raster, with time on the x-axis, neuron ID on the y-axis and a dot represents onset of calcium transient.

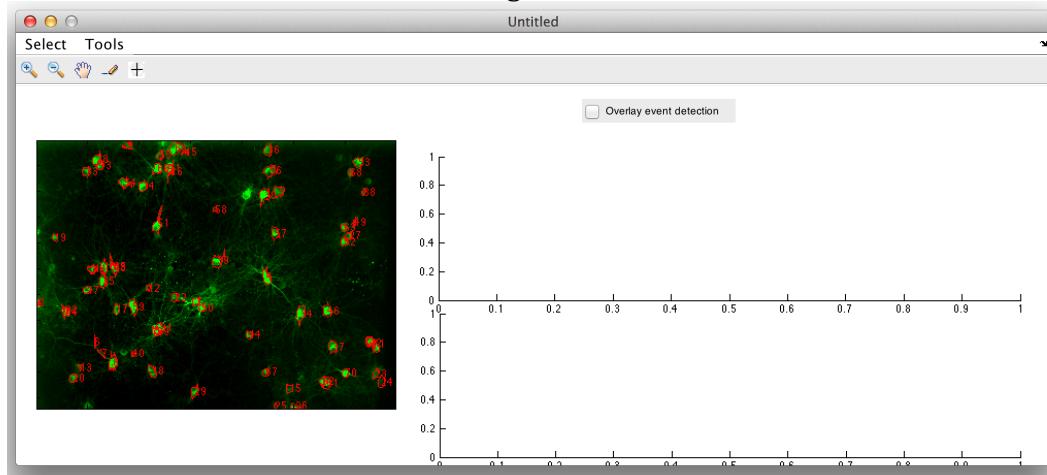
### *Raster plot (calcium, grouped by activity)*

- Same as raster plot above, but neuron IDs are grouped by their assignment into modules and color-coded. Example shown below:



#### *Calcium event inspector:*

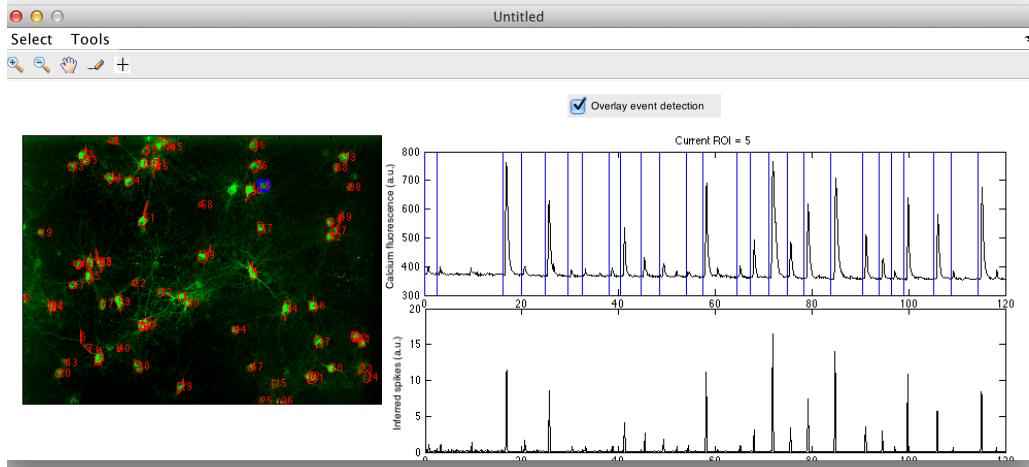
This will bring up a new GUI to interactively visualize the fluorescence trace of different ROIs and calcium events. You should have a figure like below:



- Select an ROI either by [Select -> Select ROI](#) or [Select -> Enter ROI number](#). In the former case, click anywhere inside the red boundary in the left image to select the ROI. The raw fluorescence trace for the selected ROI is displayed on the

upper right plot. The inferred spike train for the selected ROI is displayed in the bottom right plot.

- Toggle “**Overlay event detection**” to show or hide the onset of calcium events. Example shown below:



## Tools

### Remove calcium event:

- Simply draw a horizontal line across the calcium events (shown in blue) that you would like to remove. Double-click at the end of your line to accept.

### Add calcium event:

- Click on the onset of calcium transients to mark them as “calcium events”. Select as many points as you want. Once done, hit <Enter> on your keyboard.

### Set a new threshold and apply to selected ROI

- As the name implies, enter a new threshold value if you are unsatisfied with the automated event detection. This option will update events only for the selected ROI and is a good way to find an “optimal” threshold before making that change to the rest of ROIs.

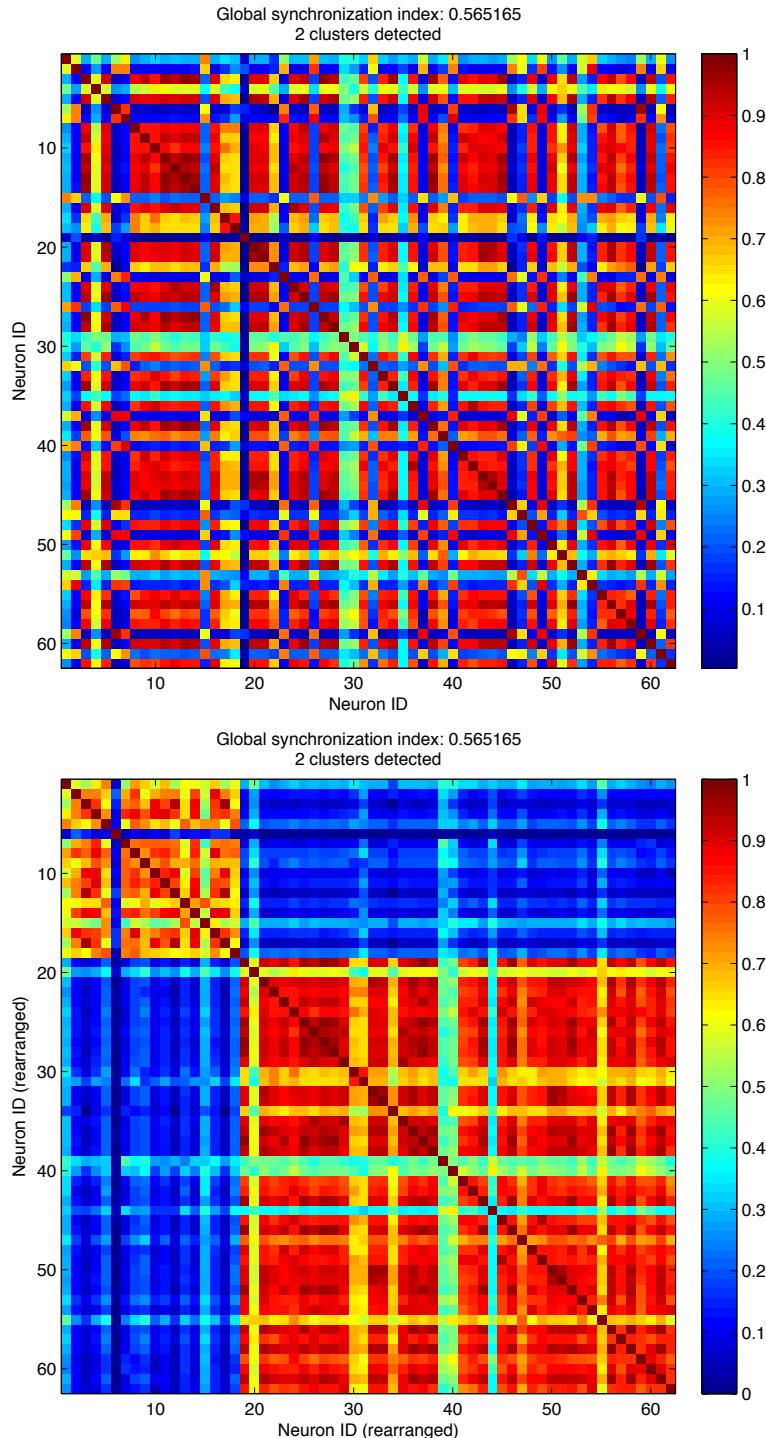
### Set a new threshold and apply to all ROIs

- Same as above, but the change is applied to all ROIs. This may take several minutes.

Upon exiting, you will be prompted if you want to save changes. If you added new events, deleted events or made changes to the threshold and you want to save and update the “analysis-\*.mat” file, click “Yes”. Note: when you go to visualize functional connectivity, select “Re-process” to reanalyze synchronization and re-compute functional connectivity measures, taking into account the changes to calcium events that you just made.

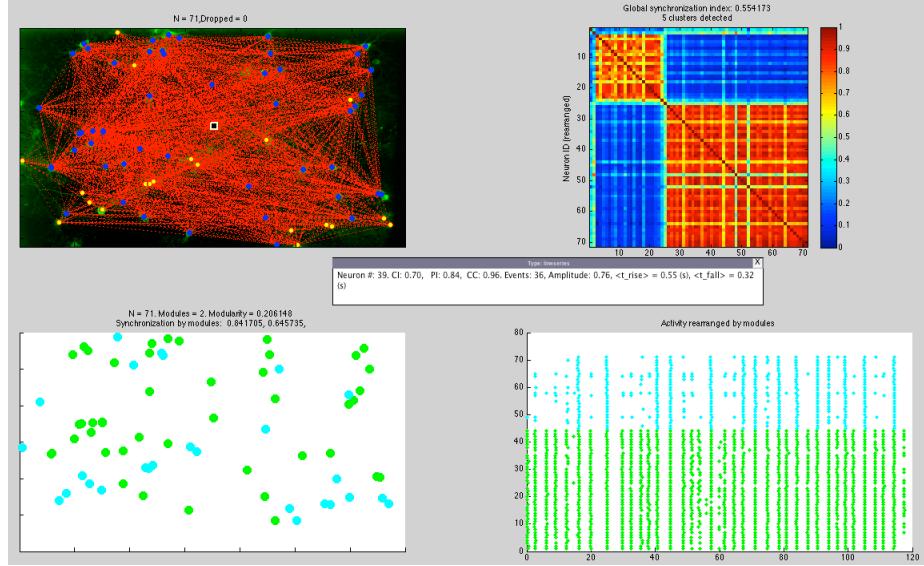
### *Synchronization matrix:*

Displays pair-wise synchronization matrix. Two figures are generated. The first figure is unordered, i.e. rows are ROI labels from segmented image – row 1 is ROI 1, row 2 is ROI 2 etc. Figure 2 shows the synchronization matrix, grouped by similar values or clusters. Here, row 1 may correspond to ROI 5 and row 2 may correspond to ROI 43 etc.



### *Summary figure:*

- You will be prompted to either use pre-processed data or re-compute. If you made changes to the calcium event detection using the “Calcium event inspector” tools or wish you select a different method for functional connectivity, select “Re-process”; otherwise, select “pre-processed”. You should get a figure like below.



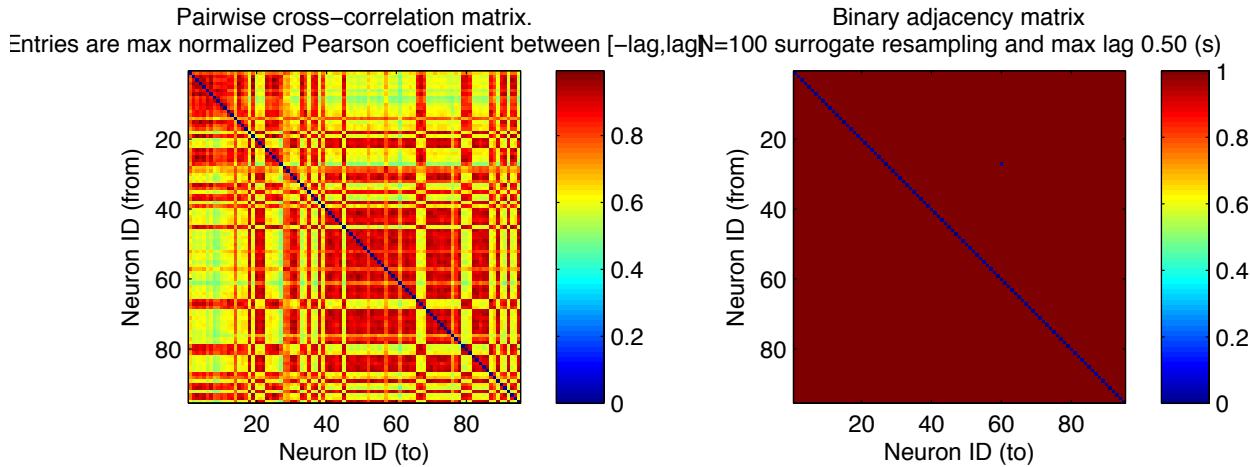
- Use your datatip to select individual nodes in the top left figure. The functionally connected nodes will be highlighted in blue and more detailed information about the selected node will be displayed in the label tip box.

### *Functional Connectivity*

#### Cross-correlation

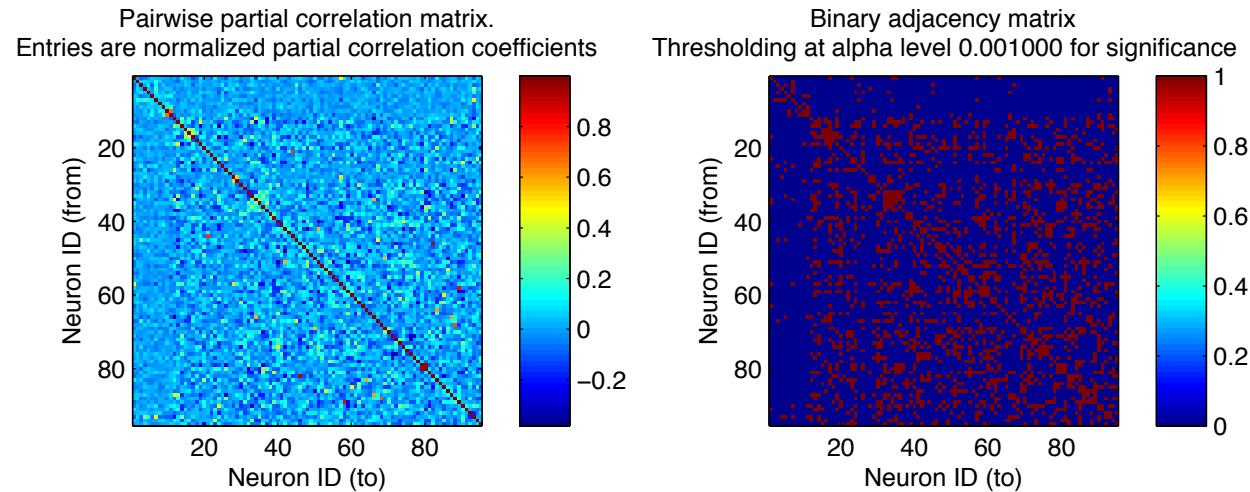
Functional connectivity reconstruction using cross-correlation is performed using standard Pearson cross-correlation between deltaF/F traces. The score assigned to each potential link is given by the largest cross-correlogram peak for lags between 0 and  $t_{max} = 500$  ms (adjustable parameter). The weighted cross-correlation matrix is then thresholded to generate an undirected binary adjacency matrix.

A different threshold is generated for each pair-wise interaction in the following way. Suppose the largest cross-correlogram peak between neurons  $i$  and  $j$  is  $r$ . Calcium event onset times for neuron  $i$  are stored in the array  $t_i$  and event times for  $j$  are stored in  $t_j$ . There are  $N_i$  total calcium transient events for neuron  $i$  and  $N_j$  events for neuron  $j$ . Furthermore, there are  $N_{total}$  total frames in the image stack. We generate surrogate dataset by randomly choosing  $N_j$  points from 1 to  $N_{total}$ . Using these  $N_{j,sur}$  points, we generate a deltaF/F trace and compute cross-correlogram peak between the original deltaF/F trace of neuron  $i$  with the surrogate trace for neuron  $j$ . This is repeated 100 times to generate 100  $r_{sur}$  values. The 95<sup>th</sup> percentile of the surrogate Pearson cross-correlation is the threshold for determining a significant correlation between  $i$  and  $j$ .



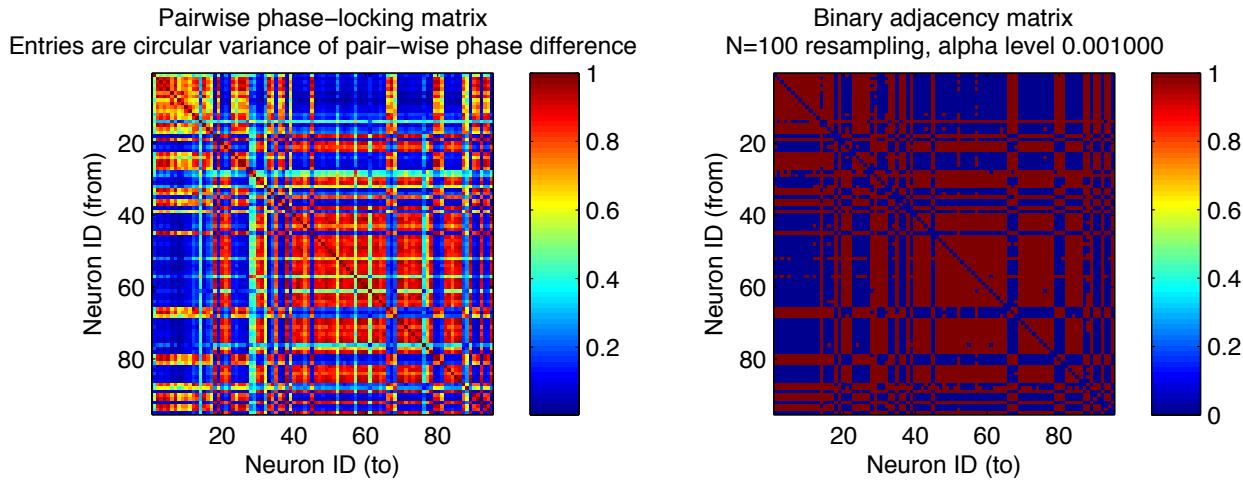
### Partial correlation

Partial correlation is a correlation matrix that removes for a given ROI pair the effect of the rest of the variables, i.e., removing the correlations contribution which are coming from common neighbors interactions. Partial correlation is computed with the *partialcorr* method in MATLAB. *partialcorr* also returns a matrix of *p*-values for testing the hypothesis of no PC against the alternative that there is a non-zero PC. These *p*-values are thresholded at alpha-level specified by the user to generate an undirected binary adjacency matrix.



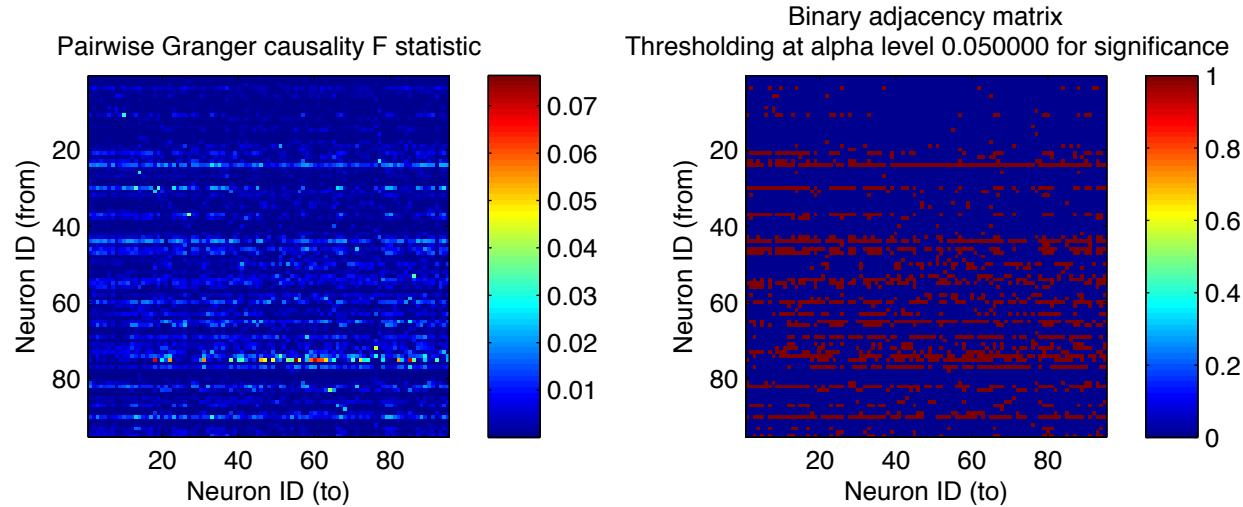
### Instantaneous phase

The instantaneous phase for each neuron is determined (see Methods section of accompanying manuscript). For each pair-wise neuron  $i$  and  $j$ , we compute the instantaneous phase difference  $\varphi_{ij}(t)$ . Surrogate instantaneous phase for neuron  $j$  is generated using an Amplitude Adjusted Fourier Transform (AAFT) and the instantaneous phase difference between  $i$  and surrogate  $j$  is computed. We then use the two-sample Kolmogorov-Smirnov test to test the equality of  $\varphi_{ij}(t)$  and  $\varphi_{ij(sur)}(t)$ . This is repeated  $N$  times (adjustable parameter) and the *p*-value is thresholded at an alpha-level specified by user to generate an undirected binary adjacency matrix.



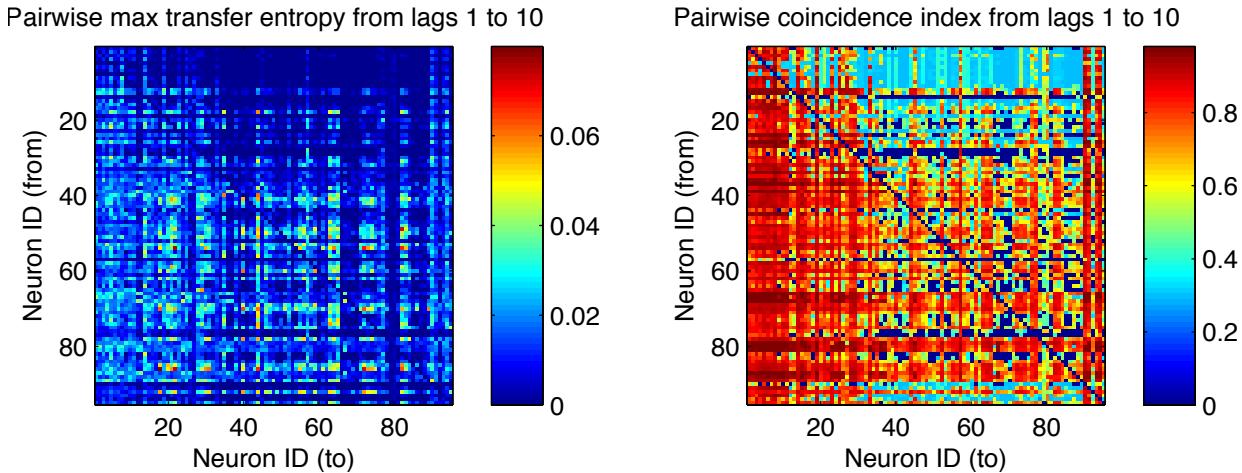
### Granger causality

Uses the deltaF/F traces to determine if one time series Granger causes another. A time series X is said to Granger-cause Y if it can be shown through a series of F-tests on lagged values of X and Y that those X values provide statistically significant information about future values of Y. The result is a directed binary adjacency matrix after thresholding at an alpha-level specified by the user. Please refer to (Barnett and Seth 2014) for more information.



### Transfer entropy

Uses transfer entropy (TE) to estimate information flow between neurons. TE is positive if including information about neuron  $j$ 's spiking activity improves the prediction of neuron  $i$ 's activity beyond the prediction based on neuron  $i$ 's past alone over time lags specified by the user. The maximum transfer entropy across different time lags (peakTE) and a coincidence index are computed for each pair. Please see (Ito, Hansen et al. 2011). Surrogate dataset were generated by random shuffling binary activity data and peakTE was thresholded at 95<sup>th</sup> percentile of surrogate distribution to eliminate peakTE and CI values that are below the threshold, generating a directed weighted adjacency matrix.



### Fast spike inference

#### View spikes

- Spike inference is done using the fast nonnegative deconvolution method described by Vogelstein et al, J Neurophysiol 2010.
- Plots the inferred spikes for all ROIs in a single plot

#### Inferred activity raster

- Select a threshold (number of standard deviations above 0) to binarize inferred spike probability.
- Plot inferred spike activity as raster

#### Network ensembles

Network ensembles were determined as described in (Miller, Ayzensthtat et al. 2014). For completeness, we have copied & pasted their method and implemented the algorithm in FluoroSNNAP.

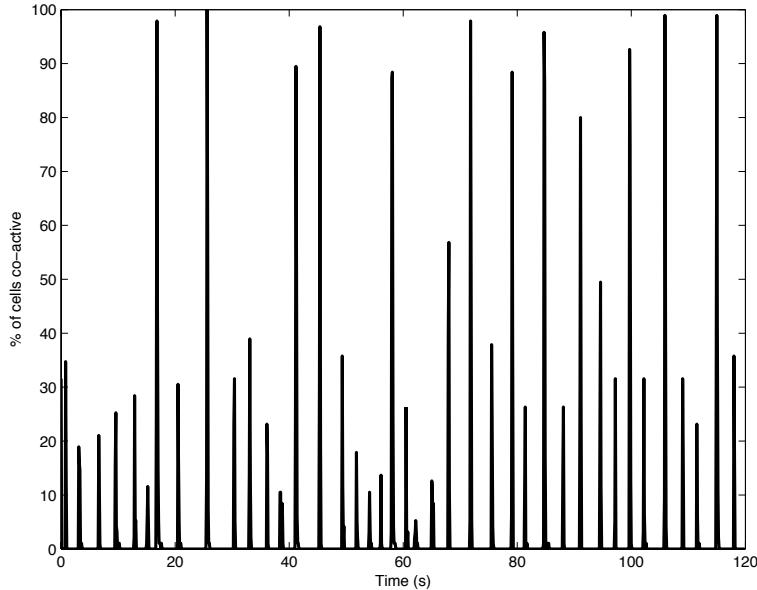
Spike probability was inferred from calcium signals using a fast, non-negative deconvolution method (Vogelstein, Packer et al. 2010). The baseline of calcium signals was detrended, and  $\Delta F/F$  was calculated before applying an algorithm to infer spike probability. The output was normalized by a maximum value in each neuron. Spike probability was then thresholded to a level of 3 standard deviations above 0 (this parameter can be adjusted by the user using the Preferences tool). The values above threshold were set to 1, and the values below threshold were set to 0. These binary activity data were then used for analysis.

An ensemble was defined as coactivation of a group of neurons in a high-activity frame in which a statistically significant number of neurons were active. To establish a threshold for the significant number of coactive neurons, binary activity data were shuffled 1,000 times (adjustable parameter) by randomly transposing intervals of activity within each cell. The threshold corresponding to a significance level of  $P<0.05$  was estimated as the number of activated cells in a single frame that exceeded only 5% of these surrogate datasets.

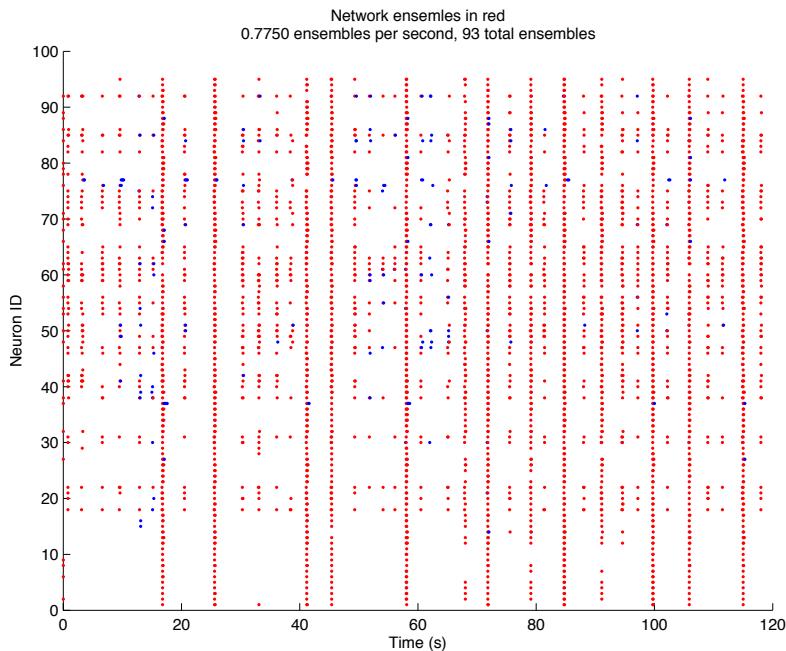
The number of ensembles per was calculated by dividing a number of high-activity frames by total number of frames and multiplying by frame rate.

Three figures are generated with this tool:

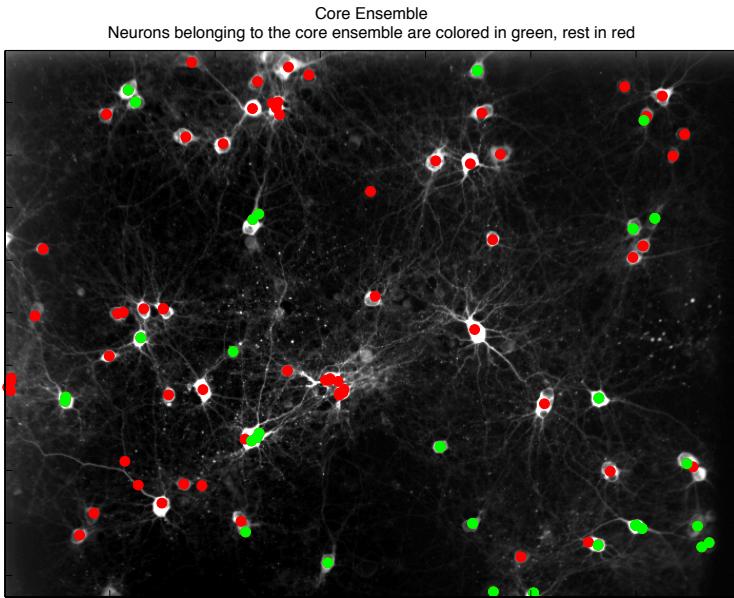
Percentage of neurons coactive in each frame:



The activity of statistically significant co-active neuronal ensembles are shown in red and rest in blue.

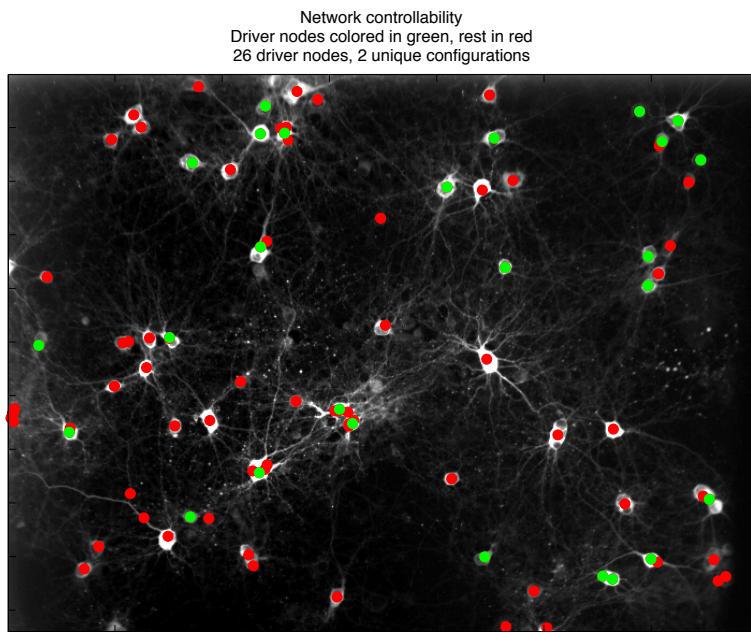


Core ensemble, defined as a group of coactive neurons that are conserved in all significantly correlated ensembles are colored in green and the rest in red:

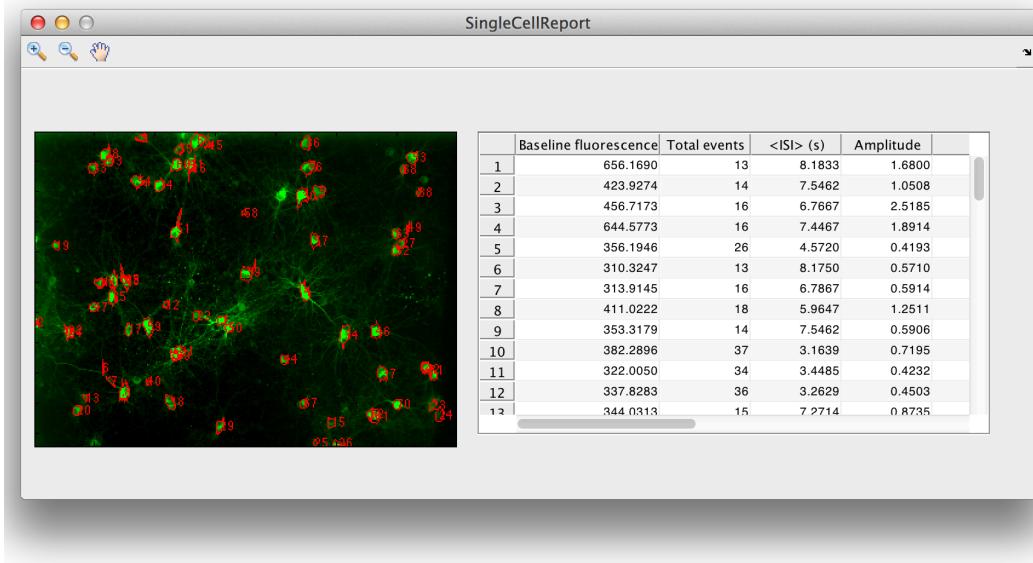


### Controllability

Uses the maximum geometric multiplicity algorithm (Yuan, Zhao et al. 2013) to identify driver nodes in an adjacency matrix. Select the underlying functional connectivity method to view its driver nodes. An example of controllability of a network generated using Granger causality is shown below, where driver nodes are colored in green and the rest in red:



### *Single cell summary*



Displays a new figure, with working image and labeled ROIs and a table that lists single-cell properties such as mean amplitude, baseline fluorescence, mean rise time, etc.

- Find the ROI from left image and scroll in the table to view summary statistics.

## Advanced use

Several .mat files are generated and saved in the working directory. Here, we will go through the contents of these files and sample matlab code to work with the data therein.

For this example, assume that our tiff stack is called “baseline.tif”.

### Segmentation

In the SegmentationGUI, clicking “Save” generates a Segmentation-baseline.mat file. In MATLAB command window, load this file:

```
>> load( '/Users/tapan/Documents/Research/Calcium image analysis/gcamp_timelapse1/Segmentation-baseline.mat' )
```

The MATLAB workspace will contain two variables: “L” and “ica”.

L is a label matrix, same size as a baseline.tif frame. The labels are numbered ROIs that delineate foreground from background. Use

```
>>figure; imagesc(L); colorbar;
```

to view the labeled image.

“ica” is either 1 or 0 indicating whether the segmentation method involved ICA-algorithm.

To use your own segmentation file with the FluoroSNNAP GUI, for example a segmentation generated using ImageJ or Photoshop, simply load the segmented image into MATLAB.

Suppose this image is called Mask.tif.

```
>> I = imread('Mask.tif'); % load the image
>> L = bwlabel(I~=0); % label the image
>> ica = 0; % no ICA algorithm was used
```

Save the workspace as Segmentation-baseline.mat

### **CaSignal**

A CaSignal-baseline.mat is generated which contains the raw fluorescence vs. frame data for each ROI. Load this file and you should have a variable “analysis”. This is a structure containing fields:

```
>> analysis
```

```
analysis =
```

```
    image: [520x696x3 uint16]
    filename: '/Users/tapan/Documents/Research/Calcium image
analysis/gcamp_timelapse1/base...'
    F_cell: [95x1200 double]
    F_whole: [1200x1 double]
    L: [520x696 double]
    fps: 10
```

The dot operator references fields of a structure.

- analysis.image is the time-averaged image frame. To view it,

```
>> figure; imshow(analysis.image, []);
```

- analysis.F\_cell is a matrix of size ROIs x frames. Entries are mean fluorescence intensity within the ROI. To see the fluorescence trace for ROI 5,

```
>> figure; plot(analysis.F_cell(5,:));
```

- analysis.F\_whole is full frame mean fluorescence.

- analysis.L is the label matrix. ROIs labeled in L index the rows in F\_cell. To view the labeled image,

```
>> figure; imagesc(analysis.L);
```

### **Analysis**

An analysis-baseline.mat is generated and contains all single-cell and network level analysis. Load this file and you should have a “data” variable in your workspace.

```
Command Window
>> data

data = 

    F_cell: [95x1200 double]
    F_whole: [1200x1 double]
    image: [520x696x3 uint16]
    filename: '/Users/tapan/Documents/Research/Calcium image analysis/gcamp_timelapse...'
    files_stiched: {'/Users/tapan/Documents/Research/Calcium image analysis/gcamp_timelapse...'}
        Frames: 1200
        fps: 10
        L: [520x696 double]
        params: [1x1 struct]
    Spikes_whole: [1x37 double]
    dF_cell: [95x1200 double]
    N: 95
    Spikes_cell: {95x1 cell}
    SynchroCluster: [1x1 struct]
        phase: [95x1200 double]
        SI: 0.4662
        FC: [1x1 struct]
        SI_m: [2x1 double]
        DF: [95x1 double]
    rise_time: {95x1 cell}
    fall_time: {95x1 cell}
        CV: [95x1 double]
    modules: [1x95 double]
    modularity: 0.0895
    foopsi: [95x1200 double]
        OP: [95x1 double]
    NetworkEnsemble: [1x1 struct]

f -- |
```

- data.F\_cell is the same raw fluorescence data, ROIs x frames.
- data.F\_whole is the full frame average image intensity
- data.image is the time-averaged image
- data.filename is the filename of the tiff stack processed
- data.files\_stiched is a cell array of files that are stitched together if the user used “Merge files” option.
- data.Frames is the total number of frames in the tif stack
- data.fps is the acquisition frame rate
- data.L is the label matrix
- data.params is a structure of parameters used in the analysis.
- data.Spike\_whole is an array of frames numbers that denote onset of transient in the full frame intensity
- data.dF\_cell is the deltaF/F matrix, rows = ROIs, columns = frames
- data.N is the total number of ROIs
- data.Spikes\_cell is a cell array of size total number of ROIs (95). Each entry in the cell is an array of frame numbers that denote the onset of calcium transient. For example, to view the calcium events for ROI 5,

>> data.Spikes\_cell{5}

To view the deltaF/F trace for ROI 5,

>> figure; plot(data.dF\_cell(5,:));

To see the calcium events overlaid on the deltaF/F trace,

```
>> OverlaySpikes(data.dF_cell(5,:), data.Spikes_cell{5});
```

### Synchronization

- data.SynchroCluster is a structure containing the result of synchronization cluster analysis. Here, the user selected to use instantaneous phase to measure synchronization, see (Patel, Ventre et al. 2012). Other options are equal-time correlation and mutual information. For calcium imaging datasets, we recommend using instantaneous phase to quantify synchronization. For micro-electrode array datasets, we recommend equal-time correlation as described in (Kang, Cao et al. 2014). Selection of method will influence the contents of data.SynchroCluster.C matrix, which contains pair-wise synchronization index.

```
>> data.SynchroCluster
```

```
ans =
```

```
    phase: [95x1200 double]
    SI: [95x1 double]
    Num: 2
    PI: [95x2 double]
    EigenVal: [95x1 double]
    Surrogate: [95x1 double]
    C: [95x95 double]
    Assembly_Contents: {[84x1 double]  [95x1 double]}
```

- data.SynchroCluster.phase is the instantaneous phase, rows = ROIs, columns = frames
- data.SynchroCluster.SI is an array of synchronization indices, most of these entries are 0 or very small; the largest entry in this array is the global synchronization index
- data.SynchroCluster.Num is the total number of synchronization clusters detected
- data.SynchroCluster.PI is a matrix of size ROIs x # of synchronization clusters. Entries indicate the strength of participation (participation index) of each ROI in each cluster.
- data.SynchroCluster.EigenVal is an array of eigenvalues of the pair-wise synchronization index matrix, C
- data.SynchroCluster.C is the pair-wise synchronization index matrix. To view,

```
>> figure; imagesc(data.SynchroCluster.C);
```

To rearrange the synchronization matrix and group by clusters,

```
>> [~,pos] = max(data.SynchroCluster.PI,[],2);
>> [~,IDX] = sort(pos);
>> imagesc(data.SynchroCluster.C(IDX,IDX),[0 1]); axis square; colorbar;
```

- data.SynchroCluster.Assembly\_Contents is a cell array of size 1x # of

synchronization clusters. Contents of this cell array are the ROI numbers that participate in the synchronization cluster. One neuron may participate in more than 1 cluster

- data.phase is an instantaneous phase matrix of size ROIs x frames
- data.SI is the global synchronization index.
- data.SI\_m is the synchronization index per module. The community structure (modules) is determined from an underlying adjacency matrix (see below) and synchronization of neurons within each module is computed. If the user selects to compute functional connectivity using all 5 methods, this routine will default to using the adjacency matrix derived from instantaneous phase.

### Functional connectivity

- data.FC is a structure containing functional connectivity measurements, depending on the method selected under Preferences. In this example, we selected to compute functional connectivity using all 5 methods. Contents of data.FC are

```
>> data.FC

ans =

    CC: [1x1 struct]
    PC: [1x1 struct]
    phase: [1x1 struct]
    GC: [1x1 struct]
    TE: [1x1 struct]
```

- data.FC.CC is functional connectivity structure using cross-correlation method.  
Contents are:

```
>> data.FC.CC
```

```
ans =

modularity_Ci: [1x95 double]
modularity_Q: -1.0732e-04
A: [95x95 double]
C: [95x95 double]
clustering_coef: [95x1 double]
Controllability: [1x1 struct]
```

- data.FC.CC.modularity\_Ci is an array of size 1 x ROIs of community structure
- data.FC.CC.modularity\_Q is the modularity
- data.FC.CC.A is the undirected binary adjacency matrix
- data.FC.CC.C is pair-wise cross-correlation coefficient
 

```
>> figure; imagesc(data.FC.CC.C);
>> figure; imagesc(data.FC.CC.A);
```
- data.FC.CC.clustering\_coef is the clustering coefficient

```
>> data.FC.CC.Controllability
```

```
ans =
```

```
    Nd: 93
    drivernodes: [1x93 double]
    Nconfigs: 59
```

- data.FC.CC.Controllability.Nd is the number of driver nodes
- data.FC.CC.Controllability.drivernodes is an array of the identity of driver nodes (ROI numbers)
- data.FC.CC.Controllability.Nconfigs is the total number unique configurations of drivernodes that are possible given the adjacency matrix A

Contents of the other methods for estimating functional connectivity are similar. Briefly,

```
>> data.FC.PC
```

```
ans =
```

```
    modularity_Ci: [1x95 double]
    modularity_Q: 0.2269
    clustering_coef: [95x1 double]
        A: [95x95 logical]
        rho: [95x95 double]
    Controllability: [1x1 struct]
```

- data.FC.PC.rho is a pair-wise partial-correlation matrix.
- data.FC.PC.A is an undirected binary adjacency matrix derived from thresholding on p-values, given user specified alpha-level

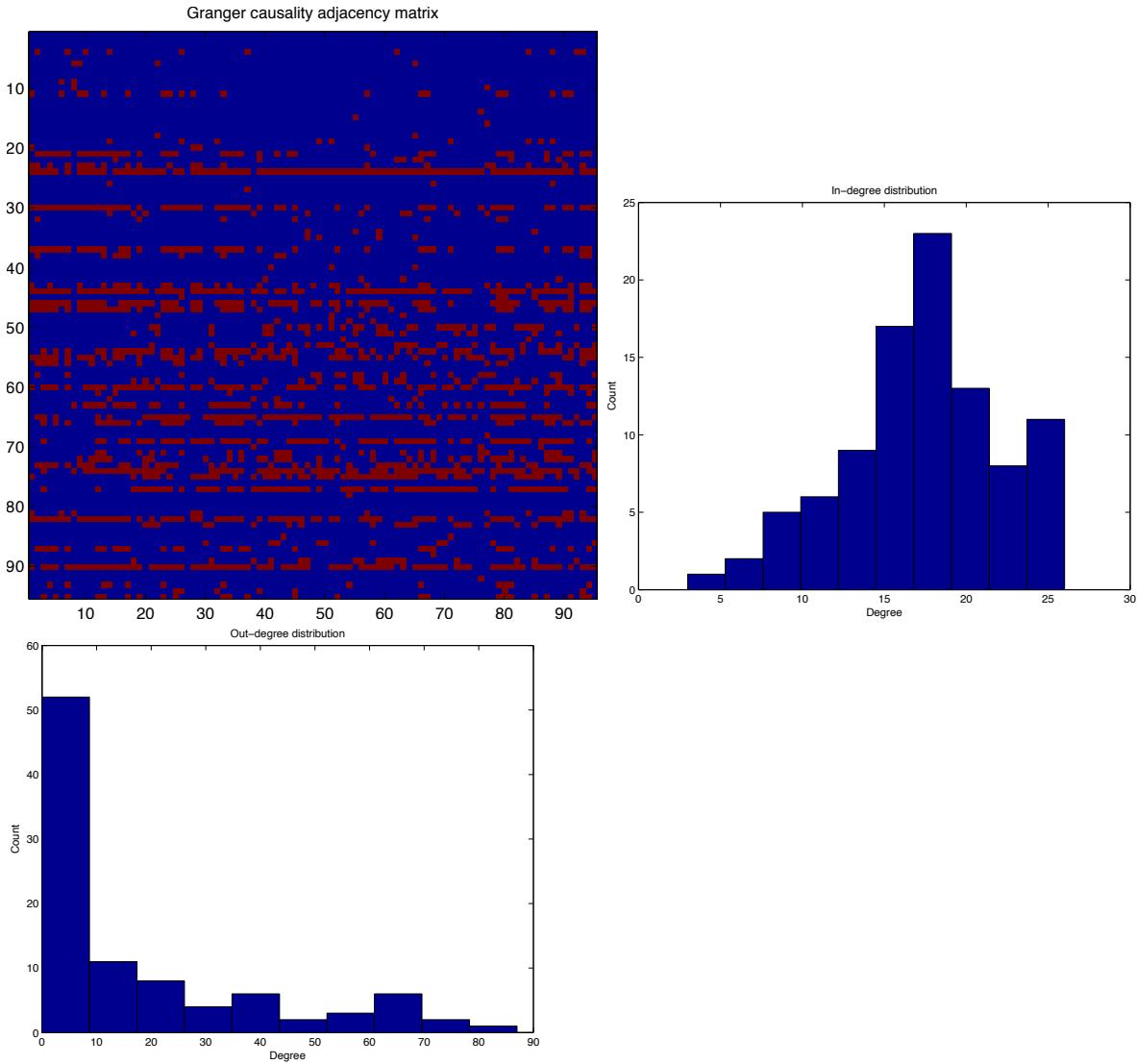
```
>> data.FC.GC
```

```
ans =
```

```
    modularity_Ci: [1x95 double]
    modularity_Q: 0
    clustering_coef: [95x1 double]
        A: [95x95 double]
        Pvals: [95x95 double]
        F: [95x95 double]
    Controllability: [1x1 struct]
```

- data.FC.GC.F is a pair-wise matrix of the F-test statistic for testing significant interaction between (i,j) using the Granger causality method
- data.FC.GC.Pvals are the p-values for testing that row i Granger causes column j
- data.FC.GC.A is a directed binary adjacency matrix – row i is functionally connected (Granger causes) column j. To view the adjacency matrix and degree distribution,

```
>> figure; imagesc(data.FC.GC.A); title('Granger causality
adjacency matrix'); axis square;
>> figure; hist(sum(data.FC.GC.A,1)); title('In-degree
distribution'); xlabel('Degree'); ylabel('Count');
>> figure; hist(sum(data.FC.GC.A,2)); title('Out-degree
distribution'); xlabel('Degree'); ylabel('Count');
```



```
>> data.FC.TE
```

```
ans =
```

```

modularity_Ci: [1x95 double]
modularity_Q: 0.0895
peakTE: [95x95 double]
CI: [95x95 double]
clustering_coef: [95x1 double]
Controllability: [1x1 struct]
```

- `data.FC.TE.peakTE` is a pair-wise transfer entropy matrix, where each entry is the maximum transfer entropy over 0 to max time lag (specified by user).
- `dataFC.TE.CI` is the coincidence index, roughly thought of as estimating the ratio: signal/(signal+background). Please see (Ito, Hansen et al. 2011) for more details.

### Single-cell descriptors

For each neuron, the kinetics of calcium transients (amplitude, rise time, fall time) are computed. And the average across all events in a given neuron is reported along with 95% confidence intervals.

- `data.DF` is an  $N \times 1$  array, where entries are the average amplitude (as  $\Delta F/F$ ) per neuron.
- `data.CV` is an  $N \times 1$  array, whose entries are the coefficient of variation in amplitude of calcium transients
- `data.rise_time` is an  $N \times 1$  cell array. Each cell is another array of length  $N_{\text{spikes}} \times 1$ . Entries are the rise time for each transient. For example, in the screenshot below, ROI 1 has 16 events and the rise time for each event is listed.

```
>> data.rise_time{1}

ans =

    Columns 1 through 9

    0.1082    0.1278    0.1082    0.1475    0.0783    0.1371    0.1770    0.1475    0.1180

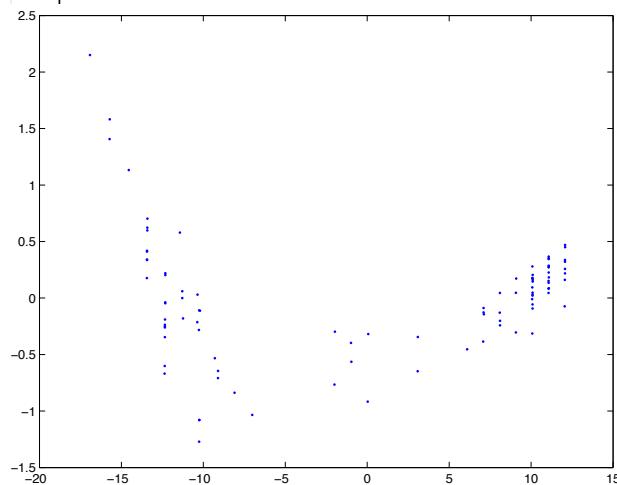
    Columns 10 through 16

    0.0885    0.0688    0.1770    0.0787    0.1180    0.1851    0.1180
```

- `data.fall_time` is similar to `data.rise_time`. Entries are event fall times.
- `data.OP` is an  $N \times 1$  array whose entries are the average oscillation period per neuron, defined as the average time between events.

For example, you may wish to explore if there are groupings of neurons based on the kinetics of their activity using principle component analysis. First, create a matrix `X` of all the single-cell measurements: mean amplitude, coefficient of variation, mean rise time, mean fall time, mean oscillation period, and number of events. Then, apply PCA to project the 6-dimensional dataset into 2-d PCA space and plot the result:

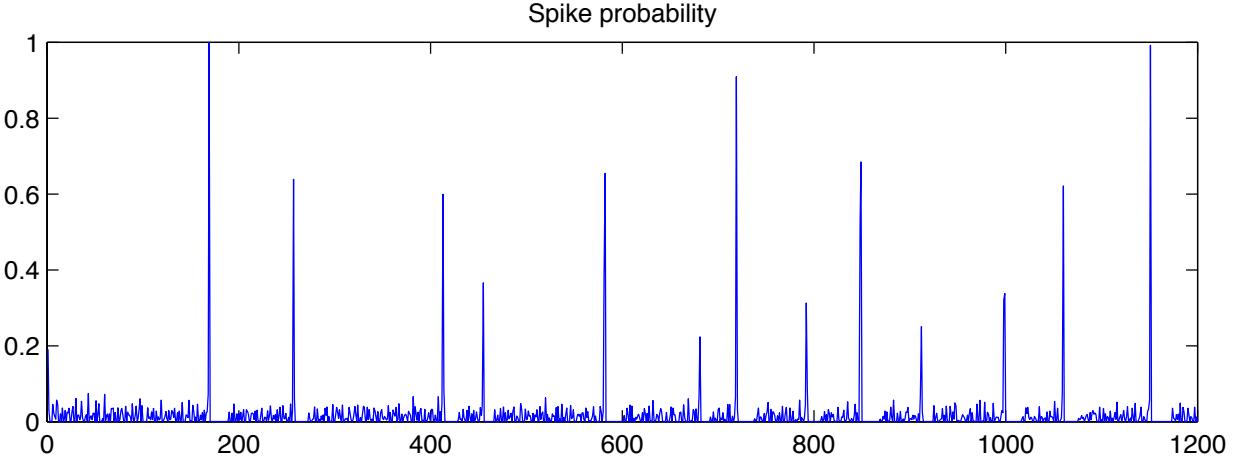
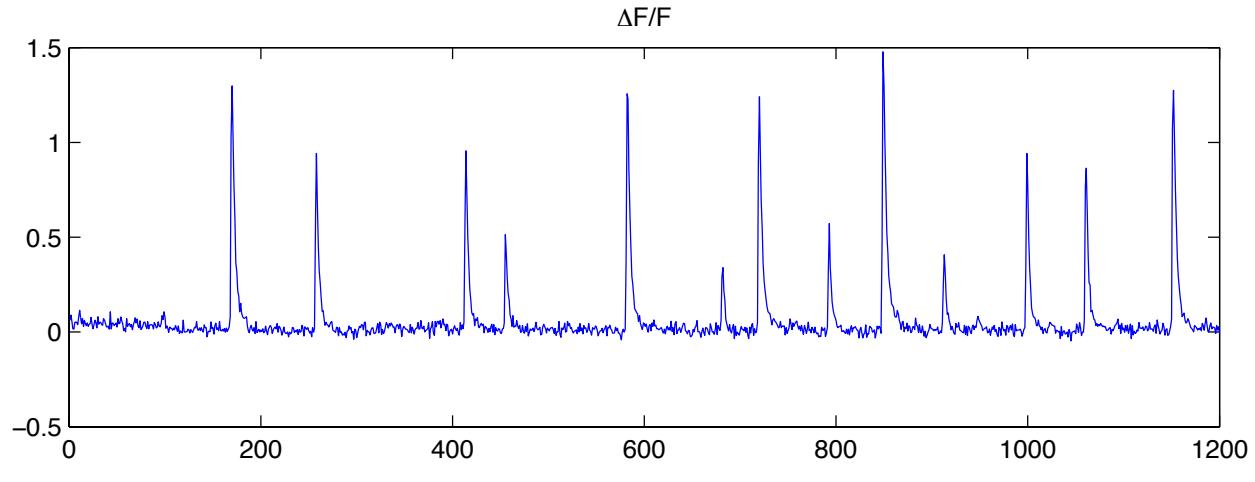
```
>> X = [data.DF, data.CV, cellfun(@mean,data.rise_time), cellfun(@mean,data.fall_time),...
data.OP, cellfun(@length,data.rise_time)];
>> [coef,score] = princomp(X);
>> figure; plot(score(:,1),score(:,2),'.')
```



### Spike probability

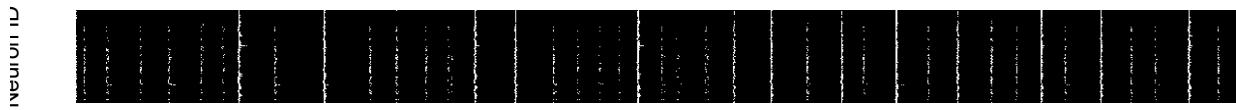
Raw fluorescence trace is converted to  $\Delta F/F$  and underlying spike probability is determined using the fast non-negative deconvolution algorithm described in (Vogelstein, Packer et al. 2010). Results are stored in data.foopsi. To view the fluorescence trace and spike probability for neuron #4:

```
>> figure; subplot(2,1,1), plot(data.dF_cell(4,:));
title('\Delta F/F');
>> subplot(2,1,2), plot(data.foopsi(4,:)); title('Spike
probability');
```



The spike probability can be thresholded to generate binary activity map. By default, we use 3 standard deviations as the threshold.

```
>> thr = std(data.foopsi,[],2);
BinaryActivity = zeros(size(data.foopsi));
for i=1:size(data.foopsi,1)
BinaryActivity(i,:) = data.foopsi(i,:)>(3*thr(i));
end
figure; imshow(BinaryActivity); xlabel('Frame #'); ylabel('Neuron ID');
```



Frame #

### Network ensembles

Statistically significant co-activation of groups of neurons in a given frame is defined as a network ensemble. See (Miller, Ayzenshtat et al. 2014) for more details.

```
>> data.NetworkEnsemble
```

```
ans =
```

```
ensembles_per_second: 0.7750
ensemble_frames: [1x93 double]
Nensembles: 93
CoreEnsembles: {1x14 cell}
CorrelatedEnsembles: [93x93 double]
```

- `data.NetworkEnsemble.ensembles_per_second` is the average number of ensembles per second
- `data.NetworkEnsemble.Nensembles` is the total number of network ensembles, i.e. total number of frames where there was a non-random activation of a group of neurons. The identify of these frames is listed in `data.NetworkEnsemble.ensemble_frames`
- `data.NetworkEnsemble.CoreEnsembles` is a cell array of size 1xN, where N is the number of core ensembles defined as unique group of neurons that are co-activated across all ensembles. Each cell array is an index of the ROIs that make up that core ensemble.
- `data.NetworkEnsemble.CorrelatedEnsembles` is a pair-wise similarity matrix between different network ensembles.

### How to cite:

Please cite the main FluoroSNNAP manuscript as:

Patel TP, Man K, Firestein B, Meaney DF (2015). "Automated quantification of neuronal networks and single-cell calcium dynamics using calcium imaging". J Neurosci Methods

In addition, please cite the following papers if you use:

- ICA based segmentation, cite: (Mukamel, Nimmerjahn et al. 2009)
- Spike probability estimation using fast non-negative deconvolution, cite: (Vogelstein, Packer et al. 2010)
- Functional connectivity using Granger causality, cite: (Barnett and Seth 2014)
- Functional connectivity using Transfer entropy, cite: (Ito, Hansen et al. 2011)

## References:

- Barnett, L. and A. K. Seth (2014). "The MVGC multivariate Granger causality toolbox: a new approach to Granger-causal inference." J Neurosci Methods **223**: 50-68.
- Ito, S., M. E. Hansen, R. Heiland, A. Lumsdaine, A. M. Litke and J. M. Beggs (2011). "Extending transfer entropy improves identification of effective connectivity in a spiking cortical network model." PLoS One **6**(11): e27431.
- Kang, W. H., W. Cao, O. Graudejus, T. Patel, S. Wagner, D. Meaney and B. Morrison Iii, 3rd (2014). "Alterations in Hippocampal Network Activity after In Vitro Traumatic Brain Injury." J Neurotrauma.
- Miller, J. E., I. Ayzenshtat, L. Carrillo-Reid and R. Yuste (2014). "Visual stimuli recruit intrinsically generated cortical ensembles." Proc Natl Acad Sci U S A **111**(38): E4053-4061.
- Mukamel, E. A., A. Nimmerjahn and M. J. Schnitzer (2009). "Automated analysis of cellular signals from large-scale calcium imaging data." Neuron **63**(6): 747-760.
- Patel, T. P., S. C. Ventre and D. F. Meaney (2012). "Dynamic changes in neural circuit topology following mild mechanical injury in vitro." Ann Biomed Eng **40**(1): 23-36.
- Vogelstein, J. T., A. M. Packer, T. A. Machado, T. Sippy, B. Babadi, R. Yuste and L. Paninski (2010). "Fast nonnegative deconvolution for spike train inference from population calcium imaging." J Neurophysiol **104**(6): 3691-3704.
- Yuan, Z., C. Zhao, Z. Di, W. X. Wang and Y. C. Lai (2013). "Exact controllability of complex networks." Nat Commun **4**: 2447.