

Beyond Workload: Paving the Road for the Next Generation of Implicit Prefrontal Cortex Based Brain-Computer Interfaces

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Motivation

- ▶ Expanding bandwidth of communication between human and machine
- ▶ Brain!
- ▶ Implicit Interfaces
- ▶ Implicit Brain-Computer Interfaces (BCIs)
 - ▶ Functional Near-Infrared Spectroscopy (fNIRS)
 - ▶ Electroencephalography (EEG)
- ▶ Prefrontal cortex (PFC)
- ▶ How can we expand the current state-of-the-art in implicit BCI using fNIRS/EEG measuring the PFC?

Contributions

- ▶ Multiple user studies focusing on lesser-explored aspects of PFC function towards real-time interfaces based on classification of more nuanced user states
- ▶ Contributions in this direction with both fNIRS and low-cost EEG
- ▶ Targeted opportunities for future work
- ▶ Analytical framework for straightforward analysis of the fNIRS signal
- ▶ Applied BCI within the context of Human-Sensor-Computer interaction

Outline

- ▶ Background (15m)
- ▶ Projects (20m)
 - ▶ Project I: two proof-of-concept fNIRS studies
 - ▶ Episodic memory for realtime fNIRS-based BCI
 - ▶ Complex decision-making during LLM use
 - ▶ Project II: Applied user study: brain-network based implicit BCI
 - ▶ Project III: Two proof-of-concept low-cost EEG studies
 - ▶ Neural correlates of chess move quality
 - ▶ Cross-task classification
- ▶ Conclusion (5m)
- ▶ Human-Sensor-Computer Interaction (HSCI) (5m)

Background

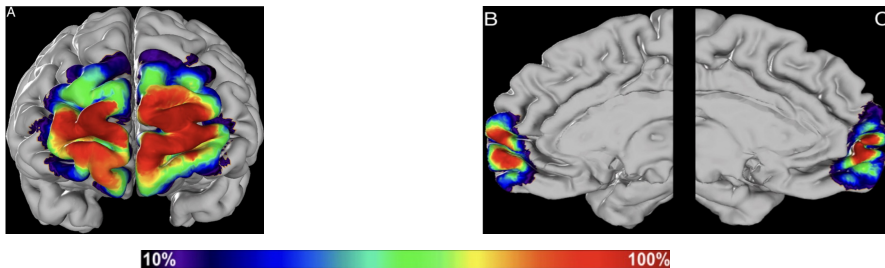
Brain-In-Action

- ▶ The work in this dissertation explores the nuances of neural state differentiation in conditions stepping towards real-world applications
- ▶ Important to consider the complexities of “real-world” neurocognitive tasks
 - ▶ Differences in characteristics of the measurement devices used
 - ▶ fNIRS vs. EEG vs. fMRI, etc.
 - ▶ Differences between individual devices within a given domain (e.g. fNIRS)
 - ▶ Extracerebral noise introduced in applied tasks
 - ▶ Participant movements
 - ▶ Environmental factors
- ▶ Subtlety of neural responses during real-world tasks

Background

Prefrontal Cortex

- **“The anterior prefrontal cortex (aPFC), or Brodmann area 10, is one of the least well understood regions of the human brain.”** (Ramnani and Owen, 2004)



Cytoarchitectonic probability maps of the lateral (left image) and medial (right images) aspects of the PFC Bludau et al. (2014). Reprinted with permission from Elsevier.

Background

Lateral PFC

Lateral aspect of the PFC has been shown to activate based on a wide variety of cognitive tasks

- ▶ **Problem-solving, planning, reasoning, working memory, and cognitive flexibility** for creative processing and thinking (Bunce et al., 2011; Koechlin et al., 1999; Ramnani and Owen, 2004; Barbey et al., 2013; Bludau et al., 2014; Dietrich, 2004; Shah et al., 2013)
- ▶ **Episodic memory** tasks (Bludau et al., 2014; Gilbert et al., 2006)
 - ▶ Episodic memory: recollection of personal past experiences; characterized by a distinct sense of reliving events from one's own history (Tulving, 1989)
- ▶ In terms of networks of brain activity, IPFC activation has been known to be part of the **Task-Positive Network (TPN)**, which increases in relation to cognitive demand (Basten et al., 2013)

Background

Medial PFC

The medial aspect has been shown to activate most commonly during emotion and social cognition (Eickhoff et al., 2016)

- ▶ **Social processing** (Amodio and Frith, 2006; Mitchell, 2009), **processing of uncertainty** (Bzdok et al., 2013), **social cognitive processes** related to theory of mind (Spreng and Grady, 2010; Spreng et al., 2009), **moral reasoning** (Bzdok et al., 2012), **“nonsocial” semantic processing** (Binder et al., 2009), and **autobiographical memory retrieval** (Spreng et al., 2009; Chen et al., 2017)
- ▶ In terms of networks of brain activity, mPFC activation has been known to be part of the **Default-Mode Network (DMN)** which activates during to social cognition, mind wandering, and self-referential processes such as thinking about the past or future (Akbar et al., 2022), and which deactivates during cognitive demand (Basten et al., 2013)

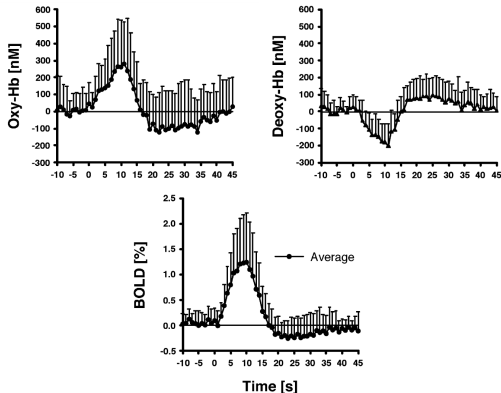
Background

fNIRS

- ▶ fNIRS uses diffuse optical imaging of near-infrared light to non-invasively measure changes in oxygenated $\Delta[\text{HbO}]$ and deoxygenated $\Delta[\text{HbR}]$ hemoglobin concentrations in the human brain (Fantini and Sassaroli, 2020)
- ▶ Light pulses of different wavelengths are sent through the forehead; detectors capture the amount of light which returns, and the Modified Beer-Lambert Law is used to calculate hemoglobin concentrations (Sassaroli et al., 2012)
- ▶ Although the depth of fNIRS is limited to the outer regions of the cortex, relatively shallow in comparison with fMRI, the precision of the localization of the measurement is approximately 2-3cm (Pinti et al., 2020), much higher than that of EEG (Nicolas-Alonso and Gomez-Gil, 2012)

Background

fNIRS: from blood to brain ($\Delta[\text{HbD}]$)



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- ▶ The optimal method of inferring neural activation from the metrics of $\Delta[\text{HbO}]$ and $\Delta[\text{HbR}]$ is still an open question (Kreplin and Fairclough, 2013)
- ▶ General principle is Hemodynamic response, where an increase in $\Delta[\text{HbO}]$ and decrease in $\Delta[\text{HbR}]$ is observed following neural activity
- ▶ In fMRI, the Blood-Oxygen-Level-Dependent (BOLD) signal measures magnetic perturbations in the vasculature in response to oxygen consumption associated with neural activity
- ▶ $\Delta[\text{HbD}] = \Delta[\text{HbO}] - \Delta[\text{HbR}]$

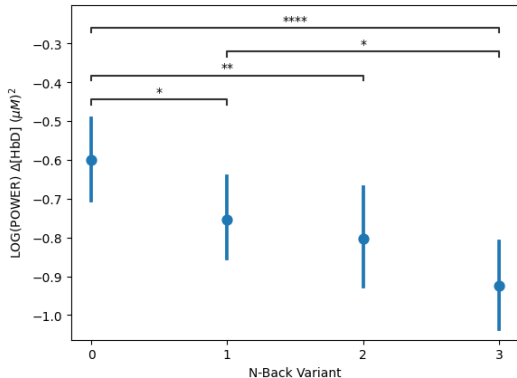
Background

fNIRS: VLF Oscillations

- ▶ Very Low Frequency (VLF) band: 0.07 Hz - 0.02 Hz [14.3 - 50 seconds]
- ▶ Previous findings:
 - ▶ Decrease in VLF band relates to task-based cortical activation
 - ▶ Observed in visual cortex (Obrig et al., 2000)
 - ▶ Observed in prefrontal cortex (Vermeij et al., 2014)
- ▶ Comprehensive understanding of the physiological mechanisms underlying this VLF correspondence to neural activity remains incomplete (Sassaroli et al., 2012)
- ▶ Prevailing theoretical basis for the physiological underpinning of these oscillations relates to cerebral autoregulation (CA), which is the body's ability to maintain consistent blood supply to the brain (Andersen et al., 2018)

Background

VLF Oscillations in Practice



- ▶ Tufts Mental Workload Dataset (Huang et al., 2021)
- ▶ 68 Participants doing N-Back
- ▶ As N-Back workload increases, corresponding decrease in VLF band-power of the left lateral PFC
- ▶ No significant differences in closest levels of N-Back outside of 0-back (1-2, 2-3)

Background

fNIRS in BCI

- ▶ Many PFC-based fNIRS studies approximate mental workload, in both **real-time tasks** (Girouard et al., 2013; Afergan et al., 2014b, 2015, 2014a; Hirshfield et al., 2011, 2009b,a) and during **offline brain state classification** (Power et al., 2010; Strait, 2014; Ayaz et al., 2012)
- ▶ Most studies train models on N-Back tasks, then apply them to modulate difficulty in separate tasks (Afergan et al., 2014b; Shibata et al., 2019; Strait, 2014; Yuksel et al., 2016; Afergan et al., 2015, 2014a)

Background

fNIRS in BCI: Applications

- ▶ Workload-based interfaces have been applied to
 - ▶ Game difficulty identification (Girouard et al., 2009)
 - ▶ Interface optimization for user state (Afergan et al., 2014b; Strait, 2014)
 - ▶ Intelligent interruption timing (Afergan et al., 2015; Shibata et al., 2019)
 - ▶ Adaptive learning environments (Yuksel et al., 2016)
 - ▶ Multitasking identification for target selection (Afergan et al., 2014a)
 - ▶ Usability testing (Hirshfield et al., 2011)
 - ▶ Operator fatigue and cognitive overload monitoring in aviation (Ayaz et al., 2012)
- ▶ Additional PFC-based fNIRS applications include
 - ▶ Consumer product preference evaluation (Luu and Chau, 2008)
 - ▶ Emotional valence during music listening (Moghimi et al., 2012)

Background

fNIRS in BCI: this work

- ▶ Notably, no fNIRS-based BCIs leveraging episodic memory
- ▶ Also, although Hincks (2019) introduced the notion of DMN/TPN-based interfaces, this is likewise underexplored in the current literature

Background

EEG

- ▶ EEG directly measures electrical activity of neuronal activation, with excellent temporal resolution (milliseconds) compared to fNIRS's hemodynamic response-based measurements (Zhang et al., 2023; Gable et al., 2022; Luck, 2014)
- ▶ EEG suffers from limited spatial resolution (Brienza and Mecarelli, 2019)
- ▶ EEG signals are commonly analyzed through rhythmic activity across multiple frequency bands (δ : 1-4 Hz, θ : 4-8 Hz, α : 8-12 Hz, β : 13-30 Hz, and γ : 30-150 Hz), which roughly correspond to distinct biological processes at the cellular level (Buzsaki, 2006; Cohen, 2014)

Background

(Low-cost) Prefrontal EEG in BCI

- ▶ Frequency-domain features of prefrontal EEG have been widely used in BCI applications to distinguish between various cognitive and emotional states, including **cognitive load** (Chikhi et al., 2022; Roy et al., 2016), **concentration vs. rest** (Kang et al., 2015), **emotional states** (Balconi et al., 2015), and **drowsiness** (Jang et al., 2013)
- ▶ Consumer-grade, low-cost EEG devices from companies like InteraXon, OpenBCI, NeuroSky, and Emotiv have emerged as viable alternatives to expensive traditional systems, offering accessibility for real-world applications despite limitations in spatial resolution and signal fidelity (Vos et al., 2025; Lee et al., 2024)
- ▶ Applications have been demonstrated in **stress detection**, **drowsiness monitoring**, **emotion classification**, and **mental workload** (Vashisht and Sharma, 2024; LaRocco et al., 2020; Girardi et al., 2017; So et al., 2017)

- ▶ Typically, EEG-based BCIs focus on leveraging a “vertical” vector of state-classification based on a single state: e.g. levels of cognitive load, negative vs. positive emotions, etc.
- ▶ The EEG work done in this dissertation attempts to abstract more subtle state-information with a low-cost EEG system
- ▶ Core hypothesis is that complex combinations of spectral features can express nuanced neurophysiological states

Background

Linear Mixed Effects Regression

Let us consider the simplest implementation of a Linear Mixed Effects Model (LMM) (Gomes, 2022)

$$Y_{ij} = \beta_0 + \sum_{k=1}^n \beta_k X_{ki} + \alpha_j + \epsilon_{ij} \quad (1)$$

- ▶ The LMM equation extends the original Linear Model by adding a new term α_j
- ▶ This represents a unique intercept for each level of the grouping category j
- ▶ For example, provided individual participant identification as a grouping factor, this extension explicitly models separate intercepts per participant
- ▶ Also possible to model nested random intercepts, and random slopes

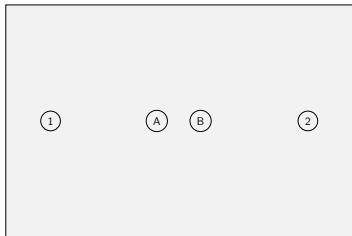
Background

Machine Learning Techniques

- ▶ Leave-One-Out Cross-Validation
- ▶ KNN, LDA, QDA, ANN, SVM, RF, SVM, SVM with RBF kernel
 - ▶ Default hyperparameters
- ▶ fNIRS
 - ▶ Transform 20-second windows of data
 - ▶ Mean, standard deviation, slope of linear regression, skew
 - ▶ Apply transformations individually across probe positions [e.g. L, R], wavelengths [HbO, HbR], and measurements [I , ϕ]
- ▶ EEG
 - ▶ Transform frequency domain features from 1-second windows
- ▶ Different models performed well for different people; report best scores per-person
- ▶ Metric: Macro-F1 (harmonic mean of precision and recall)

- ▶ Project I: two proof-of-concept fNIRS studies
 - ▶ Episodic memory for real-time fNIRS-based BCI
 - ▶ Complex decision-making with and without LLM use

- ▶ Two optical probes, 1 each over the L and R PFC
- ▶ Dual-slope method to remove extracerebral artifacts (Blaney et al., 2020)
- ▶ Resulting measures are $[DSI, DS\phi] \times [HbO, HbR] \times [L, R]$



(a) fNIRS probe configuration. 1/2 are the source locations, and A/B are the detectors.

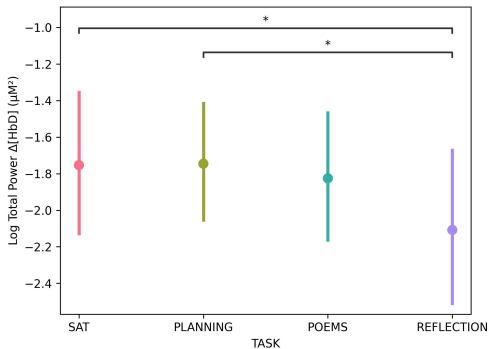


- ▶ Effects of using Large Language Models (LLMs) on human users
- ▶ Multiple metrics: fNIRS, Empatica E4, NASA-TLX, enjoyment, correctness
- ▶ Analyzed participant activity with and without LLM-help across multiple tasks
- ▶ Tasks were organized across a *gradient of subjectivity*
 - ▶ Highly structured and objective tasks were intended to be “easy” for the LLM
 - ▶ SAT reading comprehension
 - ▶ Event planning
 - ▶ Open-ended and subjective tasks were intended to be “difficult” for the LLM
 - ▶ Poetry writing
 - ▶ Personal reflection on favorite album/movie
- ▶ Endpoints of the gradient had basis in neural function: the subjective tasks were intended to activate default mode network and episodic memory
- ▶ Are neural states differentiable across tasks, and/or based on Copilot use?

- ▶ 15 participants (20 run)
- ▶ Each participant did the four task types in randomized order
- ▶ For each task, one sub-task was done with Copilot, and the other without Copilot
- ▶ Each sub-task was 6 minutes
- ▶ Sub-tasks within each task type were equally difficult
- ▶ Following each task type, participants filled out NASA-TLX and questionnaires asking about their experience

Project I

Study I: Results



- ▶ Increase in R PFC activity in the episodic memory (REFLECTION) task as compared to the two objective tasks (SAT, PLANNING)
 - ▶ Confirms work in neuroscience literature Nölde et al. (1998); Tulving et al. (1994), but in a more applied context
- ▶ No statistical differences found in PFC activation as a consequence of Copilot use
- ▶ Machine Learning
 - ▶ REFLECTION vs. SAT (61%)
 - ▶ NO-AI REFLECTION vs. NO-AI SAT (71%)
 - ▶ AI SAT vs. NO-AI SAT (69%)

- ▶ Episodic memory in comparison to reading comprehension is a viable vector for real-time implicit BCI work with fNIRS using the PFC
- ▶ LLM-use effects the fNIRS signal during reading comprehension tasks such that ML methods can be used to develop real-time interfaces with the data
 - ▶ The subtlety of this effect likely requires more participants to quantify with VLF analysis

Project I

Study II: Copilot for MS365



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- ▶ Similar to Study II, but with two complex decision-making tasks
- ▶ Copilot for MS365
- ▶ Metrics: fNIRS, NASA-TLX, valence-arousal, correctness
- ▶ Longer (25m) task design
- ▶ Given longer tasks, Copilot order was added as a between-subjects factor

Project I

Study II: Task Paradigm



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- ▶ 30 participants (ran 37)
- ▶ Each participant performed the tasks as
 - ▶ 1-minute rest
 - ▶ 25 minute task
 - ▶ NASA-TLX and valence-arousal forms

Project I

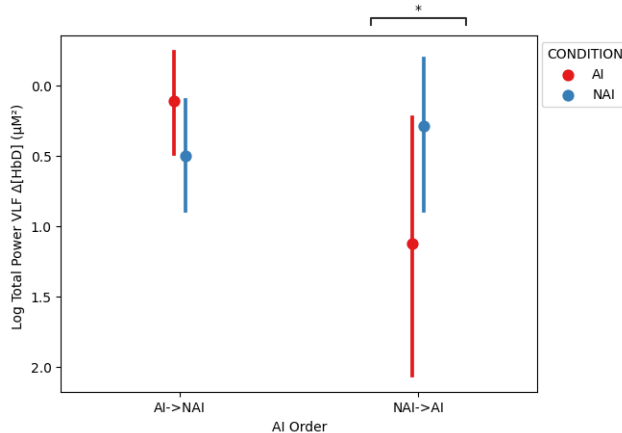
Study II Results: Neural Activity



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- ▶ R PFC DSI (y-axis inverted)
- ▶ Significant interaction effect of ORDER \times CONDITION
- ▶ Decrease in R PFC during Copilot task when experienced second
- ▶ Decrease in L PFC for both levels of ORDER during the second task

Project I

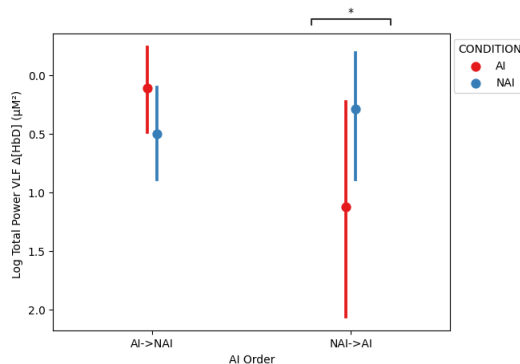
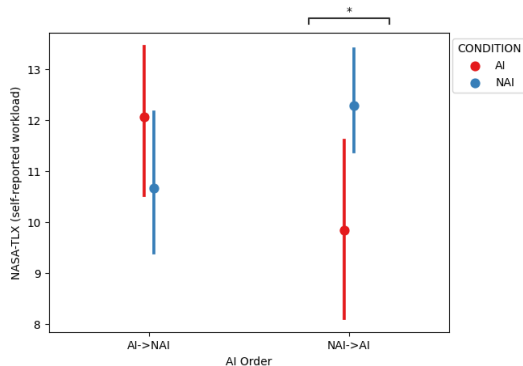
Study II Results: NASA-TLX and fNIRS



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- ▶ Best overall model: Random Forest (50.5% F1-score)
- ▶ Best per-participant average Macro F1: 56%
- ▶ Not currently viable for realtime BCI applications, although more complex ML paradigms might help classification



- ▶ Decrease in L PFC during second task signifies decrease in cognitive load due to understanding task
- ▶ Decrease in R PFC when using AI tool after experiencing the task
 - ▶ Goel (2019) has posited R PFC function to interrelate with indeterminacy tolerance, specifically in the context of an information representation system
 - ▶ This may therefore relate to a relaxation of the processes which underlie hesitance to settle on inferences from knowledge representations
- ▶ Distinction in types of workload changes as reflected in the neural data highlights a key gap in the approximation capable by NASA-TLX
- ▶ Despite statistical results, applied machine learning results indicate lack of applicability towards real-time implicit BCIs

Project II

Network-Based Implicit BCI



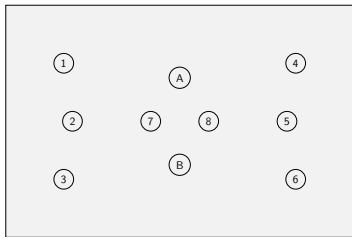
- ▶ This study tests a prototype fNIRS-based BCI leveraging TPN/DMN brain networks
- ▶ The idea follows what is proposed by (Hincks, 2019), and does so within the limitation of measurement only from the PFC
- ▶ This study is a realtime implicit BCI which represents a first prototype implementation of the memory prosthesis introduced by (Rhodes, 1997) and (Lieberman, 1995), wherein the interface presents information moment-to-moment that is appropriate to the user.

Project II

fNIRS Device



- ▶ One optical probe over the L PFC
- ▶ Recursive Least Squares (RLS) adaptive filter used to remove extracerebral artifacts (Klein and Kranczioch, 2019)
- ▶ Resulting measures are $[I] \times [HbO, HbR] \times [\text{probe-detector pair}]$



(a) fNIRS probe configuration. A/B are the detectors; 7/8 are the short sources.



Project II

Task Design



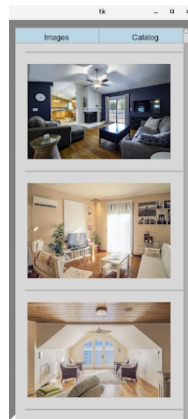
- ▶ After prototyping with 6 participants, we recruited 8 participants for the study
- ▶ Participants were tasked with designing rooms in their home
- ▶ For each of 3 rooms, we split the task up into two phases
 - ▶ Inspiration & Visualization Phase [DMN]
 - ▶ Furniture Selection Phase [TPN]

Project II

Task Design: Inspiration & Visualization [DMN]



- ▶ Participants were shown a sidebar of images
- ▶ Clicking on an image would magnify it
- ▶ Participants were instructed to consider ideas based on their preferences
- ▶ Intended to activate DMN in comparison to Furniture Selection task

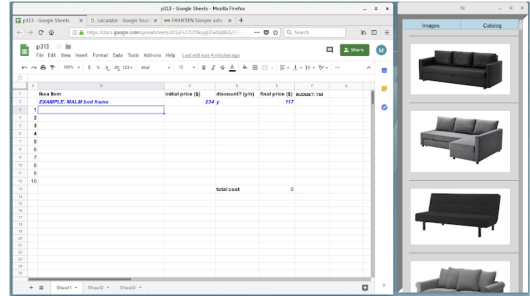


Project II

Task Design: Furniture Selection Phase [TPN]

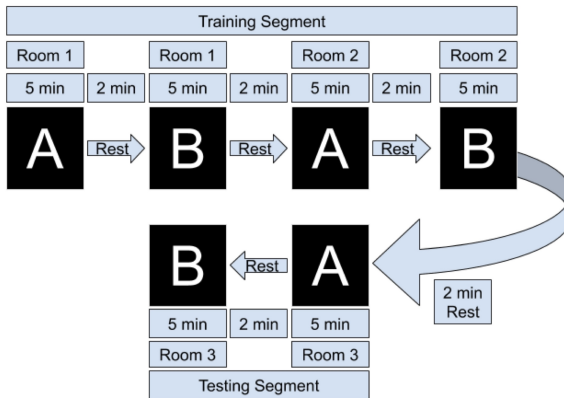


- ▶ Participants were given a spreadsheet and a sidebar with furniture items from the IKEA store
- ▶ Clicking any item opens a link in the browser to the IKEA website with prices and more information
- ▶ They were to keep track of costs
- ▶ Goal: keep total item selection under a given budget
- ▶ Intended to activate TPN in comparison to Inspiration task



Project II

Task Design: Task Structure



Project II

Analysis

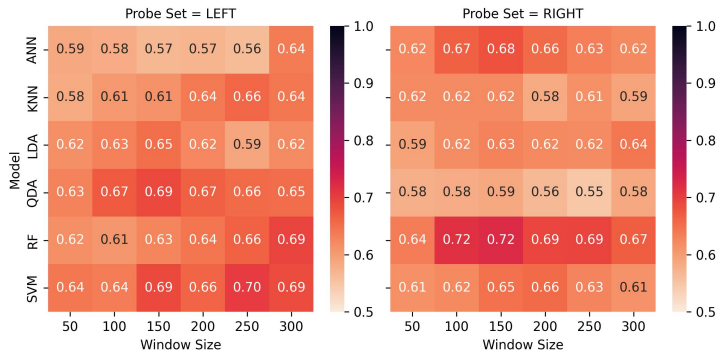


We tried a few things different from the previous work

- ▶ The analytical framework was adapted to also explore classification within the contexts of only the lateral or medial probes of the fNIRS
- ▶ We tried multiple window lengths for classification
- ▶ Performed inner hyperparameter tuning loop during LOO-CV

Project II

Results I



Increases in performance are seen for RF at lower window sizes for the right probes, whereas SVM performed best using the left probes' data at higher window sizes

Project II

Results II



- ▶ Different locations respond better to different classifiers & window sizes
- ▶ Best result per participant, probe set, window size, and model averages to 84%
- ▶ Despite the promising ML results, no significant trends visible in the VLF analysis
- ▶ More work should be done in developing meta-classification approaches, and/or in running similar studies with DMN/TPN-based classification using larger numbers of participants

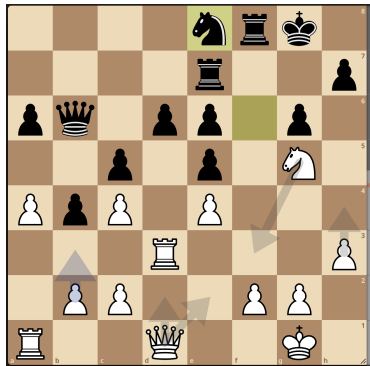
Project III

Project III: Two proof-of-concept low-cost EEG studies

- ▶ Neural correlates of chess move quality
- ▶ Cross-task classification

Study I: Neural correlates of chess move quality

-
- A black Muse 2 EEG headband is shown resting on a light-colored wooden surface. The headband features a black strap with yellow and black diagonal stripes on the right side. The word "muse" is printed in gold on the black strap. The headband is curved, showing its ergonomic design.



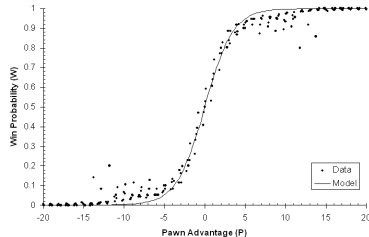
Project III

Study I: Background

What makes a “good” move?

$$W = \frac{1}{1 + 10^{\frac{-p}{4}}} \quad (2)$$

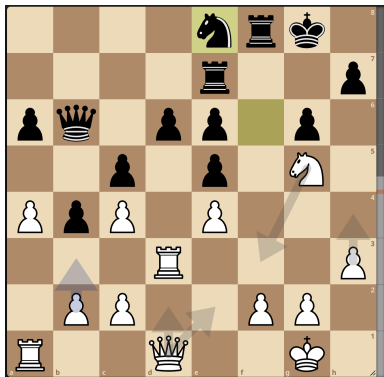
Logistic function defining probability of winning the game W as a function of pawn advantage p (Biswas and Regan, 2015)



Graph demonstrating the relation between p and W with emperical datapoints added (Chess Programming Wiki, 2025)

Project III

Study I: Background - Move Quality Score



A poor move made by White. Pawn advantage p moves from .2 to -2. Thus, $W_{\text{initial}} = 0.53$, and $W_{\text{after}} = 0.24$. Move score is thus $.24 - .53 = -0.29$.

Project III

Study I: Study Design

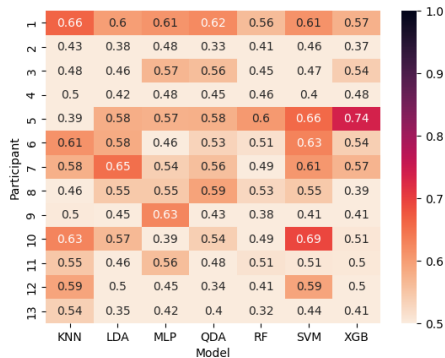
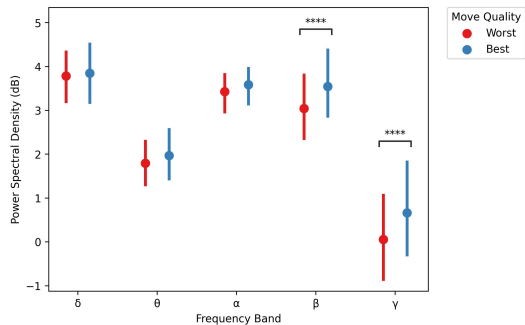


- ▶ 13 participants (17 run)
- ▶ Participants played 5, 5 minute games against a computer opponent
- ▶ They selected the difficulty rating (1-8), and could adjust it by 1 after each game
- ▶ We used the Mind Monitor application to extract frequency domain data

- ▶ For each participant
 - ▶ Split their data into three tertiles, based on move quality
 - ▶ Keep BEST and WORST, drop MIDDLE
- ▶ Results in 694 total moves, 347 per class
- ▶ Average L and R data to increase signal-to-noise ratio

Project III

Study I: Results



Average of best-scores is 60%.

- ▶ Can we distinguish between subtle aspects of human state in applied contexts?
- ▶ This study explores this idea within the context of multiple standard cognitive psychology tasks, as well as an ecological chess puzzles task

Project III

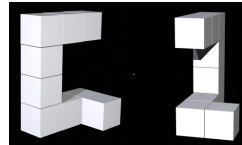
Study II: Tasks and Study Design

- ▶ 9 participants for this sub-study (30 total)
- ▶ Participants did multiple blocks of each task type

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- ▶ N-Back (working memory)
- ▶ Stroop (cognitive inhibition)
- ▶ Mental Rotation (spatial reasoning)
- ▶ Chess puzzles (complex combination)

Stroop task - participant would press 'b'



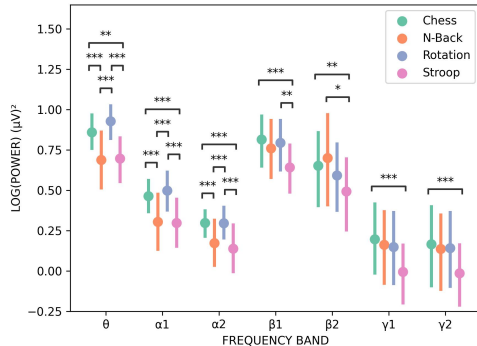
Rotation task - participant would press 'n'

- ▶ Raw data were collected with Muse-JS
- ▶ For each participant
 - ▶ 60Hz notch filter to remove electrical noise
 - ▶ Bandpass filter [.1, 45]Hz
 - ▶ AutoReject algorithm (Jas et al., 2017) used on rest data
 - ▶ Artifact Subspace Reconstruction (Chang et al., 2018) trained on resting data and applied to task data
- ▶ Data epoched to 1s samples
- ▶ Epochs containing values outside the range $[-100 \mu\text{V}, 100 \mu\text{V}]$ were excluded
- ▶ Frequency domain transformation
- ▶ Integrate over standard EEG bands to extract total power
- ▶ Log transform

- ▶ Because of differing sample sizes across tasks and participants, performed grouped and sub-sampled Monte Carlo ML procedure
- ▶ Each Monte Carlo iteration had evenly balanced training and testing samples both within and across participants
- ▶ Grouping based on task block meant that all participants were represented in training and testing data, but temporally autocorrelated samples were not present in both
- ▶ Performed 1k MC iterations; width of the 95% confidence interval converged to less than 1%

Project III

Study II: Results



Task	Precision	Recall	F1	Support
Chess	0.552	0.460	0.499	195
N-Back	0.485	0.425	0.452	195
Rotation	0.493	0.580	0.531	195
Stroop	0.474	0.519	0.494	195
Macro Average	0.501	0.496	0.494	780

With 25% baseline classification accuracy, average is 50%. These results indicate very promising ability to distinguish across classes in real time scenarios.

Conclusion

- ▶ This dissertation has been a breadth-first exploration of classification of more subtle neural states based on electrical and hemodynamic activity measured in the PFC
- ▶ fNIRS-based results indicate that episodic memory and DMN/TPN-based interfaces are viable areas for future real-time implicit BCI
- ▶ Low-cost EEG results indicate that subtle state classification both within the context of chess move quality and across tasks targeting different aspects of human state are possible
- ▶ Side quest reinforcing VLF oscillations as a correlate of neural activation

Human-Sensor-Computer Interaction

- ▶ Neural data is *noisy*, especially in applied contexts
- ▶ Primary sources of “noise” are from physiological artifacts
- ▶ What if some of this “noise” is useful towards human-state classification?
- ▶ We should work harder to
 - ▶ Quantify the utility of sources of extracerebral activity (e.g. eye blinks in EEG, extracerebral hemodynamics in fNIRS)
 - ▶ Embrace the use of such extracerebral activity for HCI
- ▶ Philosophical shifts
 - ▶ Take each sensor “at face value”: EEG measures electrical activity, fNIRS measures light, etc.
 - ▶ Consider self-report and other information as valid “sensors”
- ▶ All of these ideas in combination point to a broader umbrella of study:
Human-Sensor-Computer Interaction

Thank you!

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