Modelling the detection chamber

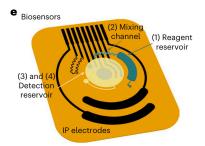


Figure 1: Inflastat chip (Tu et al. 2023).

CRP-dAb and cAb

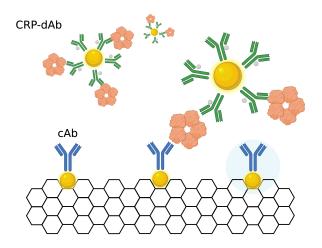


Figure 2: CRP-detector antibody and capture antibodies.

CRP-dAb concentration in the detection reservoir (Part 1)

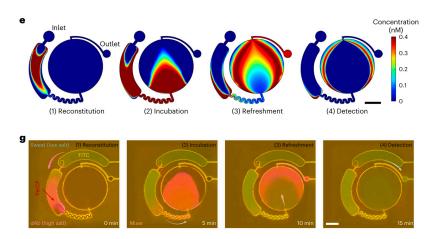


Figure 3: Numerical simulation of CRP-dAb concentrations without cAb and fluorescence flow test without dAb (Tu et al. 2023).

CRP-dAb concentration in the detection reservoir (Part 2)

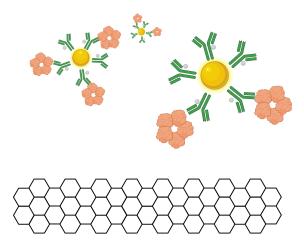


Figure 4: System studied in the literature through numerical simulation and fluorescence flow test.

Reaction-diffusion-advection numerical simulations

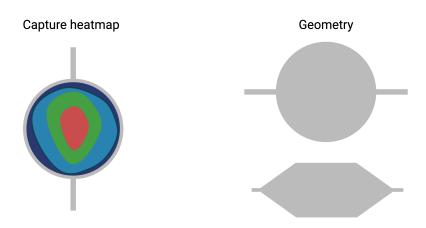


Figure 5: Objective of numerical simulations.

Fluid dynamics

- ► The velocity field v has no dependence on concentration because sweat is dilute.
- ► Solve for v using the Navier-Stokes equation for incompressible flow and the continuity equation.

$$\begin{split} \rho(\partial_t \mathbf{v} + (\mathbf{v} \cdot \nabla) \mathbf{v}) &= -\nabla \mathbf{p} + \mu \nabla^2 \mathbf{v} \\ \nabla \cdot \mathbf{v} &= \mathbf{0} \end{split}$$

Non-dimensionalized Navier Stokes

Assume steady state. Parameters aggregate into the Reynolds number.

$$\frac{\rho UL}{\mu}(\tilde{\mathbf{v}}\cdot\tilde{\nabla})\tilde{\mathbf{v}} = -\frac{\Pi L}{U\mu}\tilde{\nabla}\tilde{\mathbf{p}} + \tilde{\nabla}^2\tilde{\mathbf{v}}$$

Use the viscous pressure scale

$$\begin{split} \Pi &= \frac{U\mu}{L} \\ \mathrm{Re}(\tilde{\mathbf{v}}\cdot\tilde{\nabla})\tilde{\mathbf{v}} &= -\tilde{\nabla}\tilde{\mathbf{p}} + \tilde{\nabla}^2\tilde{\mathbf{v}} \end{split}$$

Creeping (Stokes) flow

Using sweat volumetric flowrate, the mean chamber chord length, and the width of the PET layer $(\dot{V},\ \bar{C},\ W)$.

$$Re = \frac{\rho UL}{\mu} = \frac{10^3 \cdot 10^{-4} \cdot 10^{-4}}{10^{-3}} = 10^{-2} \ll 1$$

► Fluid flow in the microfluidic channel is in the Stokes flow regime.

$$-\tilde{\nabla}\tilde{\mathbf{p}} + \tilde{\nabla}^2\tilde{\mathbf{v}} = \mathbf{0}$$

▶ Solve alongside the non-dimensionalized continuity equation.

$$\tilde{\nabla} \cdot \tilde{\mathbf{v}} = \mathbf{0}$$

▶ The Poisson pressure equation

$$\frac{\Pi}{L^2}\tilde{\nabla}^2\tilde{\mathbf{p}} = -\rho \frac{U^2}{L^2}(\tilde{\nabla}\cdot\tilde{\mathbf{v}})^2$$

$$\tilde{\nabla}^2 \tilde{\mathbf{p}} = -\frac{\rho U L}{u} (\tilde{\nabla} \cdot \tilde{\mathbf{v}})^2 + 2 \tilde{\mathbf{v}} + \tilde$$

Reaction-diffusion-advection dynamics (Part 1)

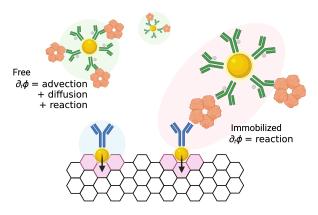


Figure 6: Mobility of different species.

Reaction-diffusion-advection dynamics (Part 2)

$$\begin{split} \partial_t \phi_p(\mathbf{x},t) &= D \nabla^2 \phi_p - \mathbf{v} \cdot \nabla \phi_p - \mathbf{R} \\ \partial_t \phi_a(\mathbf{x},t) &= - \mathbf{R} \\ \partial_t \phi_c(\mathbf{x},t) &= \mathbf{R} \\ \mathbf{R}(\phi_p,\phi_a,\phi_c) &= k_f(T) \phi_p \phi_a - k_r(T) \phi_c \end{split}$$

Non-dimensionalized reaction-diffusion-advection

▶ Parameters aggregate into two time scales.

$$\begin{split} \partial_{\tilde{t}}\tilde{\phi}_{p} &= \frac{\tau D}{L^{2}}\tilde{\nabla}^{2}\tilde{\phi}_{p} - \frac{\tau U}{L}\tilde{\mathbf{v}}\cdot\tilde{\nabla}\tilde{\phi}_{p} - \tilde{\mathbf{R}}\\ \partial_{\tilde{t}}\tilde{\phi}_{a} &= -\tilde{\mathbf{R}} \quad \text{and} \quad \partial_{\tilde{t}}\tilde{\phi}_{c} = \tilde{\mathbf{R}}\\ \tilde{\mathbf{R}} &= \tilde{k_{f}}(T)\tilde{\phi}_{p}\tilde{\phi}_{a} - \tilde{k_{r}}(T)\tilde{\phi}_{c} \end{split}$$

▶ The Peclet number compares diffusion and advection contribution.

$$Pe = \frac{\tau_{\text{diff}}}{\tau_{\text{adv}}} = \frac{L^2/D}{L/U} = \frac{LU}{D} = \frac{(10^{-4})(10^{-4})}{(10^{-12})} = 10^4$$

Advection dominates the flow. Use $\tau = \tau_{\rm adv} = \frac{L}{H}$.

$$\partial_{\tilde{t}}\tilde{\phi_p} = \frac{1}{\mathrm{Pe}}\tilde{\nabla^2}\tilde{\phi_p} - \tilde{\mathbf{v}}\cdot\tilde{\nabla}\tilde{\phi_p} - \tilde{\mathbf{R}}$$

$$\partial_{\tilde{t}}\tilde{\phi}_p = -\tilde{\mathbf{v}}\cdot\tilde{\nabla}\tilde{\phi}_p - \tilde{\mathbf{R}}_{\text{projection}}$$