

Robust PI Controller Design using Graphical Approach for Blood Pressure Regulation



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Introduction

- During surgeries, to maintain the mean arterial blood pressure, a vasodilating drug is given to lower the blood pressure to control excessive bleeding.
- Its required amount and effects greatly vary on the type of patient, so we need to monitor the effects, too, continuously.
- Such precise drug-delivery systems require a controller to work on the patient response model.
- We will use a Graphical Approach based on Maximum Sensitivity with a PI controller.
- Compare the results of the PI controller to the FOPID controller of the reference paper.

Basic Control System

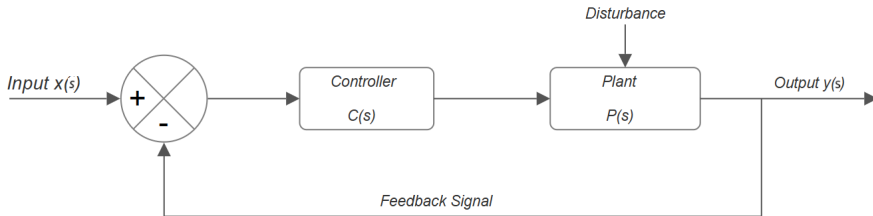


Figure: 1 : Control system Diagram.

Where:

$P(s)$: Transfer function of the plant considered

$C(s)$: Controller of the Plant

Problem Formulation

- For suboptimal control, maximum gain of S (sensitivity function) for frequency $\omega \in [0, \infty) \leq \gamma$ (max sensitivity).
- When $\gamma \geq 1$, ensures phase margin $\phi_m = 2 \sin^{-1} \left(\frac{1}{2\gamma} \right)$ degrees, and gain margin $G_m = 20 \log \left(\frac{\gamma}{\gamma-1} \right)$ dB.
- So we design a controller minimizing S , i.e.

$$\left\| \frac{1}{1 + P(s)C(s)} \right\|_{\infty} < \gamma \quad (1)$$

- The following equation of a human body plant for a drug response is considered for testing the method:

$$P(s) = \frac{Ke^{T_{id}s}(1 + \alpha e^{T_{cd}s})}{\tau s + 1} \quad (2)$$

Designing a Controller using Graphical Approach based on Maximum Sensitivity

- Substituting $s = j\omega$, in $P(s)$ so that, $e^{Tj\omega} = \cos(T\omega) - j \sin(T\omega)$ gives:

$$P_r(\omega) = \frac{K}{t^2\omega^2 + 1} (\cos(T_i\omega) + a \cos(T_i\omega + T_c\omega) - t\omega \sin(T_i\omega) - at\omega \sin(T_i\omega + T_c\omega)) \quad (3)$$

$$\omega P_i(\omega) = \frac{-K}{t^2\omega^2 + 1} (\sin(T_i\omega) + a \sin(T_i\omega + T_c\omega) + t\omega \cos(T_i\omega) + at\omega \cos(T_i\omega + T_c\omega)) \quad (4)$$

- A PI controller $C(s) = K_p - \frac{K_i}{s}$ has been used.**

- Considering $P(j\omega) = P_r(\omega) + j\omega P_i(\omega)$ and $C(j\omega) = K_p - \frac{K_i}{j\omega}$, eqn(1) is written as:

$$\left| (1 + P_r(\omega)K_p + P_i(\omega)K_i) + j \left(\omega P_i(\omega)K_p - P_r(\omega)\frac{K_i}{\omega} \right) \right| \geq \gamma, \quad (5)$$

- On simplifying and rearranging equation (5) in the parametric form of an ellipse gives:

$$K_i = C_i(\omega) + h(\omega) \cos(\theta)$$

$$K_p = C_p(\omega) + k(\omega) \sin(\theta)$$

$$\theta \in [0, 2\pi)$$

Where:

$$C_i(\omega) = -\frac{\omega^2 P_i(\omega)}{|P(j\omega)|^2}, \quad C_p(\omega) = -\frac{P_r(\omega)}{|P(j\omega)|^2},$$

$$h(\omega) = \gamma |P(j\omega)|, \quad k(\omega) = \frac{\gamma |P(j\omega)|}{\omega},$$

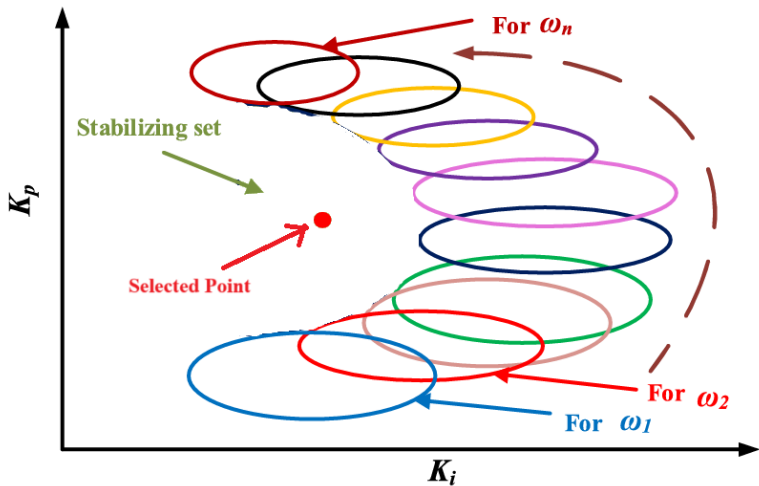


Figure: 2 : Stabilizing PI controller region for plant.

- From the figure 2, we can see that the region outside the ellipses is stable, and values of K_p and K_i can be selected from it.

Testing on a Sample Equation 1

Values for a sensitive patient are: $K = -9$ mmHg/(ml/hr), $\alpha = 0$, T_{id} (sec) = 20, T_{cd} (sec) = 30, τ (sec) = 30, $\omega = [10^{-6}, 0.68]$

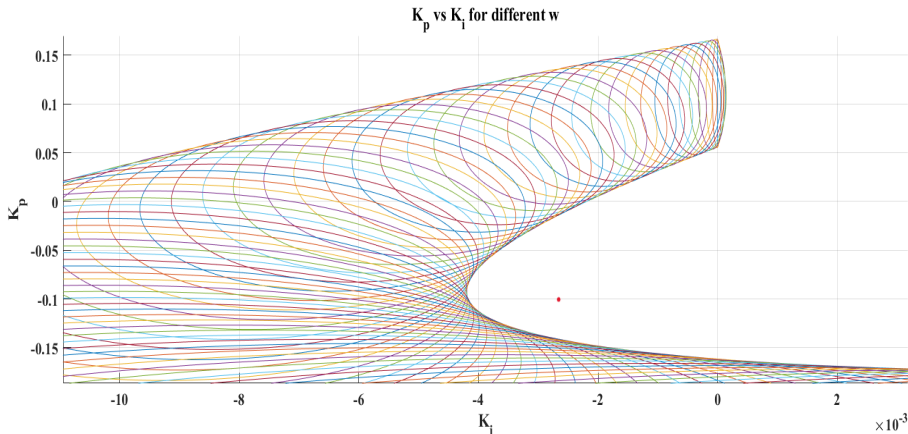


Figure: 3: Sensitive patient plot for $\gamma = 2$, Selected $K_i = -0.0025$, $K_p = -0.1$.

Testing on a Sample Equation 2

Values for a nominal patient are: $K = -0.7143 \text{ mmHg}/(\text{ml}/\text{hr})$, $\alpha = 0.4$, T_{id} (sec) = 30, T_{cd} (sec) = 45, τ (sec) = 40, $\omega = [10^{-6}, 0.68]$

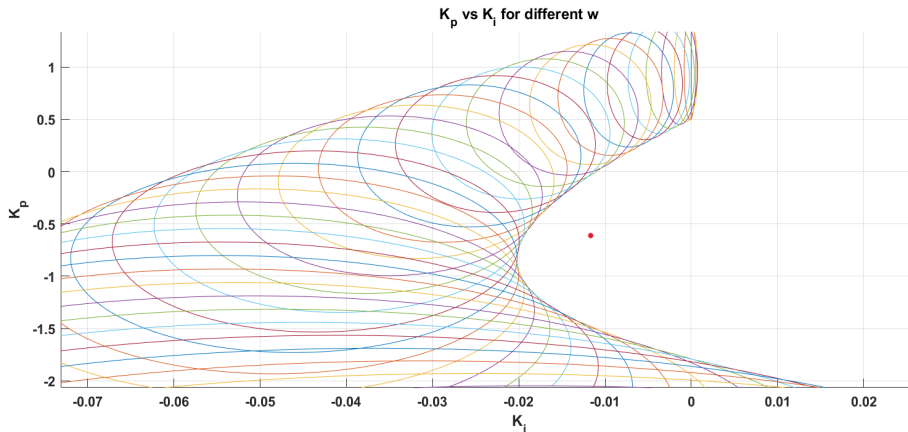


Figure: 4: Nominal patient plot for $\gamma = 2$, Selected $K_i = -0.012$, $K_p = -0.62$.

Choosing the best region for the plant

- We will use different techniques to optimize the selection of the region to choose the point.
- The Nyquist plot is analysed for encirclements of the critical point $-1 + j0$ to determine the closed-loop stability of the PI controller.

Sensitive ITAE FOPID Parameters

$K_p = -0.048$, $K_i = -0.0047$, $\lambda = 0.92$, $K_d = -0.9754$, $\mu = 0.6695$

Nominal IAE FOPID parameters

$K_p = -0.1534$, $K_i = -0.0054$, $\lambda = 0.8584$, $K_d = -9.266$, $\mu = 0.4605$

Simulation and Comparison

Figure 6 and 7 compares the FOPID and proposed PI controllers' performances.

Nyquist plot (Sensitive Patient)

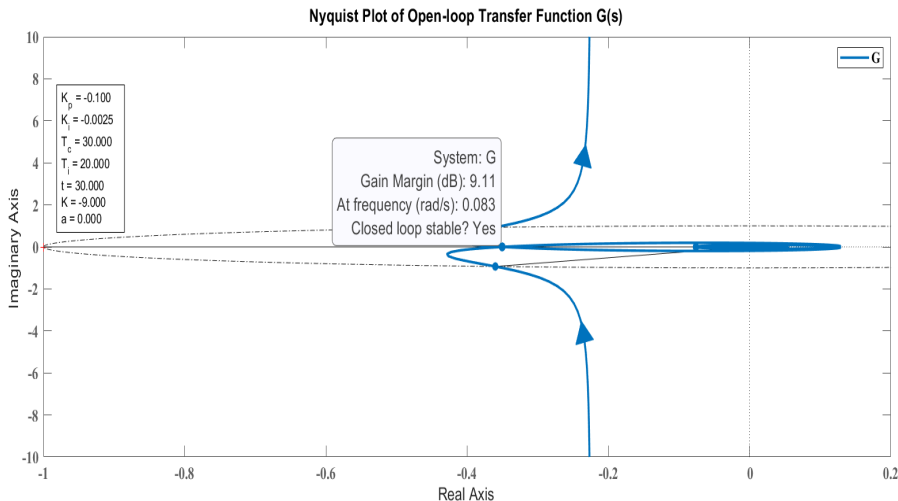


Figure: 4: Nyquist Plot for checking the Stability at the selected K_p and K_i .

Nyquist plot (Nominal Patient)

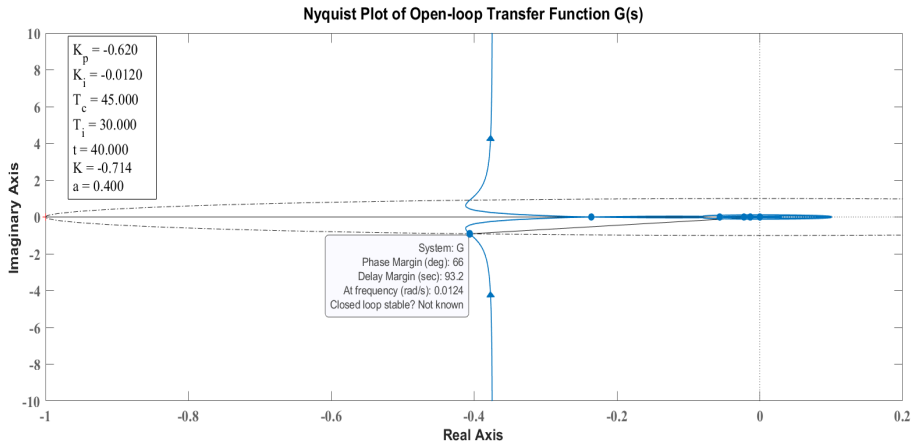


Figure: 5: Nyquist Plot for checking the Stability at the selected K_p and K_i .

Proposed Controller Performance comparison (Sensitive)

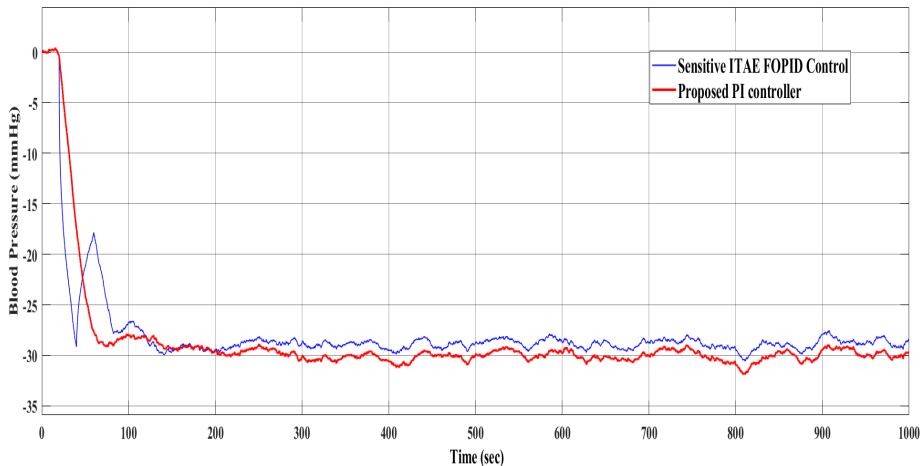


Figure: 6: Comparison between FOPID and proposed PI controller performance (Sensitive).

Proposed Controller Performance comparison (Nominal)

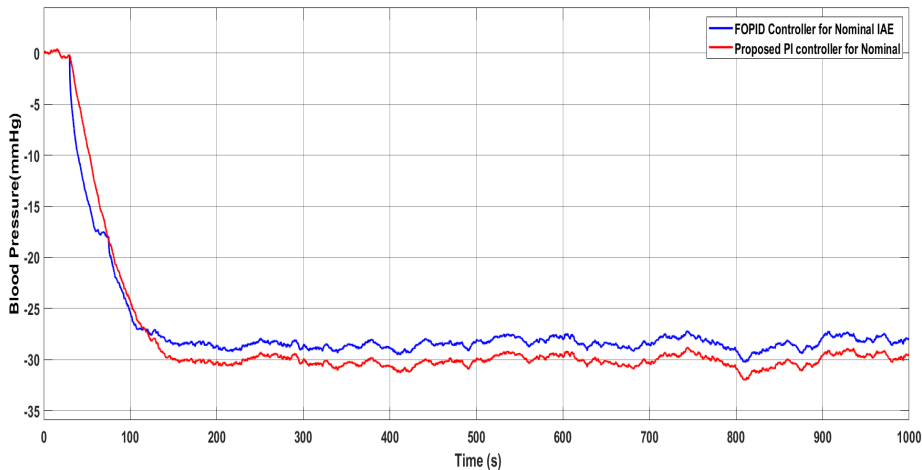


Figure: 7: Comparison between FOPID and proposed PI controller performance (Nominal).

10% Uncertainty in Plant Parameter (Sensitive)

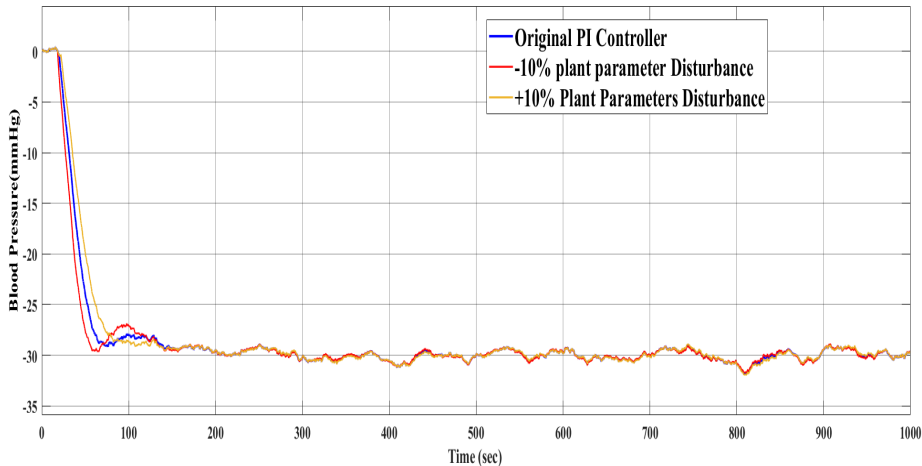


Figure: 8: Step Response with $\pm 10\%$ uncertainty in Sensitive Patient.

10% Uncertainty in Plant Parameter (Nominal)

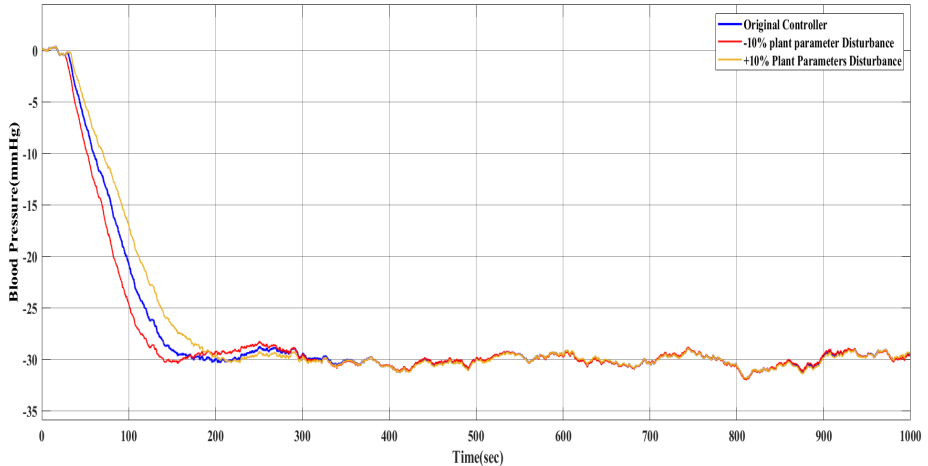


Figure: 9: Step Response with $\pm 10\%$ uncertainty in Normal Patient.

Conclusion

- PI controller designed using **H_∞ criterion** for a system with delay.
- Controller parameters selected through **trial-and-error** method from stability region.
- Stability, closed-loop gain, and phase margins analyzed using **Nyquist plot**.
- Achieved **less steady-state error** and **shorter settling time**.
- **Linear controller** ensures easy real-time implementation.
- Fewer parameters reduce the **computational burden**.
- **Future work** involves using optimization techniques for better control settings.

References

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- [3] S. R. Kumar, P. Verma, M. Ram, S. Somanshu, and M. N. Anwar, " H_{∞} criterion based PI controller for DC-DC boost converter," Dec. 2022. [Online]. Available: <https://doi.org/10.1109/ONCON56984.2022.10126845>

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